

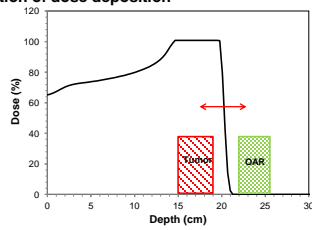
Adaptive Proton Therapy with CBCT

Kevin Teo, PhD



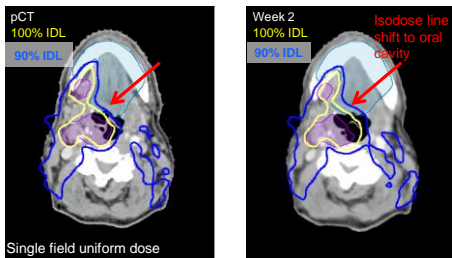
Sensitivity of Proton Dose Distribution

- Protons have finite range
- Change in material composition along beam path → Shift in position of dose deposition



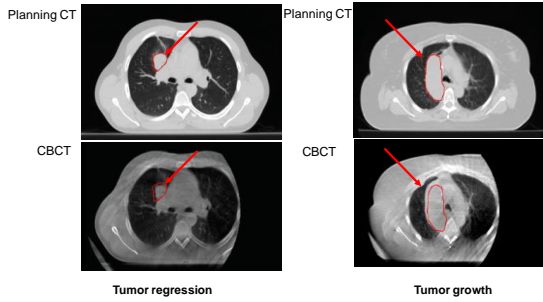
- Repeat CT imaging or in-room CBCT needed throughout treatment course to monitor anatomic change

Impact of Anatomic Change



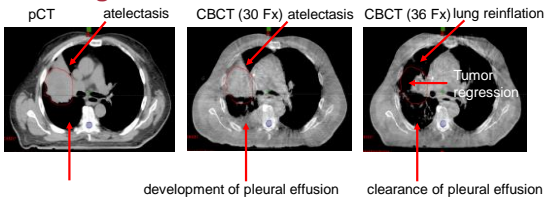
- Less optimal dose distribution- degrades with time
- OAR doses may increase eg oral cavity
- Worse with IMPT compared with single field uniform dose technique

Lung Anatomic Change



Impact on dose distribution to target and organs at risk needs to be assessed

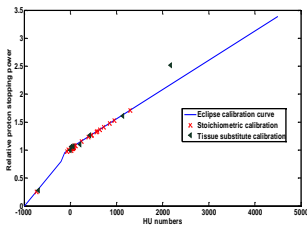
Lung: Pleural Effusion, Atelectasis, Tumor Regression



Anatomic change will impact proton range, periodic assessment during treatment is necessary

Limitations of CBCT for Dose Calculation

- Proton dose calculation is **more sensitive** to HU accuracy than photon therapy
- CBCT **cannot** be used directly for dose calculation unless HU accuracy is verified

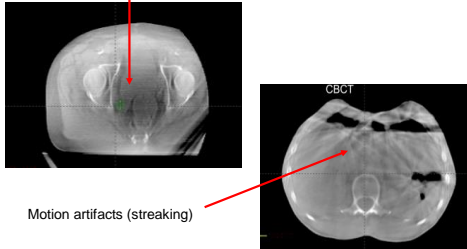


If CT number is off by 100 HU Stopping power is different by 5% For a 10cm range, error is 5 mm.

Need error in water equivalent depth << Range uncertainty of 3.5%

Limitations of CBCT for Dose Calculation

- Inaccurate HUs
- Beam hardening and scatter artifacts (dark streaks between high density structures, cupping artifacts)



Motion artifacts (streaking)

Improving Accuracy of CBCT HUs for Dose Calculation

1) Histogram matching method

K. Arai et al. Physica Medica 33 (2017) 68–76

2) A priori CT based scatter correction – More accurate correction (CBCT_{cor})

Y.-K. Park et al. Med Phys 42 4449 (2015)
Kim et al PHYSICS IN MEDICINE AND BIOLOGY Volume: 62 Issue: 1 Pages: 59-72 JAN 7 2017
Kurz et al MEDICAL PHYSICS Volume: 43 Issue: 10 OCT 2016

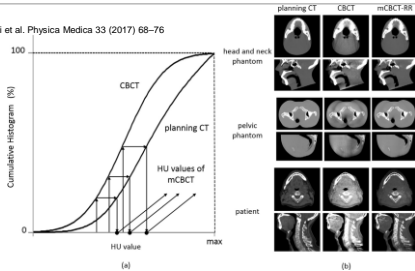
3) Deformable Image Registration (DIR) approach - Deform planning CT to geometry of CBCT (virtual CT)

C. Veiga et al. IJROBP 95 549 (2016)
Veiga et al Biomed. Phys. Eng. Express 3: 015003, Feb 2017
Landy G et al Med. Phys. 42 1364-66 2015
Veiga et al Med. Phys. 41 (3), March 2014 031703
..... Many others

Use one or combination of above methods

(1) Histogram Matching Method

K. Arai et al. Physica Medica 33 (2017) 68–76



- Replace cumulative value of CBCT HU histogram with SAME cumulative value of pCT histogram
- Apply rigid registration or DIR prior to histogram matching
- Scatter effects in CBCT as well as image artifacts may impact accuracy

(2) A priori CT Scatter Correction Method

$$I_{sca} = f(CF \times I_{raw} - I_{pri})$$

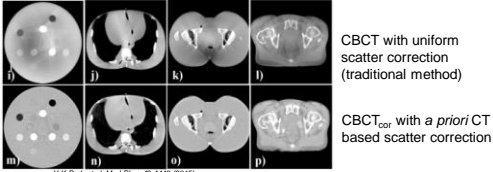
From forward projection of prior image (eg pCT)

Subtraction of primary signal (no scatter) from raw projection with scatter

$$I_{cor} = CF \times I_{raw} - I_{sca}$$

reconstruction → **CBCT_{cor}**

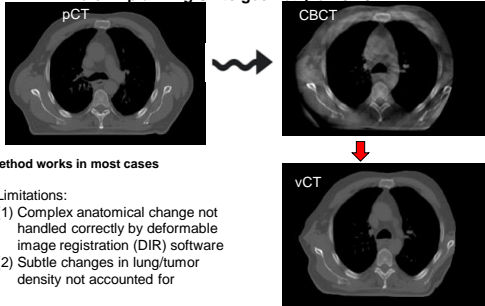
Scatter corrected projection



Y.K.Park et al. Med Phys 42 4489 (2015)

(3) Deformable Image Registration Method: Virtual CT (vCT)

Deform planning CT to geometry of CBCT



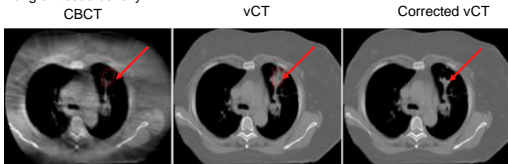
Method works in most cases

- Limitations:
- (1) Complex anatomical change not handled correctly by deformable image registration (DIR) software
 - (2) Subtle changes in lung/tumor density not accounted for

C. Velge et al. IJROBP 95 549 (2016)

Correction for Large Tumor Regression

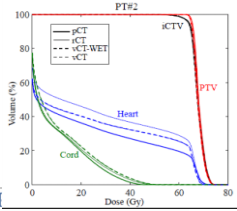
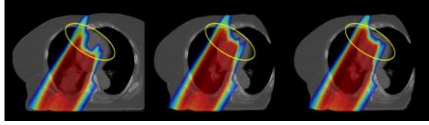
Identify gross DIR errors between CBCT and vCT and replace HU with lung or tissue density



Large tumor regression

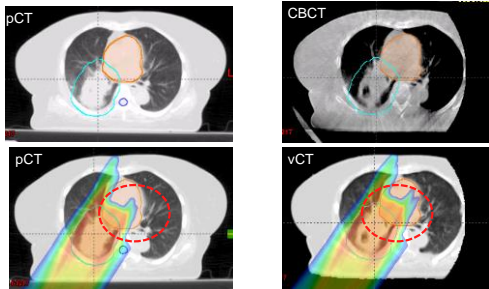
Dose Analysis with vCT

pCT and planned dose vCT and warped dose vCT and recalculated dose



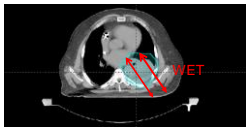
Feasible to replace evaluation CTs with CBCT
IJROBP Veiga et al 2016

Impact to Organ at Risk



Mean heart dose 16.8Gy (pCT) vs 20.0 Gy (vCT)
Identify change in OAR dose

Comparison of Virtual CT with Rescan CT



WET:
 Water Equivalent Thickness from
 entrance of beam to target

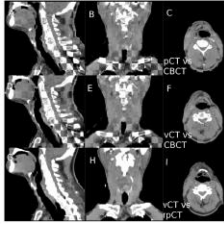
Results of 20 patient study:

Region of interest	WET _{mean} (mm)	WET _{RMS} (mm)	WET _{90%} (mm)
Distal surface	0.5±2.2	3.7±1.9	8±4
Proximal surface	0.1±1.9	2.3±1.5	4±3
PTV	0.4±2.1	3.4±2.0	7±4

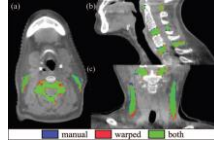
- Mean difference in WET is about 1mm
- Possible to estimate shifts in range with 2 to 3 mm accuracy

C Veiga et al, *IJROBP* 95 549 (2016)

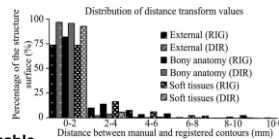
Head and Neck vCT



Landry G et al. Med. Phys. 42 1354-66 2015



Veiga et al. Med. Phys. 41 (3), March 2014 031703

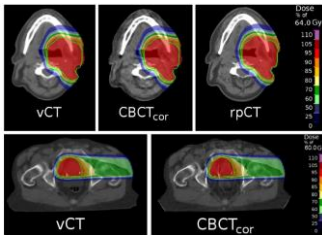


- vCT works well for head and neck
- Evaluated with a number of deformable image registration (DIR) algorithms (ANTS, Morphons, B-spline variants)

PENN RADIATION ONCOLOGY

Penn Medicine 18

Comparison of vCT and CBCT_{cor} Dose Calculation



- High agreement of vCT and CBCT_{cor} for proton range calculation for head and neck and prostate
- Between 95% and 100% of dose profiles agree to 3mm

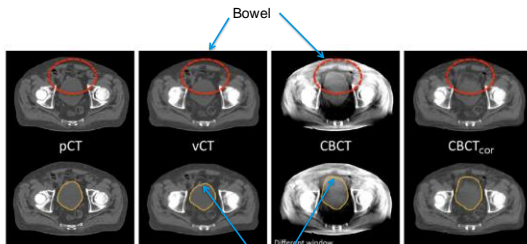
Kurz et al. MEDICAL PHYSICS Volume: 43 Issue: 10 OCT 2016

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Comparison of vCT and CBCT_{cor}

Anatomical inconsistencies between vCT and CBCT



Bladder

Kurz et al. MEDICAL PHYSICS Volume: 43 Issue: 10 OCT 2016

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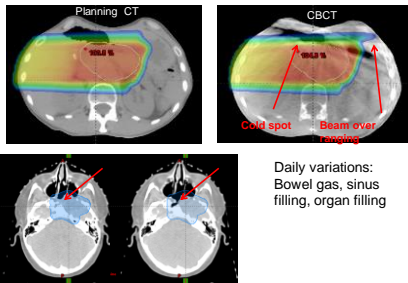
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Comparison of vCT and CBCT_{cor}

	vCT	vCT with correction	CBCT _{cor}
Head and Neck	✓✓	✓✓	✓✓
Lung	✓	✓✓	✓✓
Pelvis	✓	✓	✓✓
Prostate	✓✓	✓✓	✓✓
Contours and HU	May have some local inaccuracies	Better than vCT	Best in accuracy
Dose	May have some local inaccuracies	Fairly accurate	Fairly accurate

On-Line or Off-Line Adaptive Therapy?

- Most anatomical change especially (weight, tumor response) is gradual → offline adaptation
- In some cases, on-line adaptation would be needed but is not practical (yet)



Summary:

- Periodic monitoring of anatomy using CBCT, evaluation CT is needed for proton therapy
- Virtual CTs (deformable image registration) can be used to estimate dose
- vCTs may have local errors for large anatomical change
- Offline adaptation triggered by CBCT