

Digital Breast Tomosynthesis, VCT Research at the FDA

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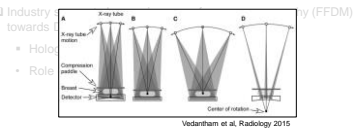
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Research Team/Collaborators

CDRH	External
OSEL/DIDSR Andreu Badal, PhD Aldo Badano, PhD Stephen Glick, PhD Christian Graff, PhD	Duke University Joseph Lu, PhD Ehsan Sarnes, PhD Paul Segars, PhD
ORISE Research Fellows Lynda Kojimba, PhD	University of Massachusetts Srinivasan Vedantham, PhD Andrew Karelas, PhD
OIR/MUIS Anita Nosratiieh, PhD	University of Texas Mia Markley, PhD
OIR/DMQS Andrey Makeev, PhD	Illinois Institute of Technology Alexei Barinikov, PhD
	DECTRIS Ltd (Baden, Switzerland) (RCA)
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	Nooshin Kiarashi, PhD
	Robert Jennings, PhD
	Subok Park, PhD
	Diksha Sharma, PhD
	Rongqing Zeng, PhD

INTRODUCTION

- Currently three FDA approved DBT systems (Hologic 2011, GE 2014, Siemens 2015)
- No standard DBT system (different detectors, acquisition geometries etc.). Continue to see submissions for design changes to approved DBT devices.
- Industry



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INTRODUCTION

- Currently three DBT (Hologic 2011, GE 2014, Siemens 2014) and one BCT (Koning Inc.) systems approved FDA
- No standard DBT system (different detectors, acquisition geometries etc.). Continue to see submissions for design changes to approved DBT devices.
- Industry seems to be moving away from mammography (FFDM) towards DBT
 - Hologic (3D + C-view), Siemens (solely 3D)
 - Role of synthetic mammography

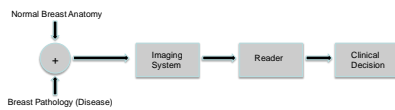
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FDA REGULATORY LANDSCAPE CURRENT ASSESSMENT OF BREAST IMAGERS

- Clinical Study (Pre-Market Approval - PMA)
 - Multiple breast radiologists reading large number of clinical cases
 - Rigorous multi-reader, multi-case ROC analysis
 - Expensive, time-consuming, and radiation risk
- Clinical Data (510k)
 - Limited number of clinical cases
 - Subjective assessment of diagnostic image quality
 - Limited ability to predicate
- Non-clinical, physics based phantom testing
 - MTF, NPS, DOE, SNR or CNR
 - Use simple unrealistic phantoms, might not apply for non-linear reconstruction, don't evaluate objective task performance

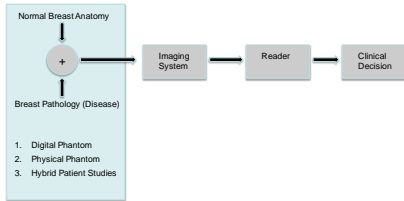
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ALTERNATIVE APPROACHES FOR ASSESSING DIAGNOSTIC ACCURACY OF BREAST IMAGING SYSTEMS



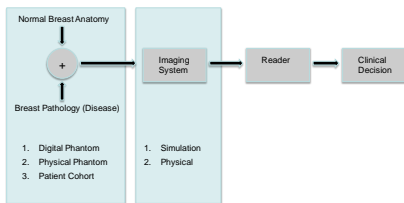
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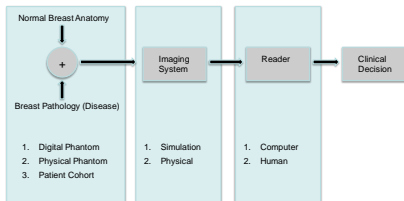
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ALTERNATIVE APPROACHES FOR ASSESSING DIAGNOSTIC ACCURACY OF BREAST IMAGING SYSTEMS



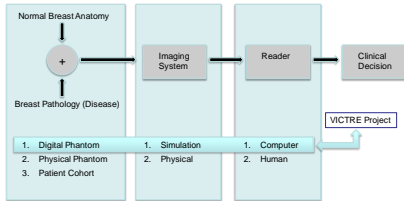
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ALTERNATIVE APPROACHES FOR ASSESSING DIAGNOSTIC ACCURACY OF BREAST IMAGING SYSTEMS



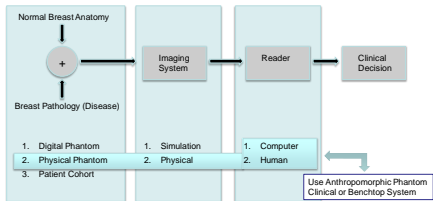
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ALTERNATIVE APPROACHES FOR ASSESSING DIAGNOSTIC ACCURACY OF BREAST IMAGING SYSTEMS



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ALTERNATIVE APPROACHES FOR ASSESSING DIAGNOSTIC ACCURACY OF BREAST IMAGING SYSTEMS - VCT



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Limited use of “virtual clinical trial” approach in FDA submissions

- ❑ BARCO Mammo/Tomosynthesis display. Temporal response claim cleared using a combination of bench testing and modeling using a computational reader approach
- ❑ GE ASiR-V image reconstruction. CT dose reduction claim in CT cleared using a homogeneous physical phantom and computational models of low-contrast detectability.

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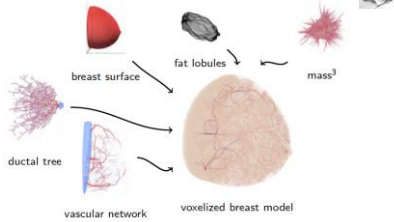
Virtual Imaging Clinical Trials Regulatory Evaluation (VICTRE) - Goals

- ❑ To perform a complete in silico clinical study for a DBT device and compare the results to those in an existing FDA submission using patients and clinicians
- ❑ To develop, validate, and distribute an open-source code that will include the complete computational imaging pipeline
- ❑ To develop draft guidelines and guidance on virtual imaging clinical trials.

- Research Team:
- Aldo Badano (lead)
 - Andreu Badal (physics)
 - Stephen Glick (physics/regulatory)
 - Christian Graf (breast models)
 - Anita Nosrati (regulatory)
 - Frank Samuelson (reader studies)
 - Diksha Sharma (pipeline)
 - Rongping Zeng (recon and readers)

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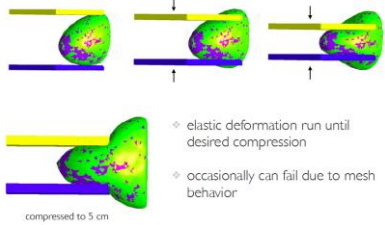
Variable and realistic model of breast anatomy



- C.G. Graf, "A new open-source multi-modality digital breast phantom," Proc SPIE 9783, 2016.
- L. Sietemes, "A computational model to generate simulated 3D breast masses," Med Phys 2015.

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Compression Implementation



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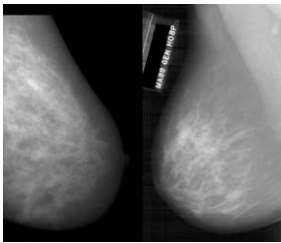
Simulation of the imaging process

FDA/DIDSR has developed open-source freely available and widely used software to simulate physics of the imaging system

- MC-GPU¹ - GPU-accelerated x-ray transport code to simulate clinically realistic images
- MANTIS² - Monte Carlo x-ray electron and optical imaging simulation tool

1. A. Badal and A. Badano, "Accelerating Monte Carlo simulations of photon transport in a voxelized geometry using a massively parallel graphics processing unit," *Med Phys*, 2009

2. A. Badano and J. Sempau, "MANTIS: combined x-ray, electron, and optical Monte Carlo simulations of indirect radiation imaging systems," *Phys Med Biol*, 2006.



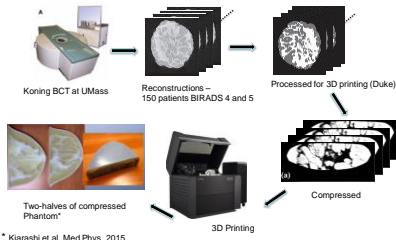
Simulated Real

Model Observers for VICTRE Project

Draw on breast imaging model observer research at FDA

- Zeng R, Park S, Bakic P, and Myers KJ. "Evaluating the sensitivity of the optimization of acquisition geometry to the choice of reconstruction algorithm in digital breast tomosynthesis through a simulation study," *Phys Med Biol*, 2015.
- Park S, Zhang G, and Myers KJ. "Comparison of channel methods and observer models for the task-based assessment of multi-projection imaging in the presence of structured anatomical noise," in press. *IEEE Transactions on Medical Imaging*, 2016.
- Young S, Bakic P, Jennings R, Myers KJ, and Park S. "A virtual trial framework for quantifying the detectability of masses in breast tomosynthesis projection data," *Medical Physics*, 40 (5), p. 051914, 2013 * Realized with * are the names of students and postdoctoral fellows who I have mentored.
- Park S. "Spatial domain model observers for optimizing tomosynthesis," in *Tomosynthesis Imaging*, edited by I. Reiser and S. Glick, Taylor and Francis Books, Inc., 2014.
- Ikejima L, Glick SJ, Samei E, and Lo JY. "Comparison of model and human observer performance in FFDM, DBT, and synthetic mammography," *SPIE Medical Imaging* 2016, Proc SPIE 9783, 2016

ANTHROPOMORPHIC BREAST PHANTOMS 3D PRINTING (Collaboration with Duke)



* Kirashi et al, Med Phys, 2015

ANTHROPOMORPHIC BREAST PHANTOMS 2D INKJET PRINTING



Ikejima et al, IWDM 2016

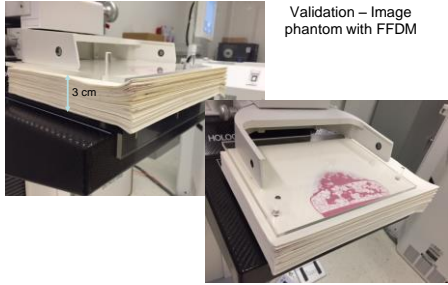
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Validation - FFD

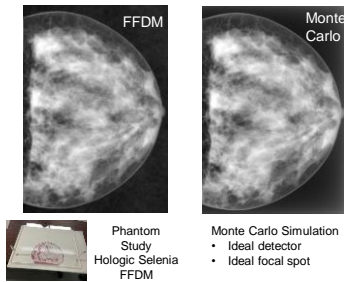


Tissue equivalent chips of known glandularity

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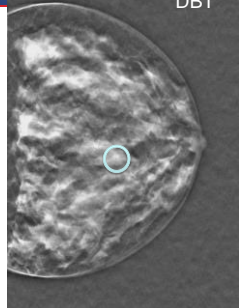
Validation – Image phantom with FFDM



Phantom Study Hologic Selenia FFDM

Monte Carlo Simulation
• Ideal detector
• Ideal focal spot

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DBT

- DBT acquisition on clinical system
- Lesion inserted in virtual model
- Slices reprinted and replaced

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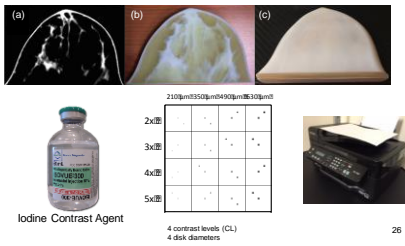
COMPARISON OF MODEL AND HUMAN PERFORMANCE IN FFDM, DBT, AND SYNTHETIC MAMMOGRAPHY*

- ❑ Compare model and human observers in reader study using anthropomorphic breast phantom and inserted low-contrast signals.
- ❑ Task-based performance of FFDM, DBT, and synthetic mammography (SM)
- ❑ Variable tasks with uniform and structured backgrounds

* Ikejima L, Glick SJ, Samei E and Lo JY, Proc SPIE 9783, 2016.

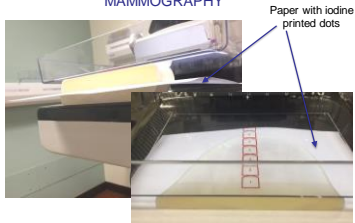
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COMPARISON OF MODEL AND HUMAN PERFORMANCE IN FFDM, DBT, AND SYNTHETIC MAMMOGRAPHY



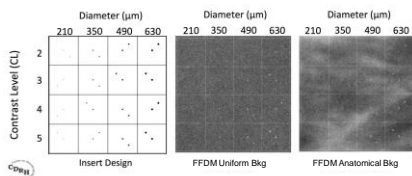
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PROJECT 2 - COMPARISON OF MODEL AND HUMAN PERFORMANCE IN FFDM, DBT, AND SYNTHETIC MAMMOGRAPHY



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COMPARISON OF MODEL AND HUMAN PERFORMANCE IN FFDM, DBT, AND SYNTHETIC MAMMOGRAPHY



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Image Acquisition

Clinical Hologic System

	FFDM	DBT and SM ¹
Detector pixel size, x-y plane (mm)	0.07	0.07 (2x2 binning)
Image pixel size, x-y plane (mm)	0.07	0.09
Target/Filter	W/Rh	W/AI
Tube voltage (kV)	28	29
Tube load (mAs)	80	42
AGD at AEC (mGy)	1	1.4

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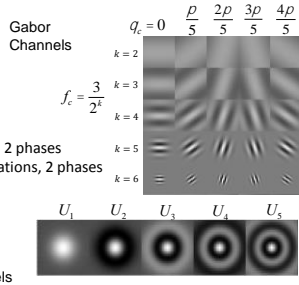
Human and Model Observer Study

- 4 alternative forced choice (4AFC)
- Human readers: Six non-radiologists
- Model Observers
 - Nonprewhitening with eye filter (NPWE)
 - Channelized Hotelling observer (CHO)
 - Gabor channels
 - Laguerre-Gauss (LG) channels

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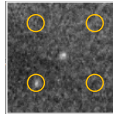
2D Observer Models

- NPWE² $E(f) = f^{7n_1} e^{af^{n_2}}$
 - Fixed viewing distance 500 mm
 - Field of view 23.9 mm
 - Display size 338 mm
- Gabor CHO (Gb-CHO)
 - DBT - 5 frequencies, 5 orientations, 2 phases
 - FFDM, SM - 7 frequencies, 7 orientations, 2 phases
- Laguerre-Gauss CHO (LG-CHO)
 - 5 channels
 - Gaussian width \propto task diameter



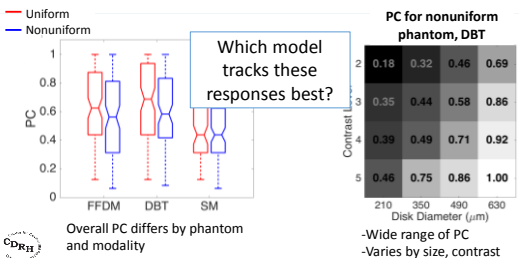
Reader Study

- Model Observer
 - Apply template matching to each corner
 - Select corner of maximum response
- Performance: Proportion Correct (PC)
 - $PC = X/n$
 - X = number of successes
 - n = number of trials
 - $0 \leq PC \leq 1$



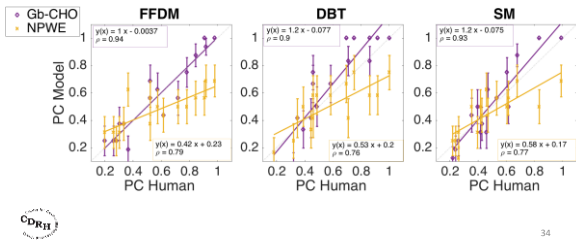
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Human Scores



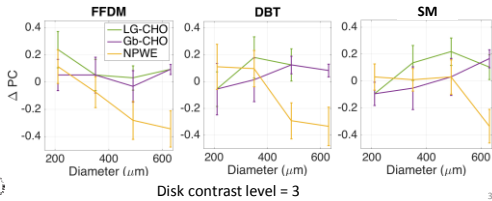
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 Effect of modality on model accuracy



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 Effect of size on model accuracy

$\Delta PC = PC(\text{Model}) - PC(\text{Human})$
 $\Delta PC > 0$, Model score higher than human
 $\Delta PC < 0$, Model score lower than human



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 DISCUSSION

- Results of task-based analysis can be impacted by phantom type and model observer
- Readers scored higher with FFDM and DBT than SM, in uniform and nonuniform backgrounds
- Gabor-CHO and LG-CHO matched well with humans, in uniform and nonuniform backgrounds
 - Gabor-CHO matched human scores more closely than LG-CHO
 - LG-CHO overperformed relative to humans



SUMMARY AND FUTURE WORK

- Anthropomorphic Breast Phantoms
 - Continue to investigate 2D and 3D printing of phantoms. Investigate new materials, new breast models, reproducibility, spatial resolution, and phantoms for dynamic imaging.
- Using new phantoms, continue to explore methodologies for assessing diagnostic task-performance that can be used to support PMAs.
 - VICTRE project (simulated objects and imaging systems)
 - VCT using physical phantoms and real imaging systems
 - Contribute to the down-classification of DBT devices (III -> II), decrease time to market
- Continue investigating new breast imaging applications including spectral imaging, material decomposition, and new detectors

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Thank you

Disclosure: The mention of commercial products herein is not to be construed as either an actual or implied endorsement of such products by the Department of Health and Human Services



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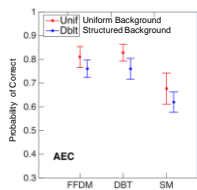


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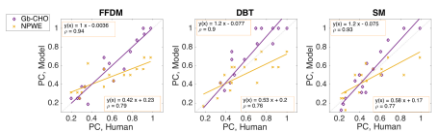
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HUMAN OBSERVER RESULTS



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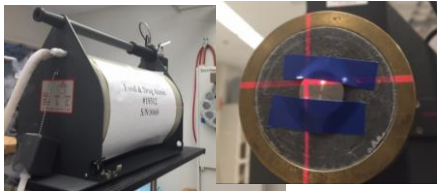
RESULTS HUMAN VS MODEL OBSERVER



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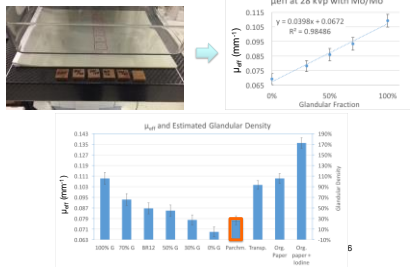
Spectral Analysis

- High purity germanium energy discriminating photon counting detector
- Source and detector collimation
- Calculated μ as a function of keV

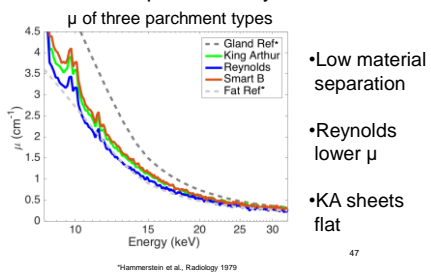


Results

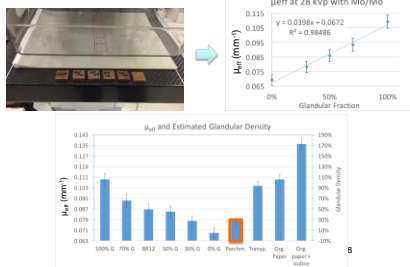
Material Validation



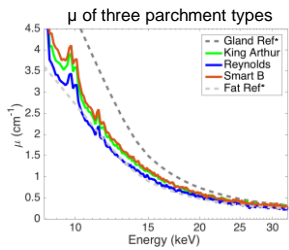
Spectral Analysis



Material Validation

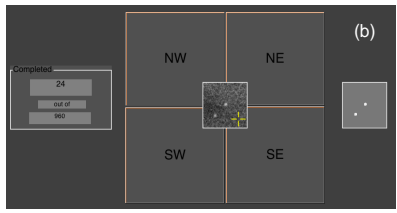


Spectral Analysis



- Low material separation
- Reynolds lower μ
- KA sheets flat

*Hammerstein et al., Radiology 1979 49



- Supervised training with easy, medium, difficult tasks
- All Modes x Tasks x Trials x Phantoms = 1536 ROIs



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