



ULTRASOUND CONTRAST AGENTS  
BASIC PRINCIPLES AND APPLICATIONS


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of NORTH CAROLINA  
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UNC NCSU  
**BME**  
BIOMEDICAL ENGINEERING



NC STATE UNIVERSITY

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DISCUSSION POINTS

- Part I
  - Microbubble Basics
  - Fundamentals in Contrast Imaging
  - Basic Imaging Applications
- Part II
  - Advanced Imaging Applications
  - Bioeffects and Therapeutic Applications
  - Safety

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PART I

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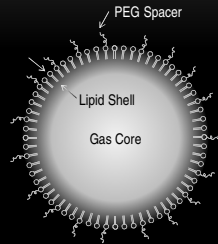
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MICROBUBBLE INTRODUCTION

- What are Microbubble Contrast Agents?
  - Gas: Air, Perfluorocarbon, Sulfur Hexafluoride, etc...
  - Shell: Polymer, Lipid, Albumin, etc...
  - Size: Typically  $< 8 \mu\text{m}$  (Size of RBC)
  - Confined to the Vascular Space



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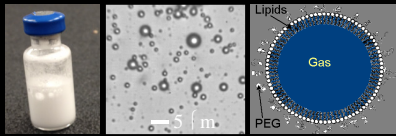
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MICROBUBBLE INTRODUCTION

- Examples



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WHY MICROBUBBLES?

- Microbubbles and Ultrasound
  - **Highly Echogenic**

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**MICROBUBBLE PROPERTIES**

- Microbubbles and Ultrasound
  - **Highly Echogenic**

Dependent On Acoustic Impedance Differences

Acoustic Impedance = Density \* SoS

Water: 1.50 MRays  
Brain: 1.56 MRays  
Bone: 1.4 MRays  
Muscle: 1.6 MRays  
Fat: 1.33 MRays

Tissue: 1.54 MRays

Orders of Magnitude Difference

Air: 0.0004 MRays

The diagram shows a list of acoustic impedance values for various materials: Water (1.50 MRays), Brain (1.56 MRays), Bone (1.4 MRays), Muscle (1.6 MRays), and Fat (1.33 MRays). These are grouped together with a bracket and labeled as 'Tissue: 1.54 MRays'. To the right, a double-headed arrow indicates an 'Orders of Magnitude Difference' between the tissue group and 'Air: 0.0004 MRays'.

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**MICROBUBBLE PROPERTIES**

- Microbubbles in an Ultrasound Field
  - Highly Echogenic
  - **Oscillate**

Oscillation Governed By...

- 1) Frequency
- 2) Pressure Amplitude
- 3) Pulse Repetition Frequency
- 4) Type of Gas Core
- 5) Damping Coefficients
- 6) Shell Properties

Quaia E, et al... Contrast media in ultrasonography-basic principles and clinical applications. New York: Springer; 2005.

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**MICROBUBBLE PROPERTIES**

- Microbubbles in an Ultrasound Field
  - Highly Echogenic
  - **Oscillate**

Stable Oscillatory Behavior at Low Pressures

The diagram shows two vertically aligned sinusoidal waveforms. The top waveform is labeled 'Pressure' and the bottom is labeled 'Radius'. Between the two waveforms, there are four circular microbubbles of varying sizes, with arrows indicating their expansion and contraction in sync with the oscillations.

Quaia E, et al... Contrast media in ultrasonography-basic principles and clinical applications. New York: Springer; 2005.

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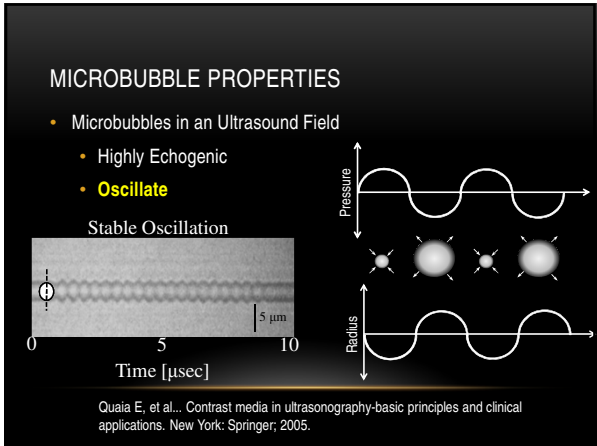
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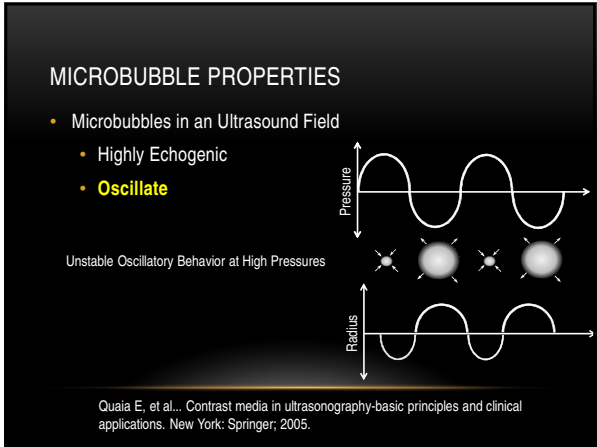
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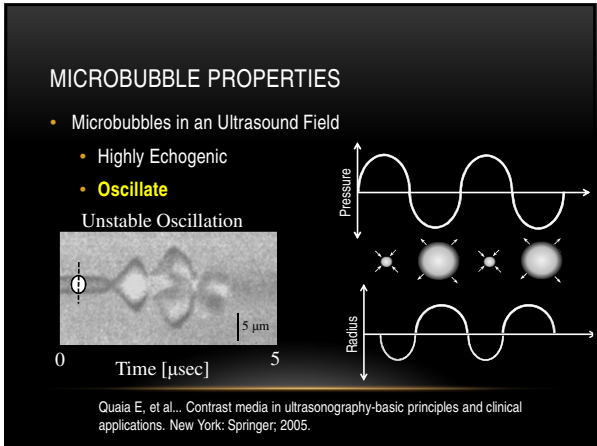
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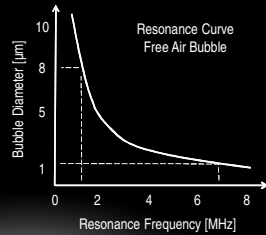
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### MICROBUBBLE PROPERTIES

- Microbubbles in an Ultrasound Field
  - Highly Echogenic
  - **Oscillate**



Quaia E, et al... Contrast media in ultrasonography-basic principles and clinical applications. New York: Springer; 2005.

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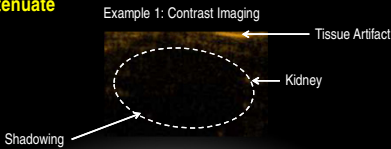
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### MICROBUBBLE PROPERTIES

- Microbubbles in an Ultrasound Field
  - Highly Echogenic
  - Oscillate
  - **Attenuate**

Concentration	↑
Attenuation	↑



Quaia E, et al... Contrast media in ultrasonography-basic principles and clinical applications. New York: Springer; 2005.

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### MICROBUBBLE PROPERTIES

- Describing the Motion of a Microbubble

- **Rayleigh - Plesset** 
$$\rho R \ddot{R} + \frac{3}{2} \rho \dot{R}^2 = p_L - p_v - \rho R \dot{R}^2 = p_L - p_v$$

Quaia E, et al... Contrast media in ultrasonography-basic principles and clinical applications. New York: Springer; 2005.

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## MICROBUBBLE PROPERTIES

- Describing the Motion of a Microbubble

- Rayleigh - Plesset** 
$$\rho R \ddot{R} + \frac{3}{2} \rho \dot{R}^2 = p_L - p_\infty - \rho R \dot{R}^2 = p_L - p_\infty$$

$\rho$  = Density of Medium  
 $R$  = Microbubble Radius  
 $\dot{R}$  = 1<sup>st</sup> Time Derivative of Radius  
 $\ddot{R}$  = 2<sup>nd</sup> Time Derivative of Radius  
 $p_L$  = Liquid Pressure at Wall  
 $p_\infty$  = Liquid Pressure Away From Wall

Quaia E, et al... Contrast media in ultrasonography-basic principles and clinical applications. New York: Springer; 2005.

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## MICROBUBBLE PROPERTIES

- Describing the Motion of a Microbubble

- Rayleigh - Plesset
- Including Shell Properties**

- Viscosity of the Shell
- Elasticity of the Shell

$$\rho R \ddot{R} + \frac{3}{2} \rho \dot{R}^2 = p_{\infty} \left( \frac{R_0}{R} \right)^{3\Gamma} - \frac{2S_L}{R} - \frac{4\eta \dot{R}}{R} - p_\infty + P_{(t)} \sin(\omega t)$$

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## MICROBUBBLE PROPERTIES

- Describing the Motion of a Microbubble

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- Including Shell Properties**

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$$\rho R \ddot{R} + \frac{3}{2} \rho \dot{R}^2 = p_{\infty} \left( \frac{R_0}{R} \right)^{3\Gamma} - \frac{2S_L}{R} - \frac{4\eta \dot{R}}{R} - p_\infty + P_{(t)} \sin(\omega t)$$

$S$  = Surface Tension  
 $\eta$  = Liquid Shear Viscosity

Quaia E, et al... Contrast media in ultrasonography-basic principles and clinical applications. New York: Springer; 2005.

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### MICROBUBBLE PROPERTIES

- Describing the Motion of a Microbubble
  - Rayleigh – Plesset
- Including Shell Properties
  - Viscosity of the Shell
  - Elasticity of the Shell
- **Complex Equation** ➡ **Difficult to model and simulate**

Quaia E, et al... Contrast media in ultrasonography-basic principles and clinical applications. New York: Springer; 2005.

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### MICROBUBBLE PROPERTIES

- Describing the Motion of a Microbubble
  - Rayleigh – Plesset
- Including Shell Properties
  - Viscosity of the Shell
  - Elasticity of the Shell
- Complex Equation ➡ Difficult to model and simulate
  - **Concentration and Size Distributions Exacerbate Complexity!**

Quaia E, et al... Contrast media in ultrasonography-basic principles and clinical applications. New York: Springer; 2005.

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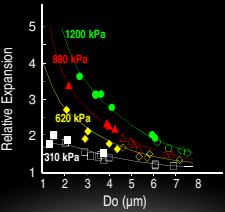
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### MICROBUBBLE PROPERTIES

- Microbubble Destruction Increases for...
  - **High Pressure Amplitudes**



Chomas J, et al... Threshold of fragmentation for ultrasonic contrast Agents. Journal of Biomedical Optics 6(2), pg. 141-150, 2001

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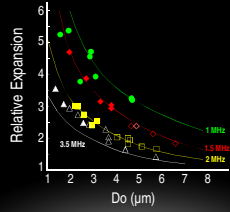
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MICROBUBBLE PROPERTIES

- Microbubble Destruction Increases for...
- **Low Frequencies**



Chomas J, et al... Threshold of fragmentation for ultrasonic contrast Agents. Journal of Biomedical Optics 6(2), pg. 141-150, 2001

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MICROBUBBLE PROPERTIES

- Microbubble Destruction Increases for...
- High Pressure Amplitudes
- Low Frequencies
- **Long Ultrasound Pulse Lengths**

Quaia E, et al... Contrast media in ultrasonography-basic principles and clinical applications. New York: Springer; 2005.

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MICROBUBBLE PROPERTIES

- Microbubble Destruction Increases for...
- High Pressure Amplitudes
- Low Frequencies
- Long Ultrasound Pulse Lengths
- **Most Important: High Pressure Amplitude, Low Frequency**

Quaia E, et al... Contrast media in ultrasonography-basic principles and clinical applications. New York: Springer; 2005.

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# BASIC CONTRAST IMAGING TECHNIQUES

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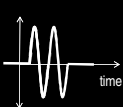
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## IMAGING MICROBUBBLES

- **Microbubble Response Related to Insonation Frequency**

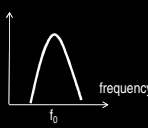
Insonation Waveform



time

FT

Fourier Domain



frequency

$f_0$

Quaia E, et al... Contrast media in ultrasonography-basic principles and clinical applications. New York: Springer; 2005.

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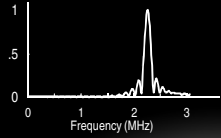
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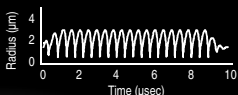
## IMAGING MICROBUBBLES

- **Microbubble Response Related to Insonation Frequency**

Insonation Parameters: 20 Cycle, 2.25 MHz



Frequency (MHz)



Radius ( $\mu\text{m}$ )

Time ( $\mu\text{sec}$ )

Chomas J, et al... Nondestructive Subharmonic Imaging. IEEE Trans. Ultrasonics 49(7), pg. 883-892, 2002

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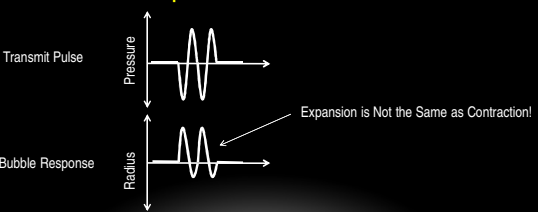
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IMAGING MICROBUBBLES

- Microbubble Response Related to Insonation Frequency
- **Microbubble Response is Non-Linear**



Expansion is Not the Same as Contraction!

Quaia E, et al... Contrast media in ultrasonography-basic principles and clinical applications. New York: Springer; 2005.

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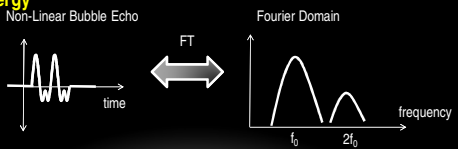
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IMAGING MICROBUBBLES

- Microbubble Response Related to Insonation Frequency
- Microbubble Response is Non-Linear
- **Microbubbles Generate Harmonic and Sub Harmonic Energy**



Non-Linear Bubble Echo

Fourier Domain

FT

time

frequency

$f_0$   $2f_0$

Quaia E, et al... Contrast media in ultrasonography-basic principles and clinical applications. New York: Springer; 2005.

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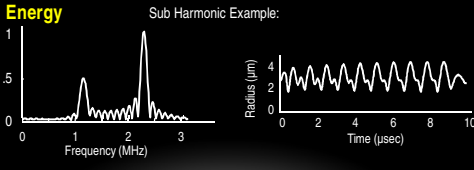
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IMAGING MICROBUBBLES

- Microbubble Response Related to Insonation Frequency
- Microbubble Response is Non-Linear
- **Microbubbles Generate Harmonic and Sub Harmonic Energy**



Sub Harmonic Example:

Frequency (MHz)

Radius ( $\mu\text{m}$ )

Time ( $\mu\text{sec}$ )

Chomas J, et al... Nondestructive Subharmonic Imaging. IEEE Trans. Ultrasonics 49(7), pg. 883-892, 2002

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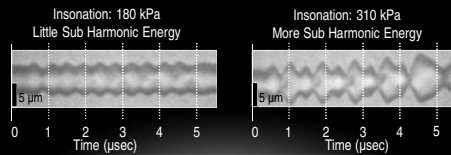
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## IMAGING MICROBUBBLES

- Microbubble Response Related to Insonation Frequency
- Microbubble Response is Non-Linear
- **Microbubbles Generate Harmonic and Sub Harmonic Energy**

Sub Harmonic Example:



Chomas J, et al... Nondestructive Subharmonic Imaging. IEEE Trans. Ultrasonics 49(7), pg. 883-892, 2002

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## IMAGING MICROBUBBLES

- Microbubble Response Related to Insonation Frequency
- Microbubble Response is Non-Linear
- Microbubbles Generate Harmonic and Sub Harmonic Energy
- **Imaging Techniques Take Advantage of Microbubble Properties**

Quaia E, et al... Contrast media in ultrasonography-basic principles and clinical applications. New York: Springer; 2005.

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## IMAGING MICROBUBBLES

- Microbubble Response Related to Insonation Frequency
- Microbubble Response is Non-Linear
- Microbubbles Generate Harmonic and Sub Harmonic Energy
- Imaging Techniques Take Advantage of Microbubble Properties
- **Goal: Separate Microbubble Signal From Tissue**

Quaia E, et al... Contrast media in ultrasonography-basic principles and clinical applications. New York: Springer; 2005.

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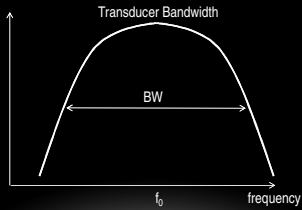
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HARMONIC IMAGING

- Transducer has Finite Bandwidth



Quaia E, et al... Contrast media in ultrasonography-basic principles and clinical applications. New York: Springer; 2005.

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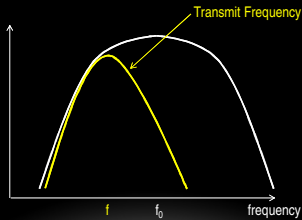
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HARMONIC IMAGING

- Insonify Microbubbles at Frequency  $f$



Quaia E, et al... Contrast media in ultrasonography-basic principles and clinical applications. New York: Springer; 2005.

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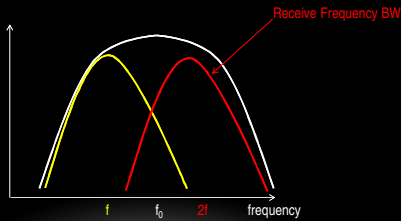
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HARMONIC IMAGING

- Receive Echo at Frequency  $2f$



Quaia E, et al... Contrast media in ultrasonography-basic principles and clinical applications. New York: Springer; 2005.

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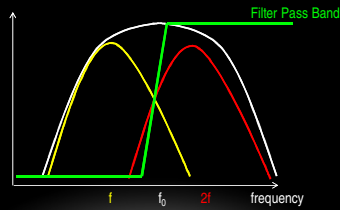
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## HARMONIC IMAGING

- High Pass Filter Received Signal



Quaia E, et al... Contrast media in ultrasonography-basic principles and clinical applications. New York: Springer; 2005.

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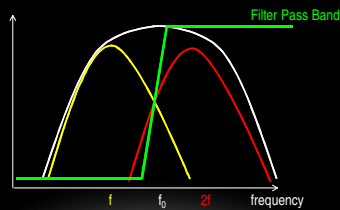
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## HARMONIC IMAGING

- Strong Tissue Signal Can Overpower Weak Harmonic!



Quaia E, et al... Contrast media in ultrasonography-basic principles and clinical applications. New York: Springer; 2005.

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## SUBHARMONIC IMAGING

- Microbubbles have Subharmonic Energies

Frinking P, et al... Ultrasound Contrast Imaging: Current and New Potential Methods. UMB 26 (6), pg. 965-975, 2000.

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SUBHARMONIC IMAGING

- Microbubbles have Subharmonic Energies
- **Occur at  $\sim 1/2$  of the Transmitted Frequency**

Frinking P, et al... Ultrasound Contrast Imaging: Current and New Potential  
Methods. UMB 26 (6), pg. 965-975, 2000.

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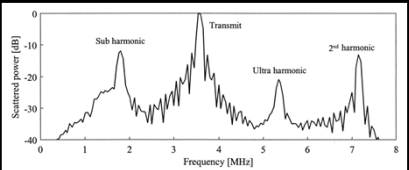
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SUBHARMONIC IMAGING

- Microbubbles have Subharmonic Energies
- **Response at  $\sim 1/2$  of the Transmitted Frequency**



Frinking P, et al... Ultrasound Contrast Imaging: Current and New Potential  
Methods. UMB 26 (6), pg. 965-975, 2000.

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SUBHARMONIC IMAGING

- Microbubbles have Subharmonic Energies
- Response at  $\sim 1/2$  of the Transmitted Frequency
- **Tissue Does Not Generate Sub Harmonic Energy**

Frinking P, et al... Ultrasound Contrast Imaging: Current and New Potential  
Methods. UMB 26 (6), pg. 965-975, 2000.

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SUB HARMONIC IMAGING

- Microbubbles have Subharmonic Energies
- Response at  $\sim 1/2$  of the Transmitted Frequency
- Tissue Does Not Generate Sub Harmonic Energy
- **Sub Harmonic Imaging**

Frinking P, et al... Ultrasound Contrast Imaging: Current and New Potential  
Methods. UMB 26 (6), pg. 965-975, 2000.

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SUB HARMONIC IMAGING

- Microbubbles have Subharmonic Energies
- Response at  $\sim 1/2$  of the Transmitted Frequency
- Tissue Does Not Generate Sub Harmonic Energy
- Sub Harmonic Imaging
  - **Easy Separation from Tissue**

Frinking P, et al... Ultrasound Contrast Imaging: Current and New Potential  
Methods. UMB 26 (6), pg. 965-975, 2000.

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SUB HARMONIC IMAGING

- Microbubbles have Subharmonic Energies
- Response at  $\sim 1/2$  of the Transmitted Frequency
- Tissue Does Not Generate Sub Harmonic Energy
- Sub Harmonic Imaging
  - Easy Separation from Tissue
  - **Lower Frequencies Mean Less Attenuation**

Frinking P, et al... Ultrasound Contrast Imaging: Current and New Potential  
Methods. UMB 26 (6), pg. 965-975, 2000.

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# SUB HARMONIC IMAGING

- Microbubbles have Subharmonic Energies
- Response at  $\sim 1/2$  of the Transmitted Frequency
- Tissue Does Not Generate Sub Harmonic Energy
- Sub Harmonic Imaging
  - Easy Separation from Tissue
  - Lower Frequencies Mean Less Attenuation
  - **Low Frequency Trade-off with Resolution**

Frinking P, et al... Ultrasound Contrast Imaging: Current and New Potential Methods. UMB 26 (6), pg. 965-975, 2000.

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# PULSE INVERSION TECHNIQUES



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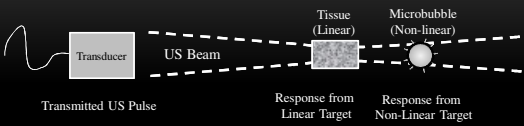
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# PULSE INVERSION TECHNIQUES



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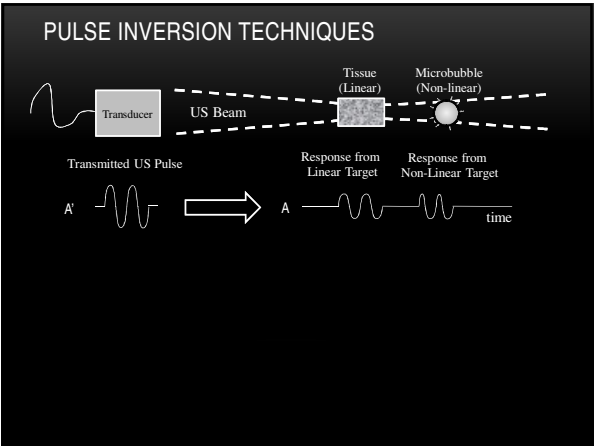
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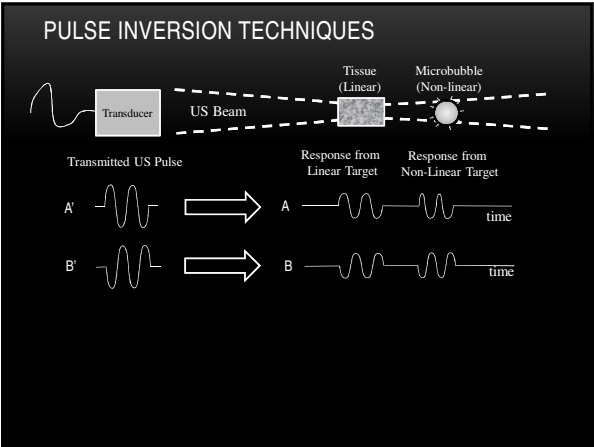
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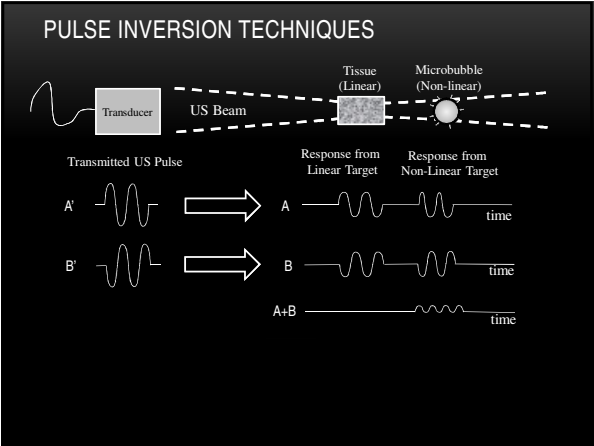
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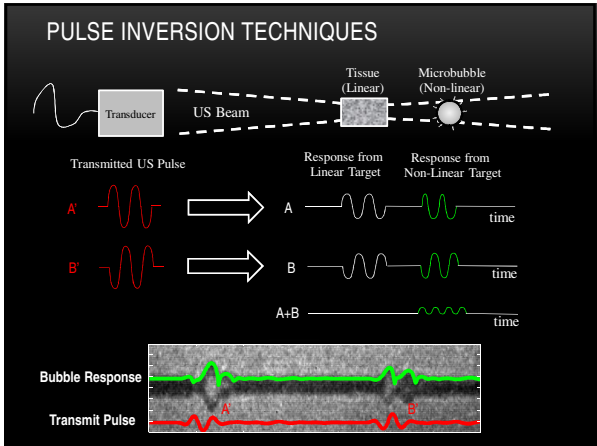
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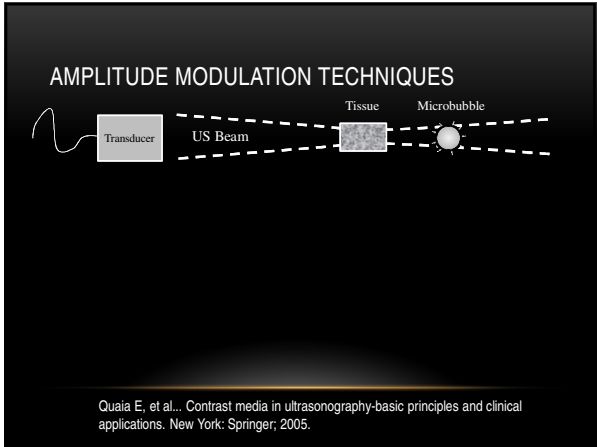
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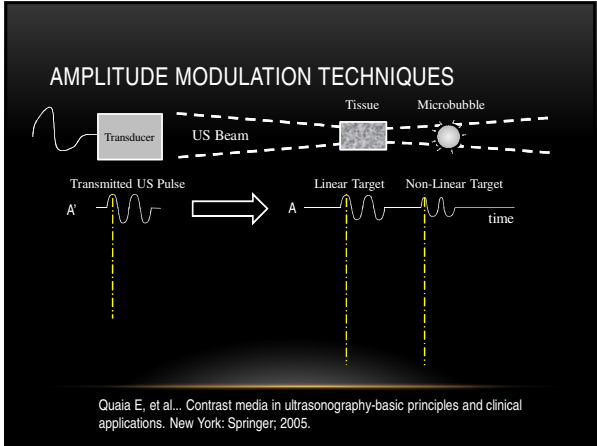
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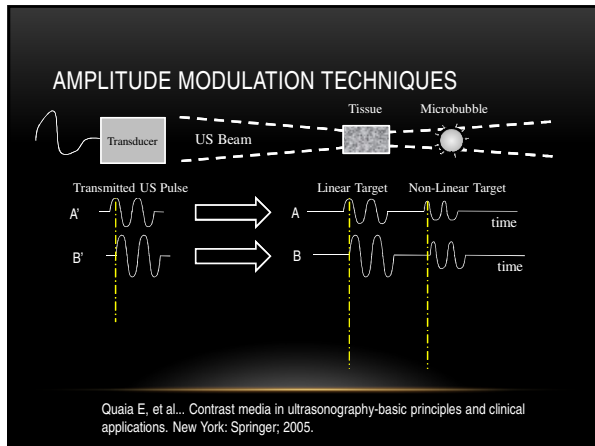
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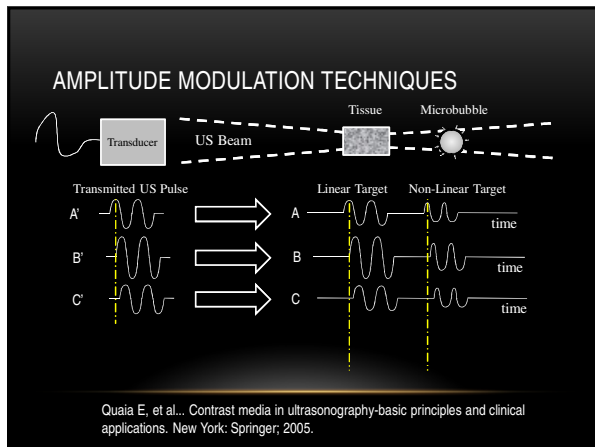
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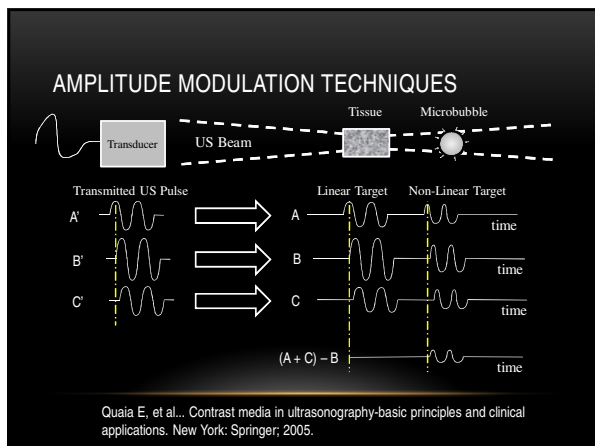
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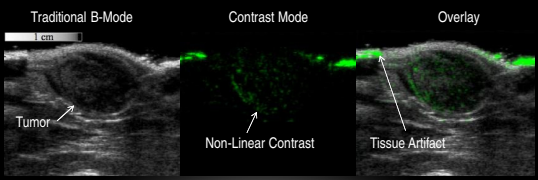
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**COMBINING TECHNIQUES**

Example:  
Siemens Sequoia – 15L8 Linear Array Transducer  
Cadence Pulse Sequencing Mode (Contrast Imaging)  
Amplitude Modulation and Pulse Inversion



Streeter - Unpublished Data.

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**IMAGING TECHNIQUES SUMMARY**

- Single Pulse Strategies
  - Harmonic Imaging
    - Disadvantage: Interference with Tissue Signal
  - Sub Harmonic Imaging
    - Disadvantage: Low Frequency = Poor Resolution
- Post-Processing Strategies
  - Pulse Inversion
    - Disadvantage: Lower Frame Rate, Sensitive to Tissue Motion
  - Amplitude Modulation
    - Disadvantage: Lower Frame Rate, Sensitive to Tissue Motion
- Most Systems Today Incorporate Some Combination!

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**BASIC IMAGING APPLICATIONS**

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CONTRAST-ENHANCED ULTRASOUND

- **Blood is a Weak Scatterer**

Quaia E, et al... Contrast media in ultrasonography-basic principles and clinical applications. New York: Springer; 2005.

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CONTRAST-ENHANCED ULTRASOUND

- Blood is a Weak Scatterer
- **Microbubbles Help Delineate Tissue From Blood**

Quaia E, et al... Contrast media in ultrasonography-basic principles and clinical applications. New York: Springer; 2005.

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CONTRAST-ENHANCED ULTRASOUND

- Blood is a Weak Scatterer
- Microbubbles Help Delineate Tissue From Blood
  - **Provides Clearer Picture For Clinicians**

Quaia E, et al... Contrast media in ultrasonography-basic principles and clinical applications. New York: Springer; 2005.

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CONTRAST-ENHANCED ULTRASOUND

- Blood is a Weak Scatterer
- Microbubbles Help Delineate Tissue From Blood
  - Provides Clearer Picture For Clinicians
- **Ability to Quantify Tissue Perfusion**

Quaia E, et al... Contrast media in ultrasonography-basic principles and clinical applications. New York: Springer; 2005.

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CONTRAST-ENHANCED ULTRASOUND

- Blood is a Weak Scatterer
- Microbubbles Help Delineate Tissue From Blood
  - Provides Clearer Picture For Clinicians
- Ability to Quantify Tissue Perfusion
  - **Transit Time Measurements**

Quaia E, et al... Contrast media in ultrasonography-basic principles and clinical applications. New York: Springer; 2005.

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CONTRAST-ENHANCED ULTRASOUND

- Blood is a Weak Scatterer
- Microbubbles Help Delineate Tissue From Blood
  - Provides Clearer Picture For Clinicians
- Ability to Quantify Tissue Perfusion
  - Transit Time Measurements
  - **Evaluation of Blood Volume**

Quaia E, et al... Contrast media in ultrasonography-basic principles and clinical applications. New York: Springer; 2005.

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## CONTRAST-ENHANCED ULTRASOUND

- Blood is a Weak Scatterer
- Microbubbles Help Delineate Tissue From Blood
  - Provides Clearer Picture For Clinicians
- Ability to Quantify Tissue Perfusion
  - Transit Time Measurements
  - Evaluation of Blood Volume
  - **Replenishment Kinetics**

Quaia E, et al... Contrast media in ultrasonography-basic principles and clinical applications. New York: Springer; 2005.

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## CONTRAST ECHOCARDIOGRAPHY

- **Assessment of Left Ventricular Cavity**

Kaufmann E, et al... Contrast Echocardiography. Curr Probl Cardiol; 32 (2), pg 51-96, 2005.

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## CONTRAST ECHOCARDIOGRAPHY

- Assessment of Left Ventricular Cavity
  - **Requires Endocardial Border Visualization**

Kaufmann E, et al... Contrast Echocardiography. Curr Probl Cardiol; 32 (2), pg 51-96, 2005.

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CONTRAST ECHOCARDIOGRAPHY

- Assessment of Left Ventricular Cavity
  - Requires Endocardial Border Visualization
  - **Adequate Visualization Not Possible in 15% of Patients**

Kaufmann E, et al... Contrast Echocardiography. Curr Probl Cardiol; 32 (2), pg 51-96, 2005.

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CONTRAST ECHOCARDIOGRAPHY

- Assessment of Left Ventricular Cavity
  - Requires Endocardial Border Visualization
  - Adequate Visualization Not Possible in 15% of Patients
- **Left Ventricular Opacification**

Kaufmann E, et al... Contrast Echocardiography. Curr Probl Cardiol; 32 (2), pg 51-96, 2005.

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CONTRAST ECHOCARDIOGRAPHY

- Assessment of Left Ventricular Cavity
  - Requires Endocardial Border Visualization
  - Adequate Visualization Not Possible in 15% of Patients
- Left Ventricular Opacification
  - **Microbubbles Improve Visualization**

Kaufmann E, et al... Contrast Echocardiography. Curr Probl Cardiol; 32 (2), pg 51-96, 2005.

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CONTRAST ECHOCARDIOGRAPHY

- Assessment of Left Ventricular Cavity
  - Requires Endocardial Border Visualization
  - Adequate Visualization Not Possible in 15% of Patients
- Left Ventricular Opacification
  - Microbubbles Improve Visualization
  - **Produces Homogenous Opacification**

Kaufmann E, et al... Contrast Echocardiography. Curr Probl Cardiol; 32 (2), pg 51-96, 2005.

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CONTRAST ECHOCARDIOGRAPHY

- Assessment of Left Ventricular Cavity
  - Requires Endocardial Border Visualization
  - Adequate Visualization Not Possible in 15% of Patients
- Left Ventricular Opacification
  - Microbubbles Improve Visualization
  - Produces Homogenous Opacification
  - **Improves Reader Accuracy and Confidence**

Kaufmann E, et al... Contrast Echocardiography. Curr Probl Cardiol; 32 (2), pg 51-96, 2005.

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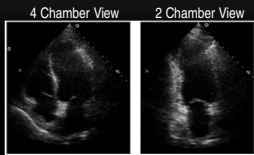
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CONTRAST ECHOCARDIOGRAPHY



Poor Endocardial Definition

Kaufmann E, et al... Contrast Echocardiography. Curr Probl Cardiol; 32 (2), pg 51-96, 2005.

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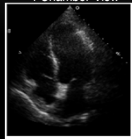
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CONTRAST ECHOCARDIOGRAPHY


4 Chamber View




2 Chamber View



Poor Endocardial Definition





Improved Definition Due to Contrast

Kaufmann E, et al... Contrast Echocardiography. Curr Probl Cardiol; 32 (2), pg 51-96, 2005.

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TIME INTENSITY CURVE

- Contrast-Enhanced Monitoring Over Time

Quaia E, et al... Contrast media in ultrasonography-basic principles and clinical applications. New York: Springer; 2005.

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TIME INTENSITY CURVE

- Contrast-Enhanced Monitoring Over Time
- Select a Region of Interest

Quaia E, et al... Contrast media in ultrasonography-basic principles and clinical applications. New York: Springer; 2005.

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TIME INTENSITY CURVE

- Contrast-Enhanced Monitoring Over Time
- Select a Region of Interest
- **Evaluate the Intensity of the Microbubbles**

Quaia E, et al... Contrast media in ultrasonography-basic principles and clinical applications. New York: Springer; 2005.

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TIME INTENSITY CURVE

- Contrast-Enhanced Monitoring Over Time
- Select a Region of Interest
- Evaluate the Intensity of the Microbubbles
- **How It Works:**

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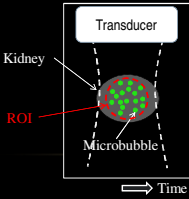
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TIME INTENSITY CURVE

- Contrast-Enhanced Monitoring Over Time
- Select a Region of Interest
- Evaluate the Intensity of the Microbubbles
- **How It Works:**



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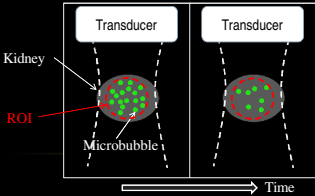
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# TIME INTENSITY CURVE

- Contrast-Enhanced Monitoring Over Time
- Select a Region of Interest
- Evaluate the Intensity of the Microbubbles
- **How It Works:**



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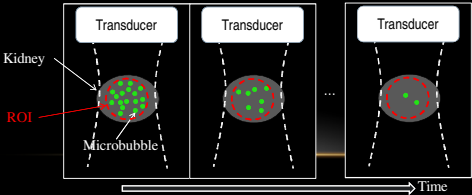
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# TIME INTENSITY CURVE

- Contrast-Enhanced Monitoring Over Time
- Select a Region of Interest
- Evaluate the Intensity of the Microbubbles
- **How It Works:**



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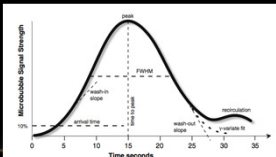
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# TIME INTENSITY CURVE

- Contrast-Enhanced Monitoring Over Time
- Select a Region of Interest
- Evaluate the Intensity of the Microbubbles
- **How It Works:**



Cosgrove D, et al. Imaging of Perfusion Using Ultrasound. Eur J Nucl Mol Imaging. 37 (Suppl 1); 2010.

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TIME INTENSITY CURVE

- Contrast-Enhanced Monitoring Over Time
- Select a Region of Interest
- Evaluate the Intensity of the Microbubbles
- **Example:**

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TIME INTENSITY CURVE

- Contrast-Enhanced Monitoring Over Time
- Select a Region of Interest
- Evaluate the Intensity of the Microbubbles
- **Example:**
  - **Evaluation of Liver Lesions**

Wilson S, et al... Microbubble-enhanced US in body imaging: What Role? Radiology: 257(1); 2010.

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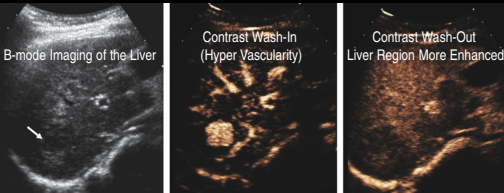
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TIME INTENSITY CURVE

- Contrast-Enhanced Monitoring Over Time
- Select a Region of Interest
- Evaluate the Intensity of the Microbubbles
- **Example:**



Wilson S, et al... Microbubble-enhanced US in body imaging: What Role? Radiology: 257(1); 2010.

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DESTRUCTION-REPERFUSION

- **Perfusion Quantification Helps Understand Diseased Tissue**

Quaia E. Assessment of tissue perfusion by contrast-enhanced ultrasound. Eur Radiology: 21 (3); 2011.

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DESTRUCTION-REPERFUSION

- Perfusion Quantification Helps Understand Diseased Tissue
- **Microbubbles are Continuously Infused**

Quaia E. Assessment of tissue perfusion by contrast-enhanced ultrasound. Eur Radiology: 21 (3); 2011.

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DESTRUCTION-REPERFUSION

- Perfusion Quantification Helps Understand Diseased Tissue
- Microbubbles are Continuously Infused
  - **Steady State Clearance Equals the Inflow**

Quaia E. Assessment of tissue perfusion by contrast-enhanced ultrasound. Eur Radiology: 21 (3); 2011.

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DESTRUCTION-REPERFUSION

- Perfusion Quantification Helps Understand Diseased Tissue
- Microbubbles are Continuously Infused
  - Steady State Clearance Equals the Inflow
- **Microbubble Destruction in a Single Plane**

Quaia E. Assessment of tissue perfusion by contrast-enhanced ultrasound. Eur Radiology; 21 (3); 2011.

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DESTRUCTION-REPERFUSION

- Perfusion Quantification Helps Understand Diseased Tissue
- Microbubbles are Continuously Infused
  - Steady State Clearance Equals the Inflow
- Microbubble Destruction in a Single Plane
- **Monitoring Microbubble Refill Rate**

Quaia E. Assessment of tissue perfusion by contrast-enhanced ultrasound. Eur Radiology; 21 (3); 2011.

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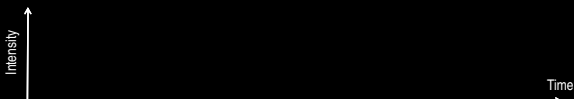
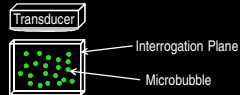
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DESTRUCTION-REPERFUSION

- Perfusion Quantification Helps Understand Diseased Tissue
- **How Does It Work?**



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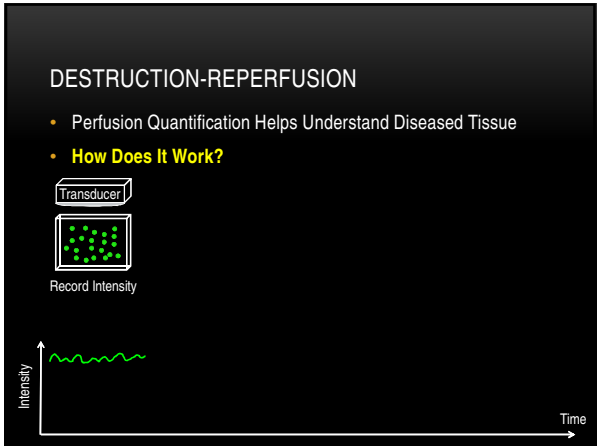
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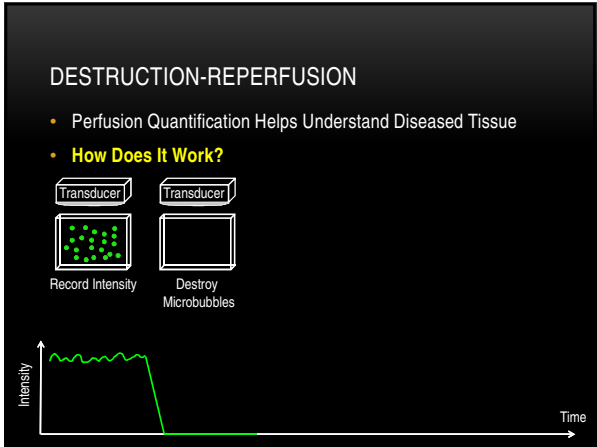
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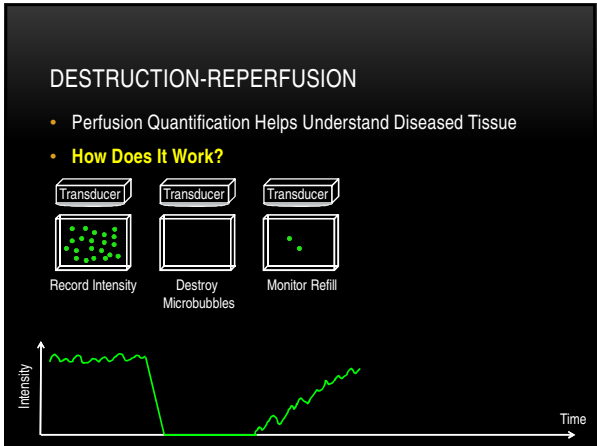
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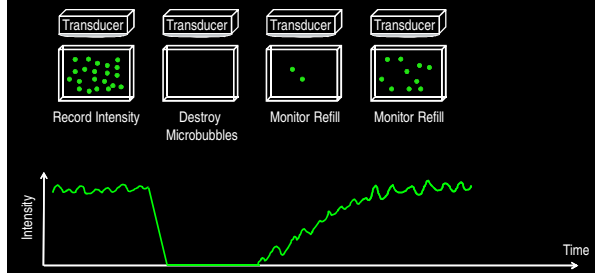
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## DESTRUCTION-REPERFUSION

- Perfusion Quantification Helps Understand Diseased Tissue
- **How Does It Work?**



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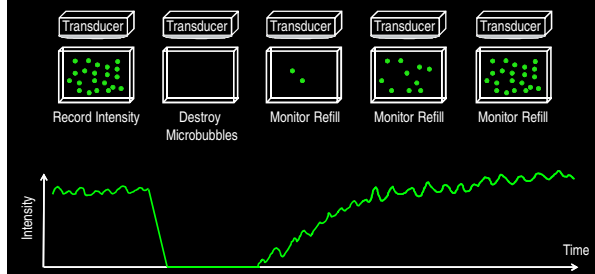
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## DESTRUCTION-REPERFUSION

- Perfusion Quantification Helps Understand Diseased Tissue
- **How Does It Work?**



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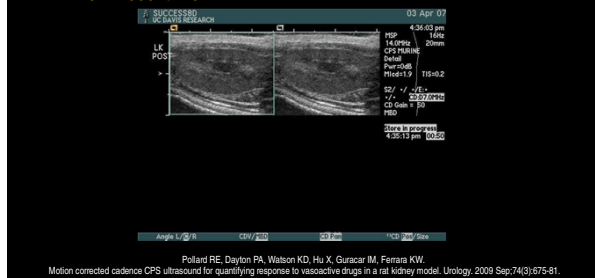
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## DESTRUCTION-REPERFUSION

- Perfusion Quantification Helps Understand Diseased Tissue
- **How Does It Work?**



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DESTRUCTION-REPERFUSION

- Perfusion Quantification Helps Understand Diseased Tissue
- **What Information Do We Get?**

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DESTRUCTION-REPERFUSION

- Perfusion Quantification Helps Understand Diseased Tissue
- What Information Do We Get?
  - **Time To Peak Intensity**

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DESTRUCTION-REPERFUSION

- Perfusion Quantification Helps Understand Diseased Tissue
- What Information Do We Get?
  - Time To Peak Intensity
  - **Blood Flow Velocity (Slope)**

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DESTRUCTION-REPERFUSION

- Perfusion Quantification Helps Understand Diseased Tissue
- What Information Do We Get?
  - Time To Peak Intensity
  - Blood Flow Velocity (Slope)
  - **Fractional Blood Volume (Max Amplitude)**

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DESTRUCTION-REPERFUSION

- Perfusion Quantification Helps Understand Diseased Tissue
- What Information Do We Get?
  - Time To Peak Intensity
  - Blood Flow Velocity (Slope)
  - Fractional Blood Volume (Max Amplitude)
  - **Blood Volume (Area Under the Curve)**

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DESTRUCTION-REPERFUSION

- Perfusion Quantification Helps Understand Diseased Tissue
- What Information Do We Get?
  - Time To Peak Intensity
  - Blood Flow Velocity (Slope)
  - Fractional Blood Volume (Max Amplitude)
  - Blood Volume (Area Under the Curve)
  - **Mean Transit Time**

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DESTRUCTION-REPERFUSION

- Perfusion Quantification Helps Understand Diseased Tissue
- Example:
- **Destruction-Reperfusion at Pixel Level**

Streeter J, et al... A Comparative Evaluation of Ultrasound Perfusion Imaging, Molecular imaging, and Volume Measurements in Evaluating the Response to Therapy. Unpublished Data. 2012.

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DESTRUCTION-REPERFUSION

- Perfusion Quantification Helps Understand Diseased Tissue
- Example:
- Destruction-Reperfusion at Pixel Level
- **Monitoring Time to 20% (Max Intensity)**

Streeter J, et al... A Comparative Evaluation of Ultrasound Perfusion Imaging, Molecular imaging, and Volume Measurements in Evaluating the Response to Therapy. Unpublished Data. 2012.

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DESTRUCTION-REPERFUSION

- Perfusion Quantification Helps Understand Diseased Tissue
- Example:
- Destruction-Reperfusion at Pixel Level
- Monitoring Time to 20% (Max Intensity)
- **Tumor Perfusion Monitoring During Therapy**

Streeter J, et al... A Comparative Evaluation of Ultrasound Perfusion Imaging, Molecular imaging, and Volume Measurements in Evaluating the Response to Therapy. Unpublished Data. 2012.

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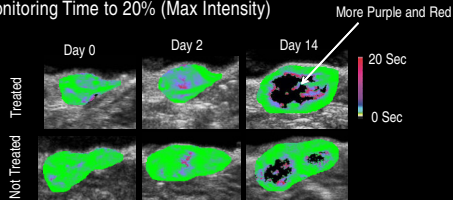
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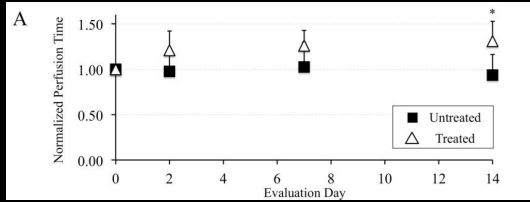
DESTRUCTION-REPERFUSION

- Perfusion Quantification Helps Understand Diseased Tissue
- Example:
- Destruction-Reperfusion at Pixel Level
- Monitoring Time to 20% (Max Intensity)



DESTRUCTION-REPERFUSION

- Perfusion Quantification Helps Understand Diseased Tissue
- Example:
- Destruction-Reperfusion at Pixel Level
- Monitoring Time to 20% (Max Intensity)



PART II

# ADVANCED IMAGING APPLICATIONS

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## MOLECULAR IMAGING

- Functional technique to evaluate changes on a molecular level
- Knowledge of molecular signature of pathology
  - Integrins, selectins etc...expressed on endothelial cells
  - VEGF,  $\alpha_v\beta_3$ , etc...

Dayton P, et al... Targeted Imaging Using Ultrasound. J Magn Reson Imaging; 16 (4); 2002.

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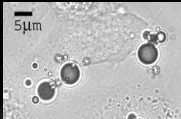
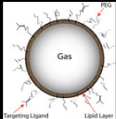
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## MOLECULAR IMAGING

- Targeted microbubble contrast agents
  - Shell material fitted with adhesion ligand
  - Example:  $\alpha_v\beta_3$  Ligand  $\rightarrow$  Cyclic RGD Peptide



Dayton et al., Mol Imaging, 2004 Apr;3(2):125-34.

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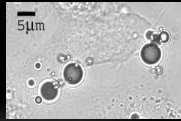
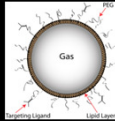
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## MOLECULAR IMAGING

- Targeted contrast agents injected intravascularly
- Collect at site of desired molecular marker expression
- Determine the presence or absence of a molecular change
- Assess disease or pathology prior to anatomical changes appear



Dayton et al., Mol Imaging, 2004 Apr;3(2):125-34.

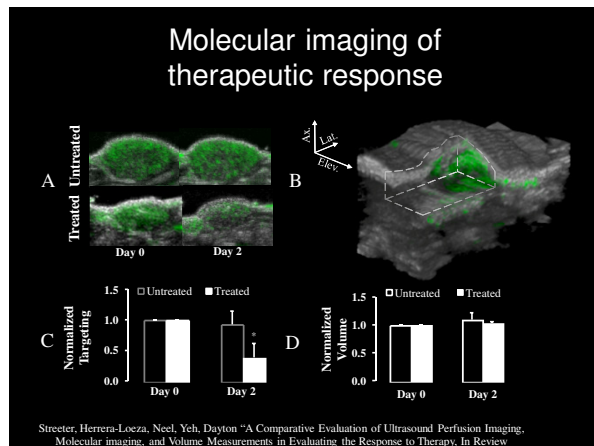
## MI & RESPONSE TO THERAPY

- Traditional methods for quantifying tumor progression – volume
  - *RECIST* (Response Evaluation Criteria In Solid Tumors)
- Size measurements provide delayed feedback
- Molecular imaging assesses molecular changes often before tumor size is affected

## MI & RESPONSE TO THERAPY

- Example:
  - Cancer Type: Human Pancreatic Adenocarcinoma
  - Animal Model: Mouse
  - Therapy: Experimental Aurora-A Kinase Inhibitor
  - Imaging target:  $\alpha_v\beta_3$

Streeter J, et al... A Comparative Evaluation of Ultrasound Perfusion Imaging, Molecular imaging, and Volume Measurements in Evaluating the Response to Therapy. Unpublished Data. 2012.

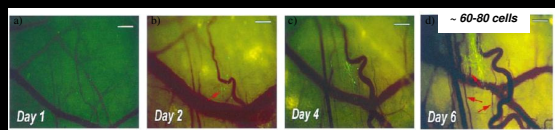


## Status of MI

- Mainly pre-clinical use
- Clinical Trials in Europe
  - Bracco, VEGFR2 targeted imaging in human prostate

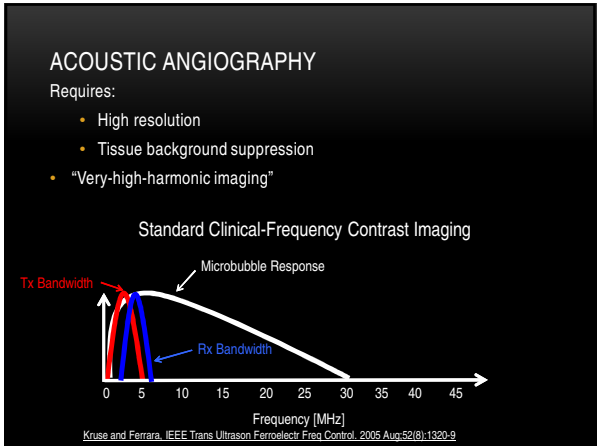
## Acoustic Angiography

- Goal:
  - Image microvasculature structure
  - Microvascular abnormalities/angiogenesis associated with malignancy



Li CY, Shan S, Huang Q, Braun RD, Lamm J, Hu K, Liu P, Dewhirst MW. "Initial stages of tumor cell-induced angiogenesis: evaluation via skin window chambers in rodent models". J Natl Cancer Inst. 2000 Jan 19;92(2):143-7.





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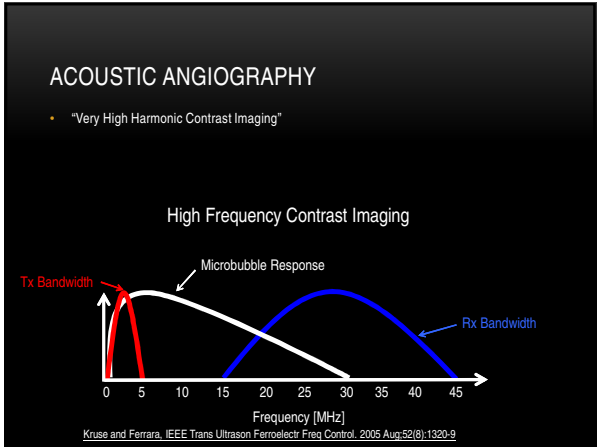
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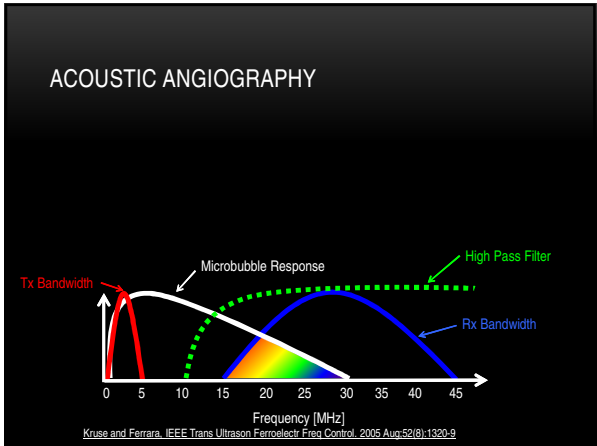
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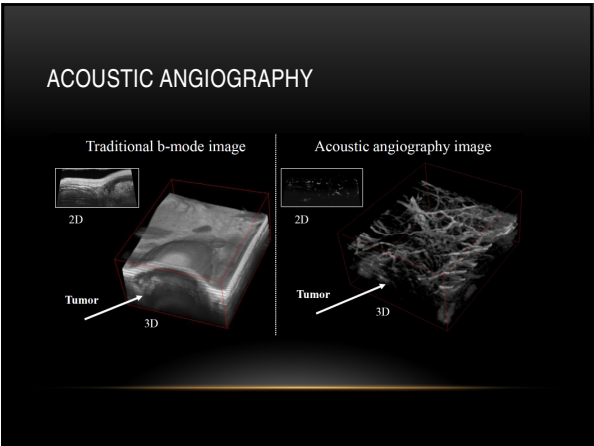
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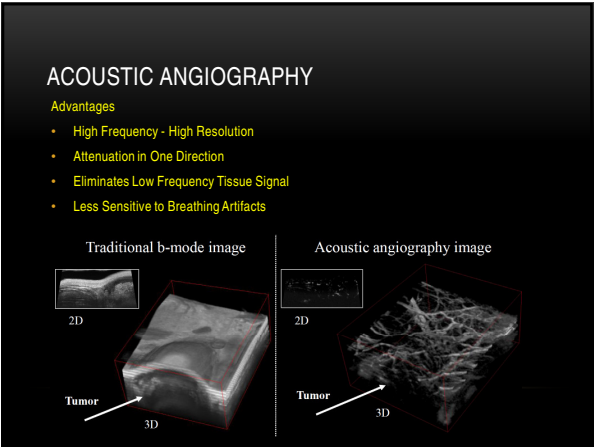
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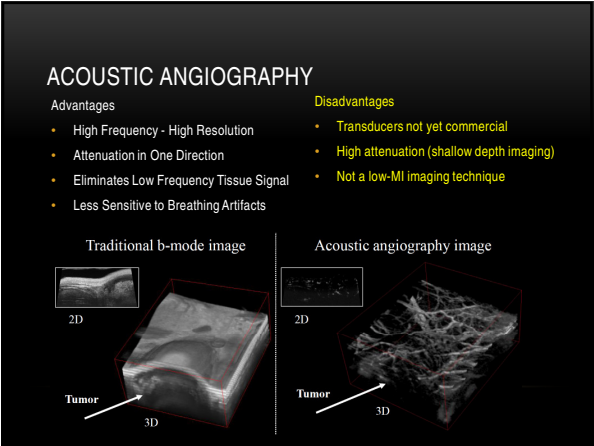
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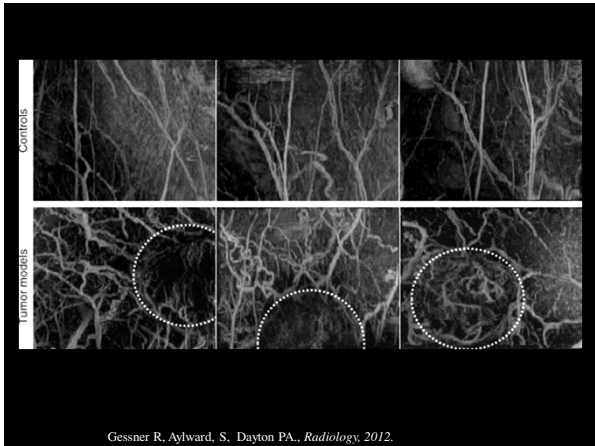
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Gessner R, Aylward, S, Dayton PA., *Radiology*, 2012.

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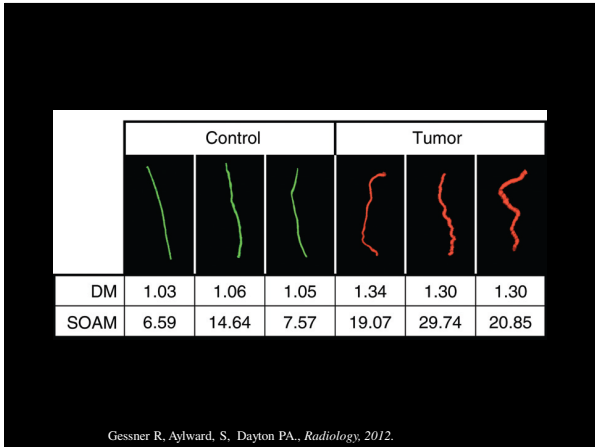
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Gessner R, Aylward, S, Dayton PA., *Radiology*, 2012.

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Table 2				
Summary of the P Values for the Statistical Tests Used to Assess Interanimal and Intrapopulation Variability in Vessel Tortuosity				
Group and Animal	DM		SOAM	
	Pooled Control Population	Pooled Tumors	Pooled Control Population	Pooled Tumors
Control animals				
1	.82	<.000147**	.75	<.000147**
2	.66	<.000147**	.47	.0010*
3	.025	<.000147**	.41	<.000147**
4	.63	<.000147**	.19	<.000147**
5	.09	<.000147**	.18	.002
6	.81	<.000147**	.95	<.000147**
7	.09	<.000147**	.99	<.000147**
Tumor-bearing animals				
1	<.000147**	.89	<.000147**	.007
2	.0002*	.41	<.000147**	.79
3	.0002*	.004	<.000147**	.79
4	<.000147**	.91	<.000147**	.47
5	.0006*	.76	.0016	.28
6	<.000147**	.94	<.000147**	.85
7	.0005*	.81	.0004*	.38
8	.0006*	.78	.0002*	.046
9	.0026	.16	.0014*	.11
10	<.000147**	.14	<.000147**	.86
Note.—Each cell indicates a comparison between the ensemble of vessel tortuosities for the animal in each row and the pooled population in each column.				
* P values are less than the Bonferroni-corrected P value of .00147.				
† P values more than 10 times smaller than the Bonferroni-corrected P value of .00147.				

Gessner R, Aylward, S, Dayton PA., *Radiology*, 2012.

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## HOW ULTRASOUND ANGIOGRAPHY CAN BE USED IN ONCOLOGY RESEARCH:

- Blood vessel structure, density, and pattern can be assessed non-invasively
- Microvascular tortuosity abnormalities are an indicator of tumor development
- Prior studies have shown that vessel morphological characteristics are related to tumor malignancy and response to treatment (Bullitt)

Bullitt E, Ewend M, Vredenburgh J, et al. Neuroimage. 2009; Aug;47 Suppl 2:T143-51

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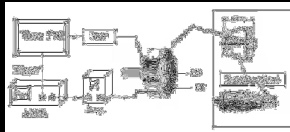
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## Acoustic Angiography

- Traditional Ultrasound Transducer
  - Transmit and Receive (x1 Frequency Bandwidth)
- Dual Frequency Imaging
  - Transmit Using Low Frequency Bandwidth
  - Receive Using High Frequency Bandwidth



Gessner R, et al... High-resolution, high-contrast ultrasound imaging using a prototype dual-frequency transducer: In vitro and in vivo studies. IEEE Trans Ultrason Ferroelectr Freq Control. 2010.

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## SUMMARY: DIAGNOSTIC IMAGING WITH MICROBUBBLES

- perfusion imaging \*\*
- quantitative dynamic perfusion imaging
- molecular imaging
- acoustic angiography
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\*\* only perfusion imaging is currently used clinically in the US

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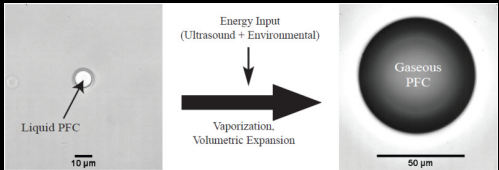
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# ULTRASONIC ACTIVATABLE CONTRAST AGENTS

- Liquid Perfluorocarbon Core
- Lipid or Polymer Shell
- Tipped to Gaseous State by Ultrasound



Sheeran P, et al... Formulation and acoustic studies of a new phase-shift agent for diagnostic and therapeutic ultrasound. Langmuir; 27, 2011.

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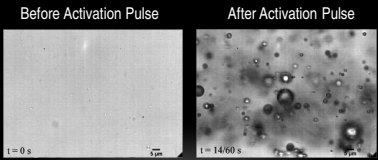
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Sheeran P, et al... Formulation and acoustic studies of a new phase-shift agent for diagnostic and therapeutic ultrasound. Langmuir; 27, 2011.

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# ULTRASONIC ACTIVATABLE CONTRAST AGENTS

- Applications
  - Vascular Occlusion
  - Extravascular Diagnostics
  - Other microbubble applications

Sheeran P, et al... Formulation and acoustic studies of a new phase-shift agent for diagnostic and therapeutic ultrasound. Langmuir; 27, 2011.

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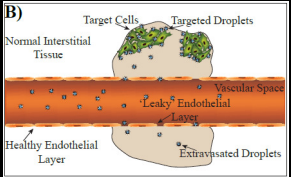
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# ULTRASONIC ACTIVATABLE NANOPARTICLES

- Liquid Perfluorocarbon Core
- Lipid or Polymer Shell
- Tipped to Gaseous State by Ultrasound

• **Example:**

A Nanoscale Approach to Molecular Imaging



Sheeran P, et al... Phase-change nanoagents for extravascular ultrasound molecular imaging: an in-vitro proof of principle. In Review, 2011.

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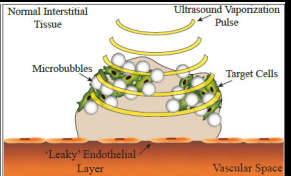
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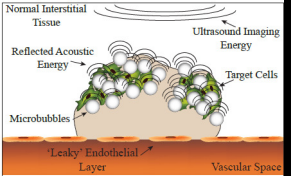
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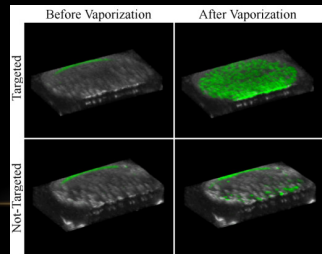
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## ULTRASONIC ACTIVATABLE NANOPARTICLES

- Liquid Perfluorocarbon Core
- Lipid or Polymer Shell
- Tipped to Gaseous State by Ultrasound

• **Example:**




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## ULTRASOUND BIOEFFECTS AND THERAPY

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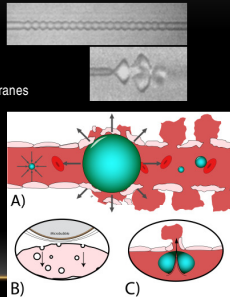
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## BIOLOGICAL EFFECTS – INTERACTION BETWEEN ULTRASOUND AND MICROBUBBLES

- Increased thermal energy conversion
- Physical effects from bubbles themselves
  - Microstreaming
  - Mechanical stimulation of biological membranes
- Cavitation (violent expand/collapse)
  - Shock Waves
  - Microbubble Jetting
  - High Pressures and Temperatures
  - Free Radical Formation




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## BIOLOGICAL EFFECTS

### Mild

- Reversible Capillary Permeability Changes
- Reversible Cell Membrane Permeability
- Small temperature changes

### Strong

- Capillary Rupture
- Tissue ablation
- Cell death

Quaia E, et al., Contrast media in ultrasonography-basic principles and clinical applications. New York: Springer; 2005.

## BIOLOGICAL EFFECTS

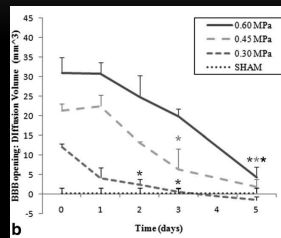
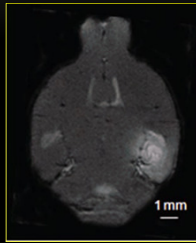
- Occur at low frequencies (~1 MHz) below that typically used for clinical imaging
- Occur at ultrasound intensity levels greater than that typically used for clinical imaging

## BIOEFFECTS USED THERAPEUTICALLY

- **Drug delivery – can be achieved LOCALLY with focused ultrasound and microbubbles**
- Enhanced blood brain barrier permeability
- Enhanced capillary permeability
- Increased cellular delivery through cell membrane permeability
- **Have been shown to significantly enhance local drug and gene delivery, and corresponding therapeutic response**
- Improved thermal ablation (requires less delivered power with microbubbles – reduces thermal damage to healthy tissues)



### EXAMPLE: TRANSIENT BLOOD BRAIN BARRIER OPENING



Samiotaki G, Vlachos F, Tung YS, Konofagou EE, Magn Reson Med. 2012 Mar;67(3):769-77

### SAFETY

### MICROBUBBLE CLEARANCE

- Microbubbles are vascular agents
- Phagocytosis in Liver and Spleen
- Gas is expelled through the lungs
- Shell content is eliminated by kidney and liver
- Phospholipids enter normal metabolism
- Typical circulation half life ~ 5-15 minutes

Quaia E, et al., Contrast media in ultrasonography-basic principles and clinical applications. New York: Springer; 2005.

### SAFETY CONCERNS

- 1994 Albunex (albumin shell – air core)
- 1997 Optison (albumin shell – perfluorocarbon core)
- 2001 Definity (lipid shell – perfluorocarbon core)

**INDICATIONS**

Activated DEFINITY® (Perflutren Lipid Microsphere) Injectable Suspension is indicated for use in patients with suboptimal echocardiograms to opacify the left ventricular chamber and to improve the delineation of the left ventricular endocardial border.

**CONTRAINDICATIONS**

Do not administer DEFINITY® to patients with known or suspected right-to-left, bi-directional or transient right-to-left cardiac shunts, by intra-arterial injection, or to patients with known hypersensitivity to perflutren.

Lantheus Medical Imaging

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### SAFETY CONCERNS

- Following reports of 11 deaths and 199 serious cardiopulmonary reactions after the administration of such agents in echocardiography.
- **2007: Black box Warning**

October 2007

**Class label changes for ultrasound contrast agents:**

- Contraindications for patients with serious cardiopulmonary conditions
- Boxed **WARNING**
- Mandatory physiologic monitoring

Lantheus Medical Imaging

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May 2008

**Class label changes for ultrasound contrast agents, based on review of new data from Lantheus and the academic community, as well as strident advocacy from physicians and ultrasound societies:**

- October 2007 contraindications were removed
- Physiologic monitoring required for patients with pulmonary hypertension and unstable cardiopulmonary syndromes

**WARNING: Serious Cardiopulmonary Reactions**

Serious cardiopulmonary reactions, including fatalities, have occurred during or following perflutren-containing microsphere administration.

- Assess all patients for the presence of any condition that precludes DEFINITY® administration (see CONTRAINDICATIONS).
- In patients with pulmonary hypertension or unstable cardiopulmonary conditions, monitor vital sign measurements, electrocardiography and cutaneous oxygen saturation during and for at least 30 minutes after DEFINITY® administration (see WARNINGS).
- Always have resuscitation equipment and trained personnel readily available.

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SAFETY CONCERNS

- Extensive Investigative Studies
  - > 5 million administered doses
    - Most frequent adverse reactions are mild
      - Headache: 5%, Nausea 4%, Flushing 4%, Dizziness 3%.
    - arrhythmias, hyper/hypotension, neurologic and anaphylactoid reactions - rare

Procedure	Severe adverse effects	Risk
Contrast Echo	Death Anaphylactoid reaction	1:500,000 1: 15,000
Myocardial scintigraphy	Fatal malignancy	1:1000- 1:10,000
Exercise ECG	MI/death	1:2,500
Dobutamine stress test	MI/VF	1:2000
Coronary angiography	Death	1:1,000
Iodine (CT) contrast exam	Life-threatening reaction	1:500 – 1:5000

Table Modified from Main et al JACC 2007;50:2434-7 and from www.ICUS-society.org

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FDA Revised Contrast Agents Labeling in Oct 2011

October 2011

**DEFINITY® label changes:**

- The following disclaimer was deleted from the Indications & Usage section:  
"The safety and efficacy of DEFINITY® with exercise stress or pharmacologic stress testing have not been established."
- The following monitoring information was deleted from the boxed **WARNING**:  
"In patients with pulmonary hypertension or unstable cardiopulmonary conditions, monitor vital sign measurements, electrocardiography, and cutaneous oxygen saturation during and for at least 30 minutes after DEFINITY® administration."
- The following statement was added to the boxed **WARNING**:  
"Most serious reactions occur within 30 minutes of administration."

**WARNING: SERIOUS CARDIOPULMONARY REACTIONS**  
*See full prescribing information for complete boxed warning*

Serious cardiopulmonary reactions, including fatalities, have occurred uncommonly during or following perflutren-containing microsphere administration (5.1). Most serious reactions occur within 30 minutes of administration.

- Assess all patients for the presence of any condition that precludes DEFINITY® administration (4).
- Always have resuscitation equipment and trained personnel readily available.

<http://www.fda.gov>

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SAFETY OF ULTRASOUND CONTRAST AGENTS: SUMMARY

- ultrasound contrast agents are very safe with a low incidence of side effects
- They are not nephrotoxic or cardiotoxic
- incidence of hypersensitivity or allergic events appears much lower than current X-ray or MR contrast agents
- As in all clinical procedures, physicians should balance potential clinical benefit against the theoretical possibility of associated adverse bioeffects in humans
- New accreditation standards (ICAEL) for the first time **require US echocardiography** laboratories to use ultrasound contrast agents to improve suboptimal echocardiograms, unless an alternative imaging plan is in place
- Cardiologists and radiologists throughout Europe, Canada, Asia and Latin America routinely and safely use CEUS to image and diagnose abnormalities throughout the body as well as tumors of the liver, ovaries, breast, testicles, lymph nodes, etc.

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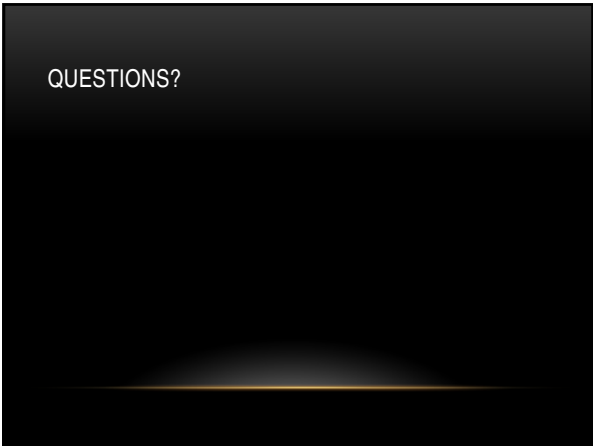
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