

## Detectors for small field and relative dosimetry

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McGill University




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## Disclosures

- My work is supported in part by the Canadian Institutes of Health Research, the Natural Sciences and Engineering Research Council, Canada through operating grants and training grants.
- I am working with Sun Nuclear Corporation and Lifeline Software Inc on technology commercialization projects
- I am working with Reflexion Medical on a nonstandard field dosimetry project
- I am a founding advisor of Gray Oncology Solutions, Inc

• Some brand names of commercial products may be mentioned in this presentation. This does not represent any endorsement of one product or manufacturer over another



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## Content

- Reference fields and small fields
  - Nonstandard reference field calibration
  - Some post-TRS483 comments
- Small field dosimetry
  - Characteristics of suitable detectors
  - Unanswered questions



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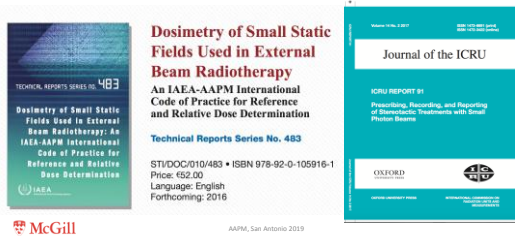
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Two important reports came out in 2017



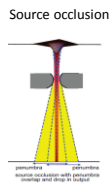
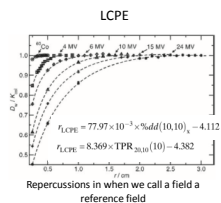
## Dosimetry of nonstandard and small fields

- Characteristics that lead to dosimetric issues of two kinds:
  - Reference dose calibration
    - Reference fields are not  $10 \times 10 \text{ cm}^2$ , SSD/SAD is not 100 cm, etc; they are called "machine-specific reference fields" (msr)
    - Flattening filter-free beams, beam quality specification
  - Output factors
    - Small fields
    - Detector correction factors
- Problem put on the backburner: calibration of composite fields

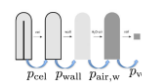


## Physics of small fields

Small field conditions

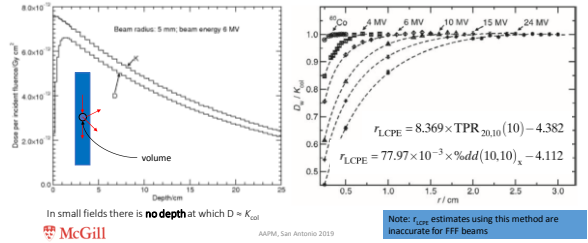


Detector correction factors



Repercussions in how we determine dose in a small field

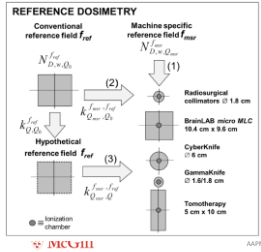
Lateral charged particle loss



Reference calibration fields



Concept of the *msr* field



$$D'_{w,Q_{ref}} = M'_{Q_{ref}} \cdot N'_{D,w,Q_{ref}} \quad \text{Route 1}$$
$$D'_{w,Q_{ref}} = M'_{Q_{ref}} \cdot N'_{D,w,Q_{ref}} \cdot K'_{Q,Q_{ref}} \cdot f_{ref} \cdot 10 \times 10 \text{ cm}^2 \quad \text{Route 2}$$
$$D'_{w,Q_{ref}} = M'_{Q_{ref}} \cdot N'_{D,w,Q_{ref}} \cdot K'_{Q,Q_{ref}} \cdot K'_{Q_{ref},O} \cdot f_{ref} \quad \text{Route 3}$$



## Getting the beam quality in nonstandard reference fields

for  $\text{TPR}_{20,10}(10) = \text{TPR}_{20,10}$

$$\text{TPR}_{20,10}(10) = \frac{\text{TPR}_{20,10}(S) + c(10-S)}{1 + c(10-S)}$$

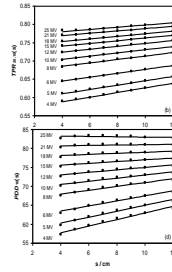
for  $\%dd(10,10) = \%dd(10,10)_x = \%dd(10)_x$

$$\%dd(10,10) = \frac{\%dd(10,S) + 80c(10-S)}{1 + c(10-S)}$$

**Note!** FFF beams → use the Pb filter and equations in TG-51 to get  $\%dd(10,10)_x$



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$$f_{\text{msr}} \geq 6 \times 6 \text{ cm}^2$$

$$f_{\text{msr}} < 6 \times 6 \text{ cm}^2$$

Table 4.2. CHARACTERISTICS OF CYLINDRICAL IONIZATION CHAMBERS SUITABLE FOR REFERENCE DOSIMETRY (FOR  $\text{FSD}_{50} = 100 \text{ cm}$ )

Ionization chamber type <sup>a</sup>	Volume, cm <sup>3</sup>	Radius, cm	Material, mm	Electrode, mm	Wet weight, g
Capintec 0R-01 (0.6 cm <sup>3</sup> )	0.60	0.48	C-101	0.080	0.080
Capintec 0R-02 (0.6 cm <sup>3</sup> )	0.60	0.48	C-101	0.080	0.080
Capintec 0R-03 (0.6 cm <sup>3</sup> )	0.60	0.48	C-101	0.080	0.080
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Capintec 0R-05 (0.6 cm <sup>3</sup> )	0.60	0.48	C-101	0.080	0.080
Capintec 0R-06 (0.6 cm <sup>3</sup> )	0.60	0.48	C-101	0.080	0.080
Capintec 0R-07 (0.6 cm <sup>3</sup> )	0.60	0.48	C-101	0.080	0.080
Capintec 0R-08 (0.6 cm <sup>3</sup> )	0.60	0.48	C-101	0.080	0.080
Capintec 0R-09 (0.6 cm <sup>3</sup> )	0.60	0.48	C-101	0.080	0.080
Capintec 0R-10 (0.6 cm <sup>3</sup> )	0.60	0.48	C-101	0.080	0.080
Capintec 0R-11 (0.6 cm <sup>3</sup> )	0.60	0.48	C-101	0.080	0.080
Capintec 0R-12 (0.6 cm <sup>3</sup> )	0.60	0.48	C-101	0.080	0.080
Capintec 0R-13 (0.6 cm <sup>3</sup> )	0.60	0.48	C-101	0.080	0.080
Capintec 0R-14 (0.6 cm <sup>3</sup> )	0.60	0.48	C-101	0.080	0.080
Capintec 0R-15 (0.6 cm <sup>3</sup> )	0.60	0.48	C-101	0.080	0.080
Capintec 0R-16 (0.6 cm <sup>3</sup> )	0.60	0.48	C-101	0.080	0.080
Capintec 0R-17 (0.6 cm <sup>3</sup> )	0.60	0.48	C-101	0.080	0.080
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Capintec 0R-19 (0.6 cm <sup>3</sup> )	0.60	0.48	C-101	0.080	0.080
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Capintec 0R-24 (0.6 cm <sup>3</sup> )	0.60	0.48	C-101	0.080	0.080
Capintec 0R-25 (0.6 cm <sup>3</sup> )	0.60	0.48	C-101	0.080	0.080
Capintec 0R-26 (0.6 cm <sup>3</sup> )	0.60	0.48	C-101	0.080	0.080
Capintec 0R-27 (0.6 cm <sup>3</sup> )	0.60	0.48	C-101	0.080	0.080
Capintec 0R-28 (0.6 cm <sup>3</sup> )	0.60	0.48	C-101	0.080	0.080
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Capintec 0R-36 (0.6 cm <sup>3</sup> )	0.60	0.48	C-101	0.080	0.080
Capintec 0R-37 (0.6 cm <sup>3</sup> )	0.60	0.48	C-101	0.080	0.080
Capintec 0R-38 (0.6 cm <sup>3</sup> )	0.60	0.48	C-101	0.080	0.080
Capintec 0R-39 (0.6 cm <sup>3</sup> )	0.60	0.48	C-101	0.080	0.080
Capintec 0R-40 (0.6 cm <sup>3</sup> )	0.60	0.48	C-101	0.080	0.080
Capintec 0R-41 (0.6 cm <sup>3</sup> )	0.60	0.48	C-101	0.080	0.080
Capintec 0R-42 (0.6 cm <sup>3</sup> )	0.60	0.48	C-101	0.080	0.080
Capintec 0R-43 (0.6 cm <sup>3</sup> )	0.60	0.48	C-101	0.080	0.080
Capintec 0R-44 (0.6 cm <sup>3</sup> )	0.60	0.48	C-101	0.080	0.080
Capintec 0R-45 (0.6 cm <sup>3</sup> )	0.60	0.48	C-101	0.080	0.080
Capintec 0R-46 (0.6 cm <sup>3</sup> )	0.60	0.48	C-101	0.080	0.080
Capintec 0R-47 (0.6 cm <sup>3</sup> )	0.60	0.48	C-101	0.080	0.080
Capintec 0R-48 (0.6 cm <sup>3</sup> )	0.60	0.48	C-101	0.080	0.080
Capintec 0R-49 (0.6 cm <sup>3</sup> )	0.60	0.48	C-101	0.080	0.080
Capintec 0R-50 (0.6 cm <sup>3</sup> )	0.60	0.48	C-101	0.080	0.080

Table 4.3. CHARACTERISTICS OF IONIZATION CHAMBERS SUITABLE FOR REFERENCE DOSIMETRY OF non FFF BEAMS ( $\text{FSD}_{50} = 100 \text{ cm}$ )

Ionization chamber type <sup>a</sup>	Volume, cm <sup>3</sup>	Length, cm	Radius, cm	Material, mm	Electrode, mm	Wet weight, g
Capintec 0R-01 (0.6 cm <sup>3</sup> )	0.60	0.48	0.48	C-101	0.080	0.080
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Capintec 0R-08 (0.6 cm <sup>3</sup> )	0.60	0.48	0.48	C-101	0.080	0.080
Capintec 0R-09 (0.6 cm <sup>3</sup> )	0.60	0.48	0.48	C-101	0.080	0.080
Capintec 0R-10 (0.6 cm <sup>3</sup> )	0.60	0.48	0.48	C-101	0.080	0.080
Capintec 0R-11 (0.6 cm <sup>3</sup> )	0.60	0.48	0.48	C-101	0.080	0.080
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Capintec 0R-45 (0.6 cm <sup>3</sup> )	0.60	0.48	0.48	C-101	0.080	0.080
Capintec 0R-46 (0.6 cm <sup>3</sup> )	0.60	0.48	0.48	C-101	0.080	0.080
Capintec 0R-47 (0.6 cm <sup>3</sup> )	0.60	0.48	0.48	C-101	0.080	0.080
Capintec 0R-48 (0.6 cm <sup>3</sup> )	0.60	0.48	0.48	C-101	0.080	0.080
Capintec 0R-49 (0.6 cm <sup>3</sup> )	0.60	0.48	0.48	C-101	0.080	0.080
Capintec 0R-50 (0.6 cm <sup>3</sup> )	0.60	0.48	0.48	C-101	0.080	0.080

$$r_{\text{LCPE}}/\text{cm} = 8.369 \cdot \text{TPR}_{20,10}(10) - 4.382$$

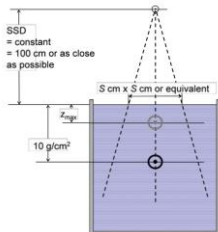
$$r_{\text{LCPE}}/\text{cm} = 0.07797 \cdot \%dd(10)_x - 4.112$$

$$\text{FWHM} \geq 2 r_{\text{LCPE}} + d$$



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## Practical implementation $\text{msr}$ dosimetry – beam quality index



**Note!** FFF beams → use the Pb filter and equations in TG-51 to get  $\%dd(10,10)_x$

$$\%dd(10,10) = \%dd^{\text{SSD}}(10,10) \times \frac{\text{TMR}(10,11)}{\text{TMR}(10, \text{SSD} + 10)} \times \frac{\text{NPSF}(11)}{\text{NPSF}(\text{SSD} + 10)} \times \left( \frac{100 + 2 \cdot \text{SSD} + 10}{110 \cdot \text{SSD} + 2 \cdot \text{SSD}} \right)^2$$

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In summary

Get  $N_{D,w,Q_0}(Co)$

For the beam of interest:

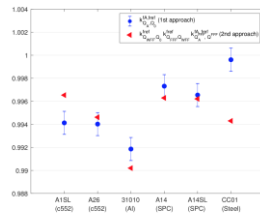
- Get equivalent square  $S$
- Measure the  $\%dd(10,S)$  (if FFF: use lead filter!)
- use conversion formula for SSD, Pb, S to get  $\%dd_x(10,10)$
- Look up  $k_{Q,Q_0}^{f_{ref}}$  or  $k_{Q_{msr},Q_0}^{f_{msr},f_{ref}}$

$$D_{w,Q_{msr}}^{f_{msr}} = M_{Q_{msr}}^{f_{msr}} N_{D,w,Q_0}^{f_{ref}} \underbrace{k_{Q,Q_0}^{f_{ref}} k_{Q_{msr},Q_0}^{f_{msr},f_{ref}}}_{k_{Q_{msr},Q_0}^{f_{msr},f_{ref}}}$$

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What to do when largest field size is not  $msr$ ?



RefleXion

- Reference dosimetry field size ( $10 \times 2 \text{ cm}^2$ )
- SDD = 85 cm
- $2r_{LCPe} + d > FWHM$
- Two approaches
  - Direct MC calculation
  - $k_{Q_{msr},Q_0}^{f_{msr},f_{ref}}$

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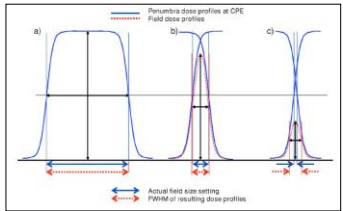
$10 \times 2 \text{ cm}^2$  field size  
Mirzakhani et al 2019 (submitted)

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Small fields and detectors

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Source occlusion



Das et al. 2008 Med Phys **35**: 206-15  
Overlapping of beam penumbra  
McGill AAPM, San Antonio 2019

FWHM > geometric field size

Small field dosimetry-related parameters must be specified as a function of FWHM

Field size specification  $S_{clin}$

$$S_{clin} = \sqrt{A \cdot B}$$
$$0.7 < A/B < 1.4$$
$$S_{clin} = r \cdot \sqrt{\pi}$$

981 Casar et al. Relative dosimetry of small static fields 981

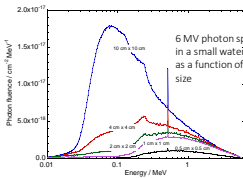
TABLE II. Nominal field sizes and corresponding equivalent square small field sizes  $S_{eq}$  on the Elekta Versa HD and Varian TrueBeam linacs measured with EBT3 films and applying Eq. (3).

Nominal square field side length (cm)	$S_{eq}$ (cm) — Elekta Versa HD				$S_{eq}$ (cm) — Varian TrueBeam			
	6 MV WFF	6 MV FFF	10 MV WFF	10 MV FFF	6 MV WFF	6 MV FFF	10 MV WFF	10 MV FFF
0.5	0.60	0.59	0.62	0.58	0.56	0.54	0.57	0.55
0.8	0.87	0.85	0.87	0.86	0.81	0.82	0.84	0.81
1.0	1.03	1.03	1.06	1.04	1.01	0.99	1.03	1.02
1.5	1.51	1.52	1.55	1.52	1.50	1.49	1.52	1.51
2.0	2.04	2.03	2.05	2.04	2.00	1.99	2.01	1.99
3.0	3.06	3.04	3.08	3.02	3.03	3.00	3.00	2.98
4.0	4.04	4.03	4.06	4.01	4.03	3.99	4.02	3.98
5.0	5.04	5.01	5.05	4.99	5.02	5.00	5.01	4.96
10.0	10.04	9.94	10.05	9.90	10.03	9.96	10.02	9.87

McGill AAPM, San Antonio 2019 Casar et al Med. Phys. (2019) 46 (2), 944

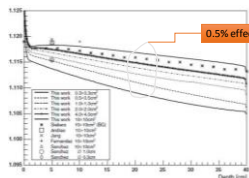
Spectral changes

- The photon fluence spectrum is modified as a function of field size



Bennakhlouf Sempau Andreo Med. Phys. **41** (2014)

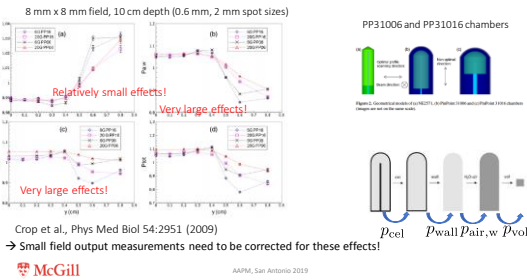
McGill



Spectral hardening does not lead to large changes in stopping power ratio! Eklund and Ahnesjö, Phys Med Biol **53**:4231 (2008)



Magnitude of  $p$  correction factors on- and off-axis



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Concept of field output correction factors

- Field output factor relative to reference field (ref stands here for a conventional reference or msr field)
- $$\Omega_{Q_{ms}, Q_{ref}}^{f_{ms}, f_{ref}} = \frac{M_{Q_{ms}}^{f_{ms}}}{M_{Q_{ref}}^{f_{ref}}} \cdot k_{Q_{ms}, Q_{ref}}^{f_{ms}, f_{ref}}$$
- Output factors are DOSE RATIOS not reading ratios!!
- Field output factor relative to reference field using intermediate field or 'daisy chaining' method
- $$\Omega_{Q_{ms}, Q_{ref}}^{f_{ms}, f_{ref}} = \frac{M_{Q_{ms}}^{f_{ms}}}{M_{Q_{ref}}^{f_{ref}}} \cdot \frac{M_{Q_{ref}}^{f_{ref}}}{M_{Q_{int}}^{f_{ref}}} \cdot K_{Q_{ms}, Q_{ref}}^{f_{ms}, f_{ref}}$$
- where
- $$K_{Q_{ms}, Q_{ref}}^{f_{ms}, f_{ref}} = k_{Q_{ms}, Q_{ref}}^{f_{ms}, f_{ref}} \cdot k_{Q_{ref}, Q_{int}}^{f_{ref}, f_{int}}(IC)$$

McGill

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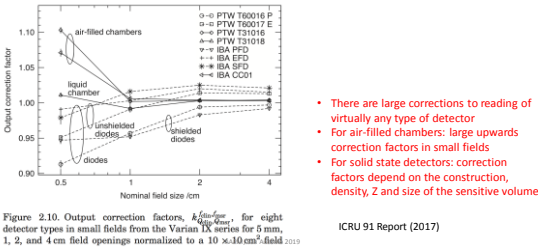
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Small field output correction factors



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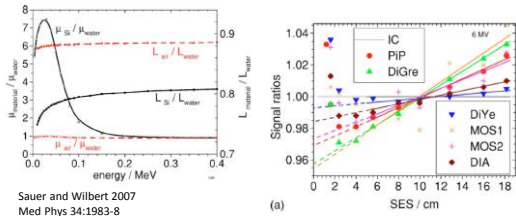
Detector suitability criteria for small fields

- There is no ideal detector
- Suitability in general is tied to
  - the sensitive region of the detector is close to water equivalent in terms of radiation absorption characteristics;
  - the density of the sensitive region is close to the density of water;
  - the size of the sensitive region can be made small compared to the field size while keeping noise levels under control.



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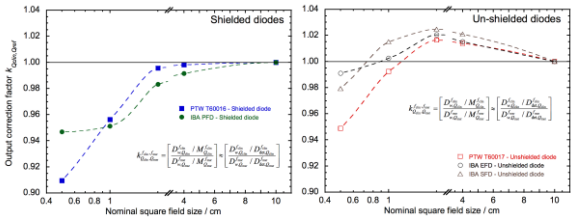
Diodes for small field dosimetry



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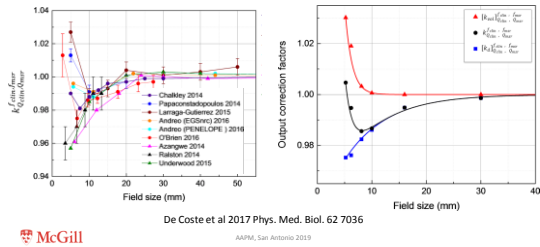
Shielded and unshielded diodes



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Benmahklouf and Andreo (2013)

Microdiamond detector



Small field correction factor issues

Table XII. Statistical significance ( $P$ -values) of differences between output correction factors  $k_{out,cor}$  for PTW 60019 nD detector given in TRS-483 and the corresponding values from this study evaluated with a one-sided Student's  $t$ -test. Data for 6- and 10-MV beams from TRS-483 were compared with data from this study for both filtered (FFF) and unfiltered (FFU) 6- and 10-MV beams on the Elekta Versa HD line.

Field size (cm)	Elekta Versa HD			
	6 MV FFF	6 MV FFU	10 MV FFF	10 MV FFU
PTW 60019 nD				
0.5	0.001	0.003	0.001	0.001
0.8	0.027	0.025	0.001	0.004
1.0	0.034	0.034	0.002	0.003
1.5	0.079	0.059	0.006	0.027
2.0	0.118	0.042	0.023	0.031

\*Field size is indicated as the nominal square field side length. The relationship between the nominal field size and the corresponding equivalent square field sizes  $E_{sq}$  is provided in Table I for all energies and field sizes.

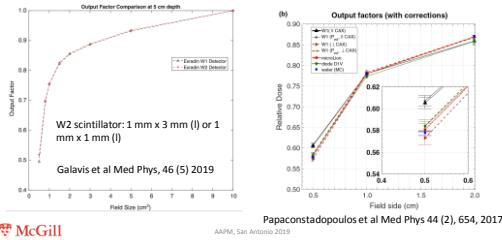
Casas et al Med. Phys. (2019) 46 (2), 944



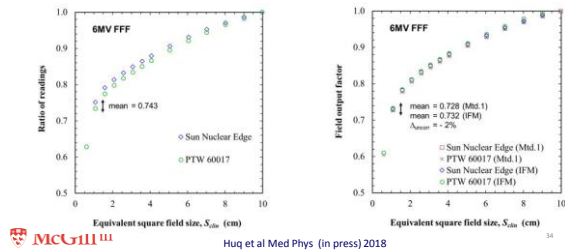
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- The correction factors are likely energy dependent
- Detailed geometry is critical for MC simulations
- SN EDGE detector below 2 cm in 10 MV FFF beam significantly different from IAEA-AAPM 483
- See left panel for similar differences with PTW microdiamond

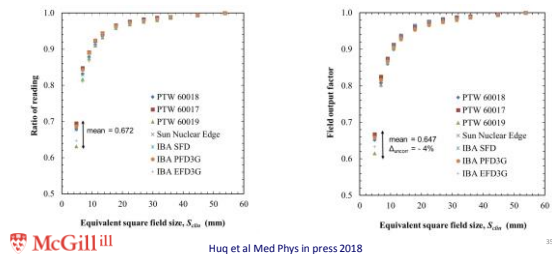
Scintillators W1 and W2



## Field output factor (TrueBeam STx)



## Field output factor (CyberKnife)



## Conclusion

- IAEA-AAPM TRS-483 has significantly improved consistency in small field dosimetry
  - The use of more than a single detector to quantify small field output factors is recommended
  - Accelerators are getting increasingly reproducible. It makes therefore sense to compare output factors of a given machine with those of a similar machine
- Post IAEA-AAPM TRS483
  - New machines will come to the market that invalidate nonstandard field conditions
  - The last word about so-called promising detectors has not yet been said
  - Small field dosimetry for field sizes below  $1 \times 1 \text{ cm}^2$  remains challenging