

Summary and Insights into the TG-43U1S2 Report on brachytherapy dosimetry

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on behalf of the report authors

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Disclosures

This session may be interpreted as societal guidance.

Specific commercial equipment, instruments, and materials are listed to fully describe the necessary procedures. Such identification does not imply endorsement by the presenters, nor that these products are necessarily the best available for these purposes.

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Learning Objectives

- 1. understand method for deriving consensus datasets see 11 practical examples
- 2. become familiar with recommendations to vendors of BT sources and TPSs
- identify reference data for BT dosimetry investigations: radionuclide source spectra and half-lives, reference dose scoring media, and TLD methodological corrections

Supplement 2 for the 2004 update of the AAPM Task Group No. 43 Report: Joint recommendations by the AAPM and GEC-ESTRO

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Radial Dose Functions





1D Anisotropy Functions



Summary and Insights into the TG-43U1S2 Report on brachytherapy dosimetry: Report summary, methods to formulate consensus data, and presentation of the consensus datasets

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AAPM Task Group 43 formed in 1988 and published its report in 1995

Dosimetry of interstitial brachytherapy sources: Recommendations of the AAPM Radiation Therapy Committee Task Group No. 43

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- Included data on ¹⁹²Ir and 3 permanent seed LDR sources
 - ¹²⁵I models 6711 and 6702 and ¹⁰³Pd model 200

Subsequent TG-43 reports

- 2004, TG-43 U1
 - Updated 3 models
 - Added 5 new seed models
 - Included Bebig and Best ¹²⁵I models
- 2007, TG-43 U1S1
 - Added 8 new seed models
 - Included IsoAid ¹²⁵I and Best ¹⁰³Pd models

Finally...!



The latest report, TG-43 U1S2 (*Med Phys*, **44**:e297–e338, 2017)

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TG-43 Update 1, Supplement 2

- Added 11 new seed models
 - Included Elekta and Theragenics ¹²⁵I, CivaTech and IsoAid ¹⁰³Pd and IsoRay ¹³¹Cs models
 - Data for 5 discontinued models included for retrospective analyses
- Contains 38 data tables
 - > 6,800 data points
 - 42 pages in *Med Phys*
 - Considerable manual labor!



- Dose rate tables for each source for r vs. polar angle
 - r range from 0.1 cm to 10 cm
 - Angles from 0° to 90°
- Dose rate tables for each source in Cartesian coordinates (along and away)
 - r from 0 to 7 cm

TABLE XVIII. Dose rates (cGy h⁻¹ U⁻¹) per unit source strength (Theragenics model AgX100 ¹²⁵I source)

	Away (cm)												
Along (cm)	0	0.5	1	1.5	2	3	4	5	6	7			
0.0		3.981	0.952	0.386	0.1950	0.0676	0.0290	0.01388	0.00718	0.00390			
0.5	1.018	1.928	0.763	0.352	0.1858	0.0667	0.0287	0.01381	0.00715	0.00389			
1.0	0.287	0.599	0.417	0.248	0.1481	0.0593	0.0268	0.01322	0.00694	0.00380			
1.5	0.1393	0.241	0.218	0.1581	0.1073	0.0491	0.0237	0.01209	0.00649	0.00361			
2.0	0.0788	0.1185	0.1202	0.0986	0.0745	0.0389	0.0201	0.01074	0.00592	0.00335			
2.5	0.0480	0.0657	0.0702	0.0628	0.0510	0.0300	0.01664	0.00929	0.00528	0.00306			
3.0	0.0316	0.0402	0.0434	0.0407	0.0349	0.0225	0.01345	0.00788	0.00462	0.00274			
3.5	0.0210	0.0256	0.0279	0.0270	0.0242	0.01686	0.01070	0.00656	0.00398	0.00242			
4.0	0.01455	0.01717	0.01860	0.01837	0.01693	0.01255	0.00841	0.00539	0.00338	0.00211			
4.5	0.01030	0.01189	0.01274	0.01275	0.01200	0.00934	0.00658	0.00438	0.00283	0.001811			
5.0	0.00747	0.00845	0.00897	0.00902	0.00861	0.00699	0.00512	0.00353	0.00236	0.001542			
5.5	0.00545	0.00607	0.00640	0.00648	0.00627	0.00524	0.00397	0.00283	0.001945	0.001303			
6.0	0.00404	0.00445	0.00465	0.00471	0.00459	0.00395	0.00308	0.00227	0.001593	0.001092			
6.5	0.00302	0.00331	0.00343	0.00347	0.00340	0.00300	0.00239	0.001803	0.001300	0.000909			
7.0	0.00229	0.00249	0.00255	0.00258	0.00255	0.00228	0.001865	0.001433	0.001058	0.000754			

Easily check your TPS (use T_{avg})

There is, of course, an erratum



- Med Phys, 45:971–974, 2018
- 6 data tables republished with errors corrected

TG-43 dose equation for a line source

$$Dose = S_K \cdot A \cdot g_L(r) \cdot F(r,\theta) \cdot T_{avg} \cdot \frac{G_L(r,\theta)}{G_L(r_0,\theta_0)}$$

 S_{κ} = air-kerma strength in $cGy \cdot cm^2/h = U$

 $\Lambda = \text{dose rate constant in } cGy / h \cdot U$

 $g_L(r)$ = radial dose function (atten & scatter)

 $F(r, \theta) = 2D$ anisotropy function

 T_{avg} = average life of the radionuclide = $t\frac{1}{2}/ln2$

 $G_L(r, \theta)$ = geometry function of source distribution

Reference quality published data necessary for consensus

- Effective active length, L_{eff}, determined for geometry function calculations
- Two methods used to determine dosimetry parameters
 - Experimental: TLD
 - Solid to liquid corrections used
 - Monte Carlo transport is up-to-date
 - cross section library
 - scoring estimator

The consensus dose rate constant, Λ

$$\Lambda = \frac{\dot{D}(r_0, \theta_0)}{S_K}$$

- The reference position: $r_0 = 1$ cm and $\theta_0 = \pi/2$
- Λ is a 50:50 average of all the valid, published TLD data and all the valid, published Monte Carlo data
 - The uncertainty for each methodology, experimental or calculational, is summed in quadrature

$$\sigma = \sqrt{\sigma \Lambda_{\rm EXPa}^2 + \sigma \Lambda_{\rm EXPb}^2}$$

Total uncertainty is the weighted quadrature sum of each methodology

$$\sigma_{\rm TOT} = \sqrt{\sigma \Lambda_{\rm EXP}^2 + \sigma \Lambda_{\rm MC}^2 + \left(\frac{\Lambda_{\rm EXP} - \Lambda_{\rm MC}}{2 \cdot \sqrt{3}}\right)^2}$$

The radial dose and 2D anisotropy functions

- The functions are intermediaries to reproduce and interpolate doses found by experiment or Monte Carlo
- g(r) and F(r,θ) are not measured quantities but are derived from the doses in order to separate factors contributing to dose.

$$g_L(r) = \frac{D(r,\theta_0)}{D(r_0,\theta_0)} \cdot \frac{G_L(r_0,\theta_0)}{G_L(r,\theta_0)}$$

$$F(r,\theta) = \frac{D(r,\theta)}{D(r,\theta_0)} \cdot \frac{G_L(r,\theta_0)}{G_L(r,\theta)}$$

Geometry functions

• $G(r,\theta)$ for a point source is simply the inverse square:

$$G_{\rm P}(r,\theta) = \frac{1}{r^2}$$

When describing the source as a line:

$$G_{L}(r,\theta) = \frac{\beta}{L_{eff} \cdot r \cdot \sin \theta}$$

- $L_{eff} = \Delta S \cdot n$ for *n* discrete pellets of spacing ΔS
- Beta, β , is the angle subtended by L_{eff} at the calculation point



All candidate data was checked for consistency

 Reported g(r) converted from line to point or vice versa using geometry functions

$$G_L(r,\theta) = \left(\tan^{-1}\left(\frac{L_{eff}}{2 \cdot r \cdot \sin\theta} + \frac{1}{\tan\theta}\right) + \tan^{-1}\left(\frac{L_{eff}}{2 \cdot r \cdot \sin\theta} - \frac{1}{\tan\theta}\right)\right) / (L_{eff} \cdot r \cdot \sin\theta)$$

- F(r, $\theta)$ and $\phi_{an}(r)$ values using geometry functions, dose weighting, and angular weighting

Calculated g(r) were plotted to reveal outliers

(Elekta model 130.002)



$F(r,\theta)$ for $r \le 1$ cm (Elekta model 130.002)



$F(r,\theta)$ for $r \ge 1$ cm (Elekta model 130.002)



Interpolation and extrapolation

- Interpolation of $F(r,\theta)$ uses a bi-linear approach
- Interpolation of g(r) uses a log-linear approach

$$g(r_x) = g(r_i) \cdot e^{\frac{(r_x - r_i) \cdot \left(\ln(g(r_f)) - \ln(g(r_i))\right)}{(r_f - r_i)}}$$

g(r)	r	linear	log-lin
r _i	0.1	0.576	0.576
r _x	0.15	0.679	0.664
r _f	0.25	0.884	0.884

Log-linear interpolation for g(r) compared to linear interpolation



In TG-43 U1S2, interpolated data is **bold** and extrapolated is <u>underlined</u>

• Those values are not derived from numbers in the printed report but from nearby high resolution values.

<i>r</i> (cm)	BEBIG S17	BEBIG S 17plus	BEBIG S18	Elekta 130.002					
Line-source approximation, $_{CON}g_{L}(r)$									
0.10	1.072	1.059	1.169	1.042					
0.15	1.090	1.080	1.152	1.062					
0.25	1.100	1.092	1.121	1.085					
0.50	1.077	1.073	1.070	1.078					
0.75	1.042	1.040	1.033	(1.044)					
1.00	1.000	1.000	1.000	1.000					
			· · · · · · · · · · · · · · · · · · ·	*					

Interpolated from r = 0.7 and 0.8

TABLE AIX. $_{\text{CON}}F(r, \theta)$ data for the CivaTech model CS10 103 Pd from the consensus $_{\text{CON}}F(r, \theta)$ dataset.



Use the report wisely, & thank you



Summary and Insights into the TG-43U1S2 Report on brachytherapy dosimetry: Dosimetry parameter dependence on radionuclide, influence of dataset grid size, and recommendations to vendors of brachytherapy sources and treatment planning systems

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Learning objectives

- show dependence of TG-43 parameter values on radionuclide
- highlight influence of consensus dataset grid size on TPS calculations
- identify societal recommendations to vendors of brachytherapy sources and treatment planning systems

Contents

- background
- dependence of TG-43 parameter values on radionuclide
- resolution grid size influence on TPS calculations
- recommendations to seed and TPS vendors

TG-43U1S2 seeds



TG-43U1S2 seeds



Dose rate constant values: Dependence on radionuclide

• dose rate constant, $_{\rm CON}\Lambda$



For seeds of the same radionuclide, the dose rate constant is approximately constant

Radial dose function: Dependence on radionuclide



2D anisotropy function values: Dependence on radionuclide

• 2D anisotropy function, $_{CON}F(r,\theta)$



For seeds of the same radionuclide, the 2D anisotropy functions are similar.

special case: S18¹²⁵I seed

1D anisotropy function values: Dependence on radionuclide



For seeds of same radionuclide, 1D anisotropy functions exhibit specific characteristics for r < 0.5 cm

special case: S18¹²⁵I seed

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1D anisotropy function functions for the 11 seed models



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Influence of the grid size resolution on TPS calculations

Data interpolation/extrapolation method recommendations

 Table III. Interpolation and extrapolation recommendations for high-energy (*low-energy*)^[3]

 brachytherapy sources for the line-source approximation.

Parameter	$r < r_{min}$ Extrapolation	$r_{\min} < r \le r_{\max}$ Interpolation	$r > r_{max}$ Extrapolation
$g_L(r)$	Nearest neighbor or zeroth-order extrapolation (<i>Ditto</i>)	Linear (<i>log-linear</i>) using datapoints immediately adjacent to the radius of interest	Linear using data of last two tabulated radii (<i>single exponential function based</i> on fitting $g_L(r)$ datapoints for the furthest three r values).
$F(r, \theta)$	Nearest neighbor or zeroth-order extrapolation (<i>Ditto</i>)	Bilinear (<i>bilinear</i>) interpolation method for $F(r, \theta)$	Nearest neighbor or zeroth-order <i>r</i> -extrapolation (<i>Ditto</i>)

Pérez-Calatayud, et al. Med. Phys. 39, 2904-2929 (2012)

Influence of grid size resolution on TPS calculations

JOURNAL OF APPLIED CLINICAL MEDICAL PHYSICS, VOLUME 16, NUMBER 4, 2015

Brachytherapy treatment planning commissioning: effect of the election of proper bibliography and finite size of TG-43 input data on standard treatments

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The aim of this work is to evaluate performance of a commercial BT TPS with vendor TG-43 data, analyze possible discrepancies with respect to a proper reference source and its implications for standard treatments, and judge the effectiveness of certain widespread recommended quality controls to find potential errors related with interpolations of TG-43 tables.

Valdés, et al., J. Appl. Clin. Med. Phys. 16, 3-17 (2015)

Influence of grid size resolution on TPS calculations



Valdés, et al., J. Appl. Clin. Med. Phys. 16, 3-17 (2015)

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Influence of grid size resolution on TPS calculations

• 2D anisotropy function grids in TG-43U1S2

					Aniso	otrop	y func	tion	grids	;				
				r (cm)							θ (de	egrees	5)	
	0	0,1	0,15	0,20	0,25	0,5	0,75	1		0	2	5	7	10
S17	о	ο	ο		ο	ο	ο	ο		0	ο	ο	ο	о
S17Plus	О				ο	ο	ο	ο		0	ο	ο	ο	о
S18	О					ο		0		ο				о
130,002	о	ο		0		ο	ο	ο		0	ο	ο	ο	о
9011	О	ο			0	ο	ο	ο		ο	ο	ο	ο	о
AgX100	о	ο			ο	0	ο	0		0	ο	ο	ο	о
CS10	О	ο			ο	ο	ο	ο		0	ο	ο	ο	о
1031L	о	ο	ο		ο	ο	ο	ο		0	ο	ο	ο	о
1032P	о	ο	о		о	0	ο	ο		0	ο	ο	0	о
IAPd-103/	А о	ο	ο		ο	ο	ο	ο		ο	ο	ο	ο	о
CS-1 Rev2	О	ο	ο		о	ο	ο	о		ο		ο		о

Consensus datasets

preferences on dosimetry datasets origin for clinical use

- societal consensus data: TG-43U1, TG-43U1S1, TG-43U1S2 reports
- data posted on the AAPM/IROC Houston Brachytherapy Source Registry



- http://rpc.mdanderson.org/RPC/BrachySeeds/Source_Registry.htm
 - for a seed not posted on the Registry: the user should perform a study similar to the ones described in the TG-43U1S2 report.
- early adopters of a seed should collaborate with vendor, vendor dosimetry consultant, and TPS vendor

Consensus datasets

preferences on dosimetry datasets origin for clinical use

- seeds approved in Europe but new in North America: follow GEC-ESTRO recommendations
- dataset on ESTRO and Carleton University websites as Excel spreadsheet formats





https://www.estro.org/about/governance-organisation/committees-activities/tg43 http://www.physics.carleton.ca/clrp

Consensus datasets



Seed and TPS vendor dosimetry recommendations

Seed vendors:

- source strength must be specified in terms of S_{K} in U units
- contained activity should only be used for regulatory purposes:
 NRC reported events due to the use of apparent activity instead of S_K

https://www.nrc.gov/docs/ML0807/ML080710054.pdf

In the manufacturer's certificate, the date format must be specified:

DD/MM/YY or MM/DD/YY or YY/MM/DD?

Seed and TPS vendor dosimetry recommendations

- TPS vendors:
 - use consensus datasets
 - use of the correct *L* (or L_{eff})
 - follow recommended methods for interpolation/extrapolation
 - the date format must be specified: DD/MM/YY or MM/DD/YY or YY/MM/DD
 - use QA tables in the report available to the user
 - implement 1D approximation for dose calculation
 - information on manu. certificate and TPS must be the same

Acknowledgements

TG-43U1S2 members

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Summary and Insights into the TG-43U1S2 Report on brachytherapy dosimetry: Radionuclide Source Spectra and Half-Lives, Reference Dose Scoring Media, and TLD Methodological Corrections

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§ 5.B. Radionuclide Half-Lives

- Recommended source: National Nuclear Data Center (NNDC) of Brookhaven National Laboratory http://www.nndc.bnl.gov/chart/
- The NNDC collects, evaluates, and disseminates nuclear physics data for basic nuclear research and applied nuclear technologies. http://www.nndc.bnl.gov/chart/reCenter.jsp?z=46&n=57
 De Frenne, Nuclear Data Sheets 110, 2081 (2009)
 http://www.nndc.bnl.gov/chart/reCenter.jsp?z=53&n=72
 Katakura, Nuclear Data Sheets 112, 495 (2011)
 http://www.nndc.bnl.gov/chart/reCenter.jsp?z=55&n=76
 Khazov et al, Nuclear Data Sheets 107, 2715 (2006)
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§ 5.A. Radionuclide Photon Spectrum

- choice of reference data not a simple decision based on current evaluations NNDC is comprehensive for gamma ray tabulations (limited for x rays)
 NIST is thorough for x-ray transition energies, but not intensities
 NCRP Report 58 is coarse and from a 1984 evaluation
 Lund University (Sweden) and Lawrence Berkeley National Lab is from 1999
 Laboratoire National Henri Becquerel (France) is missing ¹⁰³Pd and ¹³¹Cs
- combine evaluations for AAPM+GEC-ESTRO ¹³¹Cs reference data
- choice of reference data weakly influences dose calculations choice of reference data weakly influences TG-43 dosimetry parameters

§ 5.A. Radionuclide Photon Spectrum: ¹³¹Cs

TABLE XXIV. Half-life and photon spectrum for ¹³¹Cs dosimetry. X-ray transitions are listed after the elemental symbol for the daughter nuclide (i.e., Xe). Subgroups are enumerated for the K_{α} and K_{β} transitions, while the mean energies and total intensities are given for the other transitions, e.g., $L_{\gamma} = L_{\gamma 1} + L_{\gamma 2} + L_{\gamma 3}$.

	•
Photon energy (keV)	Photons per disintegration
3.760 Xe $L_{\eta+i}$	0.0037
4.109 Xe L_{α}	0.0702
4.479 Xe L $_{\beta}$	0.06302
5.138 Xe L _γ	0.00844
29.112 Xe K _{α3}	0.000022
29.461 Xe K _{α2}	0.211
29.782 Xe K _{α1}	0.389
33.562 Xe K _{β3}	0.0364
33.624 Xe K _{β1}	0.0702
33.881 Xe K _{β5}	0.00071
34.419 Xe K _{β2}	0.0213
34.496 Xe K _{β4}	0.00412
	0.8781 total photons per disintegration
30.411 mean (> 10 keV photons)	$0.7328 \text{ total} (\geq 10 \text{ keV photons})$

 131 Cs (half-life = 9.689 \pm 0.016 days)

§ 5.C. Reference Dose Scoring Media

- density of water (H₂O) at 22 °C is 0.998 g/cm³
- standard temperature and pressure (STP) of air depends on locale N. American STP is 22 °C and 101.325 kPa European STP is 20 °C and 101.325 kPa
- air composition (by mass) is fixed
 75.527% N, 23.178% O, 1.283% Ar, 0.012% C

§ 5.D. TLD Dosimetry Methodological Corrections $D_{med}(Q) = M(Q) N_{D,med}(Q)$ (1) $S_{AD, med}(Q) = \frac{M(Q)}{D_{mod}(Q)}$ (2) $S_{AD, med}(Q) = \frac{M(Q)}{D_{med}(Q)} = \frac{M(Q)}{D_{TID}(Q)} \frac{D_{TLD}(Q)}{D_{med}(Q)} = \frac{1}{k_{ba}(Q)} \frac{1}{f(Q)}$ (3) $S_{AD,med}^{rel} = \frac{S_{AD,med}(Q)}{S_{AD,med}(Q_0)} = \frac{1}{\frac{1}{\frac{krel}{ba}}} \frac{1}{f^{rel}}$ (4) $E(r) = \frac{S_{AD,med}^{rel}(Q)}{P_{phant}} = \frac{1}{\frac{1}{k_{pq}^{rel}}} \frac{1}{f^{rel}} \frac{1}{P_{phant}}$ (5)

- understand relationship between detector measurement, medium corrections, detector corrections, and absorbed dose to the medium as function of radiation quality Q (i.e., photon energy)
- convert detector measurement M(Q)

to absorbed dose to the medium $D_{med}(Q)$

via the absorbed dose calibration coefficient $N_{D,med}(Q)$

$$D_{med}(Q) = M(Q) N_{D,med}(Q)$$
(1)

- inverse of the absorbed dose calibration coefficient $\,{}^{N}_{D,\,med}(Q)$

is the absorbed dose sensitivity coefficient $S_{AD, med}(Q)$

 $S_{AD, med}(Q) = \frac{M(Q)}{D_{med}(Q)}$

(2)

• partition $S_{AD, med}(Q)$ into two components $S_{AD, med}(Q) = \frac{M(Q)}{D_{med}(Q)} = \frac{M(Q)}{D_{TLD}(Q)} \begin{bmatrix} D_{TLD}(Q) \\ D_{med}(Q) \end{bmatrix}$ avg. TLD dose for radiation quality Qintrinsic *Q* dependence $k_{bq}(Q)$ $\frac{M(Q)}{\overline{D_{TID}}(Q)} \frac{D_{TLD}(Q)}{D_{med}(Q)} = \frac{1}{k_{bq}(Q)} \frac{1}{f(Q)}$ determined only by measurement of signal formation absorbed dose sensitivity f(Q), $S_{AD,med}(Q) = \frac{1}{k_{ba}(Q)} \frac{1}{f(Q)}$ (3) dependent on medium and detector, may be estimated with Monte Carlo

- relative absorbed dose sensitivity coefficient uses ratios with Q and Q_0

$$S_{AD,med}^{rel} = \frac{S_{AD,med}(Q)}{S_{AD,med}(Q_0)} = \frac{1}{k_{bq}^{rel}} \frac{1}{f^{rel}} \quad \text{ratio to calibration}$$

$$relative \text{ intrinsic } Q \text{ dependence } k_{bq}^{rel} \text{ of the detector}$$

$$relative \text{ absorbed dose sensitivity } f^{rel} \text{ of the detector}$$

$$\mathbf{relative} = \frac{1}{2} \frac{1}{2}$$

$$S_{AD,med}^{rel} = \frac{1}{\frac{krel}{bq}} \frac{1}{f^{rel}}$$

(4)

- account for phantom presence P_{phant} different than calibration medium $\frac{S_{AD,med}^{rel}(Q)}{P_{phant}} = \frac{1}{\frac{1}{k_{pq}^{rel}}} \frac{1}{f^{rel}} \frac{1}{P_{phant}}$
- relative energy response function E(r)

dosimetry investigators should specify assumptions and methods for deriving the methodological corrections to dose

$$E(r) = \frac{1}{\frac{krel}{bq}} \frac{1}{f^{rel}} \frac{1}{P_{phant}}$$
(5)

Summary

- 11 new sources evaluated with consensus data provided
- _{CON}Λ for ¹⁰³Pd seeds all within 0.6% of 0.697 cGy/h/U except for plastic encapsulated model 1032P and CS10 sources
- _{CON}Λ for ¹²⁵I seeds all within 1.2% of 0.942 cGy/h/U except for plastic encapsulated model S18 source
- $_{CON}\Lambda$ for ¹³¹Cs (1.056) increased as expected relative to ¹⁰³Pd and ¹²⁵I
- $_{MC}\Lambda / _{EXP}\Lambda = 0.961$ on avg. for all 11 source models
- $_{\text{CON}}g(r)$ and $_{\text{CON}}\phi_{\text{an}}(r)$ varied with energy and *r* as expected
- QA tables (along-away, polar coordinates) were provided
- medical physicists should document their TPS commissioning

WAYNE'S SLIDES GO HERE