#### Calculating and Reporting Absorbed Dose from Radionuclide Therapies



UCSF .

Sara St. James, Ph.D. , DABR Assistant Professor, Radiation Oncology UCSF



### Introduction (to your speaker)

 Assistant Professor of Clinical Radiation Oncology at UCSF







## Disclosures

- No financial disclosures
- I work in therapeutic medical physics



#### Motivation

Patients treated with <sup>177</sup>Lu- DOTATATE at UCSF have a 24 hour post-administration SPECT/CT scan

What dose our patients are receiving?

Is this the right dose for them?







## Motivation

Patients treated with Lu-<sup>177</sup> DOTATATE at UCSF have a 24 hour postadministration SPECT/CT scan

These scans are used qualitatively, but they may be used to calculate the received radiation dose

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UCSF Therapeutic Lu-177 Lutathera Dispensing Checklist

Final Signatures Approving Infusion of Dispensed Activity:

ine Attending

Versian 1: Sep 12, 2016



Image courtesy of Dr. Thomas Hope, UCSF Department of Radiology





Using imaging to determine the received dose to tumors and normal tissues for patients receiving TRT

- Approach
- Validation

#### Dose effects for tumors and normal tissues

- How do we chose to report dose?
- How do we quantify response?

#### Can we use imaging to quantify the tumor response?





177LU-

DOTATATE Examples Patient Selection – The role of pretreatment imaging studies

- Patients can be imaged to see if they have tumors that the RNT is targeting
- Chemistry is identical, except for the substitution of 68Ga for 177Lu
- Examples of this are:
  - <sup>68</sup>Ga-DOTATATE
  - <sup>68</sup>Ga-PSMA PET

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<sup>68</sup>Ga has a 68 minute half-life. This is suitable for diagnostic imaging and patients are typically imaged ~ 1 hour post-administration.

#### SPECIAL CONTRIBUTION

NANETS/SNMMI Procedure Standard for Somatostatin Receptor–Based Peptide Receptor Radionuclide Therapy with <sup>177</sup>Lu-DOTATATE

Thomas A. Hope<sup>1,2</sup>, Amanda Abbott<sup>3</sup>, Karen Colucci<sup>4</sup>, David L. Bushnell<sup>5,6</sup>, Linda Gardner<sup>7</sup>, William S. Graham<sup>1</sup>, Sheila Lindsay<sup>8</sup>, David C. Metz<sup>9</sup>, Daniel A. Pryma<sup>10</sup>, Michael G. Stabin<sup>11</sup>, and Jonathan R. Strosberg<sup>12</sup>



#### Pretreatment <sup>68</sup>Ga DOTATATE PET and Post-Cycle 177Lu SPECT



Image courtesy of Dr. Thomas Hope, UCSF Department of Radiology

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#### Guidelines for Quantitative <sup>177</sup>Lu SPECT

MIRD Pamphlet No. 26 has recommendations regarding :

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Energy window Collimator Reconstruction choices SPECIAL CONTRIBUTIONS

MIRD Pamphlet No. 26: Joint EANM/MIRD Guidelines for Quantitative <sup>177</sup>Lu SPECT Applied for Dosimetry of Radiopharmaceutical Therapy

Michael Ljungberg<sup>1</sup>, Anna Celler<sup>2</sup>, Mark W. Konijnenberg<sup>3</sup>, Keith F. Eckerman<sup>4</sup>, Yuni K. Dewaraja<sup>5</sup>, and Katarina Sjögreen-Gleisner<sup>1</sup>

In collaboration with the SNMMI MIRD Committee: Wesley E. Bolch, A. Bertrand Brill, Frederic Fahey, Darrell R. Fisher, Robert Hobbs, Roger W. Howell, Ruby F. Meredith, George Sgouros, and Pat Zanzonico, and the EANM Dosimetry Committee: Klaus Bacher, Carlo Chiesa, Glenn Flux, Michael Lassmann, Lidia Strigari, and Stephan Walrand.

#### SPECIAL CONTRIBUTION

MIRD Pamphlet No. 23: Quantitative SPECT for Patient-Specific 3-Dimensional Dosimetry in Internal Radionuclide Therapy

Yuni K. Dewaraja<sup>1</sup>, Eric C. Frey<sup>2</sup>, George Sgouros<sup>2</sup>, A. Bertrand Brill<sup>3</sup>, Peter Roberson<sup>4</sup>, Pat B. Zanzonico<sup>5</sup>, and Michael Ljungberg<sup>6</sup>

In collaboration with the SNM MIRD Committee: Wesley E. Bolch, Darrell R. Fisher, Roger W. Howell, Ruby F. Meredith, and Barry W. Wessels



#### **Dose Calculation Methods**

Monte Carlo	Point Dose Kernel Convolution	Local Energy Deposition
Monte Carlo is the 'gold standard' in dosimetry Accounts for tissue heterogeneities and composition differences Post-treatment SPECT is used to localize the radionuclide The CT component is used for radiation transport The CT component is used for radiation transport <b>GATE</b> <b>CESNCE</b>	Kernels are generated with Monte Carlo methods and are convolved with the SPECT study	Most simplistic model, where all of the energy is assumed to be deposited in the voxel with activity
UCSF	2020 JULY 12-	-16 VIRTUAL EASTERN TIME (GMT-4) AAPM COMP MEETING

#### **Dose Calculation Engines**

The purpose of the dose calculation engine is to take the acquired SPECT and arrive at an estimate of dose (Gy) per voxel in the patient.



## Dose Calculation Engines (2)

- At UCSF we use an inhouse (python based) dose calculation, based
- on Monte Carlo kernels
   DICOM RTDose files are generated with GALE. created for reporting volumetric dose
- Can be read out by commercial and open source software.



	*		
		Kernel (3D)	
Activity Concentratio (per voxel)	n		Dose (Gy)



#### Reporting dose to targets and normal structures

- To report the received dose to targets and normal structures, one needs to know where they are
- Contour the kidney, spleen and lesions







#### Validation

Energy spectra compared against NIST data



Phantom measurements with <sup>177</sup>Lu to ensure accuracy of SPECT calibration & spatial resolution effects



Analytic dose calculation compared with dose calculation for uniform sphere.



COMP MEETING

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25 Gy
20 Gy
15 Gy
10 Gy
5 Gy
2 Gy

Dose from C1







R



R

25 Gy
20 Gy
15 Gy
10 Gy
5 Gy

Dose from C1 + C2 + C3





25 Gy 20 Gy 15 Gy 10 Gy 📕 5 Gy Dose from C1 + C2 + C3 + C4

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Example of Summed Doses for <sup>177</sup>Lu-DOTATATE





#### Other Commercial and In-house Methods

There are many vendors and other groups that are doing work on dose calculations for TRTs.

There will be many solutions for how dose is calculated and reported for our patients.





### The need for harmonized reporting of dose

In a dose response model, a response is seen between the absorbed dose and the response.

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# In TRT, the dose delivered is modulated by the administered activity







# In TRT, there are many additional sources of uncertainty in reported dose ...





### The impact of tumor size

Below a certain threshold, the reconstructed activity in the SPECT study is inaccurate and may results in gross errors in dose calculation

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In this example, the authors excluded tumors of diameter < 2.2 cm (based on measurements) and then applied a secondary cut of 4 cm.



**FIGURE 5.** Tumor dose–response relationship for patients with PNETs treated with PRRT using <sup>177</sup>Lu-DOTATATE, including tumors larger than 2.2 cm (A) and only tumors larger than 4 cm (B). Solid lines represent 2-parameter sigmoid fits ( $y = 100/(1 + (\alpha/x)^{\beta})$ ), where  $\alpha$  and  $\beta$  are fitting parameters. Parameters  $\alpha$  and  $\beta$  were 445 and 0.79, with SEs of 104 and 0.14, respectively, for tumors larger than 2.2 cm and 504 and 0.84, with SEs of 83 and 0.1, respectively, for tumors larger than 4 cm. Pearson correlation coefficients ( $R^2$ ) were 0.64 (A) and 0.91 (B).

Dose Response of Pancreatic Neuroendocrine Tumors Treated with Peptide Receptor Radionuclide Therapy Using <sup>177</sup>Lu-DOTATATE

Ezgi Ilan<sup>1,2</sup>, Mattias Sandström<sup>1,2</sup>, Cecilia Wassberg<sup>1,3</sup>, Anders Sundin<sup>1,3</sup>, Ulrike Garske–Román<sup>1,3</sup>, Barbro Eriksson<sup>4</sup>, Dan Granberg<sup>4</sup>, and Mark Lubberink<sup>1,2</sup>

<sup>1</sup>Nuclear Medicine and PET, Department of Radiology, Oncology, and Radiation Science, Uppsala University, Uppsala, Sweden; <sup>2</sup>Medical Physics, Uppsala University Hospital, Uppsala, Sweden; <sup>3</sup>Molecular Imaging, Medical Imaging Centre, Uppsala University Hospital, Uppsala, Sweden; and <sup>4</sup>Section of Endocrine Oncology, Department of Medical Science, Uppsala University Hospital, Uppsala, Sweden



#### The impact of tumor size : impact on dose response models





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#### Imaging at one timepoint

It may not be feasible to acquire many patient images – assumptions about physical and effective half life may or may not be included in dose calculations.

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\* Results based on planar (not volumetric) estimates of activity

#### TABLE 1

Correlation Between Approximation  $\tilde{u}_{l}(r_{S}, t_{l}) = u(r_{S}, t_{l}) \times 2 \times t_{l}/ln(2)$  Deduced from Single Measurement After 24, 48, 72, 96, 120, and 144 Hours and Actual Time Integral  $\tilde{u}(r_{S})$ 

		Pearson correlation coefficient r						
Tissue	24 h	48 h	72 h	96 h	120 h	144 h		
Kidneys	0.73	0.84	0.93	0.98	0.99	0.98		
Liver	0.67	0.84	0.93	0.98	0.99	0.99		
Spleen	0.55	0.77	0.89	0.97	0.99	0.99		
NET	0.63	0.80	0.92	0.97	0.99	0.99		

#### Dose Mapping After Endoradiotherapy with <sup>177</sup>Lu-DOTATATE/DOTATOC by a Single Measurement After 4 Days

Heribert Hänscheid<sup>1</sup>, Constantin Lapa<sup>1</sup>, Andreas K. Buck<sup>1</sup>, Michael Lassmann<sup>1</sup>, and Rudolf A. Werner<sup>1,2</sup>

<sup>1</sup>Department of Nuclear Medicine, University Hospital Würzburg, Würzburg, Germany; and <sup>2</sup>Division of Nuclear Medicine and Molecular Imaging, The Russell H. Morgan Department of Radiology and Radiological Science, Johns Hopkins School of Medicine, Baltimore, Maryland



#### Imaging at one timepoint







#### Reporting Dose : Dose Volume Histograms



### Reporting Dose : Dose Volume Histograms

The dose to different tumors in the same patient is variable.

The reporting of the received dose depends on what metric is chosen:

Average doseNear minimum doseMaximum dose

In addition, this will depend on how the tumor volume is defined (contoured)







#### Reporting Dose : Average dose, near minimum dose







Scanner Calibration: Accuracy of the dose calculation relies on the accuracy of the imaging study that it is based upon.









Uncertainties in Reported Dose and the need for harmonization, external validation methods

These sources of uncertainty in reporting the received dose need to be addressed consistently if the goal is to compare results between institutions

There may be a role for external validation (phantom) to credential sites to participate when reporting the received radiation dose





## Quantifying response

- All of the previous examples dealt with dose uncertainties ( $\Delta x$ )
- There are also uncertainties in how we quantify response
  - RECIST criteria?

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• At what time are we evaluating response?





I DON'T KNOW HOW TO PROPAGATE ERROR CORRECTLY, SO I JUST PUT ERROR BARS ON ALL MY ERROR BARS.

https://xkcd.com/2110/



#### What can we do now that we have imaging?

Course 4 Uptake

Course 1 Uptake

- We can start to look at our patient data and try to understand why some patients respond to treatment, while others do not
- Started to evaluate response by looking at the relative uptake of <sup>177</sup>Lu between Course #4 and Course #1 (tumor level)

Response = 1

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JULY 12-16 VIRTUAL EASTERN TIME (GMT-4)

#### What can we do now that we have dose?

Course 4 Uptake

Course 1 Uptake

- We can start to look at our patient data and try to understand why some patients respond to treatment, while others do not
- Started to evaluate response by looking at the relative uptake of 177Lu between Course #4 and Course #1 (tumor level)

Response =

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# How do we know that what we are reporting is accurate?

- Every site uses different scanners, protocols and there are starting to be many software solutions to calculate dose
- We performed phantom studies, and compared the results of our "inhouse" dose calculation method with analytic methods
- To compare results across institutions, we need to have harmonized approaches and ideally ways to validate the accuracy of the reported dose.





## Alliance A021901 (protocol in development)



- SSTR+ on DOTATATE PET <sup>a</sup>
- Radiographic progression within 12 months
- No limit on prior lines of therapy
  - N = 108



Dosimetry

co-Pls:

Thomas Hope Suki Pado

)

- Cross over allowed on the control arm
- \*Central review at progression
- \*\*Concurrent SSA use allowed for patients with functional tumors if on stable dose for 3 months and previous radiographic progression on SSA

Before this trial starts, we can start to plan for what reporting dose to tumors would require

#### SSTR=somatostatin receptor

a=100% of typical carcinoids are SSTR+, while 50% of atypical carcinoids are SSTR+

## Outlook

- Calculating received radiation dose to tumors and healthy structures is achievable.
- Agreeing on how to report doses to tumors and healthy structures will make comparing results across institutions feasible <u>(harmonization)</u>
- External validation has the potential to fast-track the comparison of reported doses across institutions

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