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## Towards real-time ultrasound image-guided abdominal radiotherapy

**Skadi van der Meer**, John Wong, Esther Bloemen,  
Davide Fontanarosa, Martin Lachaine, **Frank Verhaegen**




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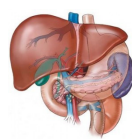
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## History liver radiotherapy

- Prognosis after radiotherapy of liver cancer patients was poor
- Tumors needed a higher radiation dose for local control
- Impossible due to normal tissue constraints
- With current techniques, IMRT, SBRT, able to treat at higher dose levels without increasing the dose at organs at risks.
- Clinical trials demonstrated; highly effective to treat liver tumors with high dose levels




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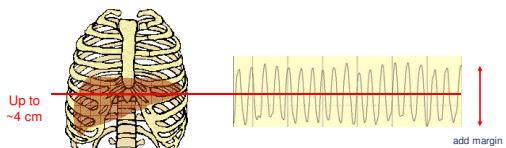
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## Image guidance of the liver

Accurate targeting liver lesions is a challenge:



 assumption lesion moves within margin

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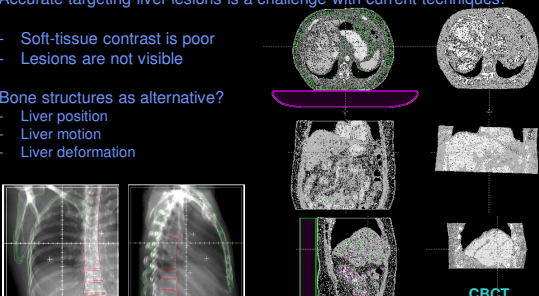
Image guidance for Liver SBRT

Accurate targeting liver lesions is a challenge with current techniques:

- Soft-tissue contrast is poor
- Lesions are not visible

Bone structures as alternative?

- Liver position
- Liver motion
- Liver deformation



CBCT

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Image guidance for Liver SBRT

Fiducials:

- Invasive
- Tumor spill
- Distance from lesion\*
- Liver inflammation

KV cone-beam:

- Soft-tissue contrast not sufficient
- (Blurring due to breathing)

Criteria for the ideal IGRT solution

- Integrated with RT
- High precision
- Good resolution
- Soft-tissue contrast
- Non invasive
- Real-time imaging (live view)
- Also during treatment
- Not too expensive

**US imaging:**

Long term experience in diagnostic applications

\*Seppenwoolde Y, Wunderink W, Wunderink-van Veen SR, et al. Treatment precision of image-guided liver SBRT using implanted fiducial markers depends on marker tumour distance. *Phys Med Biol* 56: 5445-5468.

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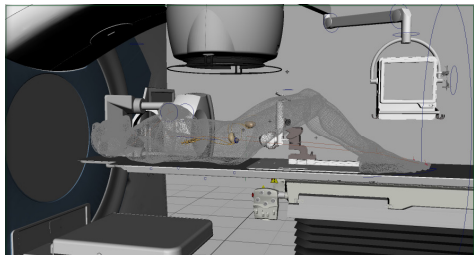
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Clarity 4D prostate system (Elekta) :  
Novel transperineal ultrasound scan




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### Towards abdominal, real-time, volumetric, soft-tissue image guidance with ultrasound

Combination of:

- 3DUS volumetric imaging
- 2DUS time series of the organ motion
- Robotic US probe placement
- US auto-contouring
- Contrast enhanced ultrasound (CEUS)

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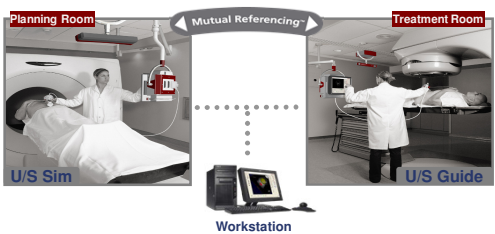
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### US image guidance

New modality: 3DUS for liver SBRT **Clarity 3DUS system (Elekta)**



**Planning Room**      **Mutual Referencing**      **Treatment Room**

**U/S Sim**      **Workstation**      **U/S Guide**

Dosimetric consequences of misalignment and realignment in prostate 3DCRT using intramodality ultrasound image guidance.  
Fraser DJ, Chen Y, Poon E, Gury FL, Falco T, Verhaegen F. Med Phys 2010;37:2787-2795.  
Dosimetric evolution of the breast electron boost target using 3D ultrasound imaging.  
Fraser DJ, Wong P, Sultanem K, Verhaegen F. Radiother Oncol. 2010 Aug;96(2):185-91

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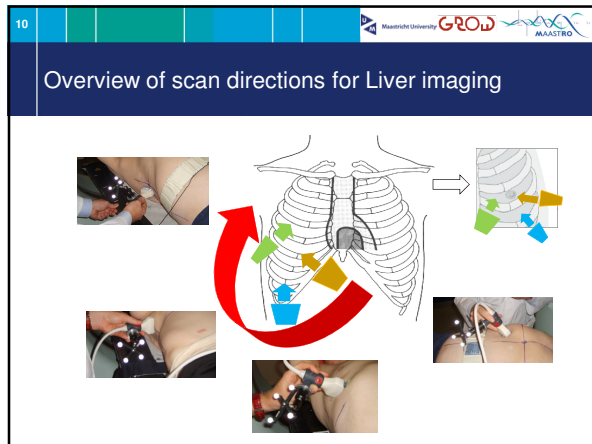
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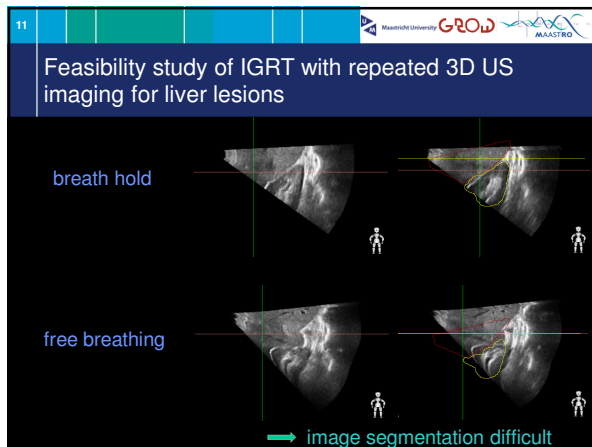
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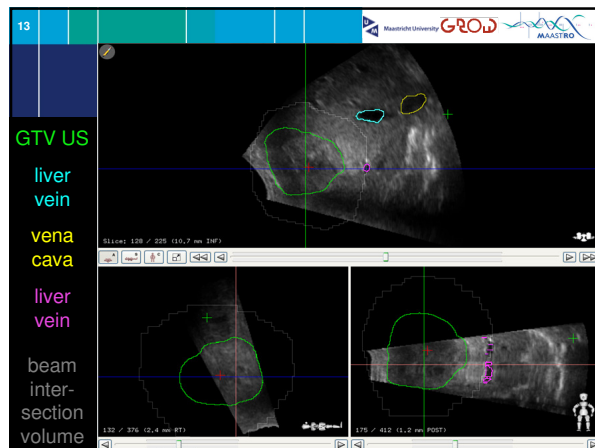
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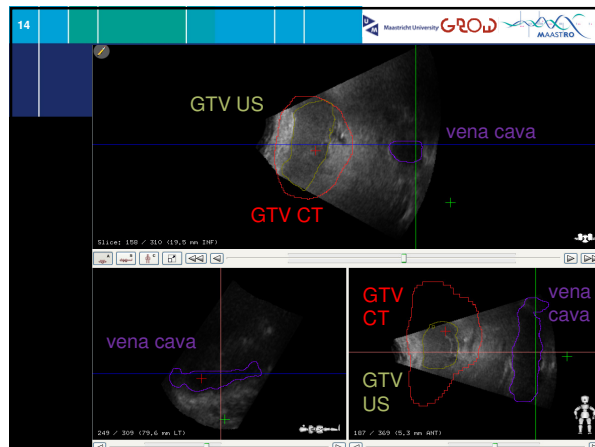
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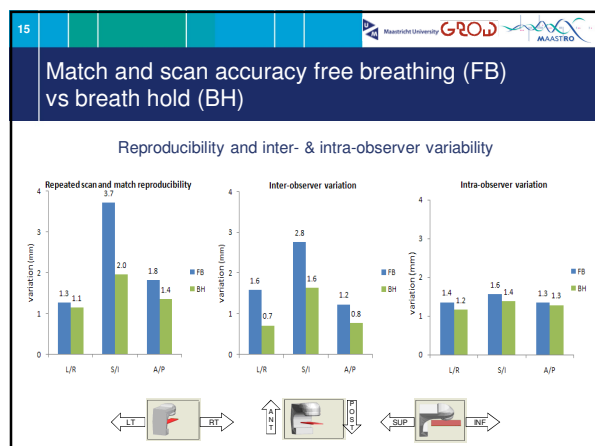
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3DUS volumetric imaging: Conclusion

- US scanning of liver lesions:
  - free breathing → causes artifacts, reducing image quality;
  - in a predefined breath hold phase → accurate  
(reference and daily scans are acquired with the liver in the same fixed position);
- The combined uncertainty (1SD) of US scanning and matching (inter and intra observer) :
  - in free breathing 4mm
  - in breath hold 2mm
- With 3D US imaging, accurate online interfraction image guidance of liver lesions and/or surrogates is feasible. → Recommended during breath hold.
- Nevertheless, integration of liver motion monitoring during treatment is still lacking

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Towards abdominal, real-time, volumetric, soft-tissue image guidance with ultrasound

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2DUS time series with spatial information

Steady probe position and orientation




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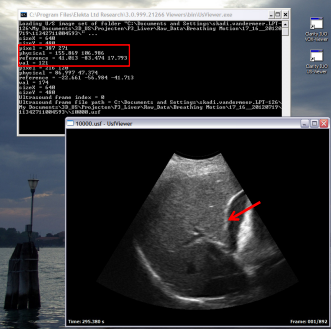
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2DUS time series with spatial information

Dedicated software

- RAW data
- Spatial information



| Time (s) | Position (mm) | Velocity (mm/s) |
|----------|---------------|-----------------|
| 0.000    | 0.000         | 0.000           |
| 0.001    | 0.001         | 0.001           |
| 0.002    | 0.002         | 0.002           |
| 0.003    | 0.003         | 0.003           |
| 0.004    | 0.004         | 0.004           |
| 0.005    | 0.005         | 0.005           |
| 0.006    | 0.006         | 0.006           |
| 0.007    | 0.007         | 0.007           |
| 0.008    | 0.008         | 0.008           |
| 0.009    | 0.009         | 0.009           |
| 0.010    | 0.010         | 0.010           |

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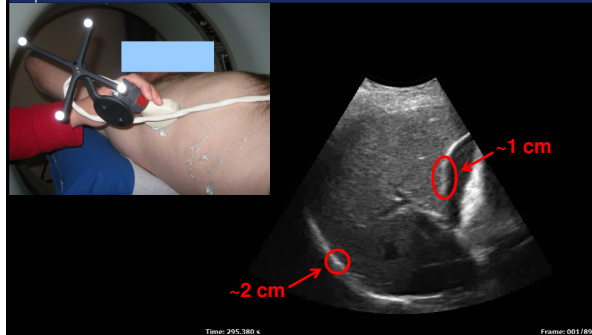
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2DUS time series with spatial information



| Time (s) | Position (mm) | Velocity (mm/s) |
|----------|---------------|-----------------|
| 0.000    | 0.000         | 0.000           |
| 0.001    | 0.001         | 0.001           |
| 0.002    | 0.002         | 0.002           |
| 0.003    | 0.003         | 0.003           |
| 0.004    | 0.004         | 0.004           |
| 0.005    | 0.005         | 0.005           |
| 0.006    | 0.006         | 0.006           |
| 0.007    | 0.007         | 0.007           |
| 0.008    | 0.008         | 0.008           |
| 0.009    | 0.009         | 0.009           |
| 0.010    | 0.010         | 0.010           |

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Towards abdominal, real-time, volumetric, soft-tissue image guidance with ultrasound

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Robot System Requirements

*Research by the Johns Hopkins University School of Medicine, Baltimore*

- Develop a robot system to:
  - Record placement of US probe by expert clinician during CT simulation
  - Assist general clinician to place US probe, considering recorded position, force, and image
  - Hold ultrasound probe (or dummy) in place during CT acquisition and radiation treatment

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Technical Approach

*Research by the Johns Hopkins University School of Medicine, Baltimore*

- Cooperative control with soft motion constraints (virtual fixtures):
  - Cooperative control: move robot by applying forces at the end-effector
  - Motion constraints: restrict motion to guide user to desired target
  - Soft motion constraints: allow motion away from desired target, but with larger effort

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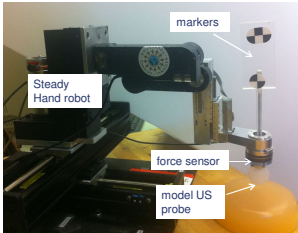
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Prototype System

*Research by the Johns Hopkins University School of Medicine, Baltimore*

- Adapted existing JHU Steady Hand robot, initially designed for retinal microsurgery
- Use Claron Micron tracking system as surrogate for Clarity optical tracking system

Claron Micron Tracker

Steady Hand robot

markers

force sensor

model US probe

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Experimental Procedure

*Research by the Johns Hopkins University School of Medicine, Baltimore*

1. Use cooperative control to guide probe to target
2. Record information (position, force)
3. Starting from an arbitrary position, use cooperative control with soft virtual fixture to guide user back to target position
4. Measure position difference using optical tracking system and robot (possible because robot base not moved during experiment)
  - Optical tracking system is less accurate than robot

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Experimental Results

*Research by the Johns Hopkins University School of Medicine, Baltimore*

- Performed three trials:
  - 3 different targets
  - 3 different users
- In each trial:
  - user defines target
  - returns to target 3 times
- User Impressions:
  - Robotic assistance made it quick and easy to accurately reproduce initial placement

|         |      | Robot<br>diff., mm | Tracker<br>diff., mm |
|---------|------|--------------------|----------------------|
| Trial 1 | 1    | 0.09               | 0.74                 |
|         | 2    | 0.05               | 0.38                 |
|         | 3    | 0.09               | 0.20                 |
|         | Mean | 0.08               | 0.44                 |
| Trial 2 | 1    | 0.13               | 0.75                 |
|         | 2    | 0.17               | 0.94                 |
|         | 3    | 0.15               | 0.57                 |
|         | Mean | 0.15               | 0.75                 |
| Trial 3 | 1    | 0.20               | 0.40                 |
|         | 2    | 0.11               | 0.36                 |
|         | 3    | 0.20               | 0.80                 |
|         | Mean | 0.17               | 0.52                 |

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Towards abdominal, real-time, volumetric, soft-tissue image guidance with ultrasound

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Automated Multimodal 3D Contouring for Prostate 3D Ultrasound

Research by TALab Tecnologie Avanzate Srl, Udine, Italy

**Problems with single modality contouring algorithm:**

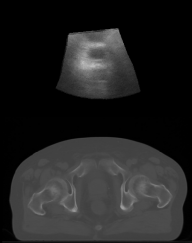
Low stability due to the lack of a complete set of features to detect the prostate boundary in CT and US images.

**US:**

- upper boundary → well enhanced
- lower boundary → sometimes a bit more confused
- Lateral boundaries → more confused

**CT:**

- sharp edges and high contrast between tissues with very different densities
- But not enough contrast in the soft-tissue range (like between prostate and its surrounding tissues)




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Multimodal 3D proposed algorithm

Research by TALab Tecnologie Avanzate Srl, Udine, Italy

Full and direct use of all **3D information** available from a scan.

Easily extensible to a **multimodal approach**:

- retrieve information from different imaging modalities
- use them **simultaneously** in the segmentation process

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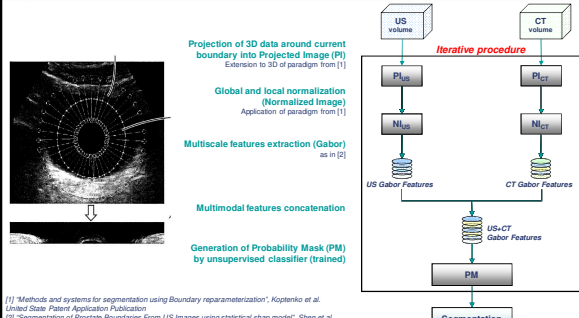
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Algorithm

Research by TALab Tecnologie Avanzate Srl, Udine, Italy



[1] "Methods and systems for segmentation using Boundary reparameterization", Koptenko et al. United State Patent Application Publication

[2] "Segmentation of Prostate Boundaries From US Images using statistical shape model", Shen et al. IEEE Transactions on Medical Imaging, Vol. 29, No. 4, April 2009

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Example

Research by TAlab Tecnologie Avanzate Srl, Udine, Italy

Segmentation on US volume

Segmentation on CT volume

Segmentation on US+CT volume

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Towards abdominal, real-time, volumetric, soft-tissue image guidance with ultrasound

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Contrast enhanced ultrasound imaging

Diffused liver metastases  
2.4 ml injection, 8 min contrast enhancement

Microbubbles Structure

Phospholipids

SF<sub>6</sub>

Hydrophilic pole

Hydrophobic chain

With Contrast

Without Contrast

M. Schneider, M. Arditi, M. B. Barau, J. Brochet, A. Broillet, R. Ventrone, and F. Yan. BR1 - A new ultrasonographic contrast agent based on sulfur hexafluoride filled microbubbles. Investigative Radiology 1995; 30 (8): 451-457.  
M. Schneider. Characteristics of SonoVue®. Echocardiography 1999; 16 (7) Part 2: 743-746.

Phase 3 SonoVue Multi-institutional trial for trans-abdominal imaging of liver lesions  
(U. Hamper, JHU Principal Investigator)

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Metastasis

Bracco Imaging

**Hypervascular**

**Hypovascular**

Baseline

Arterial phase

Portal late phase

Baseline

Arterial phase

Portale phase

Late phase

Images from Dr Lars Thorelius, Linköping, Sweden

Ref: E. Leen. The Role of contrast-enhanced ultrasound in the characterisation of focal liver lesions. Eur. Radiol 2001; 11 (suppl.3): E27-E34.

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Liver Metastasis

Bracco Imaging

Baseline

Arterial phase

Late phase

Courtesy of Prof. François Tranquart, Tours, France

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**Towards** abdominal, real-time, volumetric, soft-tissue image guidance with ultrasound

Combination of:

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**And beyond....**

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And beyond.....

**Elastography (Young's modulus estimation)**  
[European Urology, 54:1354-62, 2008]

**Tissue characterization**

**Histoscanning (frequency spectrum classification)**  
[BJU International, 101:293-98, 2008]

**Contrast Ultrasound Dispersion Imaging (CUDI)**  
Mischi et al, IEEE IUS, 2009 & IEEE TUFFC, in press.  
Kuenen et al, IEEE IUS, 2010 & IEEE TMI, 2011.  
Smeenge et al, World J Urol, 2011.

FIG. 3. Unsuspect B-mode image (only for topographical orientation) together with an elastogram, showing a clearly visible focal stiffer area on the left side (mid-gland) fulfilling all the criteria for a suspicious lesion and presenting a cancer area. The corresponding histopathological slice confirms a Gleason 7 prostate cancer. The changes in elasticity in the inner gland and at the contralateral side do not fulfil all criteria for a suspicious lesion.

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**Acknowledgements**

**Maastrro:**  
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**Elektta Ltd:**  
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Tutkun Sen

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Francesco Pascoli

**Datamind Srl:**  
Denis Ermacora

**Bracco Imaging:**  
Bart Beyloos

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