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4π radiotherapy

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Aim of therapy physics research

Find practical ways to maximize the radiation dose to tumor and minimize radiation dose to normal tissues

We optimize delivery variables

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Intensity modulated radiotherapy

Forward optimization



Tape Art by Mark Khaisman

Inverse optimization



Portrait using MLC on EBT2 by Hairong Shi

Stacking discretized shots to conform to certain pattern

$$\arg \min \| D - \sum_{i=1}^N W_i A_i x_i \|_2^2$$

3

Need for safe dose escalation: Locally advanced lung cancer UCLA

Clinical IMRT plan 50Gy

Pretreatment 3 Month post 12 Month post 24 Month post

Dose escalation?

The majority of stage III lung cancer patients die from local in field disease progression. Garg, et al. Pract Radiat Oncol. 2013 Oct-Dec;3(4):287-293. 2014 Sep-Oct;4(5):342-5.
 High BED is essential to achieve tumor local control for large locally advanced lung cancer. Zhao et al. IROBP Volume 68, Issue 1, 1 May 2007, Pages 103-110

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Need for better OAR sparing: Bone marrow sparing RT UCLA

IMRT AP/PA 4F

Volume (%) vs Dose (Gy) graph showing IMRT, AP/PA, and 4F curves.

Bowel
Tumor
BM

How to make the dose more compact?

Mell et al, Int J Radiat Oncol Biol Phys. 2008 Aug 1;71(5):1504-10

Non-coplanar radiotherapy is not new UCLA

Coplanar arc
Non-Coplanar arc

TRANSVERSE CORONAL SAGITTAL

SINGLE PLANE ROTATION

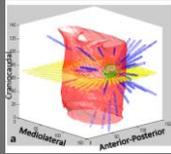
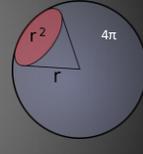
CONVERGENT ARCS (HELIX/BEAM)

Isodose lines are 90, 50, 20, 10, 5 %

Podgorsak et al. IROBP Volume 16, Issue 3, March 1989, Pages 857-865

- Non-coplanar beams and arcs show definitely advantages for intracranial SRS and are ubiquitously used in these treatments
- Non-coplanar beams are less systematically used for extracranial treatment

From fluence map optimization to beam orientation optimization UCLA

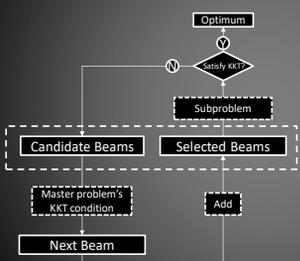
Forward optimization

of non-coplanar beams and arcs becomes increasing difficult and inefficient

Need to develop inverse AR optimization of beam orientations

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Integrated beam orientation and fluence map optimization UCLA



- Pre-compute beamlet doses for all candidate beams (~600-1000)
- Column generation used to select beams and optimize fluence
- Efficient to solve the large scale combined beam orientation and fluence map optimization problem

Karush-Kuhn-Tucker (KKT)-conditions for optimality
Romeijn, H.E., et al., Siam Journal on Optimization, 2005, 15(3), p. 838-862.

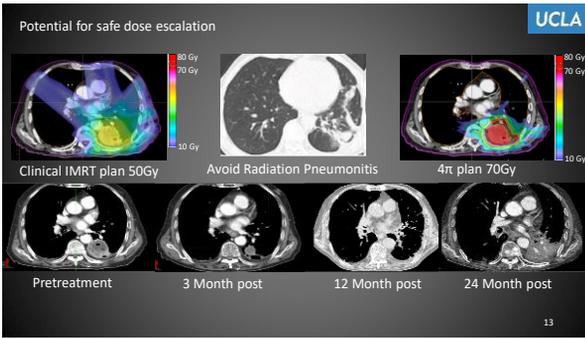
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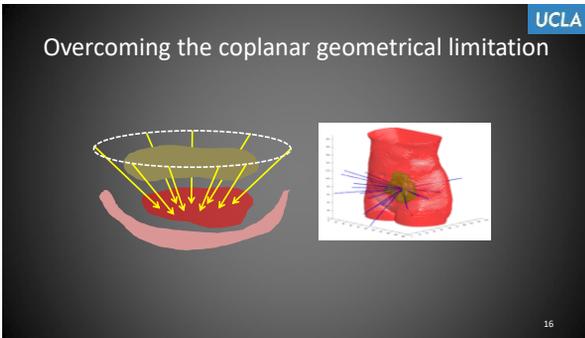
New Beam orientation optimization based on global optimization approach UCLA

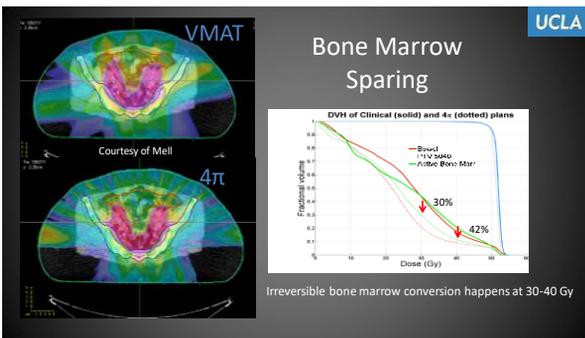
$$\underbrace{\sum_{b=1}^n w_b \|x_b\|_2}_{\text{group sparsity}} + \underbrace{\frac{\mu}{2} \|(d_0 - A_0 x^+)_+\|_2^2}_{\text{PTV}} + \underbrace{\sum_{i=1}^N \frac{\alpha_i}{2} \|(A_i x^+ - d_i)_+\|_2^2}_{\text{OARs}} + \underbrace{\sum_{i=1}^N \frac{\beta_i}{2} \|A_i x\|_2^2 + \eta \|Dx\|_1^{(\gamma)}}_{\text{additional guidance}}$$

Global optimization to avoid heuristics and improve results
O'Connor et al. 2016 AAPM TH EF-BRB-5

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Spine SBRT using 4 π

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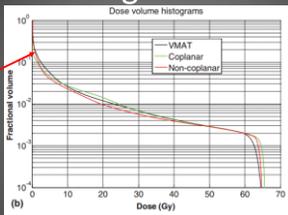
4 π improves the dose gradient by 80%
 Reduce max and mean cord dose by 22% and 42% compared to 2 ARC VMAT
 Yu et al. 2016 AAPM TH-EF-BRB-3

Cortex sparing with 4 π

VMAT cortex sparing compromises target homogeneity and hippocampus
 Substantial cortex sparing without sacrificing PTV dose homogeneity
 Woods et al. 2016 AAPM Best in Physics TH-EF-BRB-1

Integral dose

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4 π increase the volume receiving 2 Gy or lower

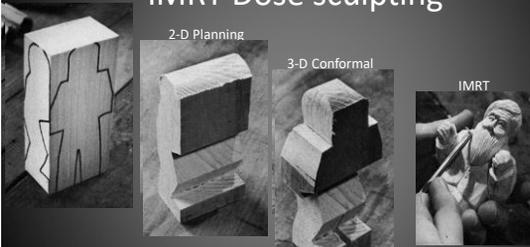
Integral dose of 4 π is lower than VMAT and comparable to coplanar IMRT

Nguyen et al. Med. Phys. 41, 011905 (2014)

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IMRT Dose sculpting

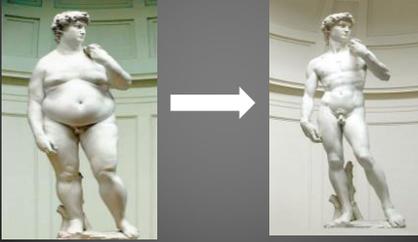
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You have seen this.....

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Compact dose distribution



.....but not this

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Manual 4π delivery



GROUND BREAKING...
AND LEG BREAKING

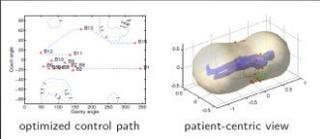
Total treatment time 45-50 minutes

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Path to safe automated delivery

Collision space modeling
Optical camera 3D surface measurement
Yu 2016 AAPM

Path navigation
Level set



optimized control path patient-centric view

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Manual vs. automated delivery

Manual: total treatment time 45 minutes

With remote couch: 28 minutes

Automated delivery 8 minutes

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Phase I 4π clinical trial study design

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graph TD; Patient --> 4pi[4π plan]; Patient --> Conventional[Conventional plan]; 4pi --> Decision{4π superior or equivalent?}; Conventional --> Decision; Decision -- Yes --> Use4pi[Use 4π]; Decision -- No --> UseConventional[Use conventional plan];
```

Aims: Safety, tolerance, treatment time and intrafractional motion

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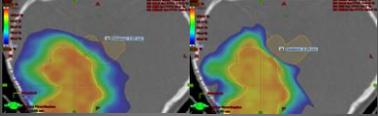
4π radiotherapy vs VMAT

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4π trial results update

- 4π plan was recalculated in Eclipse to generate a clinical plan
- Composite plan of the original and the new recurrent plans



VMAT

- 4π enables uncompromised PTV dose coverage
- 8/10 patient treated using 4π
- Prospective 4π spine SBRT ongoing

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Intrafractional motion monitoring



Intrafractional head motion <1 mm for most treatment fractions
 Patient position corrected for >1 mm motion
 Main discomfort from the tight radiosurgical mask

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Summary

- Use 4π for **confidential** + **compact** radiotherapy
- Consistent reduction in critical organs doses allows more aggressive tumor dose escalation
- The integral dose does not increase with 4π radiotherapy
- Exploring the dosimetric benefits from additional degrees of optimization freedom including **gantry and couch angles, source to tumor distances, collimator angles** and **energies**
- Automated delivery with robust collision avoidance needs to be developed and rigorously QA'd



Digital linacs enable exploration of the additional freedom

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A new delivery platform?

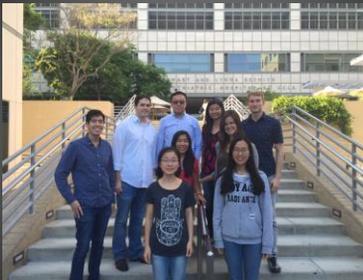


Woods et al. 2016 AAPM TH-EF-BRB-7

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The 4π Team

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Contributors

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- RadiaBeam
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UCSD

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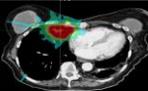
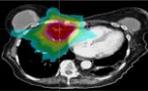
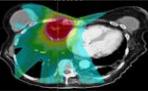
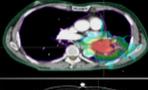
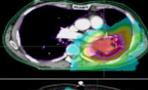
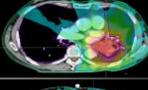
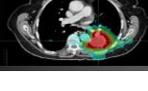
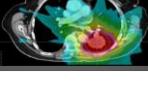


NIH U19AI067769
NIH R43CA183390
NIH R01CA188300
NSF DGE-1144087 (V. Yu)
NIH R21CA161670
NIH R21CA144063

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4 π vs. CyberKnife vs. IMRT

	4 π	CK	IMRT
Anterior			
Middle			
Posterior			

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