## Deep Learning Reconstruction Methods for Dosimetry and Acceleration

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#### Overview

#### • What? Why?

- Examples
  - Digital Breast Tomosynthesis reconstruction
    Cone Beam CT reconstruction

  - MRI reconstruction

### Our rationales for deep learning based reconstruction

- Speed (neural networks have fast inference)
  - Real time adaptive MR-guided radiotherapy
    - Lower scan time
       Faster inference (reconstruction)
- · Ability to learn a data manifold
- Dosimetry
   Digital Breast Tomosynthesis
   Cone-beam CT for prefraction adaptation

Reconstruction is an inverse problem



Reconstruction is an inverse problem

$$y = Ax + \eta$$

# **Goal:** find *B* such that $x \approx By$

We will use a neural network for this.



### Deep Learning and Reconstruction

#### · Several approaches can be envisioned

- Standard reconstruction algorithm + deep learning filtering
- Directly from measured data to output
- Model-based, combining learning with model knowledge

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#### Learned postprocessing

Low Dose CT Grand Challenge



Objectives

The overall objective of this Low Dose CT Grand Challenge was to quantitatively assess the diagnostic performance of denoising and iterative reconstruction techniques on common low-dose patient CT datasets using a detection task, allowing the direct comparison of the various algorithms. The results provided an indication of the range of performances achieved using different classes of denoising or iterative reconstruction techniques.

## Learned postprocessing



## Fully learned approach (Automap)



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## Breast Dosimetry



## Digital Breast Tomosynthesis (DBT)









Most deep learning reconstruction methods are *supervised* 

 $\boldsymbol{x} \approx B\boldsymbol{y}$ 

Most deep learning reconstruction methods are *supervised* 

 $\mathbf{x} \approx B\mathbf{y}$ 

Most deep learning reconstruction methods are *supervised* 



Most deep learning reconstruction methods are supervised  $x \approx By$ 

So how to get the ground truth if this is what we have ?







Sechopoulos et al, Medical Physics, 2012, 39(8), 5050-5059



## Learned primal dual (Adler et al. 2018)



m - mask, g - sinograms,  $h_0$  - initial dual vector (zeros),  $f_0$  - initial primal vector (zeros), Out - final reconstruction







Average Glandular Dose

## Amount of energy deposited by x-rays in glandular tissue Amount of glandular tissue

DBT reconstruction for dosimetry



## Cone-beam CT reconstruction



## Goal



## Ground truth





The ASTRA Toolbox
The ASTRA Toolbox
The ASTRA Toolbox an MATAB and Python toolbox of high-performance GPU primitive
and 3D tomography.
We support 2D parallel and too beam generative, and 3D parallel and core beam. All of the
high-finable sourcestaters positioning.

у

# Goal for reconstruction in adaptive radiotherapy

• Proper soft-tissue contrast to target malignant tissue

- Calibrated units for radiotherapy dose calculations
- Needs to scale to clinically relevant sizes, and have fast inference

# This would enable day-by-day adaptive radiotherapy

### Learned SIRT





Model trained on lung CTs Generalizes well

Cone beam geometry reflecting Elekta Synergy with 60 projections



## Generalizes well to real measurements





(b) FBP h=0.8



(d) ISIRT, low model noise (e) ISIRT, model ise (f) ISIRT, patient m high

FBP (no filter)         1.81         0.14           FBP (b=0.8)         3.95         0.27           SIRT (100 iterations)         21.76         0.40           SIRT (250 iterations)         13.67         0.28           SIRT (1000 iterations)         6.67         0.24           SIRT (1000 iterations)         6.70         0.24	Experiment	CNR	FWHM (cm)
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	SIRT (low noise model)	27.16	0.25
SIRT (mid noise model) 33.17 0.24	SIRT (mid noise model)	33.17	0.24
SIRT (high noise model) 34.52 0.22	SIRT (high noise model)	34.52	0.22
SIRT (Patient model) 17.11 0.23	SIRT (Patient model)	17.11	0.23

Generalizes well to real measurements



(a) SIRT 250 iterations (b) ISIRT, highnoise (c) ISIRT, patient model model

## MRI reconstruction







The highest sampled Frequency (Bandwidth) Determines the Image Resolution



High bandwidth

Low bandwidth

#### **MRI** Process

MR samples acquired in the spatial frequency domain, aka. k-space

Proper image is retrieved by sampling at the Nyquist-rate, i.e. "fully sampled"

Scanning time is reduced by acquiring partial measurements

 $\begin{array}{ll} \mbox{Corruption process given by the} \\ \mbox{forward model:} & \mathbf{y} = P \mathscr{F} \mathbf{x} + \mathbf{n} \end{array}$ 





Same story, use deep learning.



# How to speed up? Different sampling, different artefacts



# Recurrent inference machines

Combine convolutional layers
 and GRU cells

 Maintain two internal states
 And T external states (reconstructions)

MSE averaged over all T external states used for training:

$$L\left(\mathbf{x}_{T}\right) = \frac{1}{nT} \sum_{t=1}^{T} \|\mathbf{x}_{t} - \mathbf{x}\|_{2}^{2}$$



Putzky & Welling, IČLR 2017

#### Data Used



1.0mm transversal T1-weighted brain images from 3T scanner





0.6x0.5mm T2-weighted knee images from 3T scanner at all angles http://mridata.org/fullysa mpled/knees



### Model trained on all data, and cross validated

For acceleration factors 2x, 3x, 4x, and 5x on Gaussian distribution

SSIM, NRMSE, and PSNR were used as a metrics of reconstruction quality

Compared with

- U-net postprocessing
- Compressed Sensing



Hyun, arXiv 2017 Lustig, Signal Processing 2008

> 0.6/0.5mm T2w knee

0.7mm T2\*w brain



## RIMs Outperform U-nets for all accelerations



### 5x Accelerated T2w Knee Reconstruction

1.0mm T1-w brain

RIN

U-ne

Trained on:

#### You do not need a lot of data





# Insensitivity to acceleration factor

The RIM and U-net were trained with masks at 4x acceleration

And tested on random acceleration factors sampled from U(1.5, 5.2)





### Ratings by neuroradiologist





Questions?

