


Virginia Commonwealth University


Accounting for Large Geometric Changes During Radiotherapy

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Disclosures

- Research support: Philips Medical Systems
- Licensing: Varian Medical Systems
- Research supported by NIH R01CA166119

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Current Generation DIR in RT

- Mature commercial software and open source packages

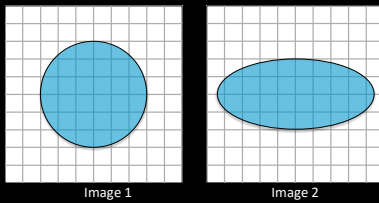
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Current Generation DIR in RT

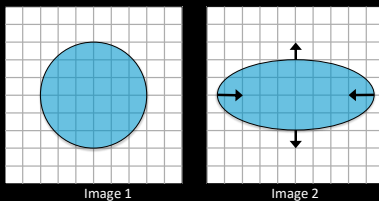
- Mature commercial software and open source packages
- Methods to improve efficiency, plausibility, and accuracy
 - Incorporate features (contours, points), although mainly rely on image intensity
 - Sophisticated representations of transforms (b-splines)
 - Regularization – preventing unrealistic deformation
 - Multiresolution – “coarse to fine”
 - Composite Transform – rigid then affine then deformable
 - Hardware acceleration – parallel processing for efficiency



Conventional Deformation



Conventional Deformation



Conventional Deformation

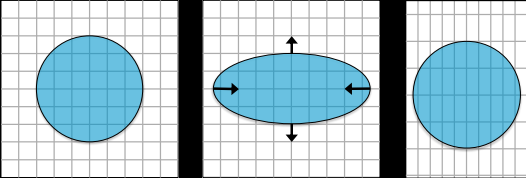




Image 1 Image 2 Deformed Image 2

Topology Preserving: Images can be stretched/squeezed to match without adding or removing image content

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Topology Preserving Deformation

- Articulation / Pose Change
- Breathing Motion

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Challenges – Topological Change

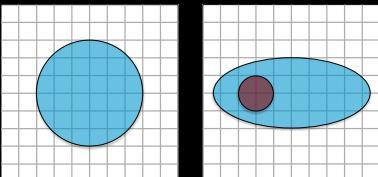



Image 1 Image 2

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Challenges – Topological Change

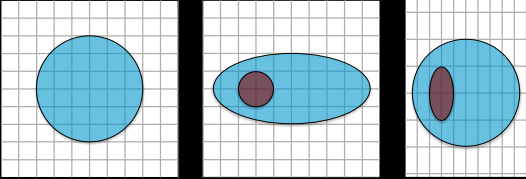



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Topology Change: Images can't be stretched/squeezed to match without adding or removing image content

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Challenges – Topological Change

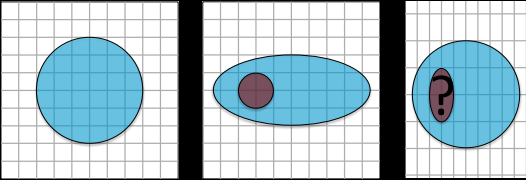



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Topology Change: Images can't be stretched/squeezed to match without adding or removing image content

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Topology Change

- Solution to new or missing image content depends on the application and content itself

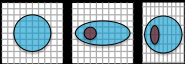

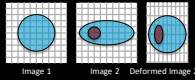


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Topology Change

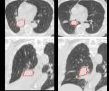
- Solution to new or missing image content depends on the application and content itself
 - For example, if we don't care about the new/missing content region, maybe 'erase' it from the image / registration
 - If a foreign object, may need to understand how it deforms adjacent tissue
 - If tumor / pathology, may need a growth model



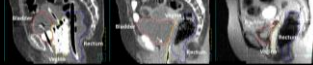
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Topology Change - Examples

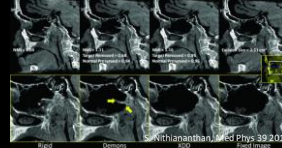
Collapsed Lung



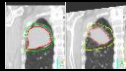
Brachytherapy Applicator



Resected Tissue



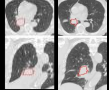
Tumor Growth / Response



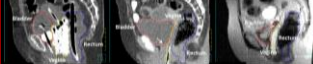
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Topology Change - Examples

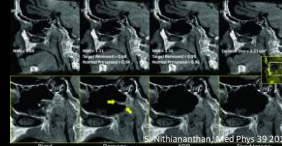
Collapsed Lung



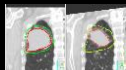
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Resected Tissue



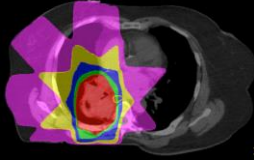
Tumor Growth / Response



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Adaptive RT in locally-advanced lung cancer

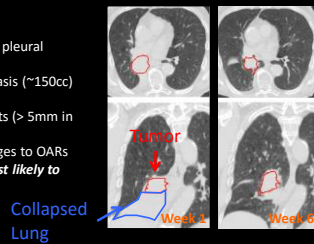
- Higher precision => smaller targets
- Higher precision => less toxicity / better local control
- Automated tools (DIR) required for efficient implementation of adaptive RT



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Atelectasis and large tissue changes

- Many patients (roughly half)
- Atelectasis (partial collapse) and pleural effusion (fluid)
- Large volume changes in atelectasis (~150cc) during RT
- Associated with large tumor shifts (> 5mm in 83% of pts)
- Associated with large dose changes to OARs
- *Patients with large changes most likely to benefit from adaptive RT*



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Guy AAPM 2015, Tennyson ASTRO 2015

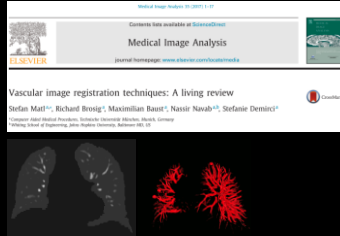
Thoracic Registration - Strategies

- Ignore regions with topology change, identify 'consistent anatomy' between images, register these regions
- Identify consistent anatomy that can be segmented (vessels, airways, lobes)
- Model other changes (tumor, atelectasis, pleural effusion, etc.)

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Vessel Registration

- Many applications (retina, heart, brain) and techniques
- Most require segmentation or enhancement of the vasculature
- Treat the vessels as an image or a tree



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Vessel Registration

- Filters applied to enhance tubular structures
- Produces a 'vesselness measure' image, [0, 1]
- 'Vesselness measure image' registered in parallel with original images

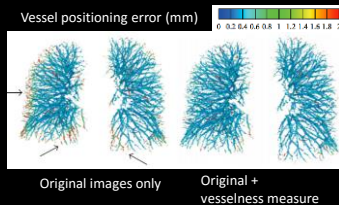


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Cao et al., WBIR 2010

Vessel Registration

- Reduces outliers and improves accuracy of low contrast, peripheral regions
- Small improvements in mean accuracy (20-25%)

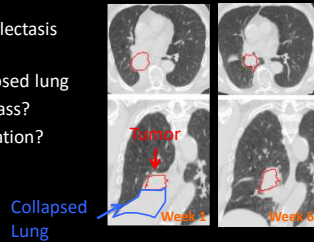


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Cao et al., JBI 2012; Hugo et al. WPIA MICCAI 2015

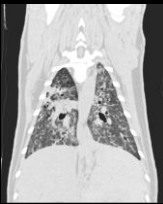
What about the atelectasis region?

- Vessels not visible in atelectasis on CT
- Atelectasis mostly collapsed lung
- Re-inflation preserves mass?
- Mass-preserving registration?



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Mass Preserving Registration



Courtesy G. Christensen

Lung CT intensity change during respiration → Preserving grayscale between two images is not applicable.

Modify the similarity term to incorporate mass preservation

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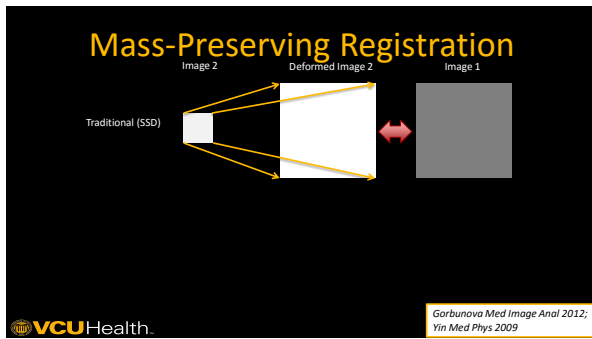
Gorbunova Med Image Anal 2012;
Yin Med Phys 2009

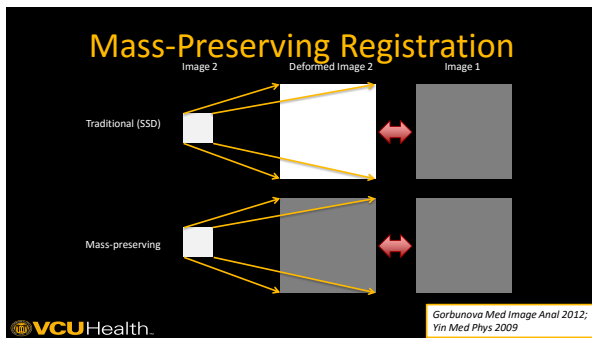
Mass-Preserving Registration

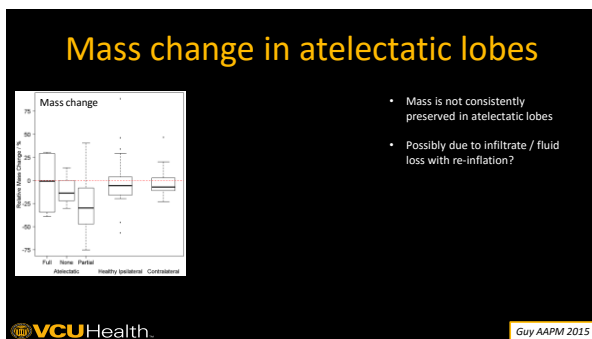


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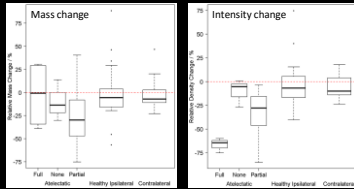
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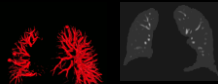
Mass change in atelectatic lobes



- Mass is not consistently preserved in atelectatic lobes
- Possibly due to infiltrate / fluid loss with re-inflation?
- However, large mean Intensity change in atelectatic lobes may still justify a mass-preserving cost function

Lung DIR – Putting it all together

- Simultaneously register
 - Vessels
 - lung parenchyma (healthy and atelectatic) with mass-preserving cost function
 - Individual lobes



Regularized, multiresolution b-spline algorithm – elastix plugins



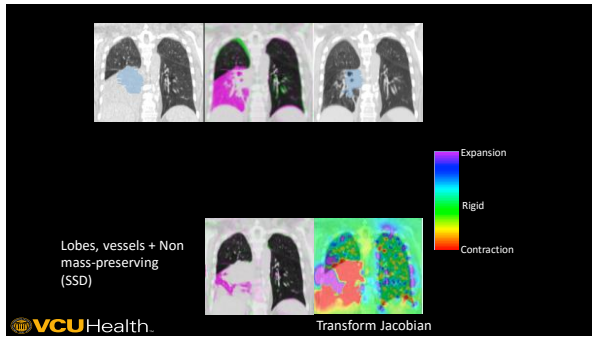
Lung DIR – Putting it all together

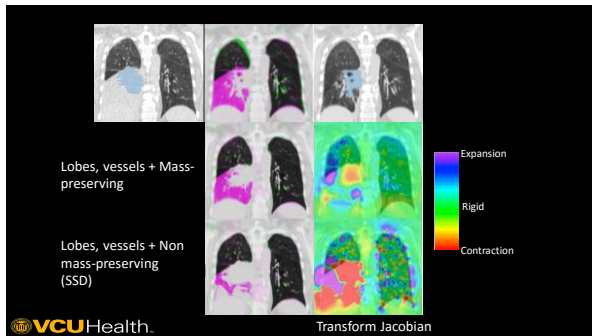


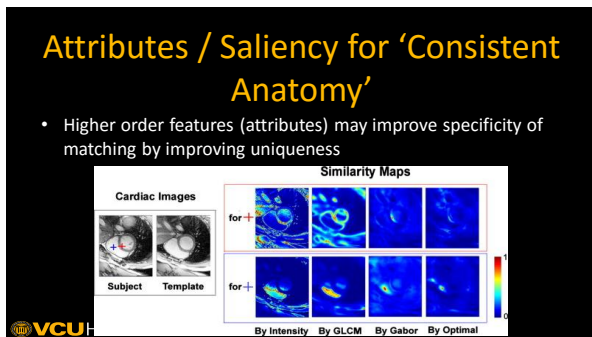
Pre-treatment

Unregistered

Mid-treatment





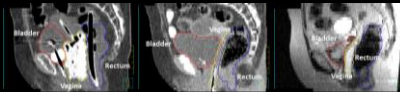


Cumulative Dose in Cervical Ca RT

- Combined external beam RT and intracavitary BT => large uncertainty in cumulative dose

Cumulative Dose in Cervical Ca RT

- Combined external beam RT and intracavitary BT => large uncertainty in cumulative dose
- DIR challenges:
 - Images with / without applicator => topology issues
 - Large motion of anatomy in abdomen => complex / large deformations
 - Mixed modality (MR and CT) => differing contrast



Cumulative Dose in Cervical Ca RT

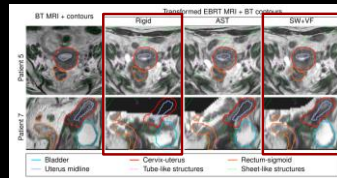
- Penn approach:
 - EBRT CT to BT CT, with/without EBRT boost
 - Pre-processing to equalize contrast and enhance organ boundaries (bladder, rectum, packing)
 - Contoured applicator
 - Commercial DIR then applied
 - Compared 'parameter adding' of D2cc to DIR-accumulated values between EBRT and BT for risk organs (bladder / rectum)
 - Rectum / bladder D2cc varied by 5% between DIR and parameter adding

Cumulative Dose in Cervical Ca RT

- Rotterdam approach:
 - EBRT MR to BT MR
 - Automated feature extraction near contoured organs (bladder, cervix/uterus, rectum) used for feature-based DIR
 - 'Feature filter' similar to vesselness measure
 - Feature DIR registers points in a 'fuzzy matching' method where point correspondence is unknown
 - Organ, feature, and background transforms combined

Cumulative Dose in Cervical Ca RT

- Rotterdam approach:
- Landmark-based accuracy assessment (mean error):
 - Rigid:
 - 22.4 mm near organs
 - 4.3 mm away from organs
 - DIR:
 - 3.5 mm near organs
 - 3.4 mm away from organs



Summary

- Additional / missing tissue is a key challenge to existing registration algorithms
- Solutions depend on the application, site, and task
- However, common strategies of identifying consistent anatomy or careful use of segmentation / masks are promising

Thanks

Clinic / Physics:

Elisabeth Weiss
Nuzhat Jan
Sid Saraiya
Nate Tennyson
Jeff Williamson

Postdocs / Students:

Chris Guy
Kishor Karki
Nicky Mahon
Seungjong Oh
Matthew Riblett

Radiology:

Robert Groves
Kathryn Olsen

U. Iowa Engineering:

Gary Christensen
Paul Song
Amanda Pan
Kunlin Cao

This project supported by NIH/NCI research grant R01CA166119