



John M. Boone, Ph.D. Professor of Radiology and Chief of Medical Physics Professor of Biomedical Engineering University of California Davis Sacramento, California

Dose Spread Functions in CT

Tu-HI-221CD • San Antonio AAPM • Patient Dose Monitoring in CT with Tube Current Modulation and Multiple Series

Conflicts of Interest:

Board Member (and Treasurer), International Commission on Radiation Units (ICRU) Board Member and shareholder, Izotropic Imaging (breast CT company) Board Member, California Radiological Society (local chapter of the ACR) (in kind) Research Funding, Canon Medical Systems Travel Funding from:

American Association of Physicists in Medicine (IPC and IEC meetings) International Commission on Radiation Units and Measurement (ICRU)

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Introduction Methods Results Consequences Summary



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1.5 decades of CT dose in the news.....

USA TODAY

CT scans in children linked to cancer 2001 alout 1.8 million children inthe USA pet CT scars to the head and and alout 1.500 of from will do later in the stradadon-induced carding to material ad solar. c. Of an energedied lowergewathy scarse given to lively and typically a status, us children almost two to an forward that wand taken to and in twanger, a second that is shown. These down and "seep larger to a finite their people of These Alls halved some gating," David also also their people and These Alls halved some gating," and also also their people and These people got a hardwards are a bandward asso. on-induced temporary hair loss diation damage only occurring sts who had the combination T and DSA LOCATE DISTORY (1991)

FDA Public Health Notification: Reducing Radiation Risk from Computed Tomography for Pediatric and Small Adult Patients

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ROLLS for and they descense. Provide the state of the state is the s







We Are Giving Ourselves Cancer

= Google Scholar radiation dose in computed tomography

Articles

About 1,130,000 results (0.11 sec)

Computed Tomography: patient dosimetry



Computed Tomography: simple phantom imaging

This Work







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This study is a Monte Carlo-based analyses

Dose spread functions in computed tomography: A Monte Carlo study John M. Boone⁰¹ Doynmor y Radiogy and Department of Biomedical Depinering. University of California. Davis Madrid Center, 4000 T Street, State 3100 Elitom Initiang, Sommernia, California 55817 (Received J Perbury 2009; revised 3 August 2009; accepted for publication 7 August 2009; published 10 September 2009)



Monte Carlo validation





Monte Carlo validation in diagnostic radiological imaging John M. Boone¹⁰ Michael H. Buonocore, and Virgi N. Cooper III Dynamic of Bahalogi, Dimany of California, Maximis Scienceson, California 08177 (Received 6 December 1999; accepted for publication 30 March 2000)



Processor





Monte Carlo: Methods



- CT scanner geometry (SIC)
- Accurate spectra using TASMIP Model (kV and HVL)
- Different bow tie filters (GE-VCT, Siemens AS+, none)
- Different diameter cylinders (10-50 cm)
- Cylinders are infinitely long
- Different materials (PMMA, water, polyethylene)
 Different regions of integration in the phantom



Monte Carlo: quantum noise and collection volume





Beam Geometry



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Dose versus position: regional differences





Dose versus position: material differences differences





Dose versus position: bow tie differences





Dose versus position: spectal differences





Dose versus position: diameter differences





Dose versus position: smaller volumes noisier



DSF: a classic bi-exponential function



DSF: a classic bi-exponential function









DSF: a classic bi-exponential function



Defining the beam profile for width W:



 $DSF(z) = fe^{-\alpha z} + (1-f)e^{-\beta z}$

Defining the beam profile (BP) for width W:





DSF(z) = P(z) + S(z).

$$\text{Dose}(z) = \int_{-\infty}^{+\infty} \text{DSF}(z - z') \Pi(z') dz',$$

where $\Pi(z)$ is a RECT function of width w defined by $\Pi(z) = P_0, \quad z = -w/2 \text{ to } + w/2,$ $\Pi(z) = 0, \quad \text{elsewhere.}$



CT scan of length L for beam width W (helical scan):

 $D(z) = BP(z) \otimes RECT\left[\frac{z}{L}\right]$







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The trouble with CTDI₁₀₀

John M. Boone⁸¹ Departments of Radialogy and Biomedical Engineering, University of California Davis Medical Center, Ellison Building, 4860 Y Street, Suite 3100, Sacramento, California 95817 (Received 1 September 2005; revised 26 October 2006; accepted for publication 6 November 2006; published 20 March 2007)





The trouble with CTDI₁₀₀

trouble with CIDI ₁₀₀			
John M. Boone ⁸¹ Departments of Radiology and Biomedical Engineering, University of California Davis Medical Center, Ellison Building, 4860 Y Street, Suite 3100, Sacramento, California 95817	з	=	$\frac{CTDI_{100}}{CTDI}$
(Received 1 September 2005; revised 26 October 2006; accepted for publication 6 November 2006; mblished 20 March 2007).			CIDI _∞





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- Dose Spread Functions (DSFs) are a useful construct for understanding the distribution of radiation dose during a CT scan in a simple, cylindrical object.
- DSFs provide the basis for a mathematical understanding of CT dose under a limited set of geometrical and scan parameters.
- This work has shown quantitatively the limitations of the CTDIvol metric and results have guided designs for more accurate – yet large – CT dose phantoms.

Dose Spread Functions in CT

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Effective Dose

	o	ICRP 103	Organ	
	urgan boses ↓	↓ ↓	↓ ↓	
Organ	OD (mGy)	W,	ED (mSv)	
Gonads	0.10	0.08	0.008	
Bone marrow	0.10	0.12	0.012	
Colon	0.10	0.12	0.012	
Lung	1.00	0.12	0.120	
Stomach	0.52	0.12	0.062	
Bladder	0.48	0.04	0.019	
Breast	0.15	0.12	0.018	
Liver	1.02	0.04	0.041	
Esophagus	0.00	0.04	0.000	
Thyroid	0.50	0.04	0.020	
Skin	0.10	0.01	0.001	
Bone surface	0.25	0.01	0.002	
Brain	0.00	0.01	0.000	
Salivary Glands	0.00	0.01	0.000	Total
remainder	0.05	0.12	0.006	
arbitrary examples			0.32 mSv	¥