

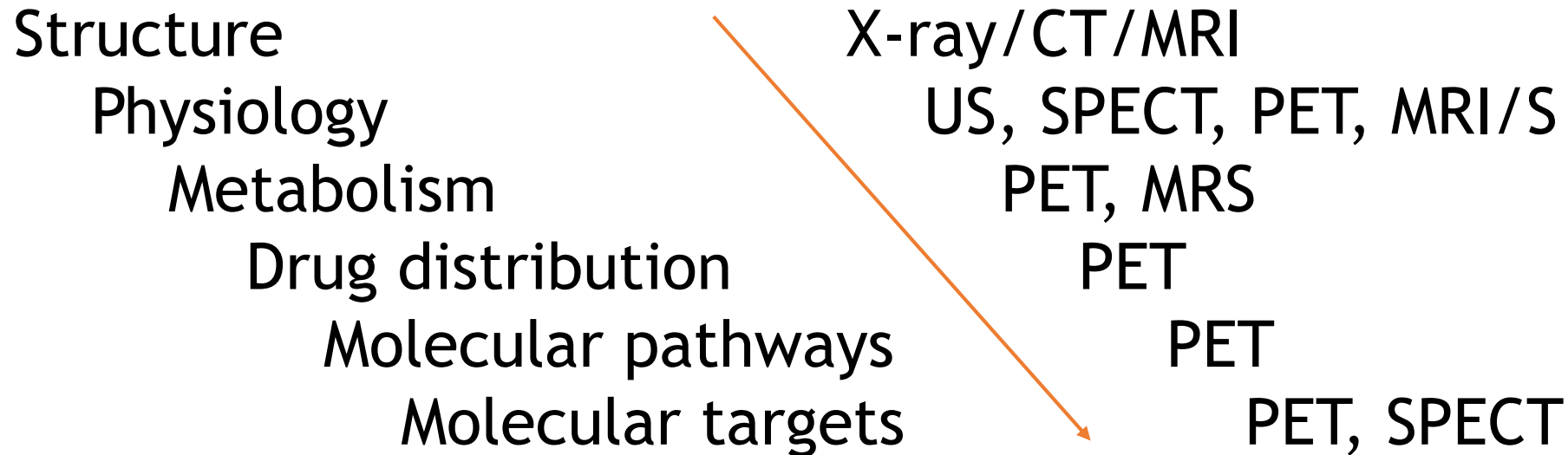
Possibilities and challenges in data analysis

Adriaan A. Lammertsma





The Spectrum of Medical Imaging



**PET: Quantitative
Picomolar Sensitivity**

Jones, 1996





Positron Emission Tomography



1975



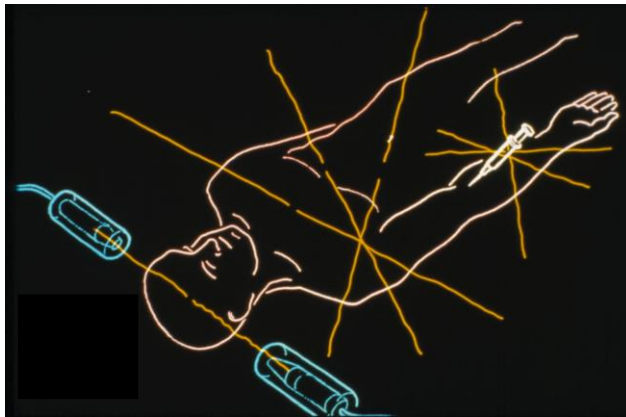
2015





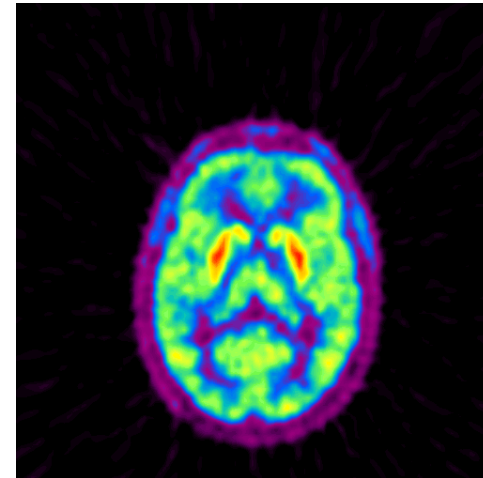
Routine Clinical Practice

Inject



Wait

Scan



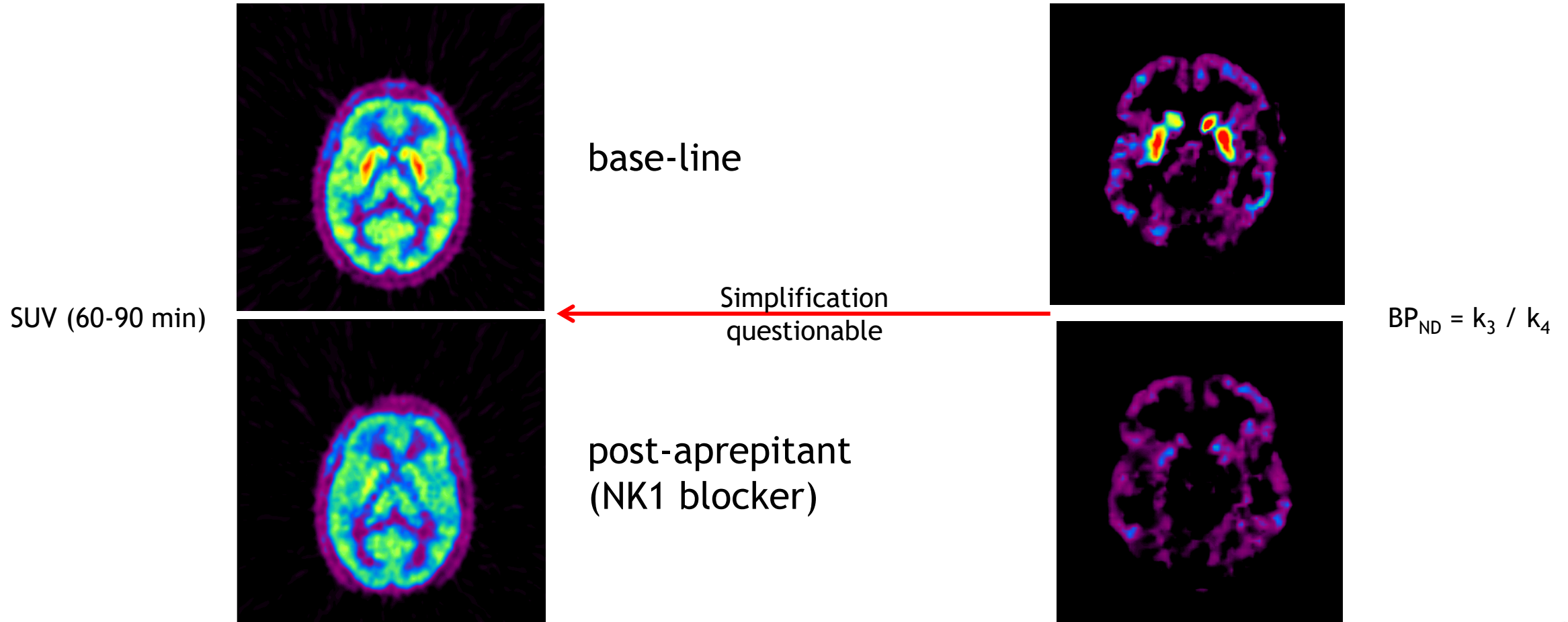
Increased uptake = increased binding
But what about:
increased flow, extraction or delivery?

Uptake (SUV)





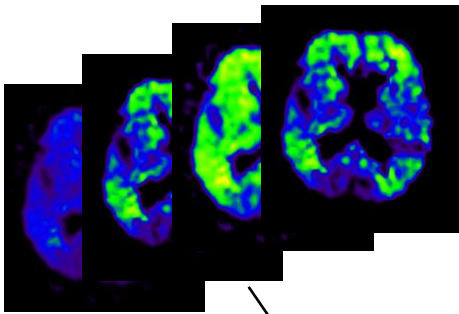
$[^{11}\text{C}]\text{R116301}$: NK1 receptor ligand



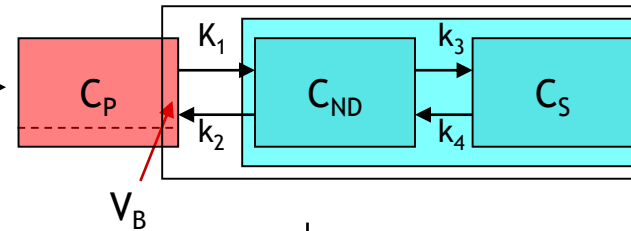


Overview kinetic analysis

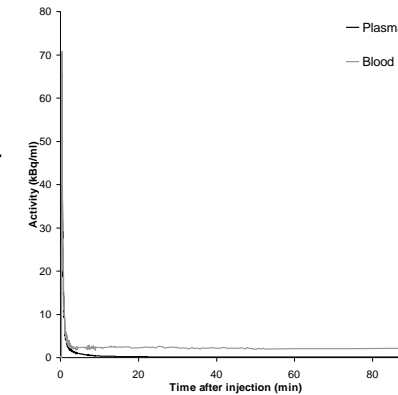
Dynamic PET scan



Kinetic model

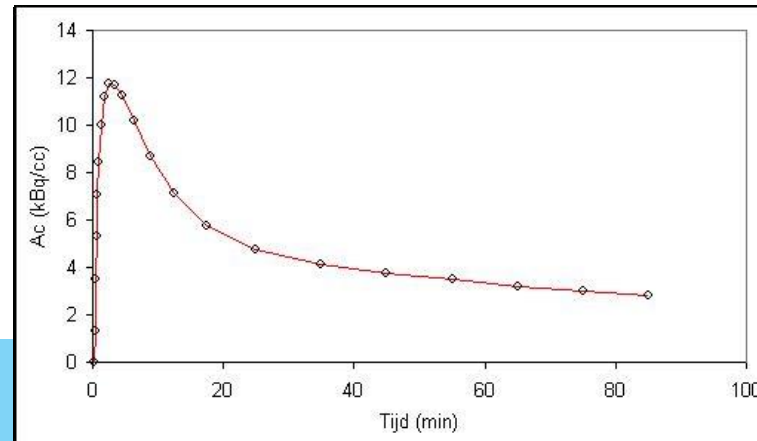


Input function



Fitting routine

Tissue
time-activity
curve



Kinetic parameters

$$BP_{ND} = k_3 / k_4 = f_{ND} \cdot B_{avail} / K_d$$

$$V_T = K_1 / k_2 \cdot (1 + BP_{ND})$$





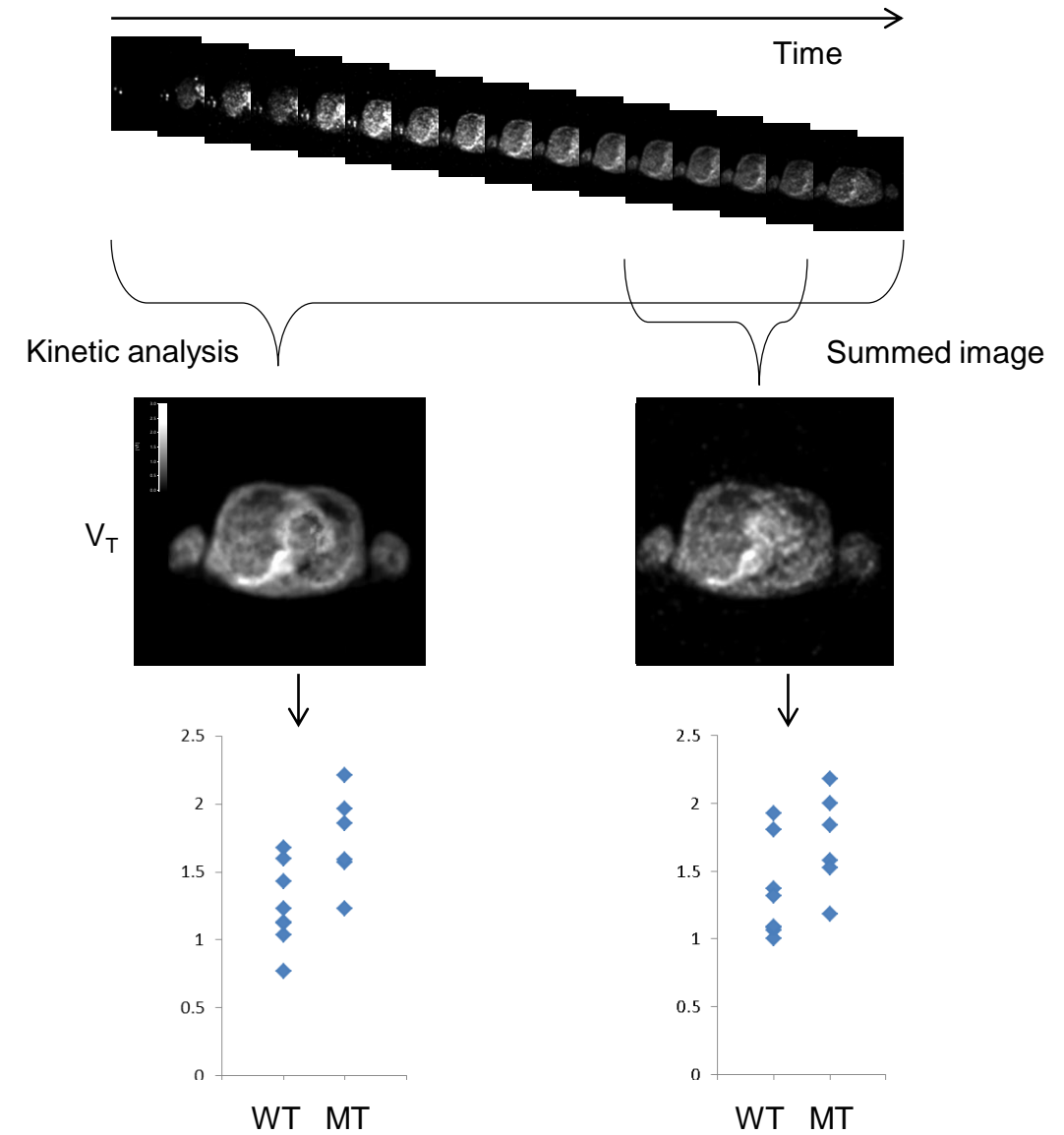
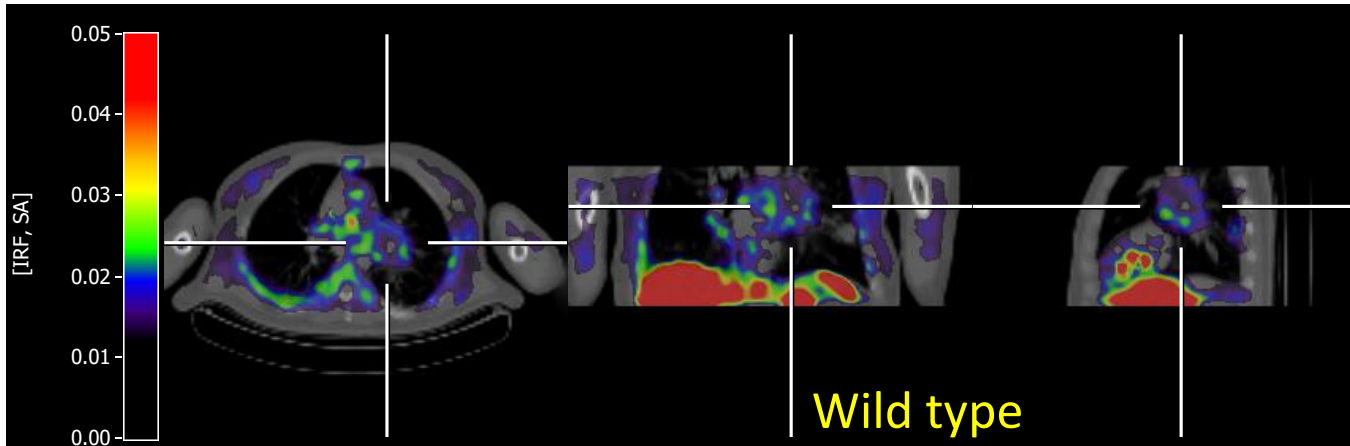
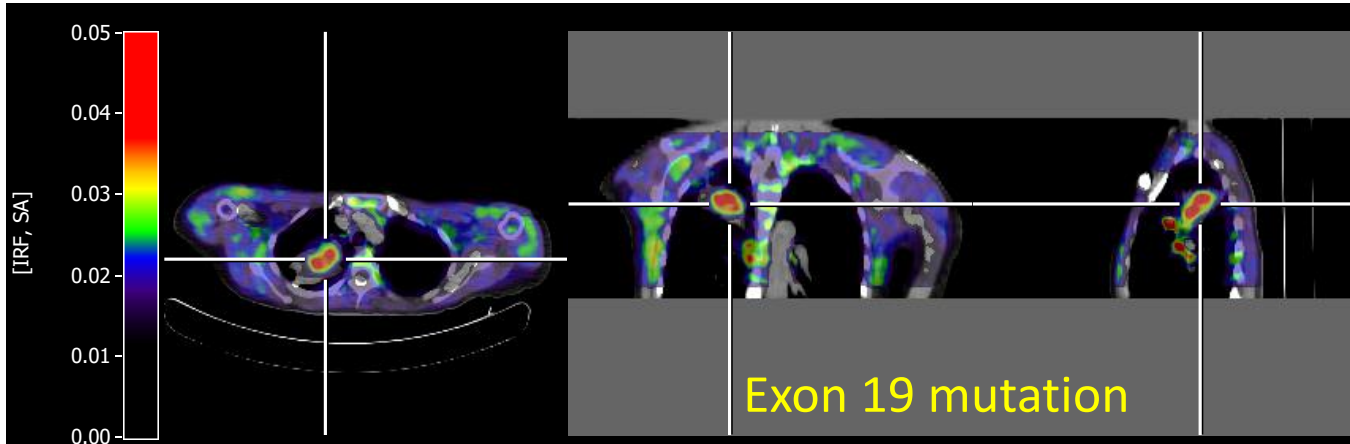
Rationale for Quantification

- Radiology & Nuclear Medicine: 1 image is worth more than 1000 words
- Imaging Science: 1 number is worth more than 1000 images
- Quantification:
 - Essential for correcting for confounding effects
 - Essential for identifying global effects
 - Essential for monitoring progression of disease and for monitoring response to therapy





[¹¹C]Erlotinib

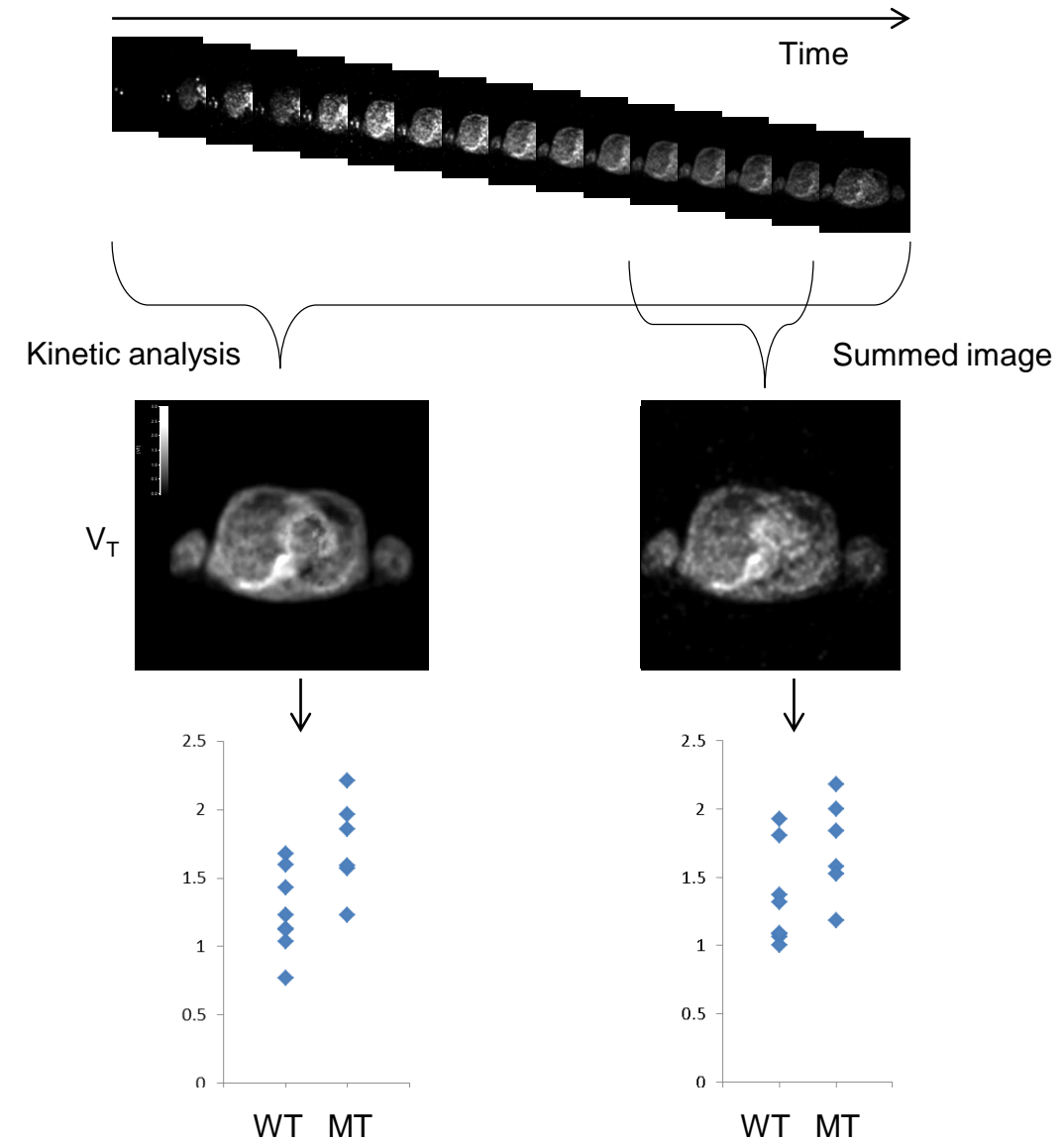




[¹¹C]Erlotinib

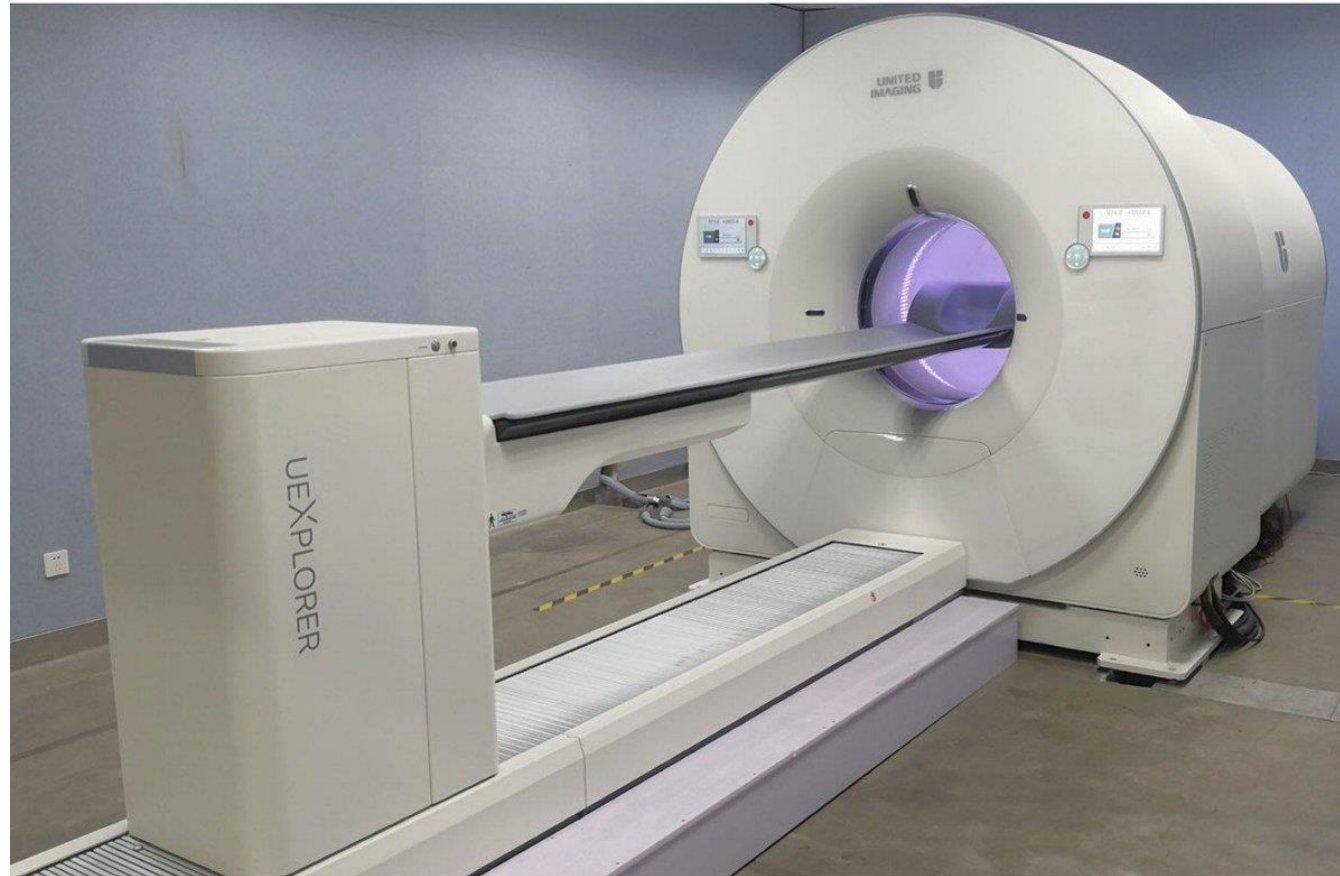
Dilemma:

1. Static whole body scan: non-informative
2. Dynamic scan: single field of view, but no information on interlesional heterogeneity





The Solution: Total Body PET



Explorer Total Body PET/CT

EXPLORER slides courtesy of Simon Cherry and Terry Jones, UC Davis



a)



0 min 0 sec

b)

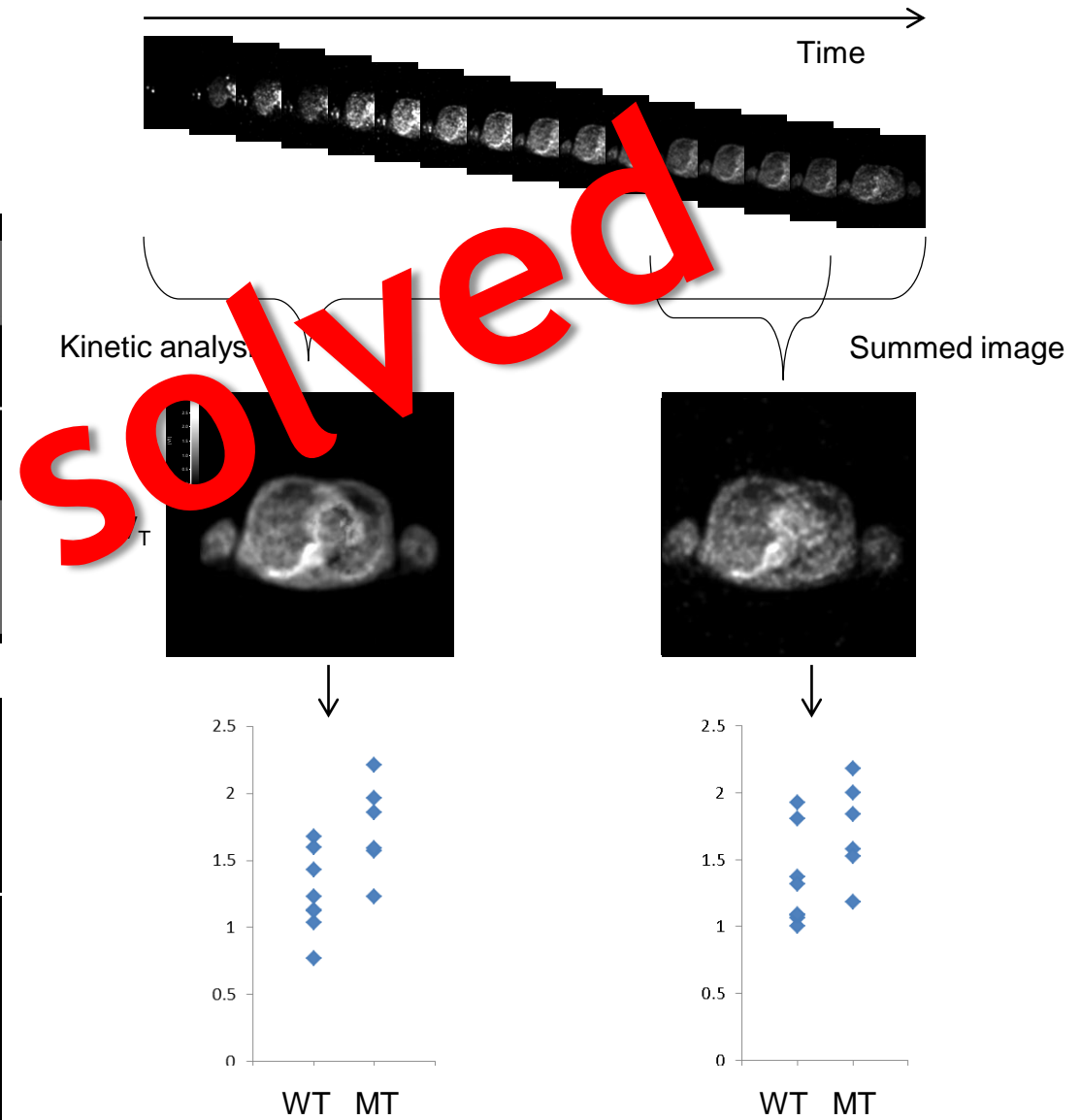
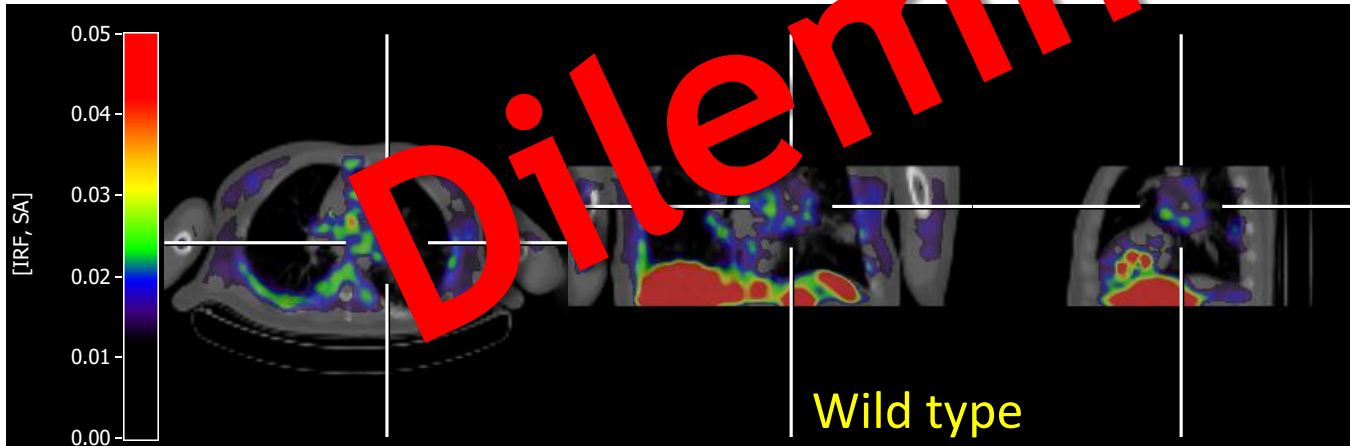
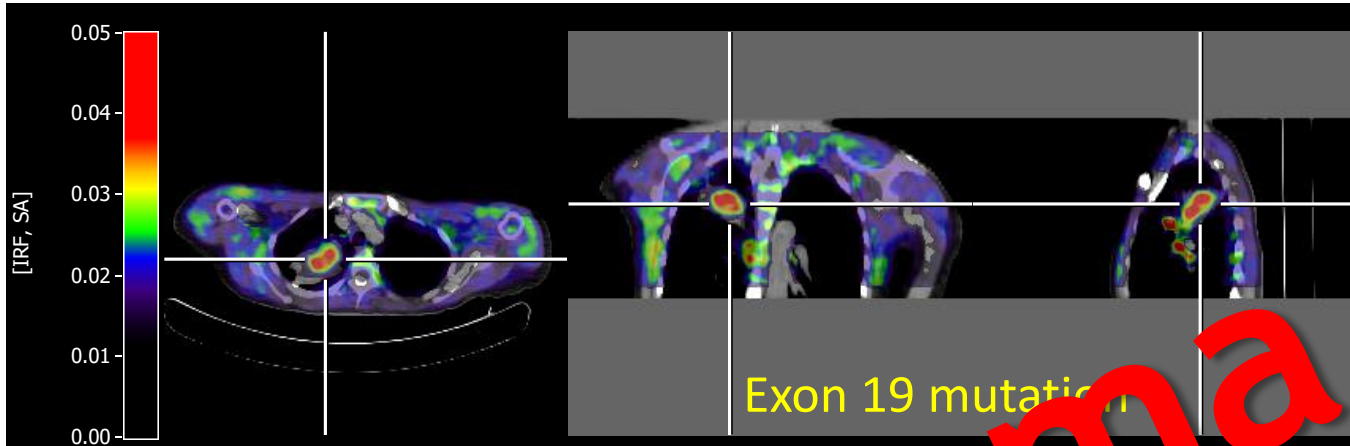


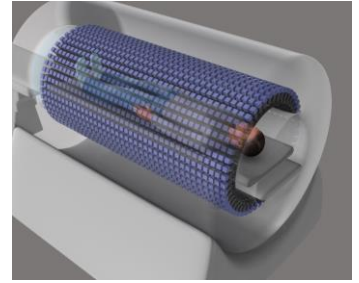
Maximum intensity projection (MIP) of late 30 min
(a) SUV; (b) indirect OSEM Patlak slope K_i (3 iterations 20 subsets)





[¹¹C]Erlotinib



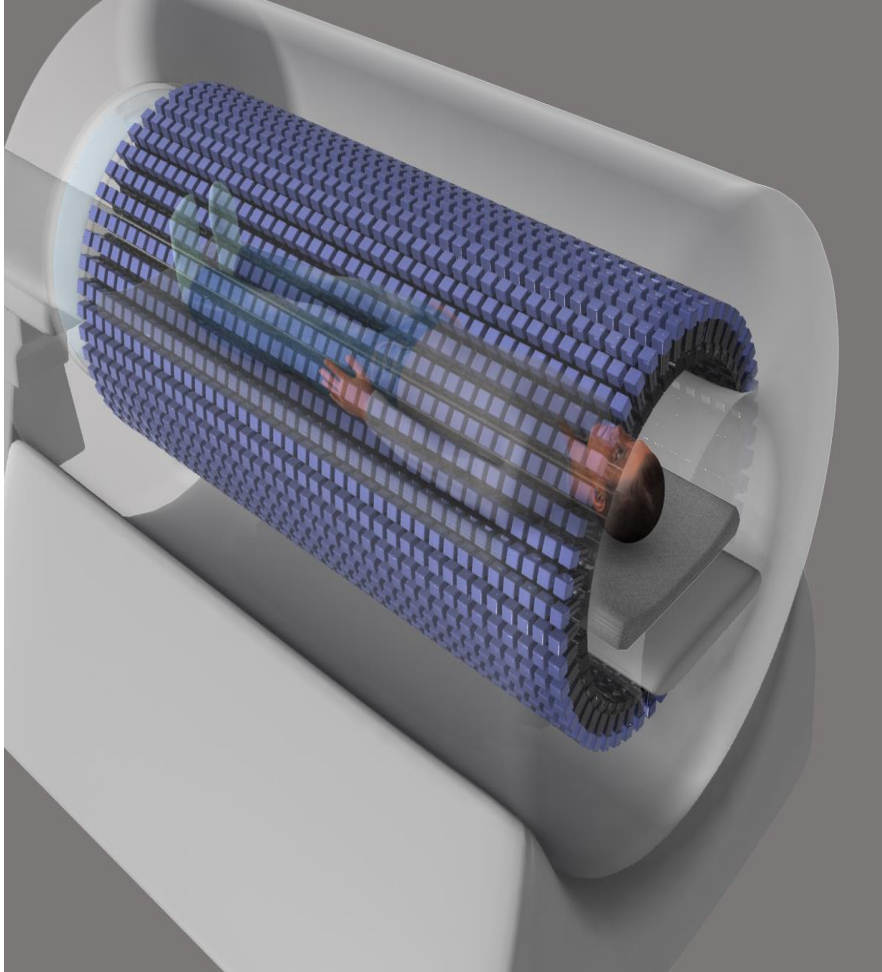


Opportunities of TB PET

- Quantitative (dynamic) scanning of total body rather than semi-quantitative (static) scanning
- Increased sensitivity



Maximizing Sensitivity by Total-Body PET



~40-fold increase
for adult total-body imaging

~20-fold increase
for pediatric total-body imaging

~4-fold increase
for single organ imaging



EXPLORER Claim: Image Longer

- Major increase in dynamic range

can image for 5 more half lives

- ^{11}C

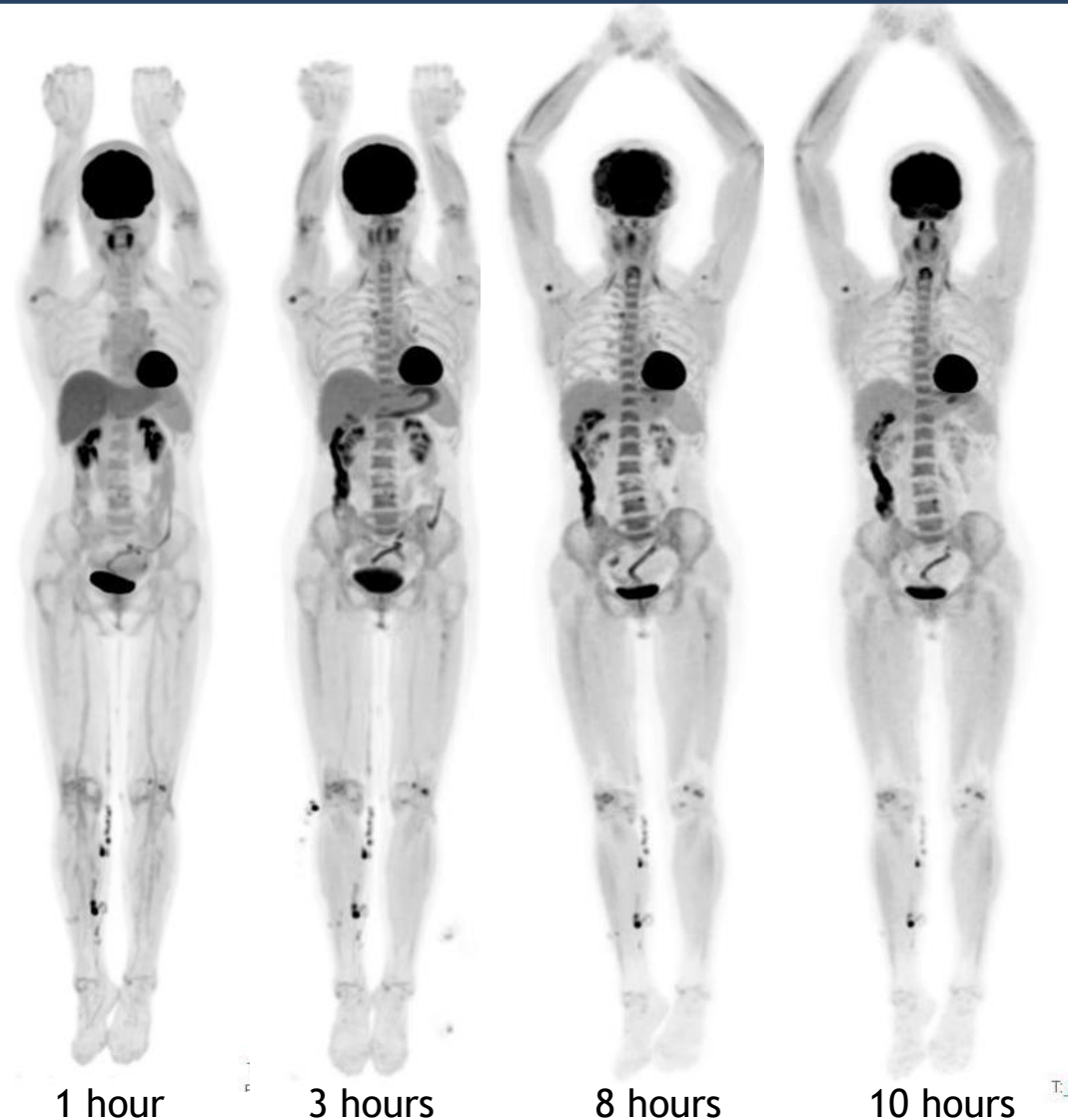
➤ 3 hours

- ^{18}F

> 16 hours

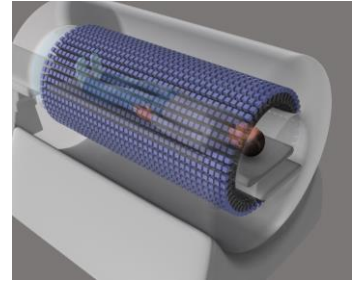
- ^{89}Zr

> 30 days



56 kg female; 6.7 mCi injected activity; 14 min acquisition



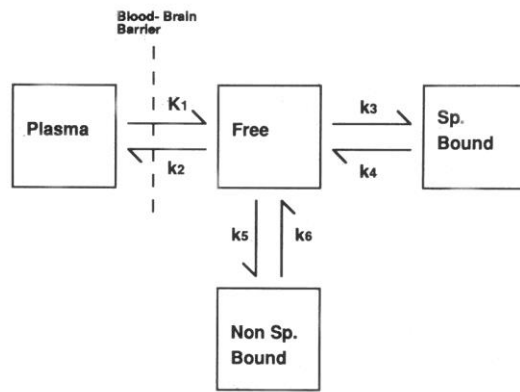


Opportunities of TB PET

- Quantitative (dynamic) scanning of total body rather than semi-quantitative (static) scanning
- Increased sensitivity
 - Longer scans possible in case of slow kinetics
 - Possibility for quantitative imaging of monoclonal antibodies (^{89}Zr labelling) in non-oncological applications
- Possibility for non-invasive measurement of arterial input function



Image Kinetics

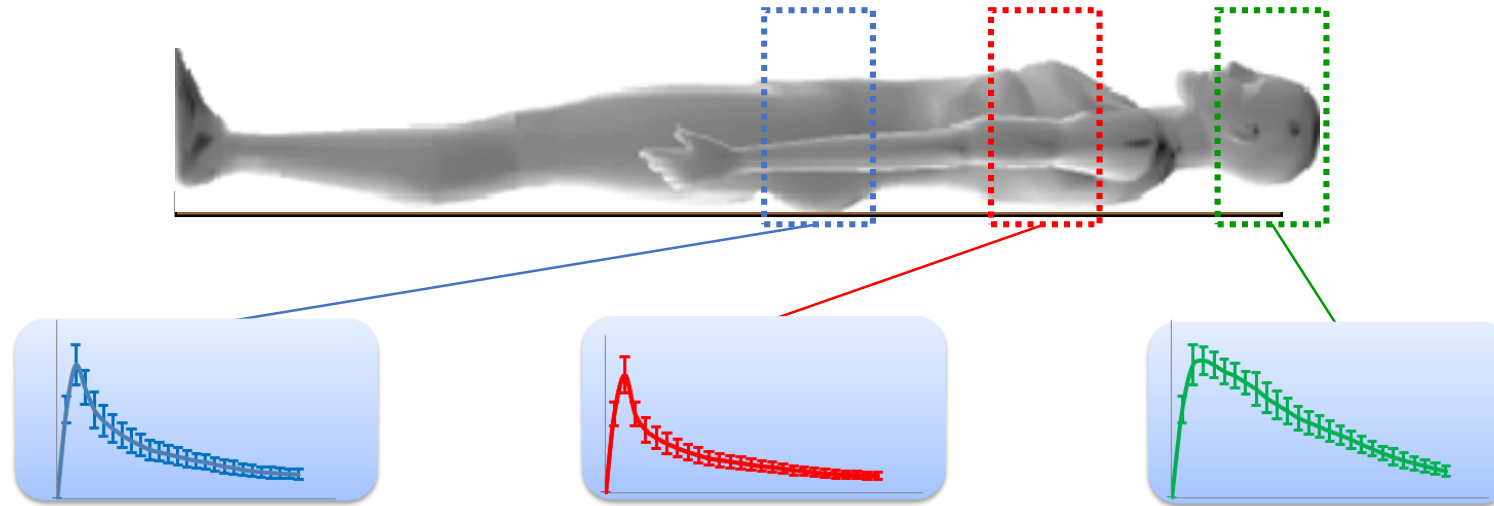


K_1 = flow \times extraction ($\text{mls min}^{-1} \text{ml}^{-1}$),

k_2 = functional efflux (min^{-1}),

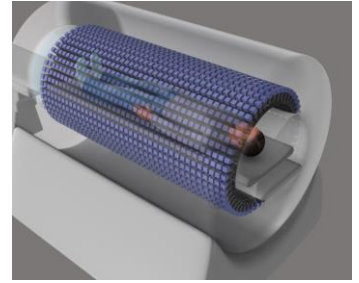
k_3 = combined forward rate constant ($K_{\text{ass}} \times B_{\text{max}}$) (min^{-1}),

k_4 = dissociation constant = k_{off} (min^{-1})



Regional tissue & *arterial blood time-activity curves* with high statistical quality





Challenges for TB PET

- Significant increase in number of lines of response



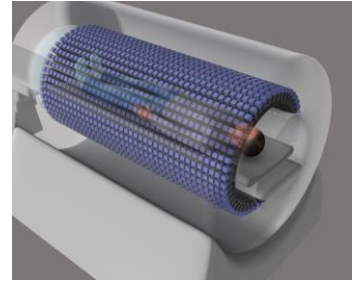
Total-Body PET: Maximizing Sensitivity



CONVENTIONAL PET



EXPLORER

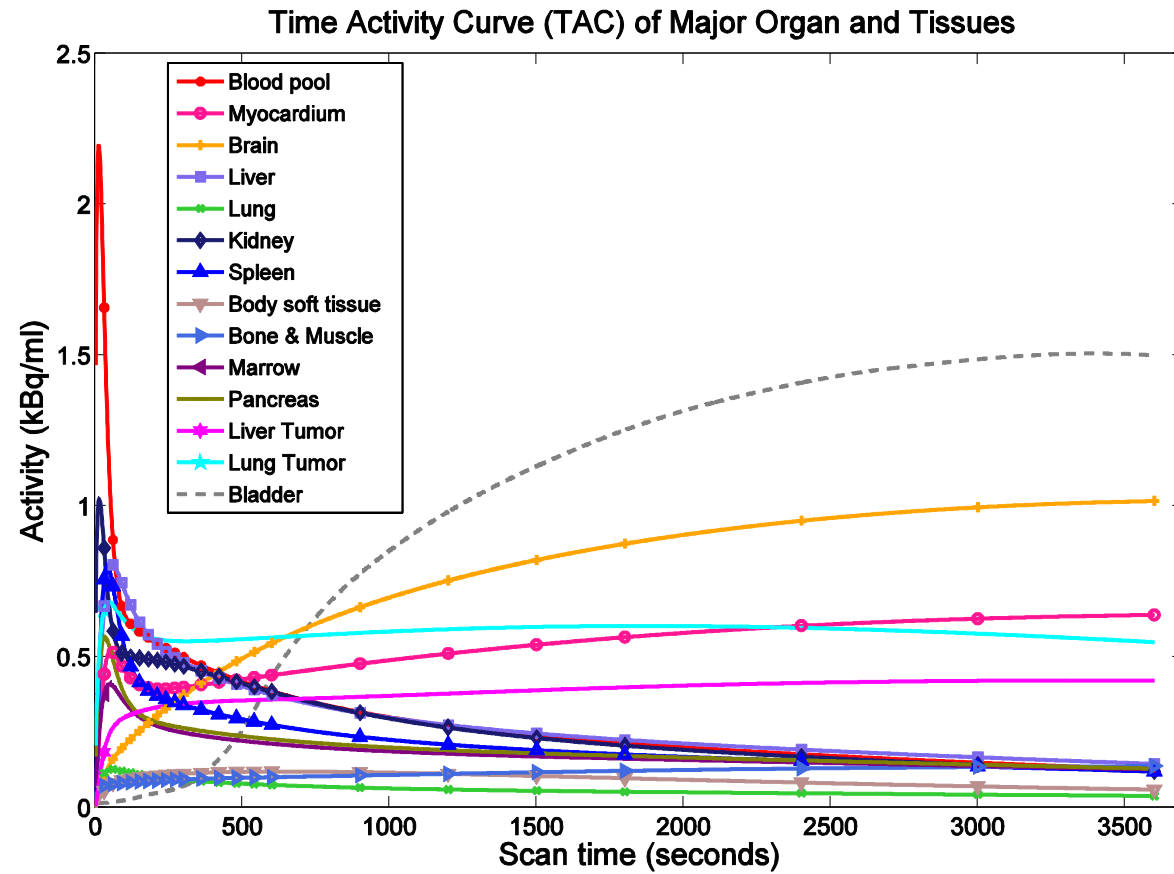


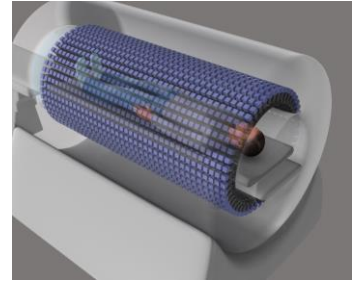
Challenges for TB PET

- Significant increase in number of lines of response → enormous datasets
- Larger axial field of view
 - More difficult for claustrophobic patients
 - Patient access: more difficult to inject tracer and to withdraw arterial blood



Total-Body Tracer Kinetics

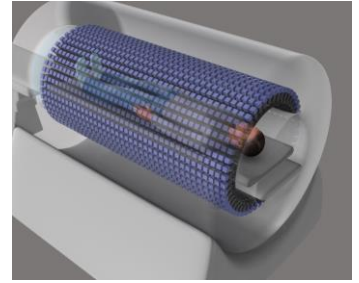




Challenges for TB PET

- Significant increase in number of lines of response → enormous datasets
- Larger axial field of view
 - More difficult for claustrophobic patients
 - Patient less accessible, i.e. difficulty to withdraw arterial blood
- Kinetic heterogeneity, i.e. different models required for different organs
- How to obtain image derived metabolite corrected plasma input functions?





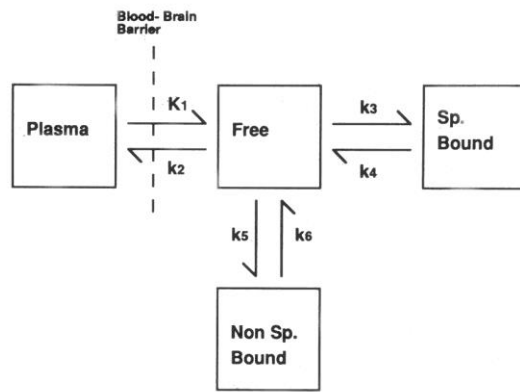
Potential Solutions

- Kinetic heterogeneity
 - Automatic segmentation of organs: cluster analysis, artificial intelligence
 - Parametric analysis: data driven methods such as spectral analysis
- Image derived metabolite corrected arterial plasma input function
 - Whole blood curve from dynamic scan: cluster analysis
 - Combine with venous plasma (metabolite) measurements
 - Derive from simultaneous fitting: same input for all voxels

Methodological building blocks already exist



Image Kinetics

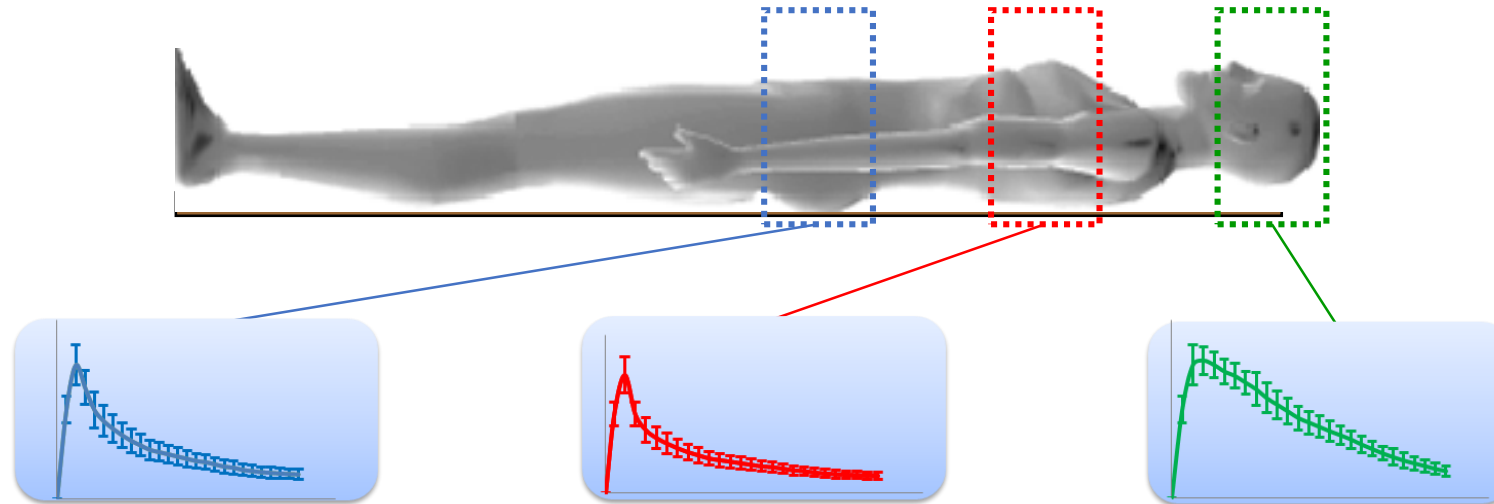


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k_4 = dissociation constant = k_{off} (min^{-1})



Regional tissue kinetics & arterial blood input functions with high statistical quality

Future: routine dynamic PET scanning as a non-invasive quantitative tool for clinical & research questions

