

IMAGE RECONSTRUCTION AND ARTIFACT REDUCTION

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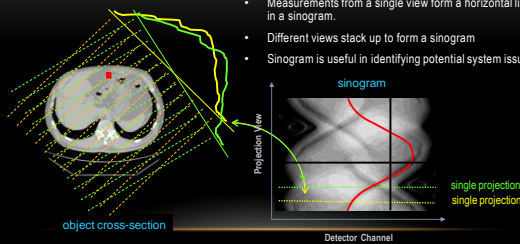
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1

SINOGRAM

- Measurements from a single view form a horizontal line in a sinogram.
- Different views stack up to form a sinogram
- Sinogram is useful in identifying potential system issues

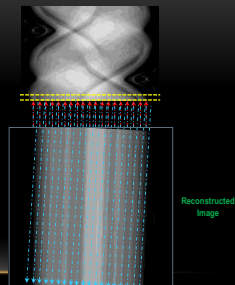


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2

INTUITIVE RECONSTRUCTION

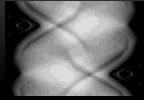
- Each measurement in the sinogram is generated by x-ray attenuated along a line
- Every point along the path has equal probability of contributing to the measurement
- The entire path is "painted" evenly with the measured intensity
- The process is repeated for all views with overlay
- This process is called "backprojection"



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Blurry effect can be compensated for by "deconvolution" in either image or sinogram
Sinogram "deconvolution" is a ramp shaped filter in frequency domain
Combined with backprojection, the process is called "filtered backprojection"



Original
Sinogram

Reconstructed
Image

$$f(x,y,z) = \int \frac{R^2}{L^2(x,y,\beta)} w(\gamma, \beta, \alpha) \int h(\gamma - \gamma') p(\gamma, \beta, \alpha) d\gamma d\beta$$

[illegible]

- Rectangular window can be modified to shape the frequency response.
- Different cutoff frequencies to create different reconstruction kernels.

[illegible]

- Higher frequency generally lead to sharper but noisier image
- For FBP, there is a tradeoff between spatial resolution and noise



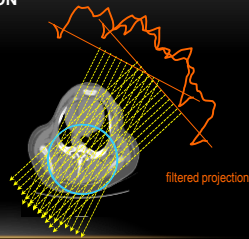
Standard

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[illegible]

TARGETED RECONSTRUCTION

- Clinical interests sometimes focus only on a small region inside the object
- If the ROI is smaller than scan FOV, backprojection can be performed over a portion of the filtered projection to form a targeted reconstruction.



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7

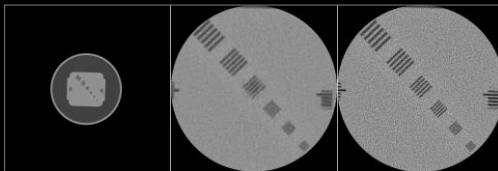
TARGETED RECONSTRUCTION

- Image pixel size changes linearly on the reconstruction FOV.
- Targeted reconstruction can result in better spatial resolution.

Recon at 50cm FOV

Interpolated to 10cm FOV

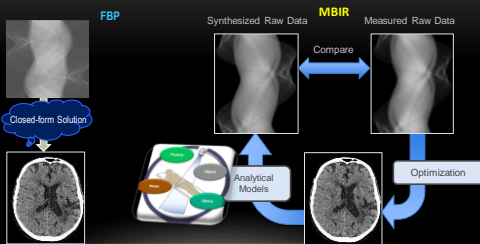
Recon at 10cm FOV



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8

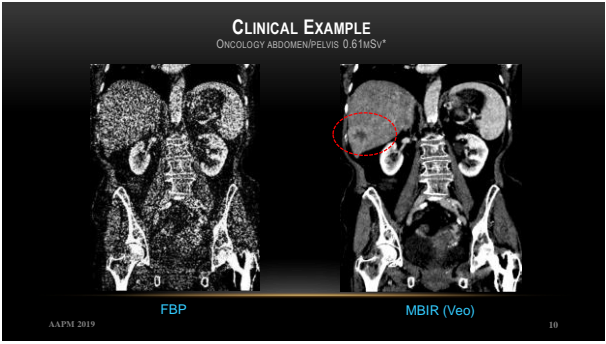
MODEL-BASED ITERATIVE RECONSTRUCTION (MBIR)

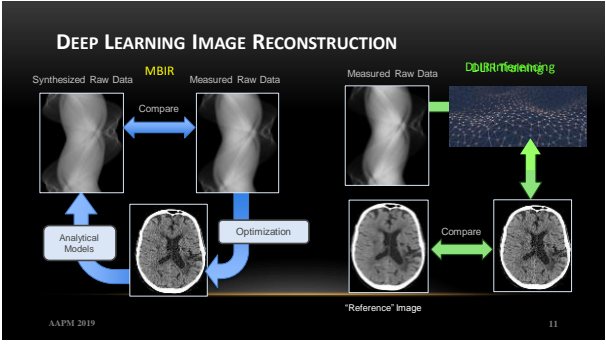


$$f(x,y,a) = \int_{\mathcal{D}(x,y)} w(y,\beta,a) \int h(y-y') p(y,\beta,a) dy' d\beta$$

$$\hat{x}_{MBIR} = \arg \max_x (P(x/y))$$

9







EXTENDED FOV RECONSTRUCTION FOV

- For RT applications, desired FOV is larger than the detector SFOV
- Conventional technology often fails to produce accurate patient skin line
- DL-based algorithm can improve the outcome



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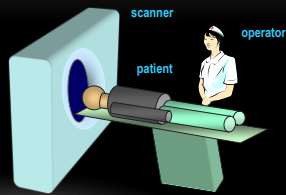
Conventional Extended FOV

DL-based Extended FOV

13

IMAGE ARTIFACTS

- Nature of the X-ray Physics
 - Beam Hardening
 - Scatter
 - ...
- Limitations of CT Technology
 - Helical
 - Cone Beam
 - ...
- Patient-induced
 - Motion
 - Photon Starvation
 - ...
- Operator-induced
 - Suboptimal protocols
 - Patient positioning
 - ...

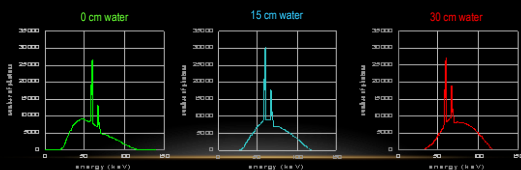
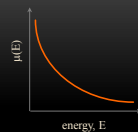


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14

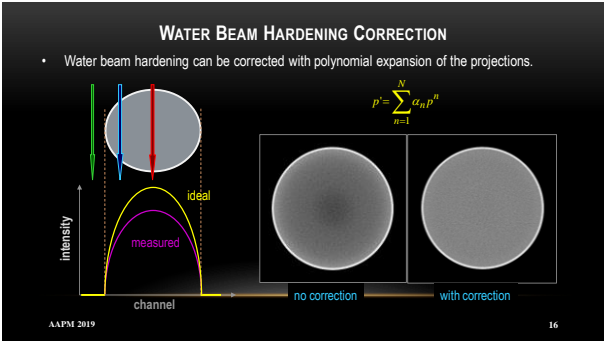
NATURE OF PHYSICS: BEAM HARDENING

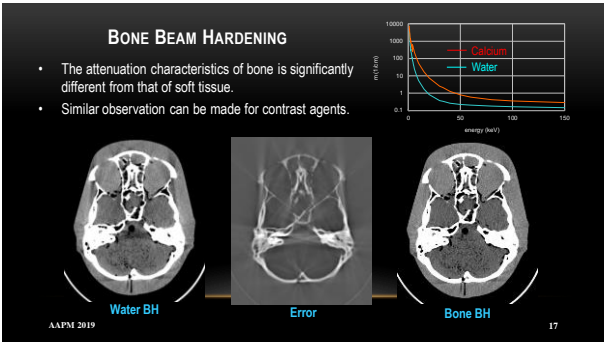
- X-ray photons in CT are poly-energetic.
- The attenuation, $\mu(E)$, is energy-dependent.
- The path length changes in objects
- The measured projection is not line integral of μ .

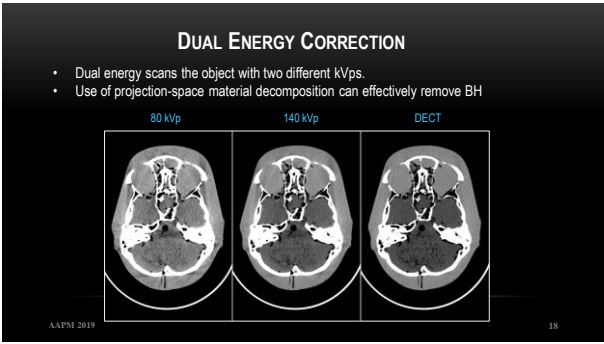


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15





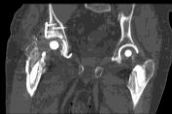


METAL ARTIFACT REDUCTION (MAR)

- Metal inside patient body is a major source of artifact
- Metal objects induce beam-hardening and photon starvation
- MAR algorithm is an iterative correction approach to restore soft-tissue in the image



without MAR



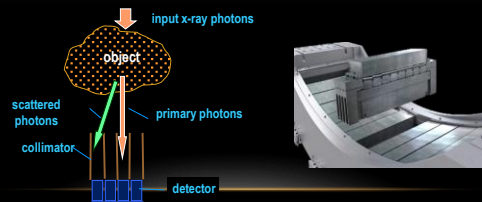
with MAR

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19

SCATTER

- Scatter increases with exposure volume.
- Post patient collimator can be used effectively to reject the scatter.
- A small portion of the scattered radiation can reach the detector.

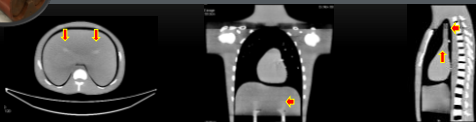


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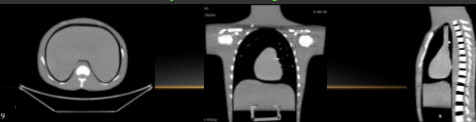
20

PHANTOM TEST

160mm System with 1D Collimator



160mm System with Focusing 2D Collimator

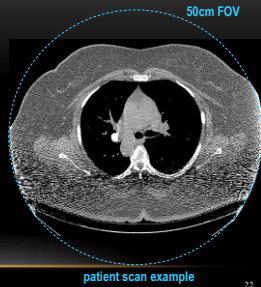


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PHOTON STARVATION

- The amount of attenuation increases exponentially with path length.
- $$\frac{I}{I_0} = e^{-\mu x}$$
- At low signal level, the noise in the projection is no longer dominated by the x-ray photon.
 - Convolution filtering operation further amplifies the noise and leads to streak artifacts.



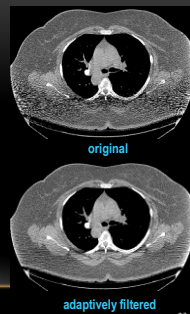
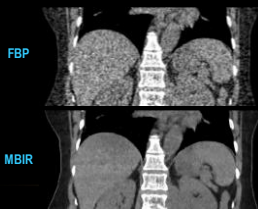
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22

ARTIFACT REDUCTION

Algorithmic Correction

- Adaptive filtering for streak reduction
- Iterative reconstruction

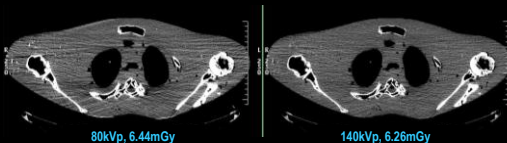
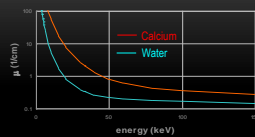


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PROTOCOL OPTIMIZATION

- Scan speed
- Helical pitch
- kVp selection
- Slice thickness
- Reconstruction kernel
- mA modulation

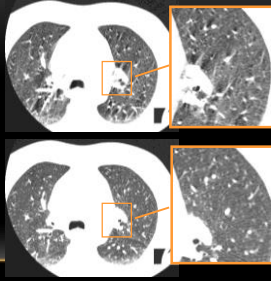


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24

VOLUNTARY MOTION

- Better patient training
- Better instruction
- Faster scan speed
- Advanced algorithm

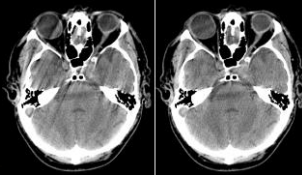


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OPERATOR-INDUCED

- CT operator plays an important role in artifact reduction.
- Improperly secured patient can lead to motion artifact.



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PATIENT CENTERING

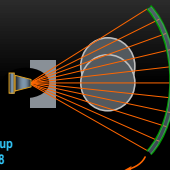
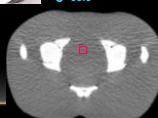
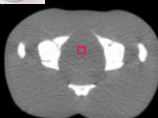
- Bowtie filter is employed in most scanners.
- It assumes centered oval shaped objects.
- Patient centering is important.



centered
 $\sigma=28.8$



10cm up
 $\sigma=53.8$

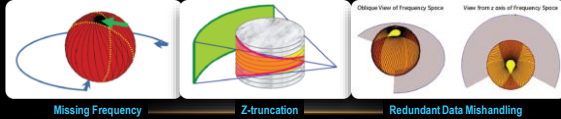


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WIDE-CONE: MATHEMATICAL CHALLENGE

- Axial wide-cone reconstruction faces three major technical challenges:
 - missing frequency (axial mode sampling pattern)
 - z-truncation (cone-beam geometry)
 - redundant data handling (half-scan to improve temporal resolution)
- Solution to these challenges requires extensive research and testing.



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28

ALGORITHM COMPARISON

Traditional Reconstruction

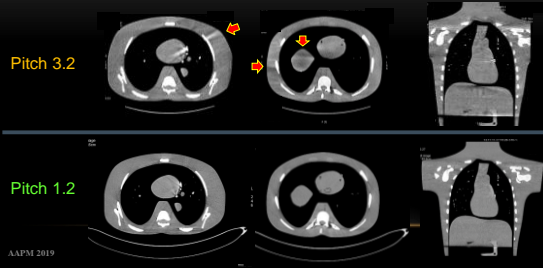


Advanced Reconstruction



HIGH HELICAL PITCH IMPACT

- When helical pitch is too large, incomplete sample can induce image artifacts



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SUMMARY

- Three generations of reconstruction algorithm
 - Filtered backprojection (FBP)
 - Iterative reconstruction (IR)
 - Deep-learning image reconstruction (DLIR)
- Many sources of CT artifacts
 - Nature of Physics
 - New Technologies
 - Patient
 - Operator
- It takes a combined efforts from manufactures, CT operators, and patients to obtain the best image quality.

Thank You!
