Photon-counting detectors in mammographic imaging

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Disclosures

Funding from:

- Philips
- Toshiba

Outline

- Introduction
- Breast density
- Lesion characterization
- Contrast-enhanced mammography
- Conclusions

Scanning multi-slit geometry





Scanning multi-slit geometry







Scatter





No Scatter





Photon counting mammography







Spectral mammography





Outline

- Introduction
- Breast density
- Lesion characterization
- Contrast-enhanced mammography
- Conclusions

Breast density

Mammographically dense breast has been shown to be strongly associated with breast cancer risk¹

Breast density

- Breast Imaging Reporting and Data System (BI-RADS)
- Histogram Thresholding



Dual Energy Mammography



H. Ding, *et al.* , Physics in Medicine and Biology 57, 4719-4738 (2012) Johnson, et al. Phys. Med. Biol. 58 (2013) 8573–8591

Human Studies

Study 1

- 93 mammography patients
- BI-RADS ranking by 10 radiologists (5 US, 5 UK)
- Standard grey level thresholding (Cumulus)
- Dual-energy mammography

Study 2

- 2034 mammography patients
- · Breast density assessed by Quantra

















Dual Energy Decomposition









| Right and left breast density comparison | | | | | | | | |
|--|---------|---------|---------|----------------|--|--|--|--|
| | BI-RADS | Cumulus | Quantra | Dual energy | | | | |
| Slope | 0.90 | 0.87 | 0.90 | 0.90 | | | | |
| Intercept | 8.1% | 5.0% | 0.8% | 1.1% | | | | |
| Pearson's r | 0.93 | 0.80 | 0.88 | 0.96 | | | | |
| SEE | 4.3% | 8.2% | 8.0% | 2.4% | | | | |
| Methodology Error | 3.9% | 7.9% | 7.7% | 1.9% | | | | |

S. Molloi, et al. Academic Radiology 22, 1052-1059 (2015).



Reliability of breast density measurement

| | No. of cases | Mean (%) | Standard Deviation (%) | Standard Error (%) | Median (%) | 25 th Percentile (%) | 75 th Percentile (%) | Minimum (%) | Maximu m (%) |
|-----------------|--------------|-------------|------------------------------|-----------------------|---------------|---------------------------------------|---------------------------------------|----------------|-----------------|
| Quantra | 30 | -0.06 | 1.64 | 0.30 | -0.25 | -1.00 | 0.68 | -4.20 | 4.00 |
| Volpara | 30 | -0.33 | 1.39 | 0.25 | -0.35 | -0.90 | 0.58 | -4.25 | 2.28 |
| Dual- Energy | 36 | 0.10 | 0.52 | 0.09 | 0.03 | -0.16 | 0.2 | -0.47 | 2.63 |
| | | | | | | | | | |
| | | | | | | | | | |

O. Alonzo-Proulx, et. al. Radiology 275, 366-376 (2015)

Conclusions

- Breast density can be accurately quantified with spectral mammography.
- The precision of spectral mammography can be 3 to 4 folds higher than current clinical standard.

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- Breast density
- Lesion characterization
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Erhard K1, Kilburn-Toppin F, Willsher P, Moa E, Fredenberg E, Wieberneit N, Buelow T, Wallis MG, Invest Radiol. 2016;51(5):340-7.











Conclusions

Discriminating cystic from solid lesions with spectral mammography demonstrates promising results with the potential to reduce mammographic recalls.

Erhard K1, Kilburn-Toppin F, Willsher P, Moa E, Fredenberg E, Wieberneit N, Buelow T, Wallis MG, Invest Radiol. 2016;51(5):340-7.

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Contrast-enhanced mammography

Quantitative contrast-enhanced mammography

- Malignant lesions are known to have higher vascular density.
- Iodine mass in a lesion is expected to be correlated with vascular density of a lesion.



Linear dual energy subtraction

Conventional CESM:

$$S_{DE} = \ln S_{l} - w \ln S_{h} \quad (w = \frac{\mu^{*} \frac{1}{k} - \mu^{*} \frac{1}{a}}{\mu^{*} \frac{1}{k} - \mu^{*} \frac{1}{a}})$$

$$S_{DE} = T + \alpha t_{i} \qquad \alpha = f(\mu^{*} \frac{1}{k}, \mu^{*} \frac{1}{a}, \mu^{*} \frac{1}{a})$$

➤ Total thickness (*T*) is not evaluated;

> conversion slope (α) depends on local breast composition;







Dual energy material decomposition

Quantitative CESM: $S_{DE} = T + \alpha t_i$











Conclusions

> Phantom studies were performed to validate the feasibility of quantifying iodine mass thickness for breasts of various thicknesses and densities.

> The results show that the proposed quantification method offers high accuracy.

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Conclusions

- Dual energy mammography can be used for accurate measurement of breast tissue composition and breast density.
- Dual energy mammography can potentially be used for characterization of cystic and solid lesions.

Conclusions

 Dual energy mammography can be used for accurate quantification of iodine in a lesion, which can potentially be used to estimate lesion vascular density.

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13

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Postmortem Study

- 40 postmortem breasts (20 pairs);
- 2 views (CC and MLO) for each breast;
- Dual-energy breast density quantification;
- Chemical analysis

Johnson, et al. Phys. Med. Biol. 58 (2013) 8573–8591

Reproducibility







Lesion characterization

| Lesion Type | Number | Size Range, mm |
|-------------------------------|--------|----------------|
| Solid lesions | 62 | 10-60 |
| Malignant solid lesions | 47 | 10-60 |
| Grade 1 (no special type) | 6 | 13-27 |
| Grade 2 (no special type) | 13 | 10-35 |
| Grade 3 (no special type) | 20 | 13-60 |
| Invasive lobular grade 2 | 5 | 14-50 |
| Invasive mucinous grade 2 | 1 | 23 |
| Micropapillary cancer grade 2 | 2 | 10-19 |
| Benign solid lesions | 15 | 10-25 |
| Fibroadenoma | 14 | 10-25 |
| Intraductal papilloma | 1 | 10 |
| Cystic lesions | 57 | 10-40 |

Erhard K1, Kilburn-Toppin F, Willsher P, Moa E, Fredenberg E, Wieberneit N, Buelow T, Wallis MG. Invest Radiol. 2016;51(5):340-7.

Lesion characterization

| Cluster | 1 | 2 | 3 | 4 | 5 | 6 |
|----------------------------------|--------|------------------|--------------------|--------------------|--------------------|----------|
| Diameter | <10 mm | ≥10 mm, ≤13.5 mm | ≥13.5 mm, ≤17.0 mm | >17.0 mm, ≤20.0 mm | >20.0 mm, ≤27.0 mm | >27.0 mm |
| No. lesions | 21 | 24 | 22 | 25 | 24 | 24 |
| Prevalence | 0.57 | 0.67 | 0.64 | 0.56 | 0.38 | 0.38 |
| AUC | 0.60 | 0.75 | 0.73 | 0.82 | 0.98 | 0.99 |
| specificity (at 99% sensitivity) | 0.04 | 0.25 | 0.33 | 0.55 | 0.80 | 0.93 |
| NPV | 0.74 | 0.93 | 0.95 | 0.98 | 0.99 | 0.99 |

Erhard K1, Kilburn-Toppin F, Willsher P, Moa E, Fredenberg E, Wieberneit N, Buelow T, Wallis MG. Invest Radiol. 2016;51(5):340-7.











Phantom studies



Breast Cancer Risk

- Women with the highest mammographic density have a factor of 4-5 increased risk of developing breast cancer compared with the lowest density.
- For every 1% increase in breast density the cancer risk is increased by 2%.*

* Boyd, et al. New England Journal Medicine, 2007. 356. p227-236

Goal

Develop a quantitative and accurate method to measure breast composition





Dual Energy Mammography













Breast Tissue Study

- 28 specimens from 14 breast pairs (right and left)
- Each sample imaged at two different orientations (view 1 and view 2)



- Dual energy decomposition (water and lipid basis)
- Chemical analysis (gold standard)

Chemical Analysis



1. Evaporate water in vacuum oven

emical analysis 2. Dissolve lipid in petroleum ether

 Remove protein using vacuum filtration

T. Johnson, et al., Physics in Medicine and Biology 58, 8573-8591 (2013)





















Examples of Spectral Mammography images





For Presentation





Comparison between right and left breasts















Human Study

- 93 mammography patients
- BI-RADS ranking by 10 radiologists (5 US, 5 UK)
- Standard grey level thresholding (Cumulus)
- Spectral mammography

Spectral Mammography images





Processed Unprocessed total

Unprocessed High energy

Adi Adi









| | Bi- RADS | Histogram Thresholding | Spectral Decomposition |
|--------------|-------------|---------------------------|---------------------------|
| | | | |
| Right - Left | 2.0 | 2.9 | 1.0 |











Generally, malignant lesions demonstrate a rapid uptake and washout of the contrast agent (type 1), whereas benign lesions are characterized by a more gradual uptake of contrast agent (type 2 and 3).

















Phantom studies

Outline Breast density and cancer risk

- Grey level thresholding
- Fuzzy C-mean segmentation
- Techniques based on breast shape model
- Dual energy material decomposition
- Two material model for breast tissue (Glandular and adipose)
- Three material model for breast tissue (Water, lipid, protein)
- Problem of single measurement but 2-3 unknowns

















BI-RADS Reader Study

- IRB approval
- 93 patients
- 10 radiologists
- CC and MLO views



 Right and left breasts viewed in random order

BI-RADS Ranking









Histogram Thresholding

- Cumulus 4
- Two thresholds
- CC and MLO views in sequence
- Right and left blinded







Right-left correlation from Cumulus





Fuzzy C-mean Clustering

- Automatic segmentation
- Total of 6
 clusters
- First three clusters glandular tissue



Automatic Segmentation using Fuzzy C-mean





Dual Energy Decomposition



CC and MLO from dual energy



Breast Volume from Dual Energy



Breast Density from Dual Energy



Conclusions

- Spectral mammography offers quantification of volumetric breast density with excellent precision.
- It largely eliminates the inter- and intra-observer variability in breast density estimation.

ACKNOWLEDGMENTS

This research was supported in part by Grant No. R01 CA136871 awarded by the NCI, DHHS.





Dual Energy Decomposition



Ducote J L, Molloi S, Quantification of breast density with dual energy mammography: An experimental feasibility study, Med. Phys. 37: 793, 2010.

Breast Tissue Composition

| Tissue | н | С | Ν | 0 | Cl | Ca | Density (g/cc) | Ash (S,P,K,Ca) |
|------------------------------------|-------|-------|------|-------|----|----|-------------------|-------------------|
| Glandular | | 10.8% | 3.2% | 75.9% | | | | |
| Tissue | 10.2% | 18.4% | 3.2% | 67.7% | | | 1.04 | 0.5% |
| (Hammerstein ⁸) | | 30.5% | 3.2% | 55.2% | | | | |
| Adipose | | 49.1% | 1.7% | 35.7% | | | | |
| Tissue | 11.2% | 61.9% | 1.7% | 25.1% | | | 0.93 | 0.1% |
| (Hammerstein ⁸) | | 69.1% | 1.7% | 18.9% | - | - | | |
| Glandular | 10.2% | 15.8% | 3.7% | 69.8% | | | 1.06 | |
| Tissue | 10.6% | 33.2% | 3.0% | 52.7% | | | 1.02 | - |
| (Woodard and White ¹⁰) | 10.9% | 50.6% | 2.3% | 35.8% | | | 0.99 | |
| Adipose | 11.2% | 51.7% | 1.3% | 35.5% | | | 0.97 | |
| Tissue | 11.4% | 59.8% | 0.7% | 27.8% | - | - | 0.95 | - |
| (Woodard and White ¹⁰) | 11.6% | 68.1% | 0.2% | 19.8% | - | - | 0.93 | - |



VLP Comparison



Fig. 5. The data in this study are shown next to the data of Woodard and White. Note for the data in this study, the error bars were too small to be seen. The RMS difference for bovine adipose and human adipose tissues was 1.2%. The RMS difference for bovine lean and human skeletain muscle tissue was 0.4% and 22.2% for bovine lean and human mammary gland tissues.

Spectral Mammography

- Philips MicroDose Digital Mammography System
- Tungsten anode x-ray tube.
- Appropriate energy bin selection.
- No Scatter correction necessary



Dual Energy Decomposition



 $t_i = \frac{a_0 + a_1 l + a_2 h + a_3 l^2 + a_4 l h + a_5 h^2}{\sqrt{1 + b_1 l + b_2 h}}$

Ducote J L, Molloi S, Quantification of breast density with dual energy manunography: An experimental feasibility study, Med. Phys. 37: 793, 2010.







Breast Tissue Composition

| Tissue | н | с | Ν | 0 | Cl | Ca | Density (g/cc) | Ash (S,P,K,Ca) |
|------------------------------------|-------|-------|------|-------|----|----|-------------------|-------------------|
| Glandular | | 10.8% | 3.2% | 75.9% | | | | |
| Tissue | 10.2% | 18.4% | 3.2% | 67.7% | - | - | 1.04 | 0.5% |
| (Hammerstein ⁸) | | 30.5% | 3.2% | 55.2% | | - | | |
| Adipose | | 49.1% | 1.7% | 35.7% | | | | |
| Tissue | 11.2% | 61.9% | 1.7% | 25.1% | | | 0.93 | 0.1% |
| (Hammerstein ⁸) | | 69.1% | 1.7% | 18.9% | - | - | | |
| Glandular | 10.2% | 15.8% | 3.7% | 69.8% | | | 1.06 | |
| Tissue | 10.6% | 33.2% | 3.0% | 52.7% | | | 1.02 | |
| (Woodard and White ¹⁰) | 10.9% | 50.6% | 2.3% | 35.8% | | | 0.99 | - |
| Adipose | 11.2% | 51.7% | 1.3% | 35.5% | | | 0.97 | |
| Tissue | 11.4% | 59.8% | 0.7% | 27.8% | - | | 0.95 | - |
| (Woodard and White ¹⁰) | 11.6% | 68.1% | 0.2% | 19.8% | | - | 0.93 | |



Breast Tissue Composition

Table 3. Summary of the apparent densities of breast tissue as compared to the composition determined from chemical analysis.

| Composition Study Author | Tissue Type | Known Density | Range in Apparent Density | Average Apparent Density | RMS Error |
|--------------------------------|----------------|------------------|---------------------------------|--------------------------------|--------------|
| Hammerstein ^a | Adipose | 0 | [–11.3 - 22.6] | 4.1 | 14.6 |
| | Glandular | 100 | [84.6 - 136.5] | 112.3 | 24.6 |
| Woodard | Adipose | 0 | [-7.6 - 26.4] | 9.0 | 16.5 |
| and White ¹⁰ | Glandular | 100 | [34.2 - 121] | 74.6 | 43.8 |
| Johns | Adipose | 0 | [–31.8 - –18.5] | -25.7 | 26.2 |
| and <u>Yaffe</u> ¹¹ | Glandular | 100 | [109.6 - 115.8] | 113.5 | 13.8 |





System requirements for patient studies

- Minimal time interval (less than 1 sec) between low and high energy images.
- Ability to switch kVp between low and high energy images (i.e. 28 kVp to 49 kVp).
- Ability to switch beam filter between low and high energy images (i.e. Rh filter to Cu filter).
- Negligible lag and ghosting between low and high energy images.

Dual Energy Imaging







Dual Energy Imaging

| | 4.5 cm Adipose |
|--|----------------------------------|
| | 3 cm Adipose + 1 cm Glandular |
| | 3 cm Glandular |







Screening Mammography



Visual estimation

Breast Imaging Reporting and Data System (BI-RADS) BI-RADS 1-4 with increasing level of glandularity.

Histogram Thresholding







Dual kVp Mammography



Breast Tissue Study

- 40 breast tissue samples
- BI-RADS ranking by 3
 radiologists
- Standard Histogram
 Thresholding
- Dual energy material decomposition
- Chemical analysis



Hologic Selenia Digital Mammography

Breast Tissue Composition

Two and three compartment models for breast composition.





Fibroglandular Volume Fraction











Histogram Thresholding









| Prooct | Donoity | Varia | hility |
|--------|---------|-------|--------|
| DIEdal | | Valla | |
| | | | |

| | Bi- RADS | Thresholding | Dual Energy |
|----------------------|-------------|--------------|----------------|
| Right - Left | 2.0 | 2.0 | 1.0 |
| Chemical Analysis | 2.1 | 1.8 | 1.0 |

Dual energy mammography requirements

- Minimize time interval between low and high energy images.
- Implement rapid kVp switching between low and high energy images.
- Implement rapid beam filter switching between low and high energy images (i.e. Rh filter to Cu filter).
- Minimize lag and ghosting between low and high energy images.
- Implement scatter correction.



Spectral mammography system

Post Mortem Study Details¹³⁹

- 28 specimens from 14 breast pairs (right and left)
- Each sample imaged at two different orientations (view 1 and view 2)
- Dual energy decomposition (water and lipid basis)



Chemical analysis (gold standard)
 T. Johnson, et al., Physics in Medicine and Biology 58, 8573-8591 (2013)

Spectral Material Decomposition





Breast Composition Variability

| | Water Content (%) | Lipid Content (%) |
|----------------------|----------------------|----------------------|
| Chemical Analysis | 3.2 | 4.7 |

