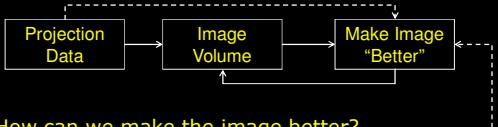


Iterative Reconstruction

- What is iterative reconstruction?

 A flowchart showing the iterative reconstruction process. It starts with "Projection Data" which feeds into "Image Volume". "Image Volume" then feeds into "Make Image 'Better'". "Make Image 'Better'" has a dashed arrow pointing back to "Image Volume", indicating a feedback loop. To the right of the main loop is a dashed box labeled "Desirable Image Properties".

- How can we make the image better?
 - Get a better match to the data
 - Requires a data model
 - Enforce desirable image properties
 - Encourage smoothness, edges, etc.
 - Need a measure of "better"

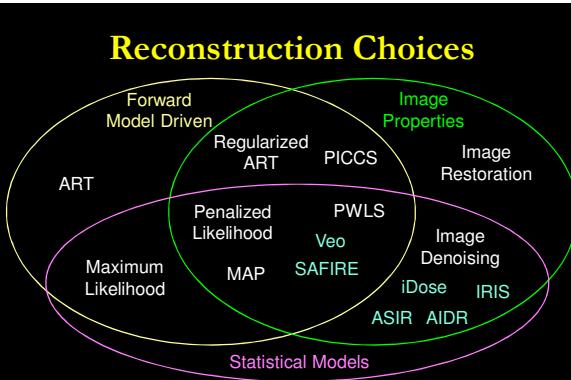
Building an Iterative Technique

- Define the objective
 - Find the volume that best fits the data and desired image quality
$$\text{volume} = \arg \max \{\|\text{data}, \text{model}\| \& \|\text{image properties}\|\}$$

$$\hat{\mu} = \arg \max \{\|y, \bar{y}(\mu)\| \& \|f(\mu)\|\}$$
- Devise an algorithm that solves the objective
 - Iteratively solve for $\hat{\mu}$
 - Decide when to stop iterating (and how to start)

Objective Function	Optimization Algorithm
--------------------	------------------------

Reconstruction Choices



A Venn diagram illustrating the relationships between different reconstruction methods. It features three overlapping circles:

- Forward Model Driven** (top circle): ART
- Statistical Models** (bottom circle): Maximum Likelihood
- Image Properties** (right circle): Image Restoration

The intersection areas represent hybrid or specific methods:

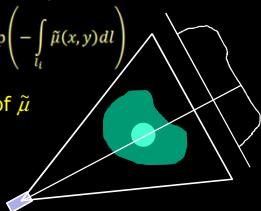
- Intersection of Forward Model Driven and Statistical Models: Regularized ART
- Intersection of Forward Model Driven and Image Properties: PICCS
- Intersection of Statistical Models and Image Properties: PWLS, Veo, SAFIRE
- Intersection of all three: MAP
- Region outside all circles but within the boundaries of the circles: Image Denoising, iDose, IRIS, ASIR, AIDR

*Disclaimer: The exact details of commercially available reconstruction methods are not known by the author.

Model-based Approaches

- Transmission Tomography Forward Model
 - Projection Physics, Beer's Law
$$P(\text{photon survives}) = \exp\left(-\int_{l_t} \tilde{\mu}(x, y) dl\right)$$

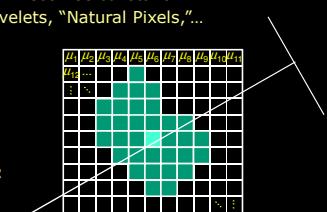
$$\bar{y}_t = E[\text{number of photons}] = I_0 \exp\left(-\int_{l_t} \tilde{\mu}(x, y) dl\right)$$
- Need a Parameterization of $\tilde{\mu}$



Parameterization of the Object

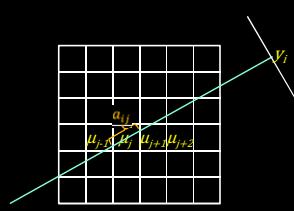
- Continuous-domain object
- Want finite number of parameters
- Choices of basis functions:
 - Point Samples - Bandlimited
 - Contours - Piecewise constant
 - Blobs, Wavelets, "Natural Pixels," ...
- Voxel Basis

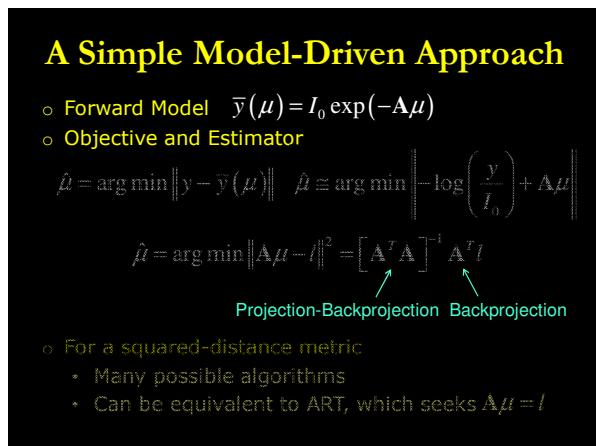
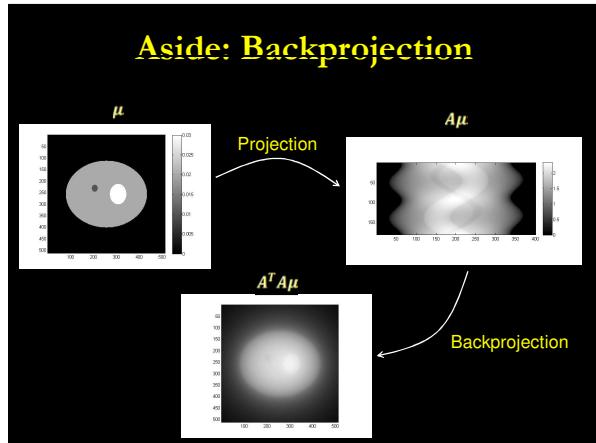
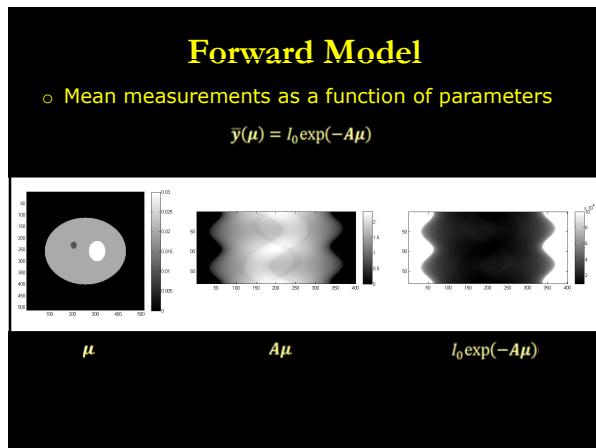
$$\boldsymbol{\mu} = \begin{bmatrix} \mu_1 \\ \mu_2 \\ \vdots \\ \mu_p \end{bmatrix}$$

$$\tilde{\mu}(x, y) \cong \mathbf{B}\boldsymbol{\mu}$$


Projection

- Linear operation $\bar{y}_t = I_0 \exp\left(-\int_{l_t} \tilde{\mu}(x, y) dl\right)$
- Discrete-Discrete for parameterized problem
$$\bar{y}_t = I_0 \exp\left(-\sum_{j=1}^p a_{ij} \mu_j\right)$$
- System matrix

$$\mathbf{A} = \begin{bmatrix} a_{11} & \cdots & a_{1j} & \cdots & a_{1p} \\ \vdots & \ddots & \vdots & & \vdots \\ a_{i1} & \cdots & a_{ij} & \cdots & a_{ip} \\ \vdots & & \vdots & \ddots & \vdots \\ a_{n1} & \cdots & a_{nj} & \cdots & a_{np} \end{bmatrix}$$




Flexibility of Iterative Methods

$$\hat{\mu} = \arg \min \|A\mu - l\|^2 = [A^T A]^{-1} A^T l$$

- For a well-sampled, parallel beam case

$$A^T A x \approx \frac{1}{r} * * x \rightarrow [A^T A]^{-1} x \approx F^{-1} \{[\rho_{ab}]\} * * x$$

- For other cases

$$[A^T A]^{-1} A^T l$$

- Iterative methods implicitly handle the geometry

- Find the correct inversion for the specific geometry
- Cannot overcome data nullspaces (needs complete data)

More Complete Forward Models

- More physics

- Polyenergetic beam, energy-dependent attenuation
- Detector effects, finite size elements, blur
- Source effects, finite size element
- Scattered radiation

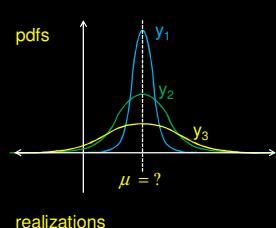
- Noise

- Data statistics
- Quantum noise – x-ray photons
- Detector Noise

Toy Problem

3 Random Variables
Different std dev ($\sigma_1, \sigma_2, \sigma_3$)

Best way to estimate μ ?



Maximum Likelihood Estimation

- Find the parameter values most likely to be responsible for the observed measurements.

- Properties
 - Asymptotically unbiased and efficient under general conditions

- Likelihood Function

$$L(y; \mu) = p(y_1, y_2, \dots, y_N | \mu_1, \mu_2, \dots, \mu_M)$$

- Maximum Likelihood Objective Function

$$\hat{\mu} = \arg \max L(y; \mu)$$

ML Estimate for the Toy Problem

Likelihood function: $L(y, \mu) = p(y_i | \mu) = \prod_{i=1}^3 p(y_i | \mu)$

$$p(y_i | \mu) = \frac{1}{\sqrt{2\pi\sigma_i^2}} \exp\left[-\frac{1}{2\sigma_i^2}(y_i - \mu)^2\right]$$

Log-Likelihood function:

$$\log L(y, \mu) = -\frac{1}{2} \sum_{i=1}^3 \log(2\pi\sigma_i^2) - \sum_{i=1}^3 \frac{1}{2\sigma_i^2} (y_i - \mu)^2$$

Maximize over μ : $\hat{\mu} = \arg \max \log L(y; \mu)$

$$\frac{\partial}{\partial \mu} \log L(y, \mu) = \sum_{i=1}^3 \frac{1}{2\sigma_i^2} (y_i - \mu)^2 \iff \boxed{\hat{\mu} = \frac{\sum_{i=1}^3 \frac{y_i}{\sigma_i^2}}{\sum_{i=1}^3 \frac{1}{\sigma_i^2}}}$$

ML for Tomography

- Need a noise model
- Depends on the statistics of the measurements
- Depends on the detection process
- Common choices
 - Poisson – x-ray photon statistics
 $y_i \sim \text{Poisson}[\bar{y}_i(\mu)] \quad P_{\mathcal{H}} = \exp[-\bar{y}_i(\mu)] \frac{[\bar{y}_i(\mu)]^{y_i}}{y_i!}$
 - Poisson-Gaussian mixtures – photons + readout noise
 $y_i \sim \text{Poisson}[\bar{y}_i(\mu)] + N(0, \sigma_{r0}^2)$
 - Gaussian (nonuniform variances) – approx. many effects
 $y_i \sim N(\bar{y}_i(\mu), \sigma_i^2) \quad P_{\mathcal{H}} = \frac{1}{\sqrt{2\pi\sigma_i^2}} \exp\left(-\frac{1}{2\sigma_i^2}(y_i - \bar{y}_i(\mu))^2\right)$

Poisson Likelihood Function

- Marginal Likelihoods

$$p(y_i|\mu) = \exp[-\bar{y}_i(\mu)] \frac{[\bar{y}_i(\mu)]^{y_i}}{y_i!}$$

- Likelihood

$$L(\mathbf{y}; \mu) = p(\mathbf{y}|\mu) = \prod_{i=1}^N p(y_i|\mu) = \prod_{i=1}^N \exp[-\bar{y}_i(\mu)] \frac{[\bar{y}_i(\mu)]^{y_i}}{y_i!}$$

- Log-Likelihood

$$\log L(\mathbf{y}; \mu) = \sum_{i=1}^N y_i \log \bar{y}_i(\mu) - \bar{y}_i(\mu) - \log y_i!$$

- Objective Function

$$\hat{\mu} = \arg \max \log L(\mathbf{y}|\mu)$$

Gaussian Likelihood Function

- Marginal Likelihoods

$$l_i = -\log \left(\frac{y_i}{I_0} \right) \quad p(l_i|\mu) = \frac{1}{\sqrt{2\pi\sigma_i^2}} \exp \left[-\frac{1}{2\sigma_i^2} (l_i - [\mathbf{A}\mu]_i)^2 \right]$$

- Likelihood

$$L(l|\mu) = p(l|\mu) = \prod_{i=1}^N p(l_i|\mu) = \prod_{i=1}^N \frac{1}{\sqrt{2\pi\sigma_i^2}} \exp \left[-\frac{1}{2\sigma_i^2} (l_i - [\mathbf{A}\mu]_i)^2 \right]$$

- Log-Likelihood

$$\log L(l|\mu) = \sum_{i=1}^N -\frac{1}{2\sigma_i^2} (l_i - [\mathbf{A}\mu]_i)^2$$

- Objective Function and Estimator

$$\hat{\mu} = \arg \max \log L(l|\mu) = \left[\mathbf{A}^T \mathbf{D} \begin{bmatrix} \frac{1}{\sigma_1^2} & \dots & \frac{1}{\sigma_N^2} \end{bmatrix} \mathbf{A} \right]^{-1} \mathbf{A}^T \mathbf{D} \begin{bmatrix} \frac{1}{\sigma_1^2} & \dots & \frac{1}{\sigma_N^2} \end{bmatrix} l$$

Iterative Algorithms

- Plethora of iterative approaches

- Expectation-Maximization – General Purpose Methodology
- Gradient-based Methods – Coordinate Ascent/Descent
- Optimization Transfer – Paraboloidal Surrogates
- Ordered-Subsets methods

- Properties of iterative algorithms

- Monotonicity
- True convergence
- Speed
- Complexity

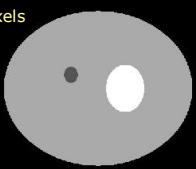
Statistical Reconstruction Example

o Test Case

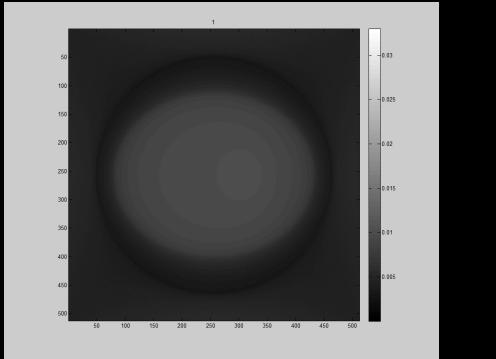
- Single slice x-ray transmission problem
- 512 x 512 0.3 mm volume
- 400 detector bins over 180 angles (360 degrees)
- Poisson noise: 1e5 counts per 0.5 mm detector element
- SO: 380 mm, DO: 220 mm

o Reconstruction

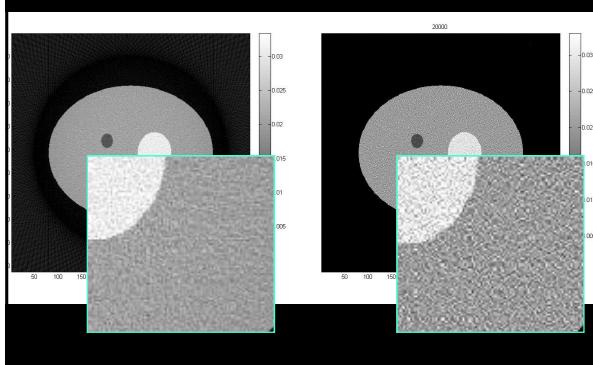
- Voxel basis: 512 x 512 0.3 mm voxels
- Maximum-likelihood objective
- EM-type algorithm
- Initial image – constant value
- Lots of iterations



ML-EM Iterations



FBP vs ML-EM Comparison



Enforcing Desirable Properties

- o FBP
 - Filter designs – cutoff frequencies
- o Iterative methods
 - Modify the objective to penalize "bad" images
 - Discourage noise
 - Preserve desirable image features
 - Other prior knowledge
- o Image-domain Denoising

$$\hat{\mu} = \arg \max F(\mu) - \beta R(\mu)$$
- o Model-based Reconstruction

$$\hat{\mu} = \arg \max F(y, \mu) - \beta R(\mu)$$

Local Control of Image Properties

- o Pairwise Penalty
 - Penalize the difference between neighboring voxels
$$R(\mu) = \sum_j \sum_{k \in N} w_{jk} \psi(\mu_j - \mu_k)$$

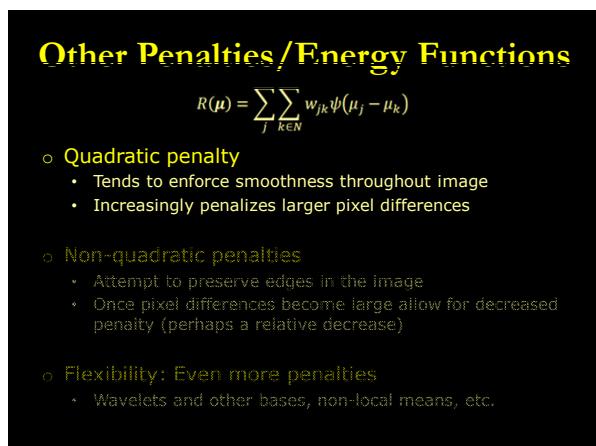
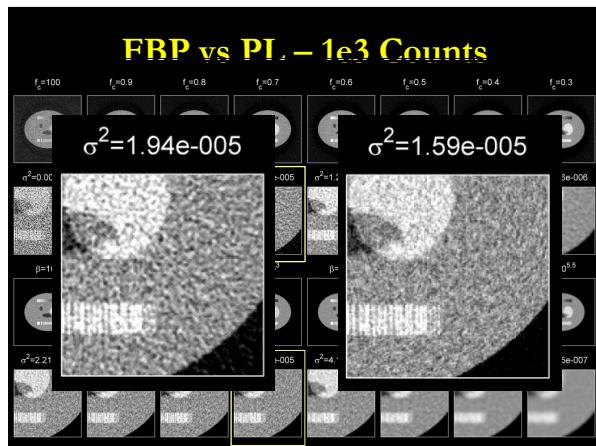
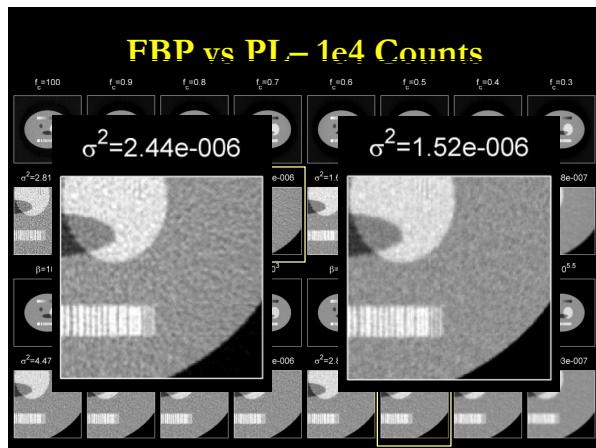
$$k_{1st} = \begin{bmatrix} -1 & -1 & -1 \\ -1 & 4 & -1 \\ -1 & -1 & -1 \end{bmatrix} \quad k_{2nd} = \begin{bmatrix} -1 & -1 & -1 \\ \frac{-1}{\sqrt{2}} & 4 + \frac{4}{\sqrt{2}} & -1 \\ \frac{-1}{\sqrt{2}} & -1 & \frac{-1}{\sqrt{2}} \end{bmatrix}$$
- o Quadratic Penalty

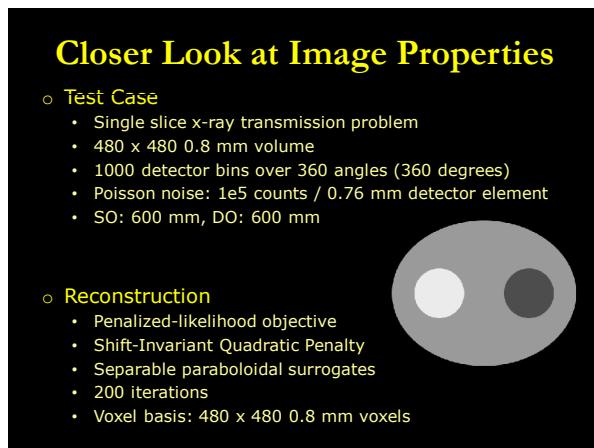
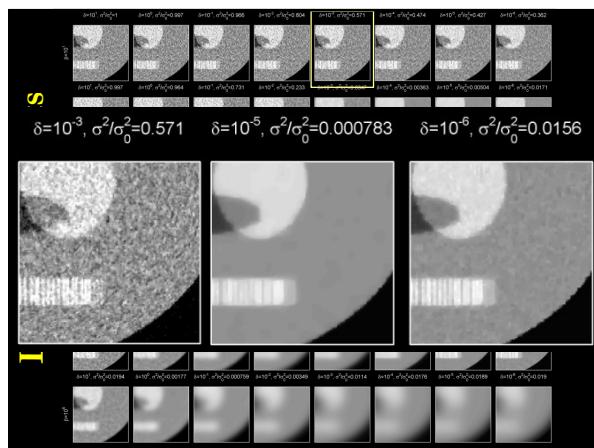
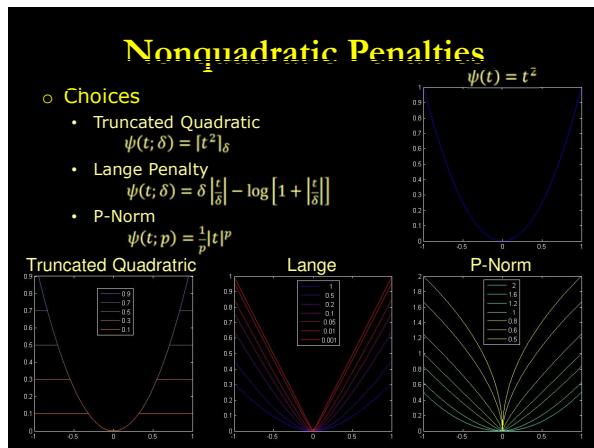
$$R(\mu) = \sum_j \sum_{k \in N} w_{jk} (\mu_j - \mu_k)^2$$

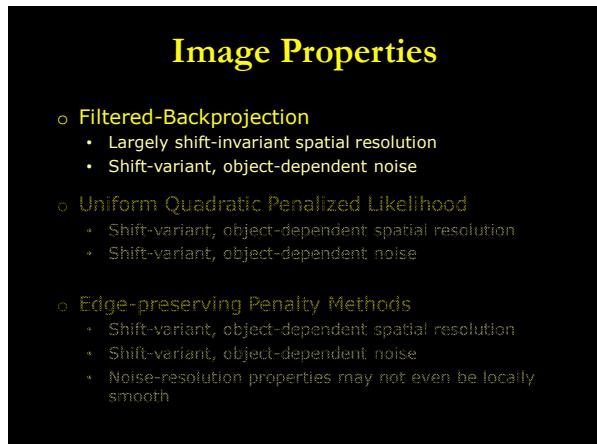
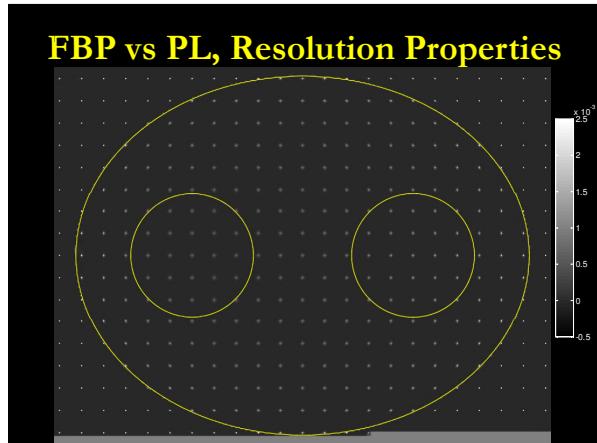
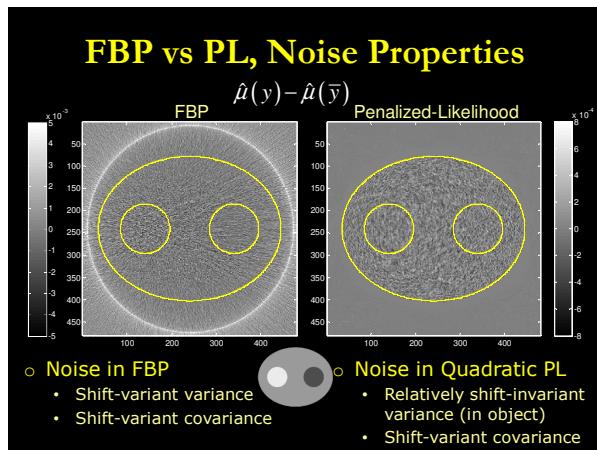
Penalized-Likelihood Example

- o Forward Model
 - Fan-beam Transmission Tomography
 - 512 x 512 0.3 mm volume
 - 400 detector bins over 180 angles (360 degrees)
 - Poisson: {1e4, 1e3} counts per 0.5 mm detector element
 - SO: 380 mm, DO: 220 mm
- o Objective Function
 - Poisson Likelihood
 - Quadratic, first-order Penalty
- o Algorithm
 - Separable Paraboloidal Surrogates
 - 400 iterations – well-converged









Learning Objectives I

- o Fundamentals of iterative methods

- Approach to forming an iterative algorithm
 - * Forward Model
 - * Objective Function
 - * Optimization Algorithm
 - Identify particular classes of methods
 - * Model-based vs. Image Denoising approaches
 - * Statistical vs. Nonstatistical approaches
 - * Kinds of regularization

Learning Objectives II

- o Advantages of iterative approaches

- Intuition behind what these algorithms do
 - * Fitting reconstruction to observations
 - * Data weighting by information content
 - * Importance of regularization
 - Flexibility of these techniques
 - * Arbitrary geometries
 - * Sophisticated modeling of physics
 - * General incorporation of desired image properties through regularization

Learning Objectives III

- o Images produced by iterative methods

- Differences from traditional reconstruction
 - * Regularization is key
 - * Image properties are tied to statistical weighting
 - * Can depend on algorithm when iterative solution has not yet converged
 - Image properties associated with iterative reconstruction
 - * Highly dependent on regularization
 - * Can be more shift-variant (esp. edge-preservation)
 - * Different noise, texture

Thank You