### Bottleneck Issues in Proton Monte Carlo Clinical Implementation and Companion Imaging Techniques – Report of NRG Survey Results

Liyong Lin, PhD, DABR, FAAPM, Associate Professor Department of Radiation Oncology, Emory University @Session "Bottleneck Issues in the Clinic Implementation of Monte Carlo Method in Proton Therapy" Virtual AAPM 2021 07/25/2021







# Two Following Talks in Session

 Jan Schumann "Proton Monte Carlo Platforms – The way towards treatment planning and latest developments"

 Shuai Leng "Dual Energy CT and Metal Artifact Reduction -Fundamentals and Recent Development"









# Why NRG survey?

• No publication about how proton therapy centers implement Monte Carlo (MC) and complimentary imaging

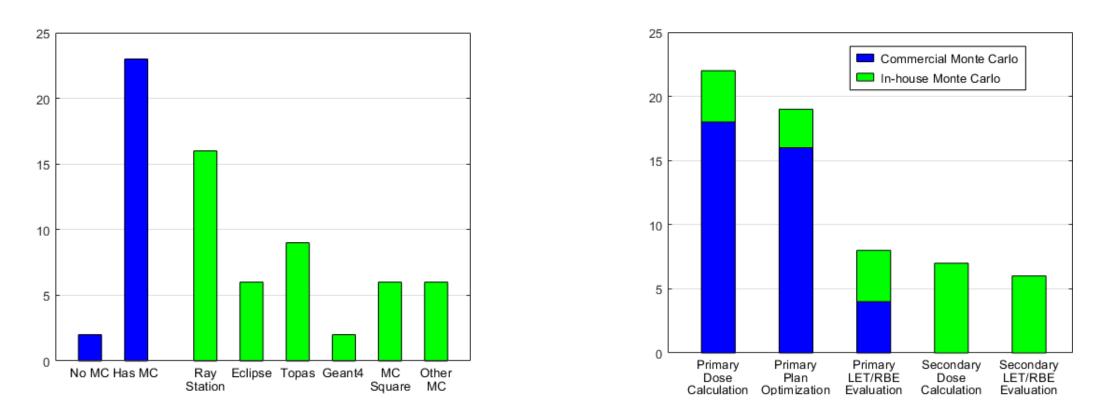
• Current practice pattern assessment is required to determine the feasibility of including them in clinical trials.

Lin et al "NRG Oncology Survey of Monte Carlo Dose Calculation Use in US Proton Therapy Centers" IJPT In Press

### Goals of NRG survey

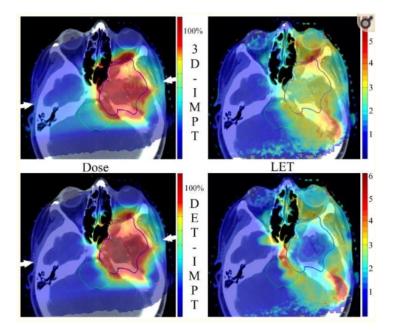
- Scope of MC utilization
- Validation methods in heterogeneous phantoms
- Clinical site-specific imaging guidance and proton range uncertainties
- How metal implants are handled in MC

### NRG survey result 1



- 1. 25/28 centers responded to the survey distributed on 5/13/19
- 2. Commercial Monte Carlo are in the super majority

### Discussion of survey results 1a



$$LET_d(v) = rac{\sum\limits_{events} dE \cdot (dE/dx) rac{1}{
ho}}{\sum\limits_{events} dE} \qquad \qquad LET_d(v) = rac{\sum\limits_F LET_d^F(v) imes D_F(v)}{\sum\limits_F D_F(v)}$$

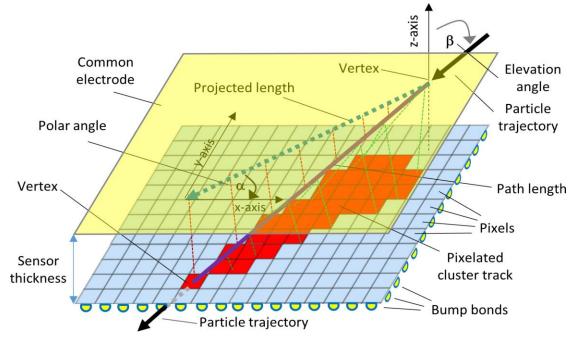
3D modulation IMPT (3D-IMPT) vs. Distal Edge Tracking IMPT (DET-IMPT).(a) In DET-IMPT the optimization routine assigns weights only to the distal beam spots, fewer # of spots.

(b) In 3D-IMPT, Bragg peaks are selected that cover the whole target volume.

- 1. Dose-averaged LET (LETd) should be considered for central serial OAR (brainstem as shown; optic chiasm, rectum and bladder Not shown )
- 2. LET feature is not available at current clinical commercial MC but they are available at in house and research versions.
- 3. RBE (relative biological effectiveness): Paganetti "Report of the AAPM TG-256 on the relative biological effectiveness of proton beams in radiation therapy" Medphys 2019

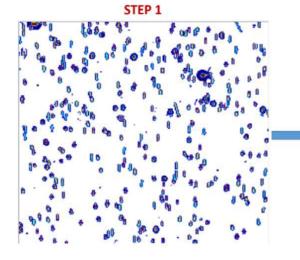
Grassberger et al "Variations in linear energy transfer within clinical proton therapy fields and the potential for biological treatment planning" IJROBP 2011

### Discussion of survey results 1b



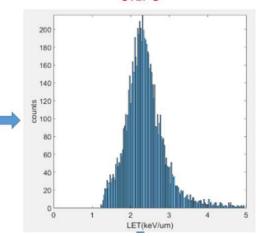
LET distributions can be detected by pixelated proton counting detectors by characterizing simultaneous events extracting multi parameters at micron and nano second levels.

- Granja C et al 2018 Resolving power of pixel detector Timepix for wide-range electron, proton and ion detection Nucl. Instrum. Methods Phys. Res. A 908 60–71
- 2. Charyyev S et al 2021 A novel proton counting detector and method for the validation of tissue and implant material maps for Monte Carlo dose calculation Phys. Med. Biol. 045003

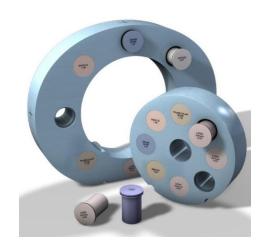


Timestal	and T3P	- 11	DA -									
Coincl			Size	Volu	me Cente	eX Cente	rY MaxV	al MaxT	ine MaxX P	LAXY F	latness	ć.
1 1	84467440	37095	51570	1	3.04383	2	169	3.04383	-46,875	2	169	
1 1	84467448	37095	51584	1	7.77391	117	83	7.77391	-32.8125	337	83	
1 1	844674482	37895	51584	1	10.4383	180	62	18,4383	32.8125	180	62	
1 1	84467440	137095	51584	1	29.2925	117	80		-32.8125	117	88	
1 1	84467440	27095	51585	1	21.6693	118	87	21.6693	-31.25	118	87	
	84467448			. 9	405.874	22.038	86.7471	130.347	-31.25	22	87 8.	
	844674483			. 9	726.419	22	68.5898	107.911	-31.25	22	69 0.	
	84467440			27	1043.02	152.427	16.3517		-29.6875	153	20	
1 1	84467440	37095	51587	1	4.43289	57	28	4.43289	-29.6875	57	28	
1 1	844674482	37895	51591	13	390.437	147.761	144.219	94.8466	-29.6875	148	147 0.	
1 1	84467448	37095	51588	15	951.489	151.305	157.658	123.902	-29.6875	151	161 0.	
1 1	84467448	37895	51588	1	4.48442	155	170	4.40442	-28.125	155	170	
1 1	84467448	37095	51588	1	7.96442	251	13	7.96442	-28.125	251	13	
	844674483			1	4.32131	251	9	4.32131	-28.125	251	9	1
1 1	84467448	37895	51588	1	24.0903	155	176	24.8983	-28.125	155	176	
1 1	84467448	37095	51588	1	11.8226	155	172	11.8225	-28.125	155	172	
1 1	84467448	37095	51601	12	370.228	51.2586	235.334	88.7842	-9.375	51	238 0.	
1 1	84467440	37095	51588	2	26.5836	186	92.6127	16.289	-28.125	186	93 e.	
1 1	84467440	37095	51588	7	235.211	246.15	253.076	75.2949	-28.125	246	253 0.	
1 1	84467448	137095	51588	4	111.94	186	96.6673	42.7201	-28.125	186	98 0.	
1 1	84467440	37095	51588	12	\$49.421	88.5976	210.358	87.7649	-28,125	88	208 0	6
1 1	84467440	37095	51590	1	5.03509	53	204	5.03509	26.5625	53	204	
1 1	84467440	37895	51598	1	3.54073	61	23	3.54073	-26.5625	61	23	
1 1	84467440	37095	51590	1	16.1272	124	57	16.1272	-26.5625	124	57	
1 1	84467448	37095	51590	10	703.207	92.061	202.188	128.394	-26.5625	92	205 0.	
1 1	84467440	37095	51590	9	815.217	221	178.645	164.362	-26.5625	221	180 C.	
1 1	84467440	37095	51592	.9	234.24	31.1176	145.216	72.5566	+25	31	145	
1 1	84467440	37095	51593	21	938.301	223.954	142.534	138,745	-23.4375	224	146 e.	
1 1	84467448	37895	51591		635.958	31	110.104	98,4359	+25	31	109 C.	
1 1	844674483	37095	51593	5	129.699	96.0234	137.969	48.7919	-23.4375	96	139 e.	
1 1	84467448	37895	51593	8	147.575	65	213.14	47.6638	-23.4375	65	213 8.	

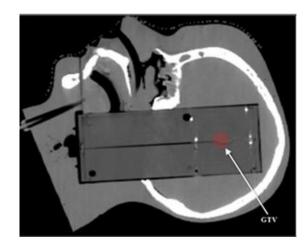
### STEP 3



### NRG survey result 2- Heterogenous validation



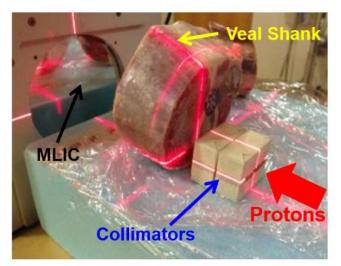
Electron density phantom (84%)



IROC phantom (92%)

Stoichiometric calibration

Heterogeneous validation

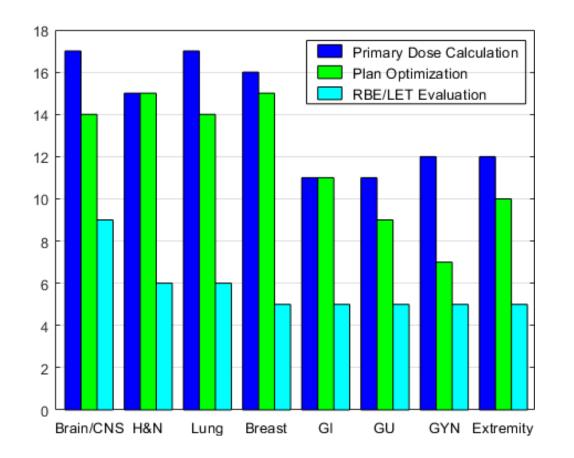


### Animal tissues (40%)



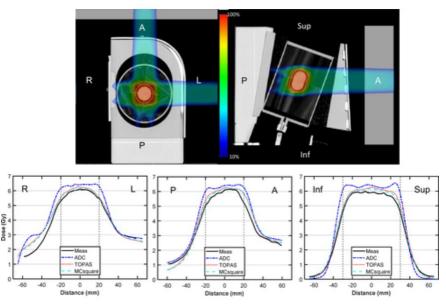
Animal tissues (28%)

### NRG survey result 3



- 1. 17/25 centers primary dose calculation while 15/17 primary dose optimization
- 2. More heterogenous sites used MC more often.
- 3. Some centers don't have MC optimization capability yet.

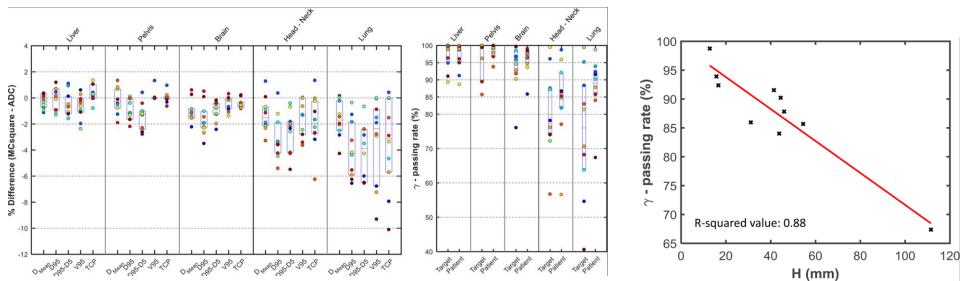
### Discussion of survey result 3



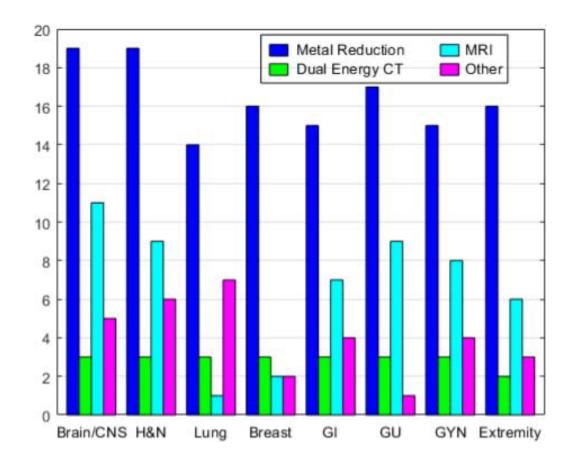
Two main issues of analytical dose calculations:

- Absolute output due to modelling of variable air gaps and large angle scattering of range shifters
- 2. Multi Coulomb scattering over heterogenous tissues (shown too sharp in analytical method)

Huang et al "Validation and application of a fast Monte Carlo algorithm for assessing the clinical impact of approximations in analytical dose calculations for pencil beam scanning proton therapy" Med Phys 2018

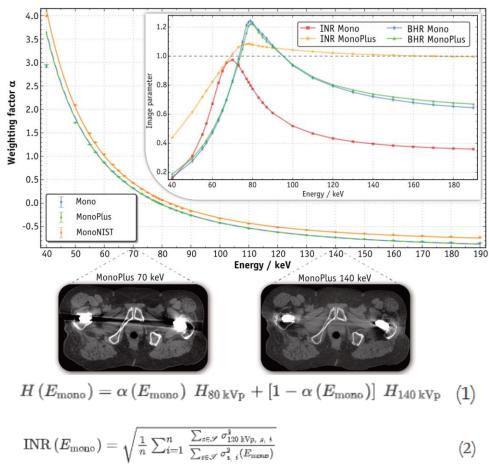


### NRG survey result 4



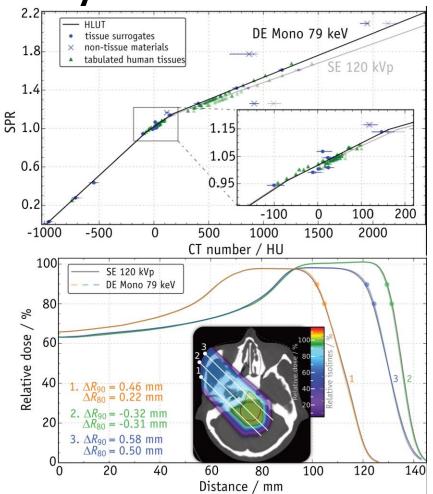
- 1. 19/25 centers used MAR but only 3/25 centers used DECT
- 2. 11/25 centers used MRI and 7/25 centers used other proton imaging methods

### Discussion of survey result-4a



and beam-hardening ratio (BHR):

$$\operatorname{BHR}\left(E_{\operatorname{mono}}\right) = \frac{\sum_{i}^{n} \left(\max_{s \in \mathscr{S}} \{H_{120 \text{ kVp}, s_{i}, i}\} - \min_{s \in \mathscr{S}} \{H_{120 \text{ kVp}, s_{i}, i}\}\right)}{\sum_{i}^{n} \left(\max_{s \in \mathscr{S}} \{H_{s_{i}, i}(E_{\operatorname{mono}})\} - \min_{s \in \mathscr{S}} \{H_{s_{i}, i}(E_{\operatorname{mono}})\}\right)}$$

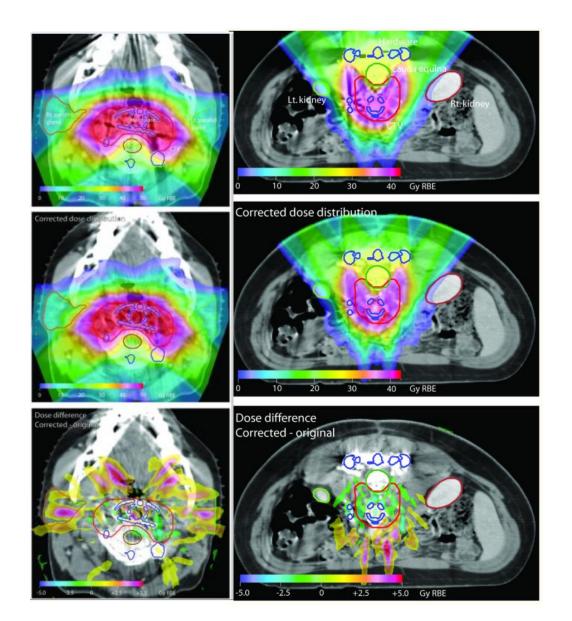


Issues for virtual mono energy images of 79 keV from DECT to replace SECT: (1) not optimal for implant (2) 140 keV images sub optimal INR and BHR

Wolfhart P "Clinical Implementation of Dual-energy CT for Proton Treatment Planning on Pseudo-monoenergetic CT scans" IJROBP 2017

(3)

### Discussion of survey result -4b



- 1. Compared Metal Artifact Reduction (MAR) images to images without MAR
- 2. Compared Analytical dose calculation to Monte Carlo method
- 3. Concluded that extra 10 mm treatment margins are needed
- 4. Limited to titanium implant & did NOT consider complex implant structure that contain materials beyond titanium
- 5. Did not consider residual artifacts in MAR images
- 6. Most clinics overwrite implant & surrounding tissues without consensus on how to overwrite (NRG surveys)

Vurberg et al "Dosimetric accuracy of proton therapy for chordoma patients with titanium implants" Med Phys 2013

### Acknowledgement

- NRG Proton Monte Carlo workgroup members
- AAPM TG-349 members
- Emory radiation oncology colleagues and trainees

### Thank you for your attention! Questions...





