

Most pediatric patients should be treated at proton therapy centers

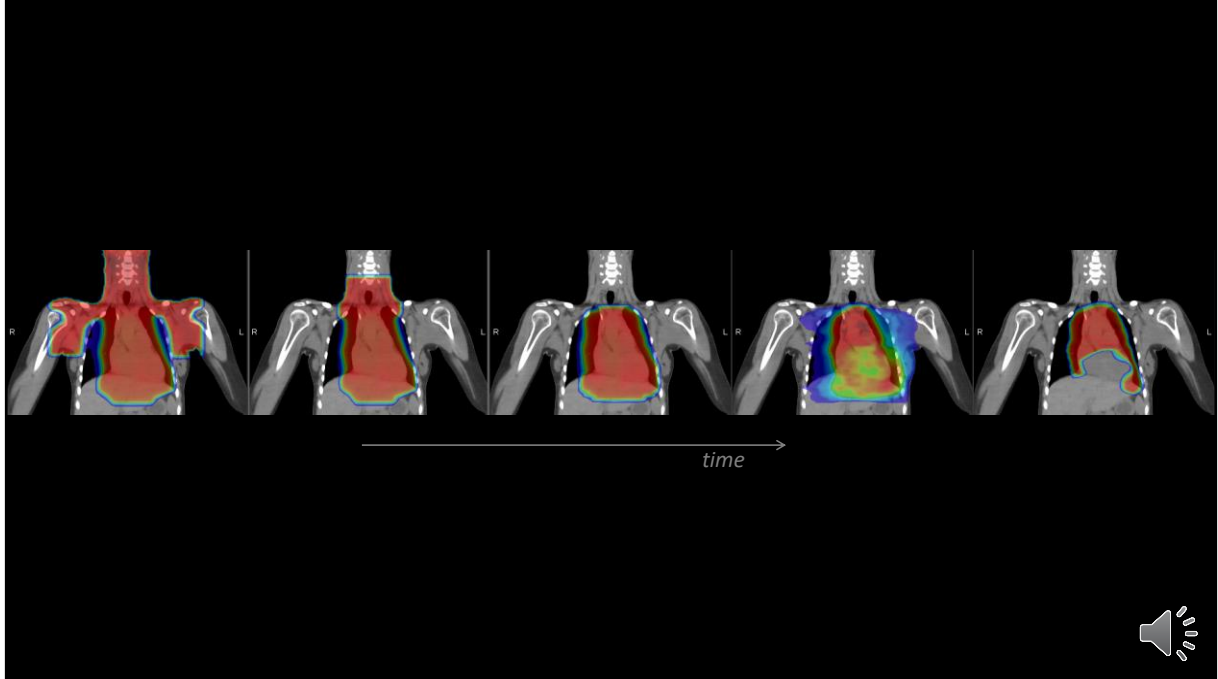
Yes, because proton therapy is technically superior to photon therapy

Stella Flampouri

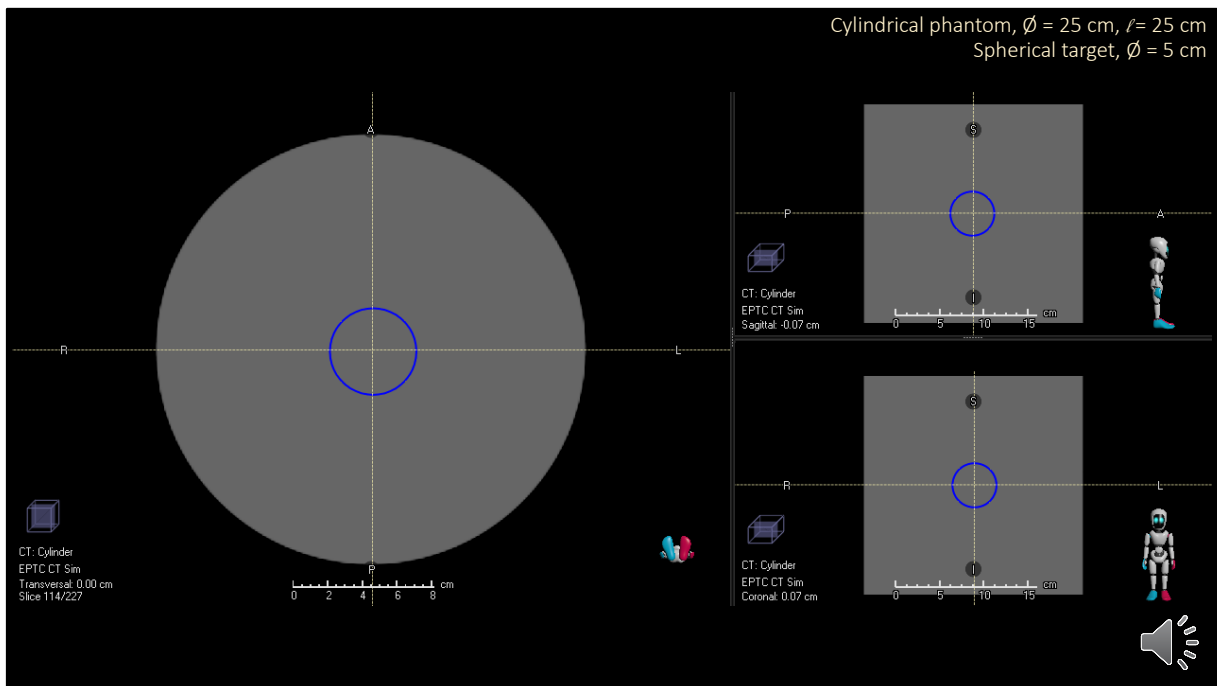
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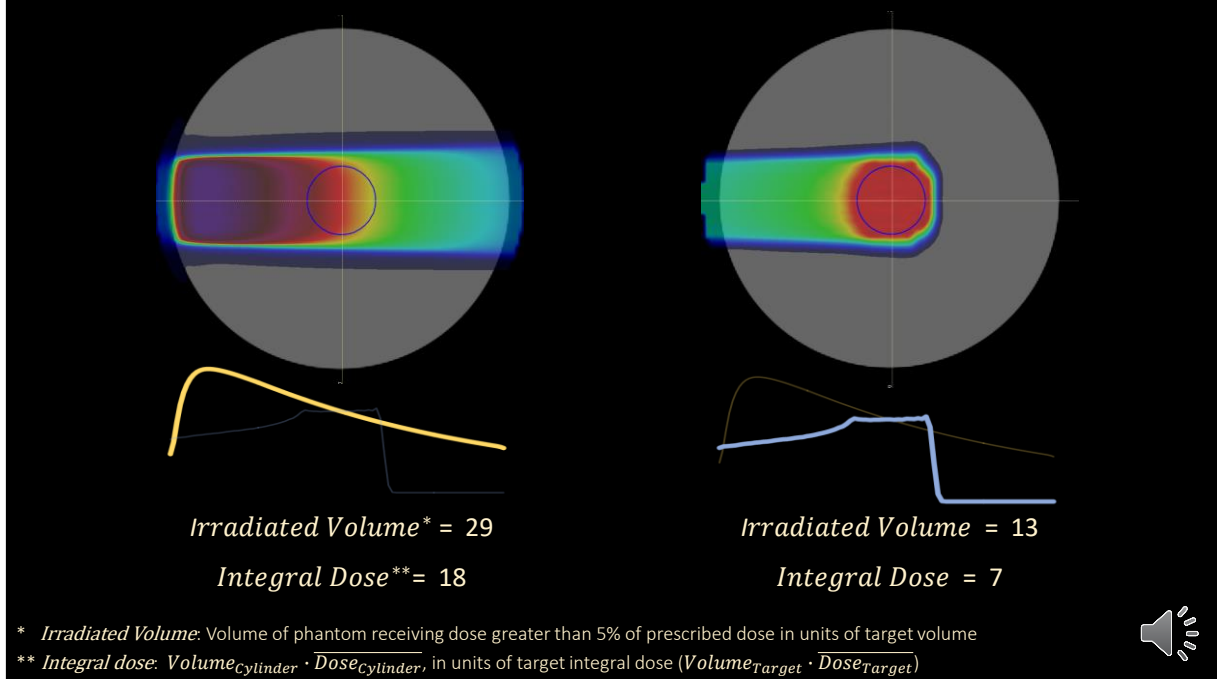
Protons are more suitable than photons for children in need of radiation treatment



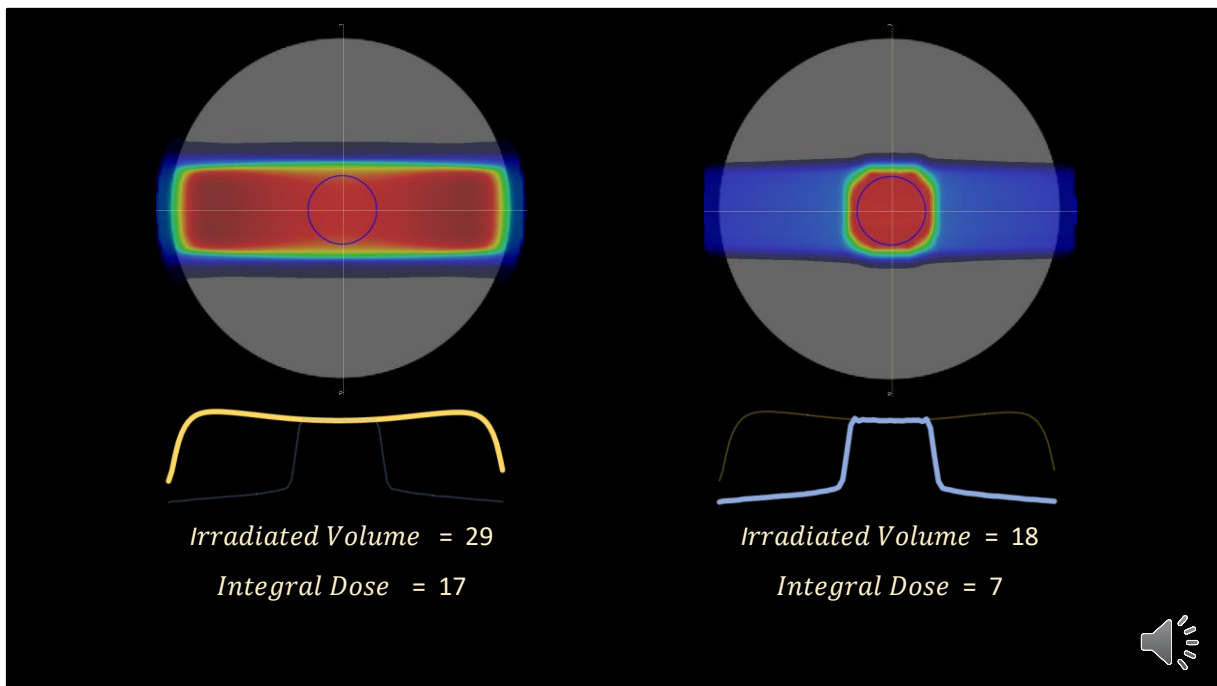
Progress in radiotherapy means less dose to non-target tissue.



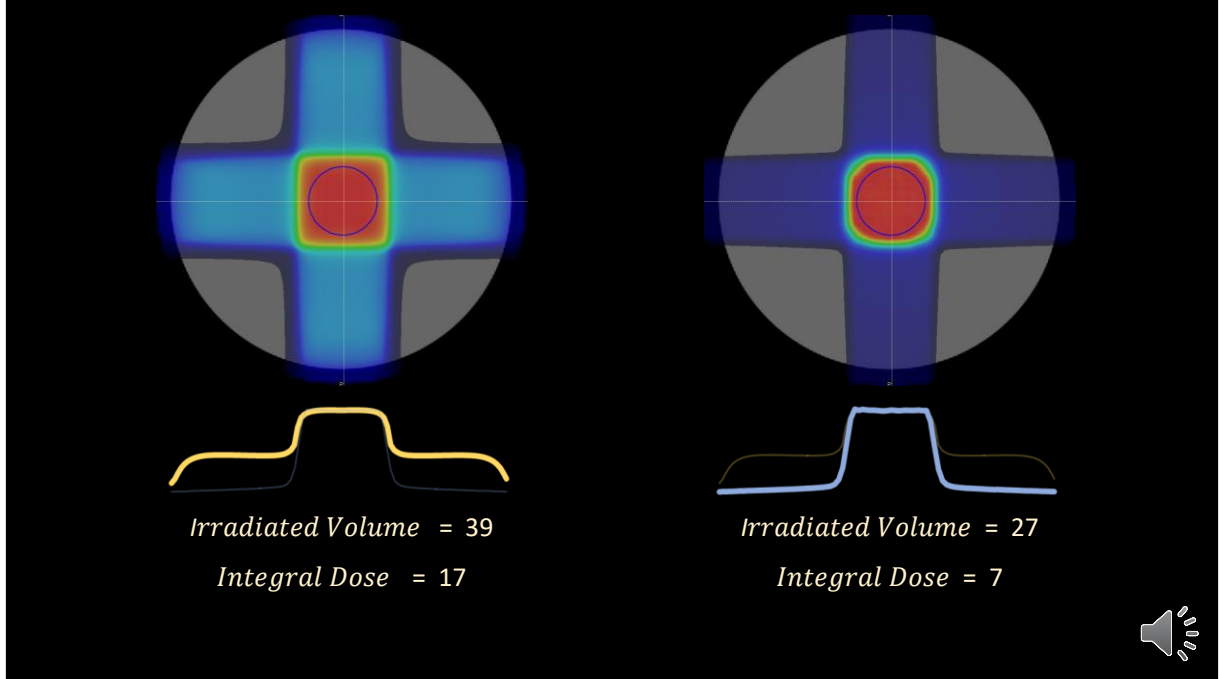
Protons are 'technically' better than photons because they treat the target while irradiating less of non-target tissue or to lower doses
Water phantom example



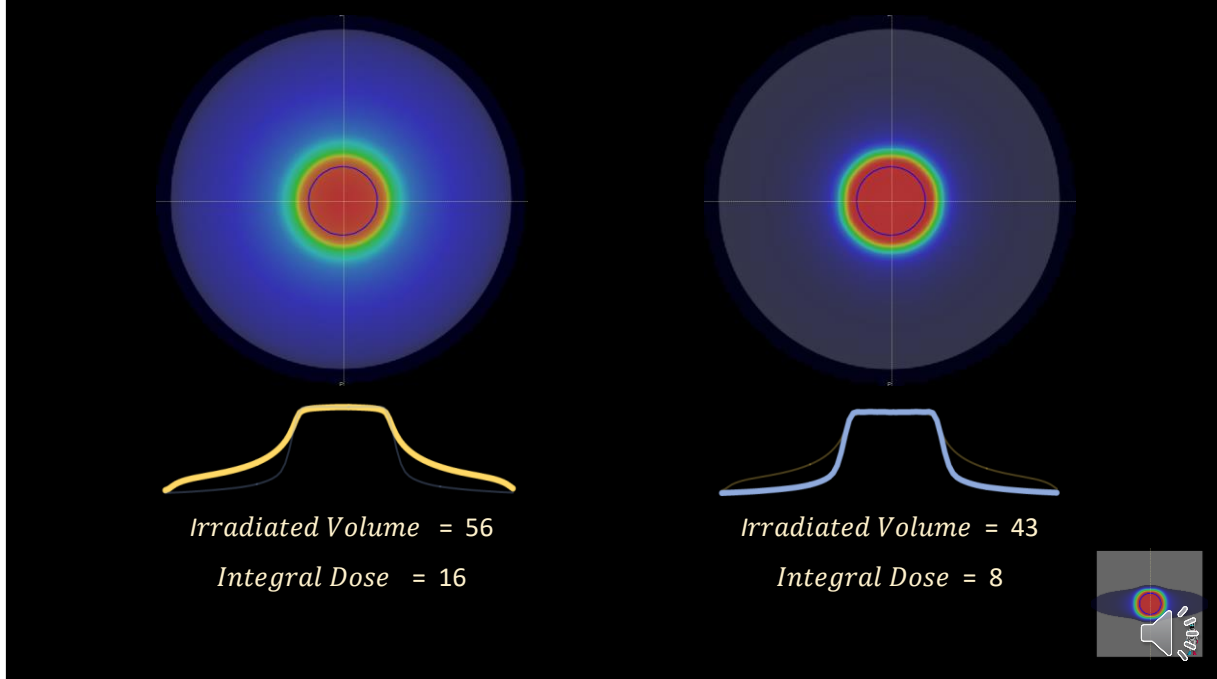
Single proton field treats target with homogenous dose while irradiating less volume and depositing less energy outside the target



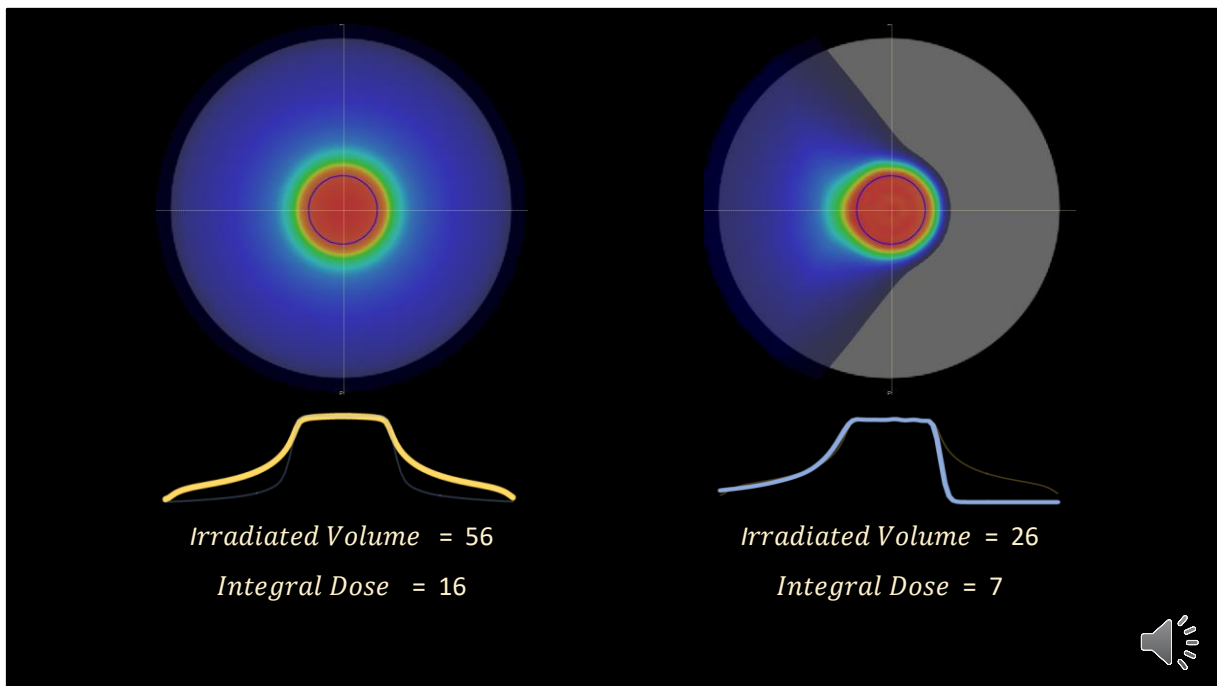
For 2 fields, photons treat the target almost as well as protons but do not spare non-target tissues



With 4 fields photons are improving



Photon state of the art treatments are delivered by arcs. Similar field arrangement with protons still deposits less dose outside the target.



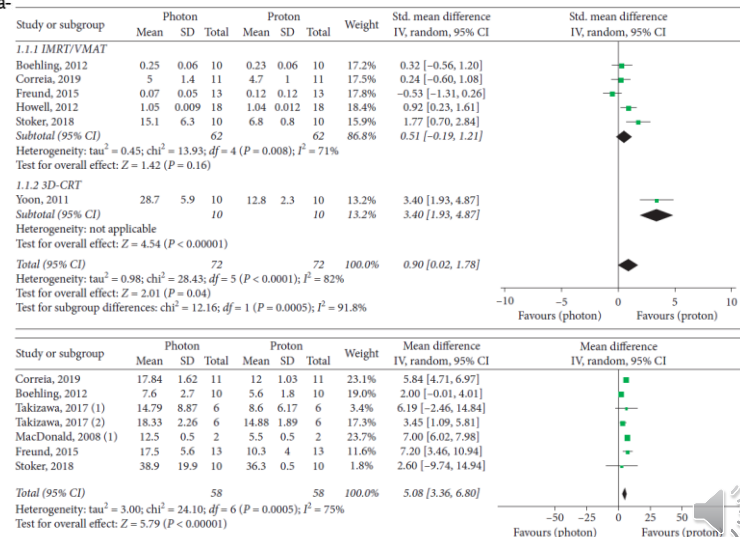
Accepting similar proximal non-target dose, protons can deliver the same target dose with partial arcs and spare completely tissues (full photon arc versus 130degree proton arc)

Proton versus Photon Radiotherapy for Pediatric Central Nervous System Malignancies: A Systematic Review and Meta-Analysis of Dosimetric Comparison Studies

Roberta Carbonara, Alessia Di Rito, [...], and Angela Sardaro

Homogeneity Index

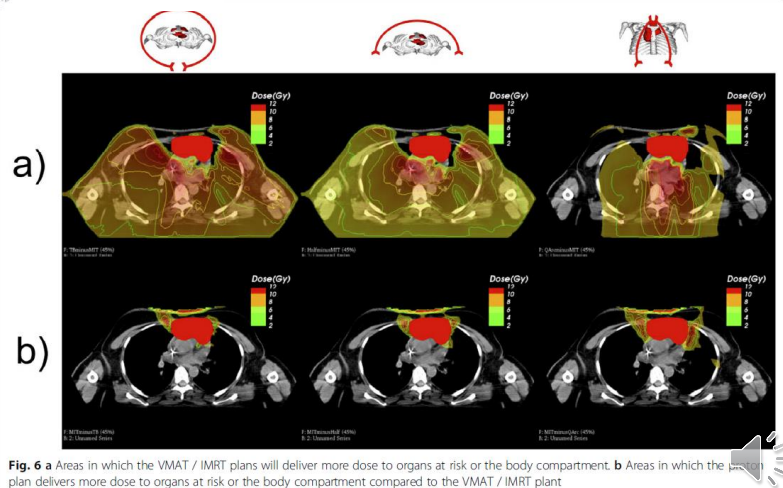
Normal Brain D_{mean}



Superior proton distribution holds not only for the simple example but also patients. It is very difficult to find a dosimetric comparison study that photon dose is better. This is a recent review of dosimetric comparisons between protons and photons for pediatric CNS. Protons better on everything but conformity

Advantage of proton-radiotherapy for pediatric patients and adolescents with Hodgkin's disease

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Pediatric HL dose comparison. State of the art plans for both modalities

Evaluating the Benefit of PBS vs. VMAT Dose Distributions in Terms of Dosimetric Sparing and Robustness Against Inter-Fraction Anatomical Changes for Pediatric Abdominal Tumors

Filipa Guerreiro ¹, Cornel Zachiu ², Enrica Seravalli ³, Cássia O Ribeiro ⁴, Geert O Janssens ⁵, Mario Ries ⁶, Baudouin Denis de Senneville ⁷, John H Maduro ⁸, Charlotte L Brouwer ⁹, Erik W Korevaar ¹⁰, Antje C Knopf ¹¹, Bas W Raaymakers ¹²

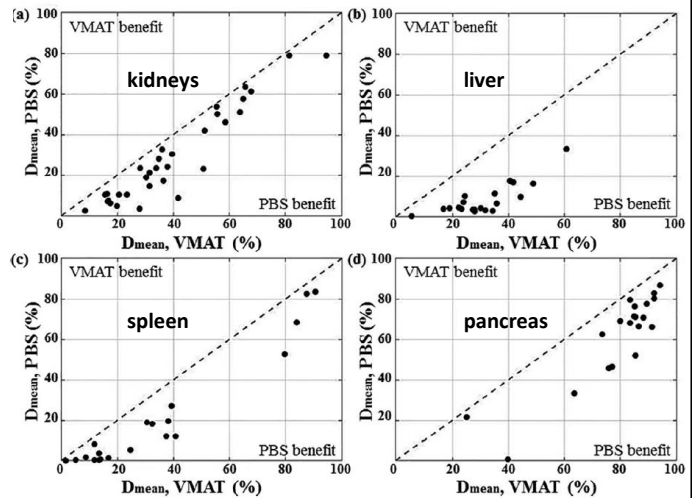


Fig. 2. D_{mean} delivered by VMAT and PBS to the OARs for the kidneys (a), liver (b), spleen (c) and pancreas (d).

This dose comparison includes daily setup errors and their dosimetric effects

A review of the impact of photon and proton external beam radiotherapy treatment modalities on the dose distribution in field and out-of-field; implications for the long-term morbidity of cancer survivors

ÅSA PALM & KARL-AXEL JOHANSSON

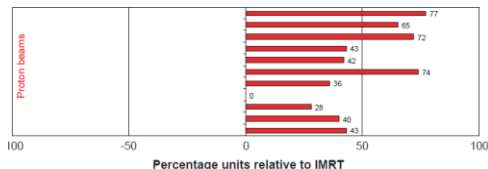
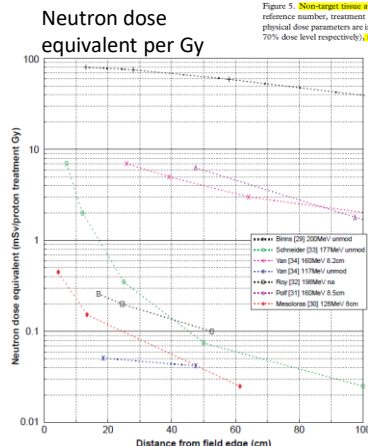
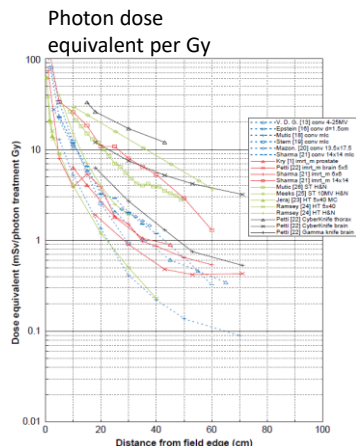
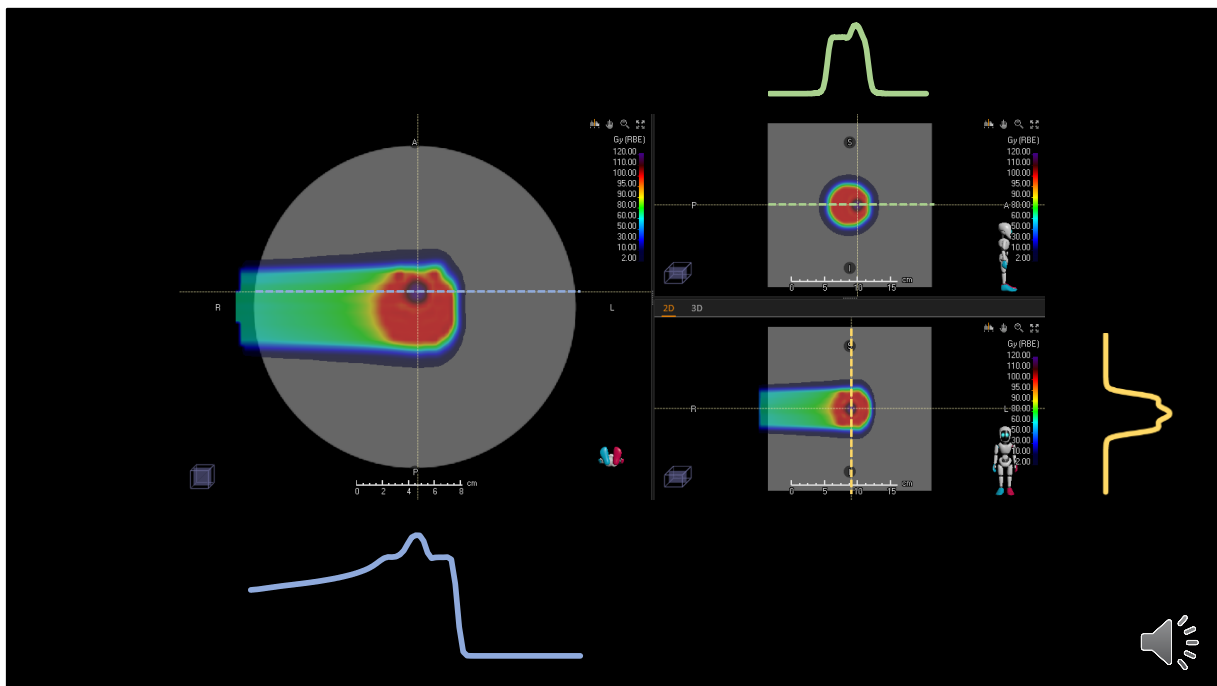
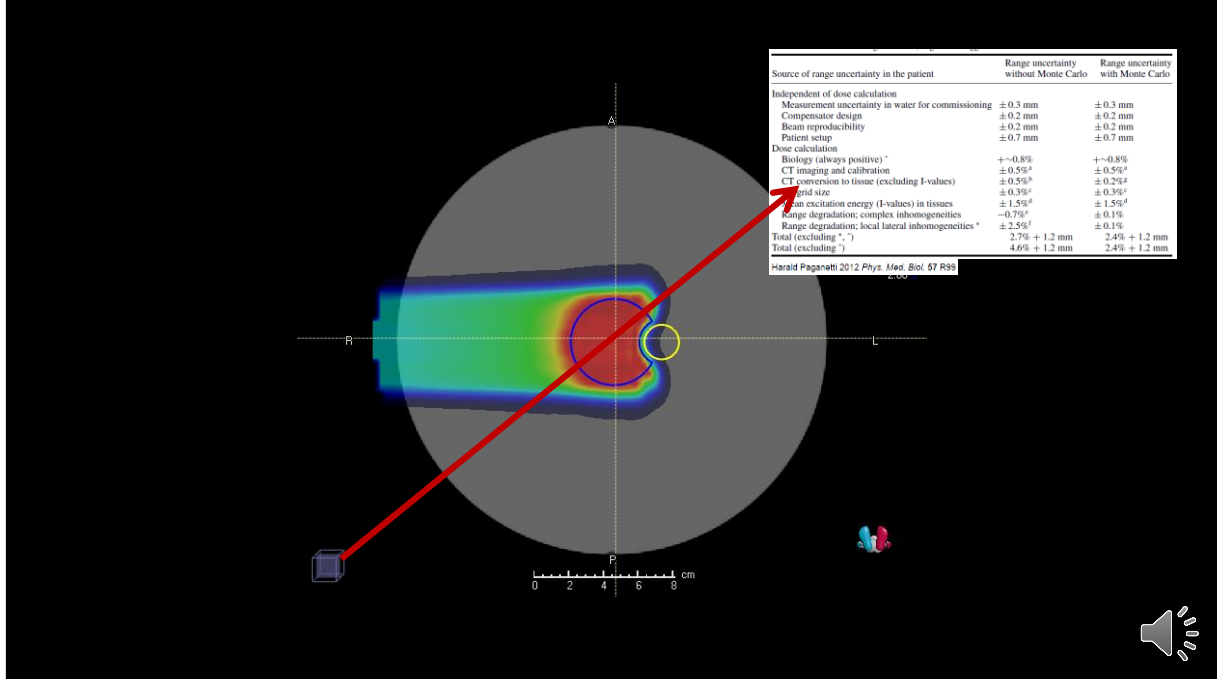


Figure 5. **Non-target tissue average dose.** Data from treatment planning studies [8–11,49–56], see Table 1 for an overview. First author, reference number, treatment size, and value are shown. A positive value indicates that the technique is superior to IMRT. The following physical dose parameters are included: mean dose, V30, V50, V70 (volume in percent where the cumulative DVHs intersect with 30, 50 and 70% dose level respectively), **integral dose** (mean dose times volume graduated to any dose).

Not pediatric specific but this study includes integral dose and out of field dose.



Another inherent quality of protons is our ability to modulate them in depth, an additional dimension compared to photons



There are uncertainties, but proton planning is more advanced than photon planning and takes care of them efficiently. 4D robust optimization is just an example.

Robust Proton Treatment Planning: Physical and Biological Optimization

Jan Unkelbach, PhD,^a and Harald Paganetti, PhD^b

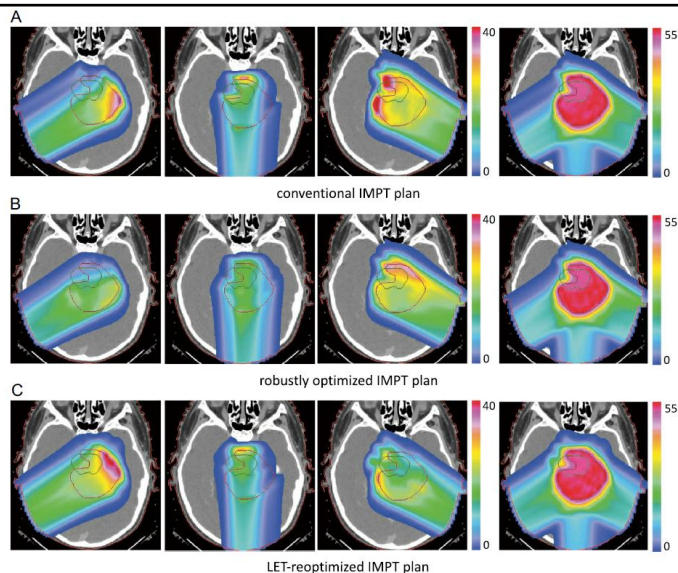
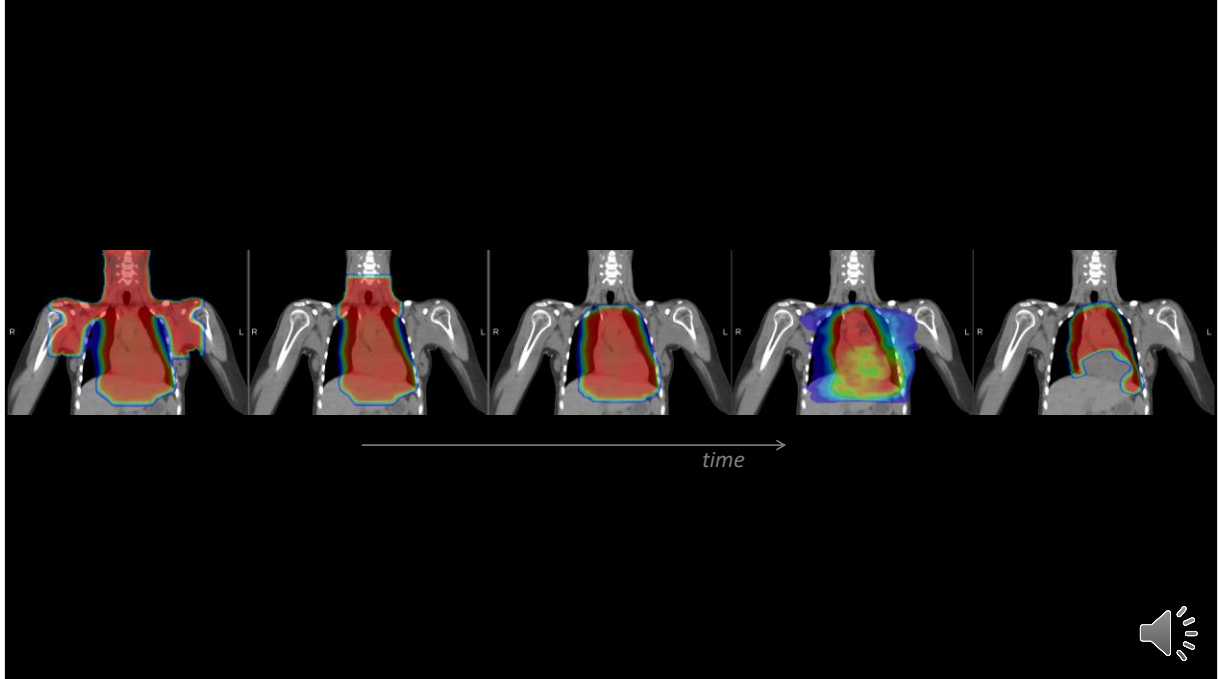


Figure 1 IMPT plans for an ependymoma patient in whom the target volume involves parts of the brainstem. The patient is treated with 3 posterior oblique beams. Pencil beams of approximately 3–5 mm sigma are assumed, corresponding to the latest generation of proton therapy machines. Shown is the dose distribution (right panel) and the dose contributions of the 3 beams. (A) conventional IMPT plan created based on a 2-mm CTV to PTV expansion. (B) Robustly optimized plan accounting for range uncertainty. (C) LET re-optimized plan obtained after minimizing LET \times dose in the brainstem while constraining the dose distribution to remain close to the conventional plan.



From PTV optimization we moved to robust optimization and soon to LET-optimization.



Remember what progress in radiotherapy means!