

Digital Radiographic Tomosynthesis QA/QC, Dosimetry, and More

John M. Sabol, PhD

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Disclosures

John Sabol is:

- Former employee of Sterling Diagnostic Imaging, now owned by Agfa Healthcare.
- Former employee of GE Healthcare.
- Currently employed by Konica Minolta Healthcare.

Input for this presentation has been kindly received from employees of Agfa, Carestream Health, GE Healthcare, and Shimadzu Medical Systems

The views expressed on this presentation are my own and do not necessarily reflect those of any commercial entity.

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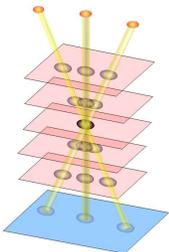
- Tomosynthesis Imaging
- Parameters and Artifacts
- Clinical Applications
- Dosimetry
- Features of Available Systems
- QA/QC

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Classical Tomography

Synchronously move the x-ray source and detector so that one plane of the object remains in focus



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Classical Tomography

Technique invented by Ziedses des Plant in 1932 for Temporal Mandibular Joint Imaging

Implemented on fluoroscopy systems

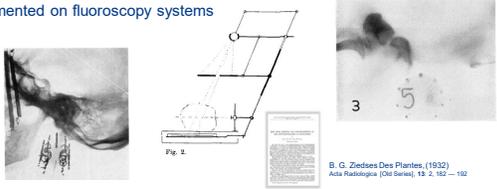


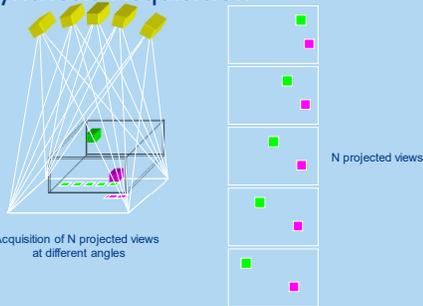
Fig. 5.

B. G. Ziedses Desi Planten. (1932) Acta Radiologica (Old Series), 13, 2, 192 - 192

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Tomosynthesis Acquisition



Acquisition of N projected views at different angles

N projected views

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Tomosynthesis: Image Reconstruction

Reconstruction of a slice close to the detector

Step 1: Small shift

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Tomosynthesis: Image Reconstruction

Step 2: Add

Reconstruction of a slice close to the detector

Step 1: Small shift

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Tomosynthesis: Image Reconstruction

2: Add

Reconstruction of a slice far from the detector

1: Large shift

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Tomosynthesis Image Reconstruction

- Reconstruction Algorithms:
 - Shift-and-Add (the digital equivalent to linear tomography)
 - ART (Algebraic Reconstruction Techniques)
 - Iterative Methods (MLEM)
 - Filtered Backprojection
 - Feldkamp limited angle cone beam tomography
 - Matrix Inversion tomosynthesis (MTS)

Why is specialized reconstruction needed?

Intuitive Explanation:
 Backprojection, or shift-and-add, causes blurring
 > Correct blurring with an inverse filter
 > Ram-Lak filter

In Practice:

- Higher frequencies are apodized to minimize noise.
- Filter shape can be customized for different exam types
 - e.g.: bone detail vs. pulmonary

Sample practical Inverse filter

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Linear Tomogram vs. Tomosynthesis

Linear Tomogram

Tomosynthesis

Linear Tomogram

Tomosynthesis

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Tomosynthesis: Iterative Reconstruction

Some artefacts in this plane originate from objects in a different plane

Reconstructed plane

Assume the reconstructed plane is the reality.....
 what would

The differences between the measured projections and the synthetic projections are used in the next iteration to reduce image imperfections

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Tomosynthesis – Acquisition Parameters

- Sweep Angle
- Number of Projections
- Sweep Direction
- Sweep Speed
- Pixel Binning
- Dose

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Tomosynthesis – Reconstruction Parameters

- Start & stop heights – anatomy covered
- Slice pitch and thickness
- Slice averaging, slab thickness
- Pixel Binning
- Reconstruction method (e.g.: FBP, Iterative, ...)

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Potential Artifacts & Adjustable Parameters

Image artifacts	Imaging parameters
Blurring artifact	Slice interval
Ripple artifact	Sweep direction
Ghost artifact	Projection density $(= \frac{\text{Number of Projections}}{\text{Sweep Angle}})$
Metallic artifact	Sweep direction
Motion artifact	Number of Projections, Sweep speed
Limited depth resolution	Sweep angle

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Blurring

Blurring occurs along the sweep direction and results from imaging a high contrast structure that exists out of the slice plane continuously perpendicular to the sweep direction.

Note the two surgical nails.
 Blurring appears different depending on the sweep direction

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Slice Interval – Effect on blurring artifact

To optimize DT blurring artefact, a small slice interval through the metal hardware should be used as a reconstruction parameter.

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Ripple

Ripple occurs by a similar mechanism as blurring and is a result of the limited number of projections in a sweep.

Ripple is caused by high contrast structures far out of the image plane whose contribution to the plane in focus is not sufficiently blurred or filtered because of limited projection density.

$$\text{Projection Density} = \frac{\text{No. of Projections}}{\text{Sweep Angle}}$$

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Ripple Artifact

Ripple artifact is reduced/removed with increased projection density

Sweep angle	No. of projections	Projection density
a 40°	30	0.75
b 40°	40	1.00
c 40°	60	1.50

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Ripple artifact

Another example of increasing the projection density to minimize DT ripple artifact

Projection Density = $\frac{30}{40^\circ} = 0.75$

Projection Density = $\frac{60}{30^\circ} = 2.00$

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Blurring or Ripple?

Blurring changes into ripple as the distance from the ripple source (a high contrast structure) to the reconstructed plane increases.

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Ghost artifact

Ghost artifact results from a high contrast structure that exists out of the slice plane and has a long axis parallel to the sweep direction.

With incorrect sweep direction, the out of the plane fibula is insufficiently blurred and appears as ghost image in the right image.

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Metal Artifact

Metallic artifact (→) occurs along the sweep direction in DT.

DT with a cranio-caudal sweep direction can offer detailed information regarding loosening around a prosthesis stem with much less metallic artifact compared to CT.

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Machida, Haruhiko, Toshiyuki Yuhara, Takako Mori, Eiko Ueno, Yoshio Moribe, and John M. Sabol, "Optimizing parameters for full-panel detector digital tomosynthesis," *RadioGraphics*, 36(2): 2015, 549-552.

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Metal Artifact Reduction (MAR)

Projection Domain Segmentation Approach

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MAR Results

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Zhaoxia Zhang, Ming Yan, Kun Tao, Xiao Xuan, John M. Sabol, and Hao Lai "Metal artifact reduction in tomosynthesis imaging," *Proc. SPIE 9412, Medical Imaging 2015: Physics of Medical Imaging*, 94125A.

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MAR Results

	In-plane	6mm off center	20mm off center
No MAR			
With MAR			

Undershooting Reduction Blurring Reduction Ripple Reduction

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T-smart – Iterative Metal Artifact reduction

Iterative reconstruction with user adjustable levels

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Motion Artifact

Tomosynthesis exams take between 2-12 sec to acquire
 Patient motion can be a significant problem

Clinical experience shows that gross patient motion can be a problem
 When high resolution is required (e.g.: sinus)
 Pediatric imaging

Interestingly, cardiac motion does not create diagnostically significant artefacts

Patient immobilization devices can be helpful

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High Speed Acquisitions

If patient immobilization is not feasible, high speed acquisition may help

Carestream and Shimadzu offer high speed acquisitions using fewer projection images

e.g.: Shimadzu Multi-purpose G4 system:

- Default exam: 17° FOV, 76 projections, 2 x 2 binning, (5.0 sec)
- Fast Exam: 17° FOV, 38 projections, 2 x 2 binning, (2.5 sec) half dose of default

Can be combined with other parameters:

e.g.: Shimadzu Multi-purpose G4 system:

- Chest: 40°, 'fast'
- Broncho: 20°, 'slow'



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Limited Depth Resolution



Abnormal opacity (→) seems to exist in the frontal sinus due to partial volume effect of the adjacent bony structure on coronal DT (Left), although this sinus is actually clear (→) on sagittal DT (Right)

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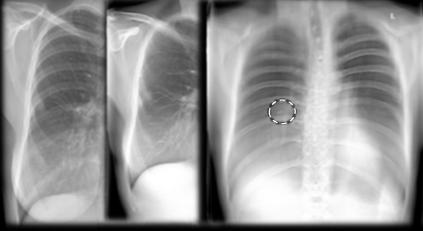
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Case 52: Multi-Center Clinical Trial



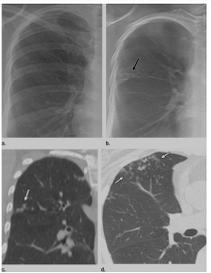
True Positive Nodule Finding

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TB Detection

- ~3 million deaths per year...
- more than any other infectious agent
- leading cause of death among people with HIV/AIDS.
- Significant global health challenge
- Sputum test is current gold standard for diagnosis, but takes weeks
- Chest x-rays are routinely used for detection, but lack sensitivity, specificity
- Kim, Chung, *et al* Radiology 2010 demonstrated:
 - Significantly improved accuracy of Tomosynthesis compared to CXR
 - Greatly improved sensitivity for cavity detection (76% vs. 19%)



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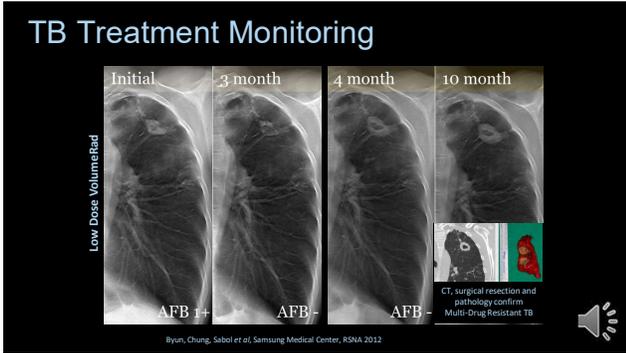
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TB Treatment Monitoring

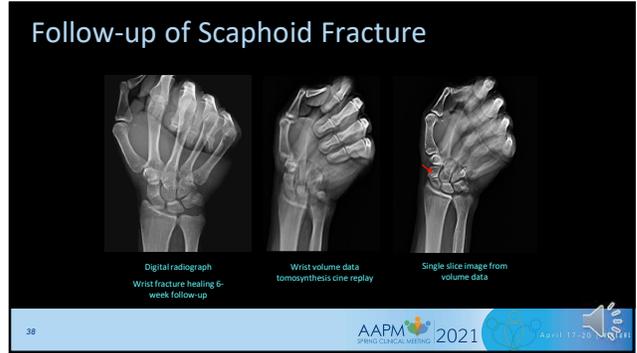
	Initial	2 Month F/U
CXR		
Low Dose Volumetric		

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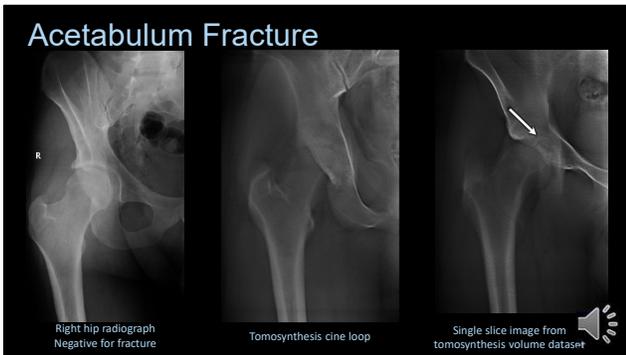
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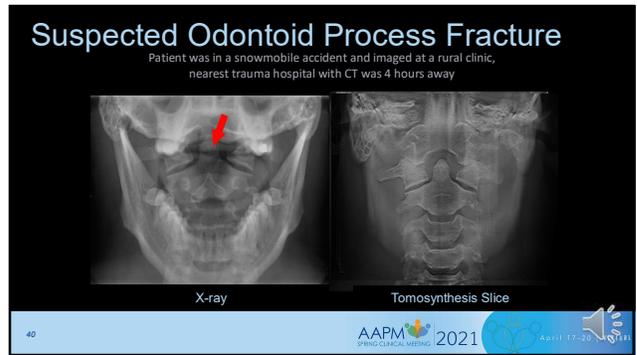
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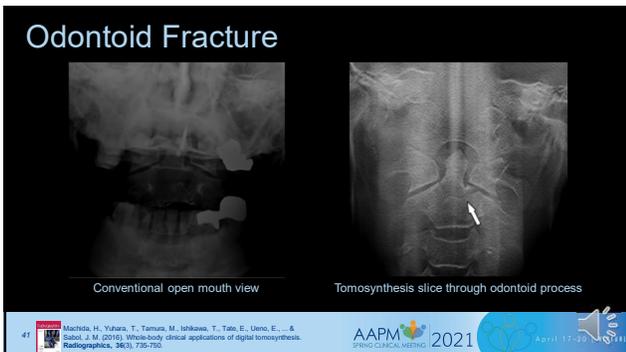
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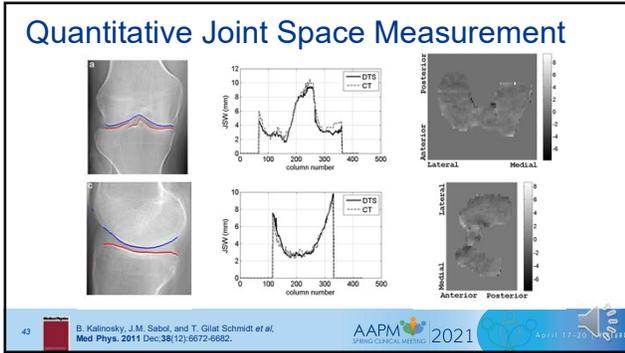
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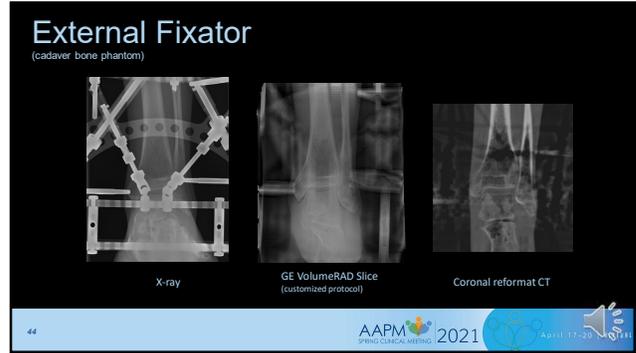
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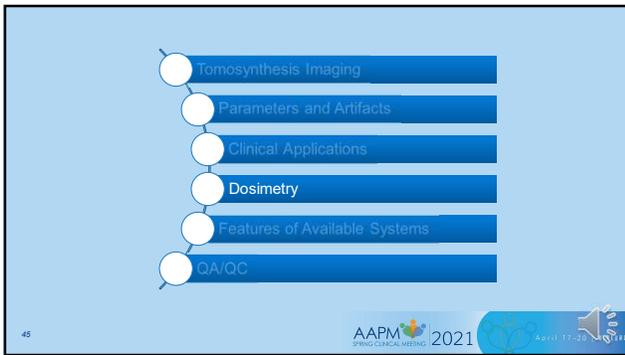
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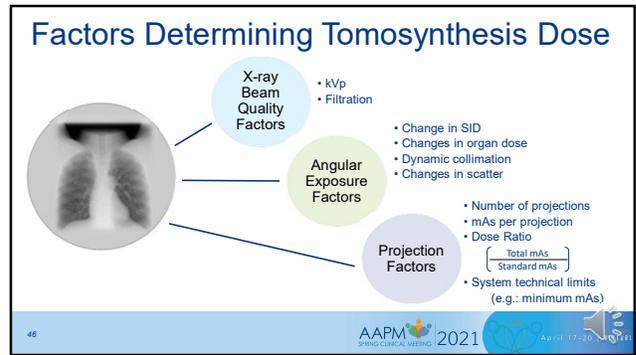
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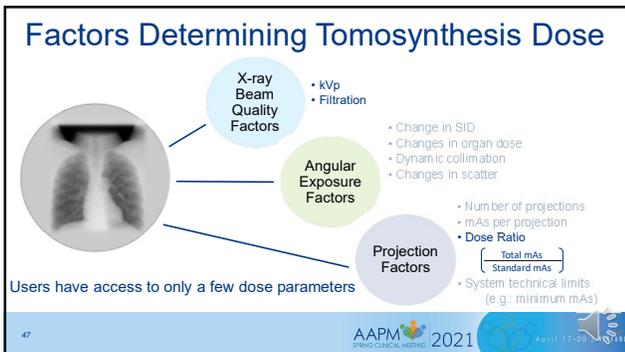
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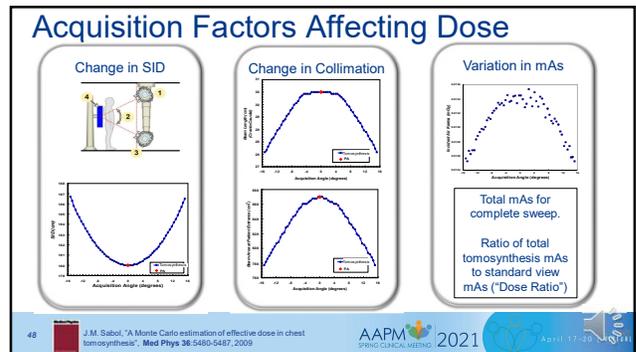
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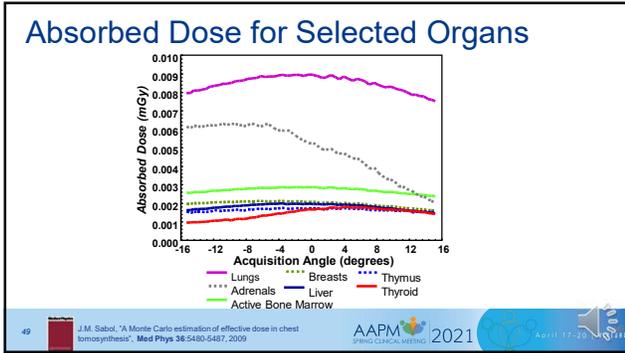
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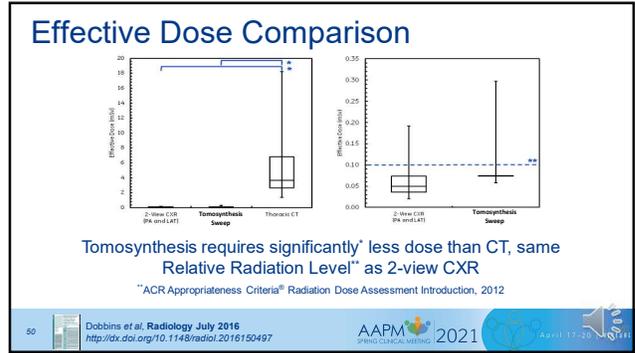
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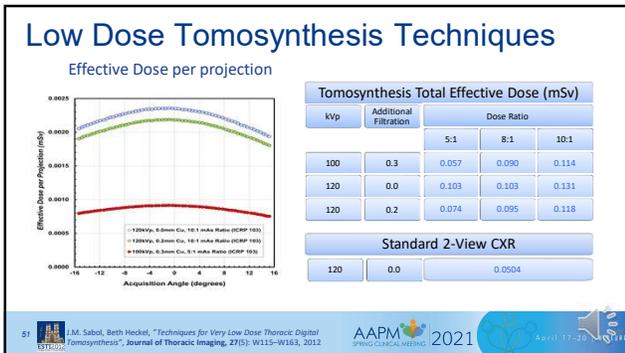
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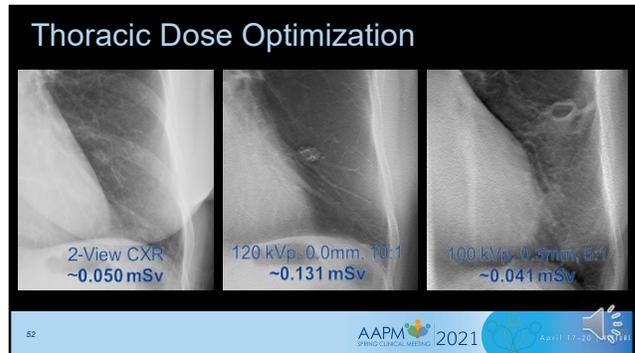
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Sinus Imaging and Radiation Dose

- Prevalence of sinusitis is estimated to be ~14% of general population, ~32% in young children
- 31 million individuals diagnosed each year in US
- Definitive diagnosis and treatment recommendations are often based on CT findings
- Increasing recognition of sensitivity of the eye lens to radiation damage
- Radiation cataractogenesis is deterministic with threshold of 0.5 Gy (ICRP ref 4825-3093-1464)

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Sinonasal Exam Dose Measurement

- Alderson-RANDO phantom scanned covering frontal to maxillary sinus using the clinically routine protocol by MDCT and tomosynthesis
- Measured the dose of internal organs (brain, submandibular and thyroid glands) and on the surface at various sites including the eyes using glass dosimeters

	MDCT (μ Gy)	Tomosynthesis (μ Gy)	MDCT/DT Dose Ratio
Eye	32500 \pm 2500	112 \pm 6	290
Skin	20000 \pm 9300	1160 \pm 2100	17
Submandibular gland	17000 \pm 2300	1400 \pm 80	12
Brain	14300 \pm 2200	1770 \pm 560	8
Thyroid gland	1230 \pm 160	230 \pm 90	5

54 Machida et al. "Radiation Dose of Digital Tomosynthesis for Sinonasal Examination: Comparison with MDCT", *European Journal of Radiology*, 81(6), Pages 1140-1145, 2012

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Dose from Abdominal Exams



Effective Dose

Exam Type	Effective Dose (mSv)
KUB	0.63
Tomographic Image	1.1
IVP / KUB with Tomograms	3.93
Stone Protocol CT	3.04
Digital Tomosynthesis	0.63

Mermuys et al.:
 Clinical study of detection of urinary stones: 0.85 mSv for DTS (~1.7 times DR, 7-34% of CT)

K. Mermuys et al.: "Digital Tomosynthesis in the detection of urolithiasis: diagnostic performance and dosimetry compared with digital X-ray using MDCT as a reference" *AJR* 195:161-167, 2010

Astroza GM, Lipkin ME et al.: "Radiation exposure in the follow-up of patients with urolithiasis comparing digital tomosynthesis, non-contrast CT, standard KUB, and IVP." *J Endourol* 2013 Oct;27(10):1187-91. doi: 10.1097/end.2013.0255

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Dose from MSK Exams

Two studies of lateral thoracic spine exam Effective Dose (mSv)

	Svalkvist	Geijer
AP	0.07	0.10
LAT	0.13	0.11
Scout	0.05	0.11
Tomosynthesis	0.47	0.66
Total T-Spine Exam:	0.57	0.87
CT		6.6

Geijer, M. et al.: "Tomosynthesis of the thoracic spine: added value in diagnosing vertebral fractures in the elderly." *European Radiology* (2016): 1-7.

Svalkvist A, Söderman C, Båth M.: "Effective Dose To Patients From Thoracic Spine Exams With Tomosynthesis." *Radiat Prot Dosimetry*. 2016 Jun;169:274-80.



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Extremity Dose Results

Noël, A., Ottenin MA, Blum A. et al Nancy Université:

- Study of wrist imaging
- 2 tomo views, 5 conventional radiography views
- Tomo uses 25% of radiographic exam dose
 - (0.72 compared to 0.96 mGy)
- 28 times lower than CT exam dose

Canella et al Lille FR:

- Clinical study of rheumatoid arthritis of the wrist
- 0.1166 µSv (~2.6 times DR)

R.E. Gazaille, M. Flynn et al Henry Ford Hospital:

- Monte Carlo simulation of hip tomosynthesis
- 0.24 mSv per view, (typical exam of 3 views)
- ~3-4 times dose of radiographic exam dose
- ~10% of CT exam dose

Noël, A., Ottenin MA, Germain C, Soler M., Vitani N, Grosjeune O, Blum A et al.: "Comparison of irradiation for tomosynthesis and CT of the wrist." *Journal de Radiologie* 92.1 (2011): 32-39.

Canella et al.: "Use of Tomosynthesis for Erosion Evaluation in Rheumatoid Arthritic Hands and Wrists." *Radiology* 258: 199-205, 2011

R. E. Gazaille et al.: "Technical Innovation: Digital Tomosynthesis of the Hip Following Intra-articular Administration of Contrast". *Skeletal Radiology* 40, 1467-1471, 2011



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AAPM TG 223 and TG 321 Dosimetry in Tomosynthesis Imaging

Charge: Develop methods to estimate dose from mammographic and radiographic tomosynthesis exams.

- Compute normalized dose data for relevant acquisitions
- Obtain absolute dosimetry values for anthropomorphic phantoms
- Enable routine QC/QA measurements and information that can be communicated by physicist to physician/patient

Med. Phys. 41 091501 (2014): <http://dx.doi.org/10.1118/1.4892600>



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Body Exam Phantoms and Protocol

Pediatric: 1, 5, 10, 15 yrs
 Adult: 10th, 50th, 90th percentile
 Both Male and female
 28 phantoms in total

Exam	View	Table	Wallstand
Spine	C-Spine	AP	Table
		Left Lateral	Table
	T-Spine	AP	Table
		Left Lateral	Table
	L-Spine	AP	Table
		Left Lateral	Table
Abdomen	Hip	AP Hip, Proximal Femur	Table
		Wallstand	Table
	Abdomen	AP Supine	Table
Extremity	Knee	PA Bilateral	Wallstand
		AP Bilateral	Table

Head and Neck	Sinus/Facial Bones	PA Caldwell	Table	Wallstand
Thoracic	Chest	PA Waters	Table	Wallstand
		Lateral	Table	Wallstand
		PA	Table	Wallstand
		Left Lateral	Table	Wallstand
		AP Supine	Table	Wallstand

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The dose of body tomosynthesis exams is:

- Dependent on numerous acquisition factors that include:
 - The same factors that impact projection x-ray (spectra, technique etc)
 - Angular exposure factors (changes in SID, dynamic collimation, scatter)
 - Projection factors (Number of projections, dose per projection, ...)
- Total dose from all views is comparable for tomosynthesis and projection radiography for most exams
 - In a clinical trial, a chest tomosynthesis acquisition required ~2% of the dose of CT, comparable to a two-view x-ray exam
- More understanding, accuracy, and consistent reporting is required
 - AAPM TG#321 will provide data for research and clinical communication

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Comparison of Some Commercial Systems

	AGFA	Carestream	Fujifilm Healthcare	GE	SHIMADZU
System Type	Multi-purpose Radiographic	Radiographic	Radiographic	Radiographic	Multi-purpose Radiographic
Sweep angle	15° 22° 30°	40°	10° – 60°	20° – 40°	MP: 8° 20° 30° 40° R: 20° 30° 40° 60°
Maximum Number of Projections	40	80	60	60	76
Binning	1 x 1 (148 µm)	1 x 1 (139 µm) 2 x 2 (278 µm)*	N/A	1 x 1 (200 µm)	1 x 1 (139 µm) 2 x 2 (278 µm)
Reconstruction	Iterative	Feldkamp	N/A	FBP	Shift and Add FBP Iterative

* Selected on reconstruction, independent of acquisition

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Notable system features

- Systems require a scout or prescan image
 - Serves as standard projection image
 - Used to determine mAs technique for sweep
- High Speed acquisition option:
 - Reduced number of projections to minimize motion artefacts
- Change reconstruction post-acquisition
 - Alter layer height, slice thickness, slice pitch, reconstruction method, and dynamic range
- Shimadzu offers Oblique plane reconstruction
- Shimadzu detector can move, preventing collimator cut-off and increasing FOV



Shimadzu oblique plane reconstruction (±20°)

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QA/QC

Carestream

Provides users with a geometry calibration phantom

- Machine calibration
- QC check of overall system tomosynthesis functionality



No recommended QA or QC procedures (other than those for regular system and detector functionality)

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***Thank you for your attention,
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Ken Brown, Charles Cassidakis (Shimadzu Medical Systems)***

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