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CT Clinical Innovation Center


Multi-Energy CT: Principles, Processing and Clinical Applications

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Clinical Motivation

- ▶ CT number depends on x-ray attenuation
 - Physical density (g/cm^3) [electron-densit
 - Atomic number (Z)
- ▶ Different materials can have the same CT number if atomic number differences are offset by appropriate density differences



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Technical Implementations of DECT



Slow kVp Switching
Inter-scan delay = scan time + table move time

Fast kVp Switching

Low kVp
High kVp

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Technical Implementations of DECT

The diagram shows a dual source X-ray tube with two beams, one yellow and one blue, emerging from a central source. To the right, two energy spectra are shown: 'Low Energy' (blue) and 'High Energy' (red). The spectra show peaks at different energy levels, with the high energy spectrum having a higher peak energy.

Dual Source

Use twin beam filters

Low kVp
High kVp

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Technical Implementations of DECT

The diagram illustrates two detector types. On the left, 'Dual Layer "Sandwich" Detectors' show X-rays passing through two layers (blue and yellow) with arrows indicating 'Read out low-energy data' and 'Read out high-energy data'. On the right, a 'Photon Counting Detector' shows X-rays hitting a 'Semiconductor detector directly converts x-ray to charge (e.g. CdTe)'. Below this is a block diagram of the electronics: 'Preamps' feed into 'Shapers', which then feed into 'DAC' (Digital-to-Analog Converter) blocks. These DACs feed into 'Comparators' and 'Thresholds to pulse height comparator', which then feed into 'Counter 1', 'Counter 2', and 'Counter N', each producing a 'Digital output'.

Dual Layer "Sandwich" Detectors

Photon Counting Detector

C. McCollough, S Leng, L Yu, JG Fletcher. Dual- and Multi-Energy CT: Principles, Technical Approaches, and Clinical Applications. Radiology, 2015

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DECT Image Type and Processing Algorithms

The image shows three axial CT scans of the abdomen. The top left scan is labeled '100 kV' and shows high contrast. The top right scan is labeled '140 kV' and shows lower contrast. The bottom scan is labeled 'Mixed' and shows a combination of the two. Yellow arrows point from the 100 kV and 140 kV scans towards the Mixed scan.

100 kV

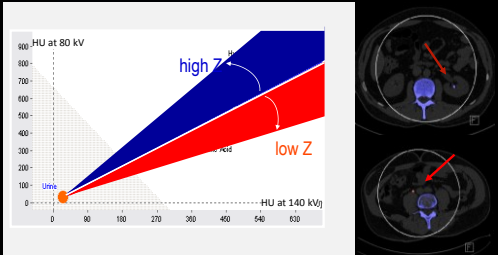
140 kV

Mixed

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Material Differentiation

- ▶ Differentiate two different type of materials (no quantification)




The slide features a graph on the left with a y-axis labeled 'HU at 80 kV' ranging from 0 to 800 and an x-axis labeled 'HU at 140 kV' ranging from 0 to 670. Two lines originate from the origin: a steeper blue line labeled 'high Z' and a less steep red line labeled 'low Z'. To the right of the graph are two axial CT scan images of a human torso, with red arrows pointing to specific regions in the spine area.

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Iodine and Water Quantification

Iodine Image Water Image



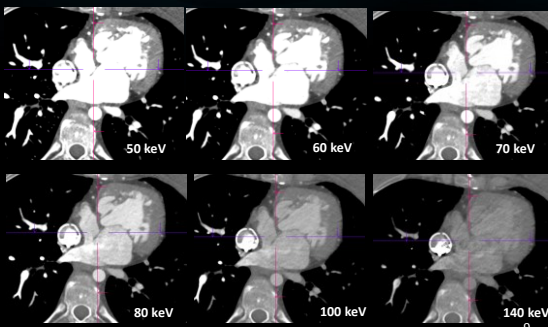
The slide shows a workflow for quantification. At the top left, an 'Iodine Image' displays several colored spots. At the top right, a 'Water Image' shows a grayscale representation of the same spots. Two orange arrows point from these images down to a 'Fused Image' at the bottom, which shows the spots with a numerical value of '20 mg/cc' overlaid on them.

Fused Image

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Virtual Monoenergetic Images



The slide displays a grid of six axial CT scan images of a human torso, arranged in two rows of three. The top row images are labeled '50 keV', '60 keV', and '70 keV'. The bottom row images are labeled '80 keV', '100 keV', and '140 keV'. The images show the progression of virtual monoenergetic images as the keV value increases.

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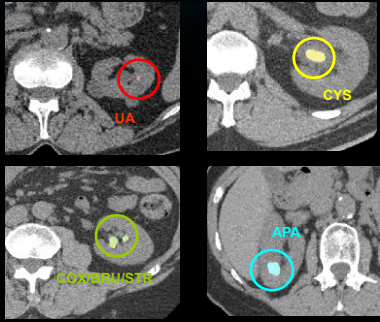
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Clinical Applications

- ▶ Renal stone differentiation
- ▶ Bone/Plaque removal in CTA
- ▶ Virtual noncontrast (VNC) image from contrast scans
- ▶ Bone bruise (VNCa)
- ▶ Lung perfusion
- ▶ Cardiac perfusion (blood pool)
- ▶ Gout detection and quantification
- ▶ Tumor treatment response assessment
- ▶ ...

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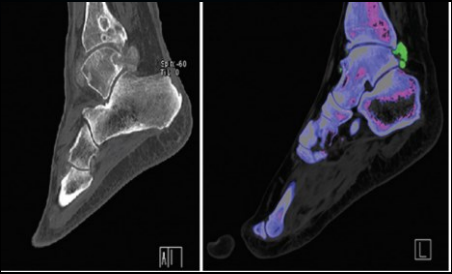
Renal Stone Differentiation



Qu et al, AJR, 2011

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Material Differentiation - Gout





Glazebrook et al, Radiology, 2011

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Material Differentiation - Gout



► All accurate assessment of disease burden to monitoring treatment effectiveness

90% reduction in volume of uric acid crystals over 8 months after receiving multiple infusions of rasburicase.

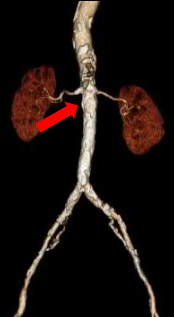
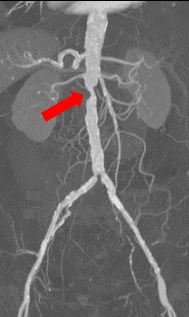
| April | December |
|---|---|
|  |  |

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Bone Removal

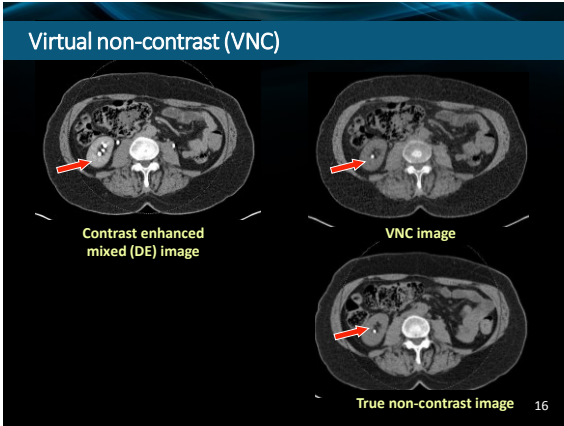
| | |
|--|--|
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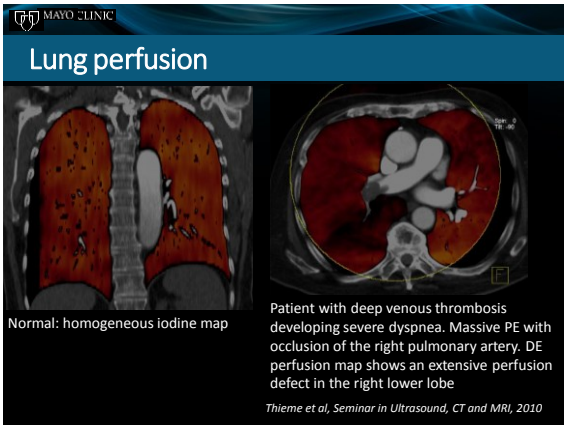
Courtesy Terri Vrtiska, MD

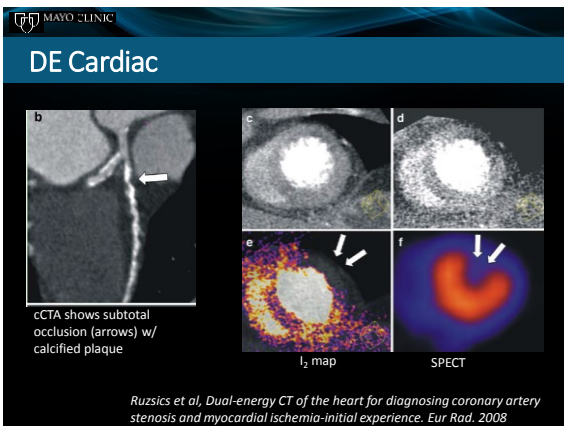
| | |
|---|---|
|  |  |
|---|---|

AP images

Routine volume rendered 3D images obscured the stenosis (left)
The high grade stenosis is easily depicted with DECT subtraction (right)







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Virtual non-calcium Image

SECT DECT - VNCA MRI

S. Ai et al, Use of dual-energy CT and virtual non-calcium techniques to evaluate post-traumatic bone bruises in knees in the subacute setting. Skeletal Radiology; 2014

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Monoenergetic Image

40 keV 85 keV

120 keV 140 keV (narrower window setting)

Image window was adjusted individually.

Silva et al, Radiographics 2011

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Metal Artifacts Reduction

Standard Image Monoenergetic Image (105 keV)

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Dual Energy in Oncology

Iodine Maps - Characterization

Iodine Color Map – late arterial phase

VNC – late arterial phase

Courtesy of Dr. Joel G. Fletcher

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Dual Energy in Oncology

Iodine Quantitation & Response to Rx

| ROI | Mean HU | SD | Min | Max |
|--------|---------|----|-----|-----|
| Iodine | 115 | 15 | 85 | 145 |
| Blood | 115 | 15 | 85 | 145 |
| VNC | 115 | 15 | 85 | 145 |

Courtesy of Dr. Joel G. Fletcher

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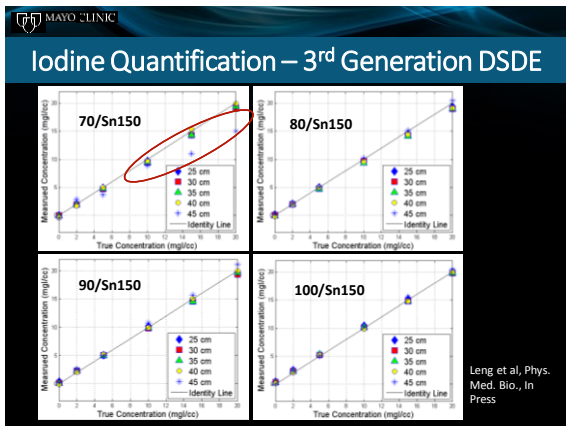
Iodine Quantification – 2nd Generation DSDE

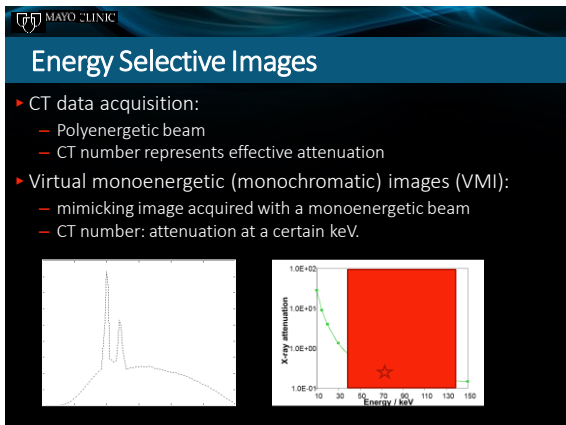
80/Sn140 kV

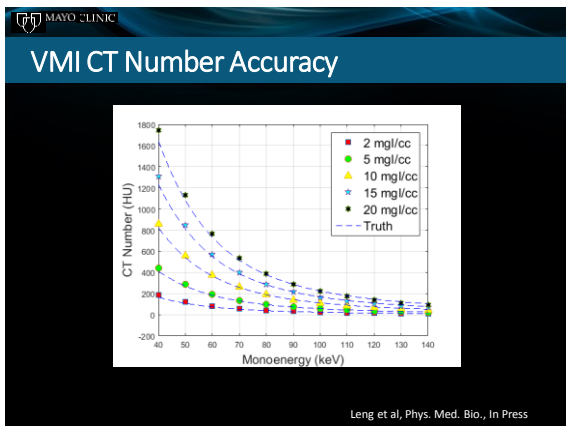
100/Sn140 kV

| Scanner Model | DE Mode | 25 cm | 30 cm | 35 cm | 40 cm | 45 cm | All Sizes |
|-------------------------|-------------|-------|-------|-------|-------|-------|-----------|
| 2 nd Gen. DS | 80/Sn140kV | 0.4 | 0.3 | 0.4 | 0.8 | 1.7 | 0.7 |
| | 100/Sn140kV | 0.3 | 0.3 | 0.3 | 0.5 | 0.5 | 0.4 |

Leng et al, Phys. Med. Bio., In Press







CT number stability

- ▶ Across scanner models and phantom sizes
- ▶ VMI CT numbers for 10 mgI/cc at 60 keV

| Scanner Model | CV |
|---------------|-------|
| -PCD | 0.036 |
| 80/Sn140 | 0.038 |
| 100/Sn140 | 0.013 |
| 70/Sn150 | 0.042 |
| 80/Sn150 | 0.032 |
| 90/Sn150 | 0.022 |
| 100/Sn150 | 0.016 |

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Iodine Quantification and CMI CT Number Accuracy

Philips iQon scanner

Courtesy of Dr. Xinhui Duan, UT South Western



MD Anderson Cancer Center

Iodine Quantification

- Error in iodine measurement generally within 10% across vendors (horizontal lines)
- Split-filter system within 10% of nominal value post-calibration

| Nominal Iodine Concentration [mg/mL] | Default Settings [mg/mL] | Calibrated Settings [mg/mL] |
|--------------------------------------|--------------------------|-----------------------------|
| 2 mg/mL | 1.3 ± 0.2 | 2.0 ± 0.2 |
| 5 mg/mL | 4.6 ± 0.2 | 5.4 ± 0.2 |
| 15 mg/mL | 13.5 ± 0.2 | 14.2 ± 0.2 |

Courtesy of Dr. Dianna Cody



Radiation Dose

- ▶ Dual-energy scans don't need to increase dose
 - Dose distributed between low/high energy acquisitions, each has a fraction of the total dose
 - Mixed images use all photons (dose)

Radiation Dose

Single Energy (120 kv)
March 2009
CTDIvol: 18.65 mGy

Indication: HCC
35 - 36 cm lateral width

Dual Energy Mixed
April 2009
CTDIvol: 15.59 mGy

Radiation Dose

- ▶ Dual-energy scans don't need to increase dose
 - Dose distributed between low/high energy acquisitions
 - Mixed images
 - VMI
 - Energy domain noise reduction

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Energy Domain Noise Reduction

Original

HYPR-LR

50 keV 60 keV

• Leng et al, Med. Phys. 2011
• Leng et al, Radiology, 2015

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Energy Domain Noise Reduction

CNR

Monoenergetic Images (keV)

DECT VMI

SECT

Single Energy CT Images (kV)

• Leng et al, Med. Phys. 2011
• Leng et al, Radiology, 2015

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Summary

- ▶ Multiple technical approaches have been implemented to perform DECT
 - Low/high/mixed images
 - Material specific images
 - Energy selective images (VMI)
- ▶ Wide range of clinical applications
- ▶ Considerations in clinical trial
 - Accurate iodine quantification
 - Accurate and stable VMI CT number
 - Radiation dose comparable to SECT
 - Impact of patient side on DE mode selection