

Listening to Cell Membrane Potential: a new diagnostic and interventional ultrasound imaging approach

Emad M. Doctor, Ph.D.

Assistant Professor of Radiology,
Computer Science, and Electrical Engineering Departments

Director of the Medical Ultrasound Imaging and Intervention Collaboration
(MUSiiC) Research Laboratory

Collaborators: Arthur Burnett, Peter Gehlbach, Maged Harraz, Jin Kang,
Dean Wong, Arman Rahmim, Les Loew
MUSiiC Lab Members: Jesun Kang, Kai Zhang

July 16th 2019



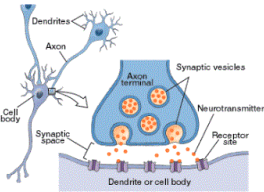
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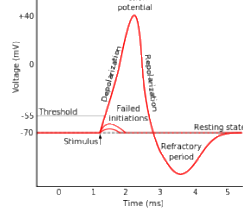
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Neuro-transmitter (NT) and electrophysiological change



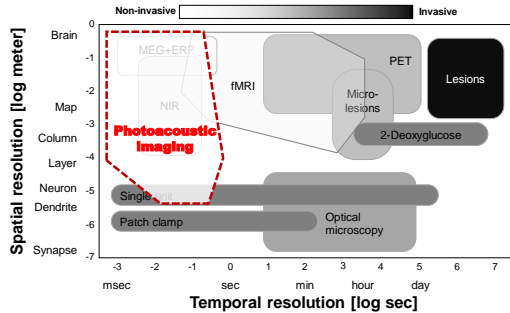
- Action potential; clue of NT event
 - msec time scale
 - -70~40 mV voltage change



1. Synthesis of the neurotransmitter. This can take place in the cell body, in the axon, or in the axon terminal.
2. Storage of the neurotransmitter in storage granules or vesicles in the axon terminal.
3. Calcium enters the axon terminal during an action potential, causing release of the neurotransmitter into the synaptic cleft.
4. After its release, the transmitter binds to and activates a receptor in the postsynaptic membrane.
5. Deactivation of the neurotransmitter. The neurotransmitter is either destroyed enzymatically, or taken back into the terminal from which it came, where it can be reused, or degraded and removed.

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Functional neuro-sensing

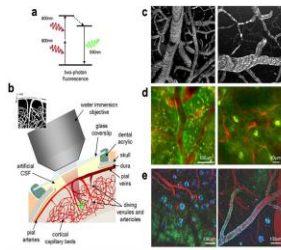


Reproduced from Cohen M. S. and Bookheimer S. Y., *Trends Neurosci* 17(7), 268-77 (1994).

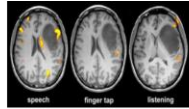
† Wang L. V. and Song H., *Science* 335(3075), 1458-1462 (2012).

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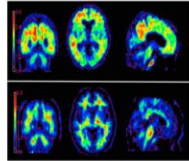
Functional neuro-imaging



Optical imaging (e.g., two-photon microscopy): shallow imaging depth due to diffraction limit (< 1mm), necessitates craniotomy to have sufficient sensitivity

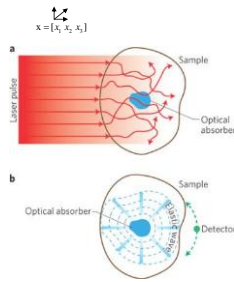


fMRI: only provide contrast based on blood oxygen-level dependent (BOLD) signals



PET: low temporal resolution (> 40min)

Photoacoustic effect

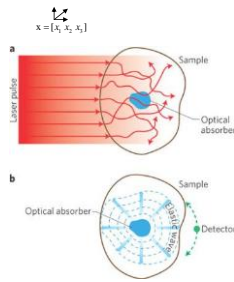


Equation of state
 → Temperature T , density ρ , pressure p
 (In fluid with homogeneous thermodynamic property)
 $\frac{\partial p}{\partial t} = \frac{1}{\rho k_T} \frac{\partial p}{\partial t} + \frac{\beta}{k_T} \frac{\partial T}{\partial t}$
 ρ : mass density [kg/m^3]
 k_T : isothermal compressibility [$\Delta V/V$]
 β : volume thermal expansivity of the fluid [$\Delta V/(V \cdot K)$]

Heat equation
 $\rho C \frac{\partial T}{\partial t} = -\chi \nabla^2 T + H(x) f(t)$
 χ : Thermal conductivity [$\text{W}/(\text{m} \cdot \text{K})$]
 C : Heat capacity at constant volume [$\text{J}/(\text{kg} \cdot \text{K})$]
 $H(x)$: Absorbed energy density [J/m^3]
 $f(t)$: temporal pulse shape function with unit integral [$1/s$]

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Photoacoustic effect



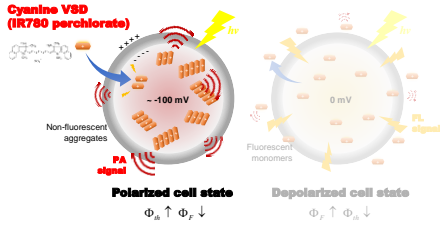
$\frac{\partial p}{\partial t} = \frac{1}{\rho k_T} \frac{\partial p}{\partial t} + \frac{\beta}{k_T} \frac{\partial T}{\partial t}$ **Equation of state**
 ↓ **stress confinement (-ns)**
 Isochoric condition (fixed volume)
 $\frac{\partial p}{\partial t} = \frac{\beta}{k_T} \frac{\partial T}{\partial t}$
 ↓ **Heat equation**
 $\rho C \frac{\partial T}{\partial t} = \chi \nabla^2 T + H(x) f(t) \Rightarrow \frac{\partial T}{\partial t} = \frac{1}{\rho C} \nabla^2 H(x) f(t)$
 ↓ **thermal confinement (-µs)**
 → Heat delivery faster than conductive heat diffusion
 $\frac{\partial p}{\partial t} = \frac{\beta}{\rho C k_T} H(x) f(t)$
 ↓ **Integral over short pulse duration**
 $p_0 = \frac{\beta}{\rho C k_T} H(x) = \Gamma H(x) = \Gamma \mu_a \Phi(x)$

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Towards sensing electrophysiological activity in deep brain

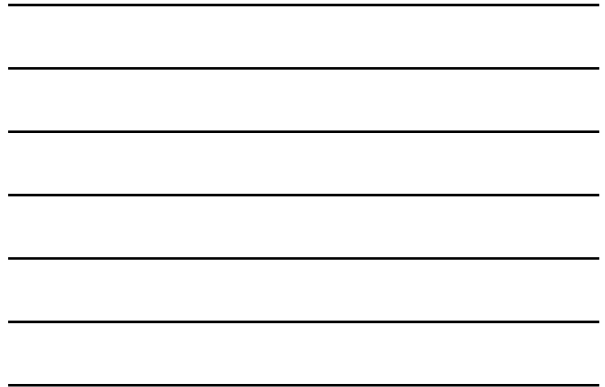


- Objective: real-time, transcranial photoacoustic (PA) sensing of electrophysiological brain activity at deep rat brain *in vivo*
- Voltage-sensing mechanism using near-infrared cyanine dye □



- Cyanine dye with positive polarity is attracted into cell membrane
- The aggregation of VSD leads to fluorescence (FL) quenching, which increases PA generation efficiency

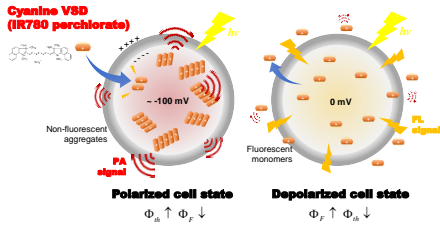
□ Zhang, H. K. et al. *J. Biomed. Opt.* 22, 045006 (2017).



Towards sensing electrophysiological activity in deep brain



- Objective: real-time, transcranial photoacoustic (PA) sensing of electrophysiological brain activity at deep rat brain *in vivo*
- Voltage-sensing mechanism using near-infrared cyanine dye □



- Dispersion of VSD gives high FL efficiency

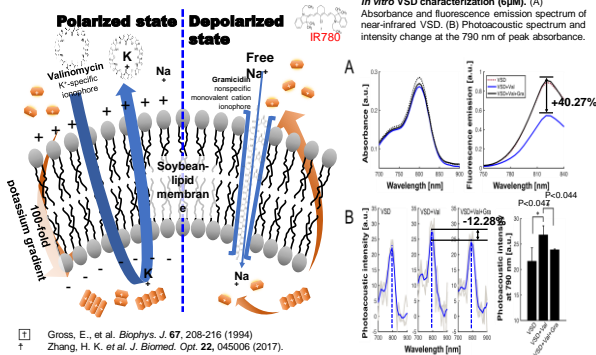
□ Zhang, H. K. et al. *J. Biomed. Opt.* 22, 045006 (2017).



VSD characterization using artificial membrane potential model



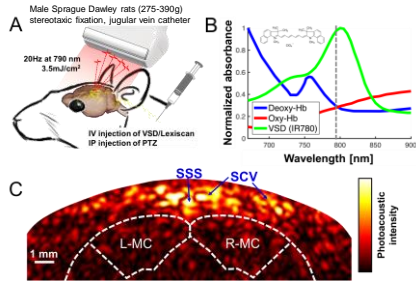
- Artificial membrane diffusion potential model □



□ Gross, E. et al. *Biophys. J.* 67, 208-216 (1994)
 □ Zhang, H. K. et al. *J. Biomed. Opt.* 22, 045006 (2017).

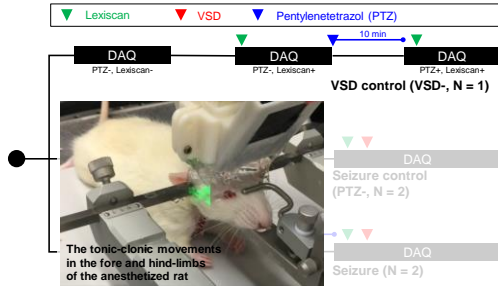


In vivo experimental setup



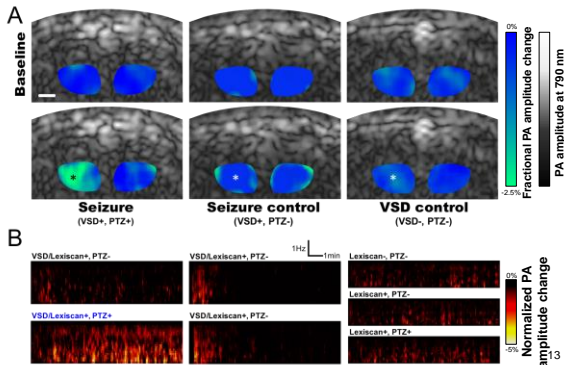
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In vivo experimental protocol

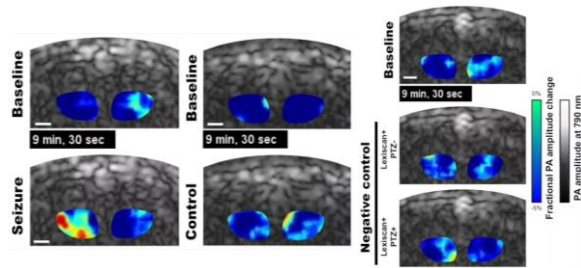


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In vivo photoacoustic VSD imaging

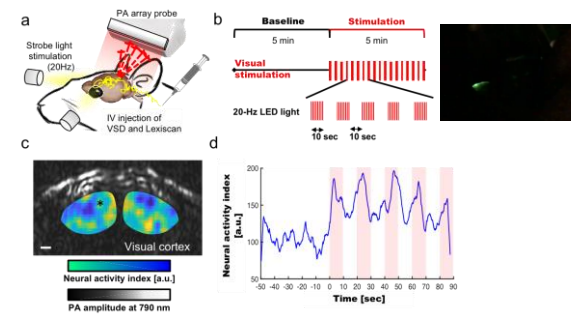


In vivo photoacoustic VSD imaging



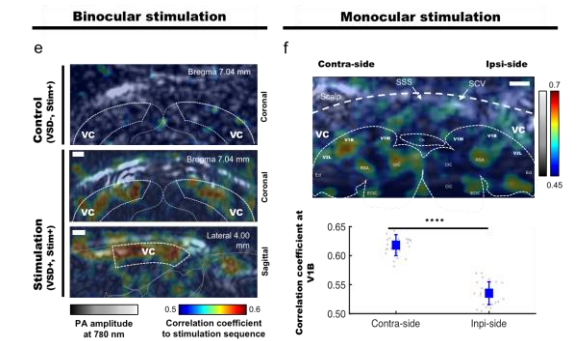
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Visual cortex stimulation and monitoring



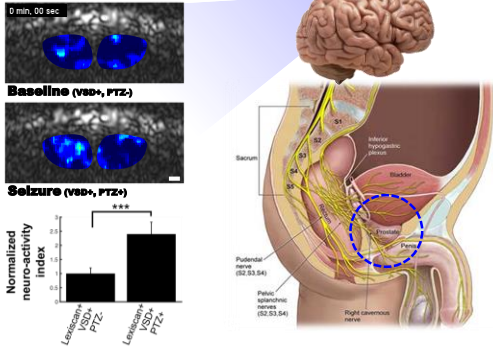
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Visual cortex stimulation and monitoring



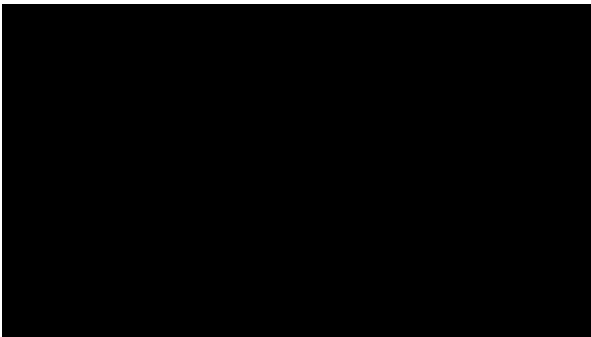
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From Brain to Prostate



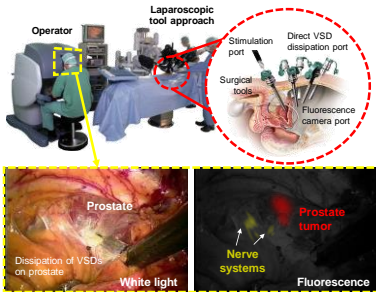
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Need for nerve guidance during peeling out procedure of fascia



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Proposed nerve-guided robot-assisted laparoscopic prostatectomy



- Step 1: Robotic tool approach through the ports on the abdominal incisions.
- Step 2: Direct VSD staining of a prostate tissue through the abdominal incision port.
- Step 3: Flushing out of the VSD on the prostate surface which is not bound at tissue membrane.
- Step 4: Stimulation on nerves in the surgical region-of-interest, and
- Step 5: Nerve-sparing prostatectomy with the augmented nerve map.

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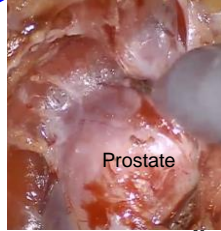
Available time for VSD staining



Dissection of colon adhesions -0:31
Posterior approach with dissection of the seminal vesicles -2:47
Dissection of the anterior abdominal wall-10:50
Opening of the endopelvic fascia and dissection of the periprostatic fat
Suture of the dorsal venous complex
Preservation of neurovascular bundles during left sided dissection
Dissection of the left posterior pedicle -33:20
Apical and urethral dissection -49:01
Evaluation of nerve sparing with the ProPep electrodes -54:14
Vesicourethral anastomosis -55:12
Surgery ended -1:07

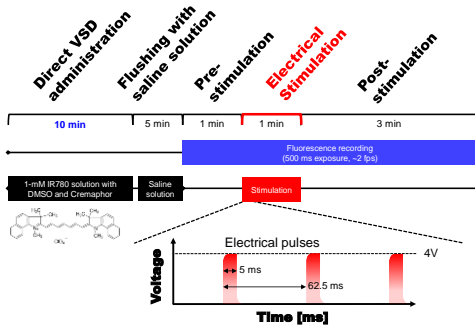
Time point completing exposure of prostate capsuled with periprostatic fascia

8-10 min



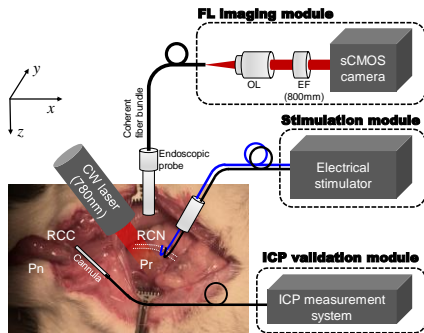
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In vivo experimental protocol



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In vivo experimental setup



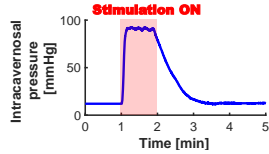
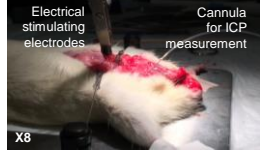
Pr: prostate; Pn: penis; RCN: right cavernous nerve; RCC: right corpus cavernosum
ICP: intracavernous pressure

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Validation of erectile stimulation

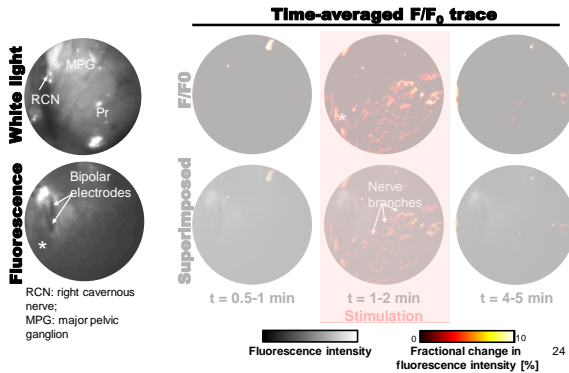


Validation of erectile stimulation



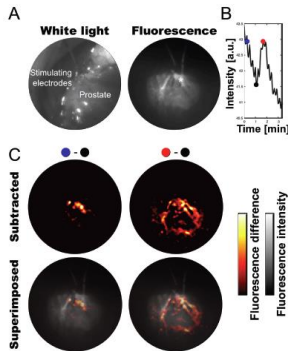
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Real-time prostate nerve mapping in vivo



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Real-time prostate nerve mapping in vivo (2nd attempt)



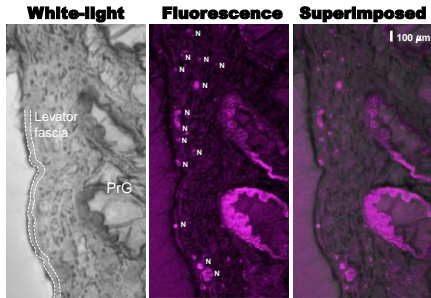
Preliminary *in vivo* results on nerve localization on rat prostate:

- (A) White light and FL images;
- (B) Evolution of FL intensity during stimulation. The gradual decrease is due to photo-bleaching;
- (C) Subtracted images between indicators, and its fusion on FL images.

Histological validation of direct VSD administration



- Confirmed direct staining procedures can deliver VSD > 2-mm deep in prostate

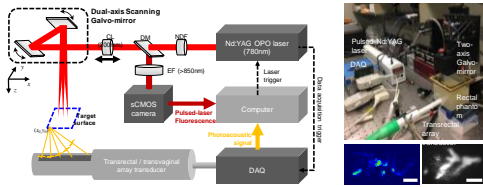


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Discussion



- We presented the preliminary results of real-time nerve guidance using dual-modal VSD and intra-operative FL imaging
- Our further works will be focused on
 - Developing pulsed laser-based dual-modal intra-operative guidance

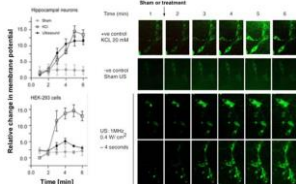


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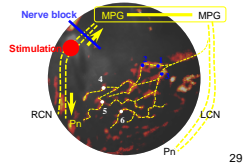


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Discussion



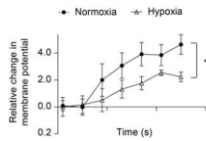
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 - Constructing control group with CN block



Discussion



- We presented the preliminary results of real-time nerve guidance using dual-modal VSD and intra-operative FL imaging
- Our further works will be focused on
 - Developing pulsed laser-based dual-modal intra-operative guidance
 - Integrating non-invasive ultrasound neural stimulation
 - Constructing control group with CN block
 - Evaluating nerve trauma with VSD sensing



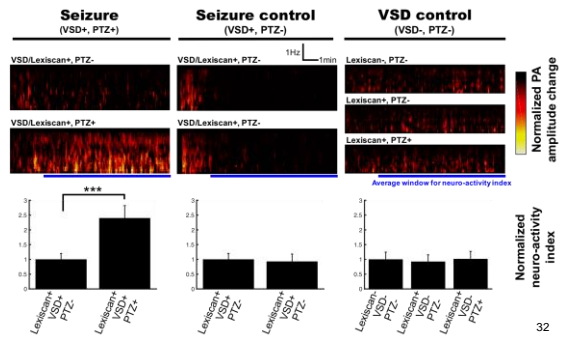
Thank you



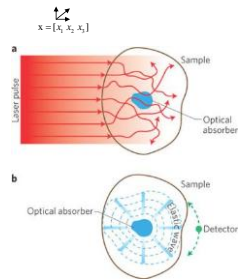
Quantitative comparison



- Normalized neuro-activity index (projected during 2-10 min)



Photoacoustic effect

- **Equation of state**
 → Temperature T , density ρ , pressure p
 (In fluid with homogeneous thermodynamic property)

$$\frac{\partial p}{\partial t} = \frac{1}{\rho k_T} \frac{\partial p}{\partial t} + \frac{\beta}{k_T} \frac{\partial T}{\partial t}$$

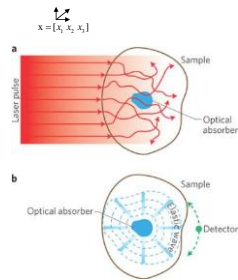
 ρ : mass density [kg/m^3]
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- **Heat equation**

$$\rho C_v \frac{\partial T}{\partial t} = -\chi \nabla^2 T + H(x) f(t)$$

 χ : Thermal conductivity [$\text{W}/(\text{m} \cdot \text{K})$]
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Photoacoustic effect

$$\frac{\partial p}{\partial t} = \frac{1}{\rho k_T} \frac{\partial p}{\partial t} + \frac{\beta}{k_T} \frac{\partial T}{\partial t} \quad \text{Equation of state}$$

↓ stress confinement (-ns)
 Isochoric condition (fixed volume)

$$\frac{\partial p}{\partial t} = \frac{\beta}{k_T} \frac{\partial T}{\partial t} \quad \text{Heat equation}$$

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↓ thermal confinement (-µs)
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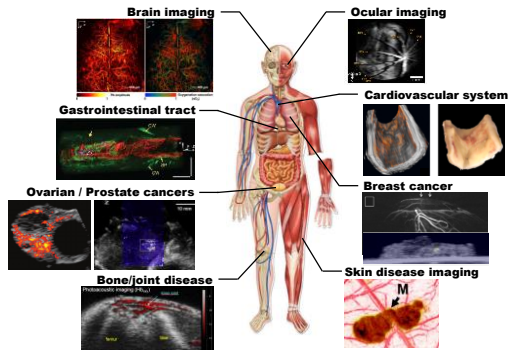
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↓ Integral over short pulse duration

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Clinical applications



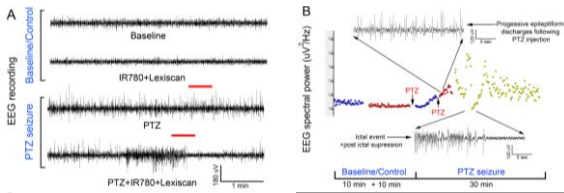
Reproduced from Zackrisson, S., et al., *Cancer Research*, 74(4), 979–1004 (2014)

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EEG confirmation of *In vivo* protocol



- EEG confirmation of seizure induction using PTZ administration



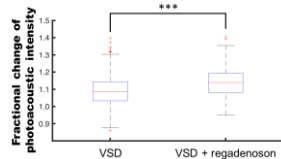
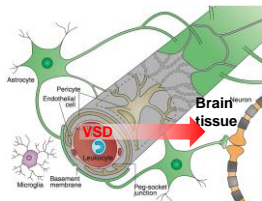
Evolution of EEG signal in the *in vivo* protocol identical to transcranial PA imaging: (A) Representative EEG traces recorded from rat motor cortex before and during induction of status epilepticus using chemoconvulsant PTZ. (B) EEG spectral quantitation of the EEG recording done every 10 sec epoch during the EEG showed the expected progressive rise in EEG power associated with evolution of the PTZ induced status epilepticus.

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Validation of important assumptions



- Pharmacological treatment for BBB opening
 - Blood-brain barrier (BBB): semipermeable membrane barrier separating the circulating blood from the brain in the central nervous system (CNS) ¹
 - Regadenoson (i.e., LexiscanTM) can modulate adenosine receptor signaling to enhance the permeability of VSD through BBB^{1,2}



-5% more PA intensity have observed at motor cortex with the systemically injected Lexiscan and VSD. (N = 2 for each case)

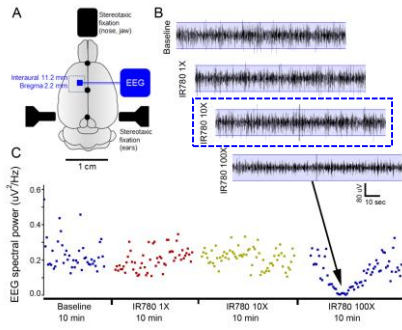
¹ Obermeier B., et al. *Nat. Med. Rev.* 19, 1584-1596 (2013)
² Carman A. J., et al. *J. Neurosci.* 31(37), 13272-80 (2011).
³ Bynoe, M. S., et al., *Fluids Barriers CNS* 12(20) (2015)

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Validation of important assumptions



- Robustness on VSD interference on neuro-activity



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