

## The Promise and Potential Pitfalls of Deformable Image

### Clinical applications in the Head&Neck: *Verification using 3D dosimetry*



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## Disclosures

- NCI R01 funding
  - RPC collaboration (IROC)
- Several sponsored research agreements involving the application of 3D dosimetry



## Outline

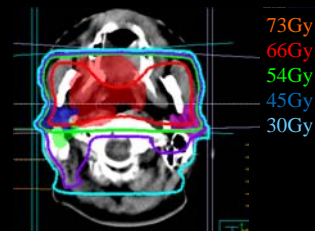
- Basics of H&N IMRT
  - Key challenges
- DIR can help with .....

  - Contouring: - greater efficiency and accuracy ?
  - Dose accumulation: intra-Tx dose acceptable ?
  - Adaptive planning: create a more optimal plan ?
  - Treatment response assessment ?

- Role of 3D Dosimetry in DIR Validation

## An old-school H&N treatment plan !

- Problem ...
  - This plan is not conformal enough !



## Theoretical birth of IMRT

- 1988 Brahme – 1<sup>st</sup> inverse planning.
- 1989 Webb - simulated annealing.

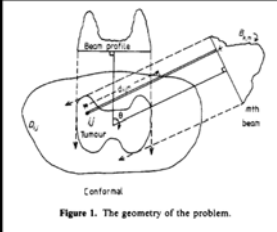


Figure 1. The geometry of the problem.

Optimisation of conformal radiotherapy dose distributions by simulated annealing

1989

S. Webb

Johns Department of Physics, Institute of Cancer Research and Royal Marsden Hospital, Downs Road, Sutton, Surrey, UK

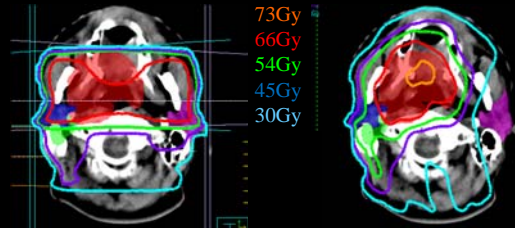


Anders Brahme



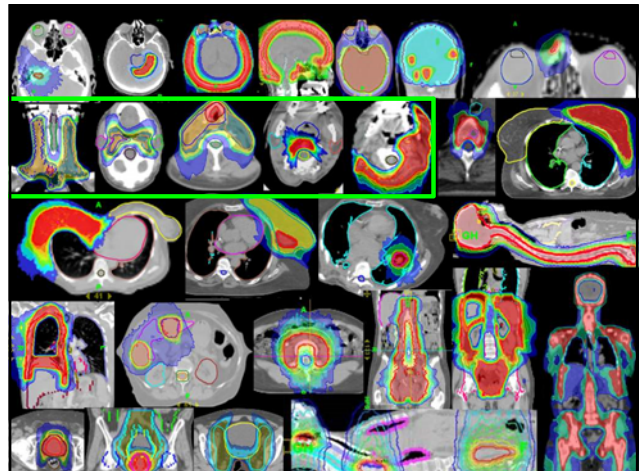
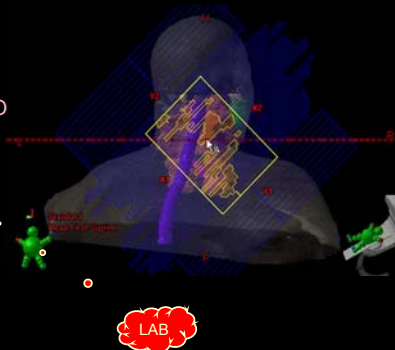
Steve Webb

- Problem ...
  - This plan is not conformal enough !
- Solution – fluence modulation



## We are now masters of fluence !

- Fluence modulation
  - IMRT, VMAT
  - Tomotherapy
  - Cyberknife, VERO
- New challenges
  - PTV definition
  - Adaptive therapy
  - Efficiency
  - Optimal Plan
  - Knowledge guide
  - Commissioning\ Verification



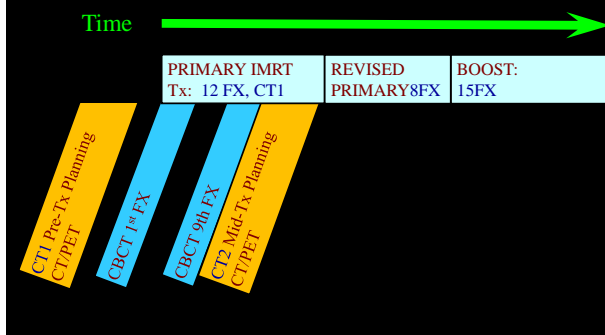
## The role of DIR in H&N RT

- DIR can help with .....
  - Contouring: greater efficiency and accuracy ?
  - Dose accumulation: intra-Tx dose acceptable ?
  - Adaptive planning: create a more optimal plan ?
  - Treatment response: enable more precise assessment ?

## Clinical Example

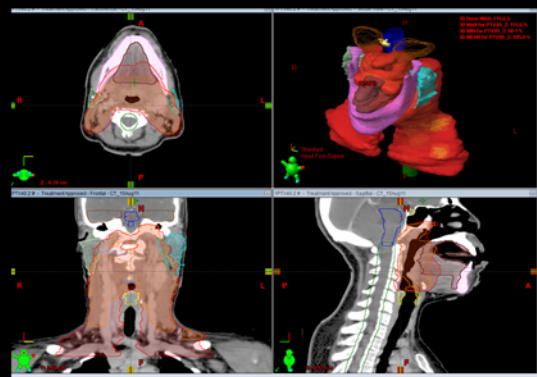
- Nasopharynx, with Bilateral Necks
  - T4N3a
    - Primary - 20fx of 2Gy/day, 40Gy total
    - Boost - 15fx of 2Gy/day, 30Gy total
- H&N with substantial tumor shrinkage
  - Adaptive Planning: How to ensure adequate
    - PTV coverage
    - OAR sparing
  - Dose Warping and Dose Accumulation

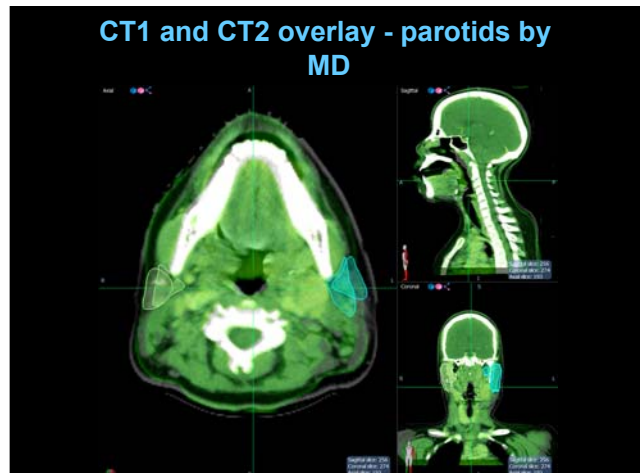
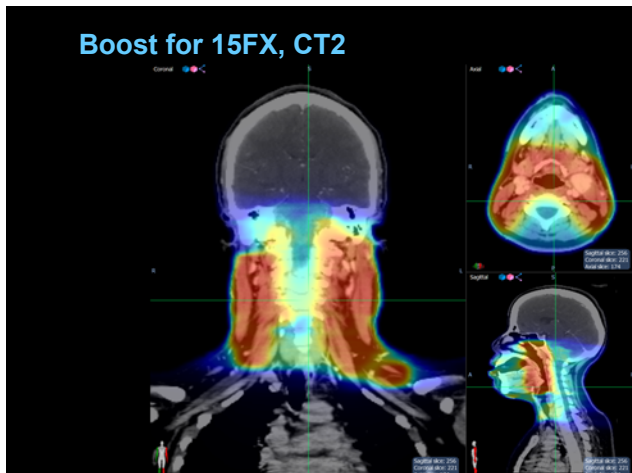
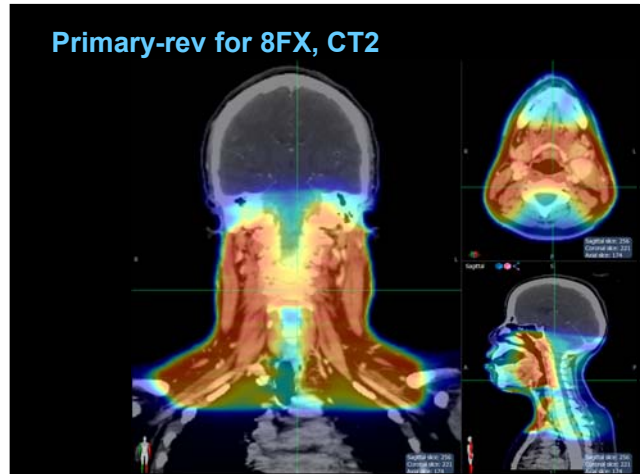
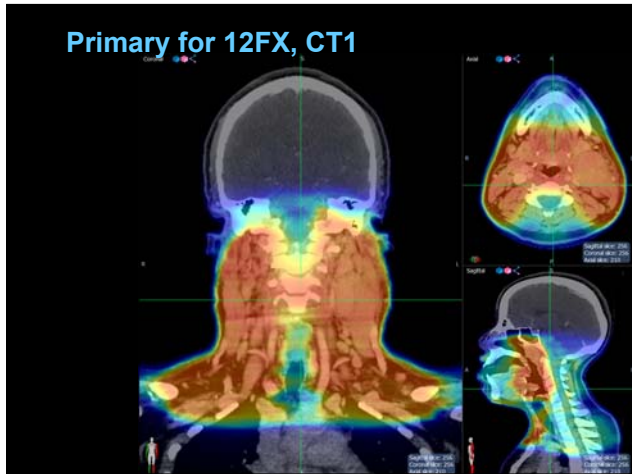
## Treatment timeline



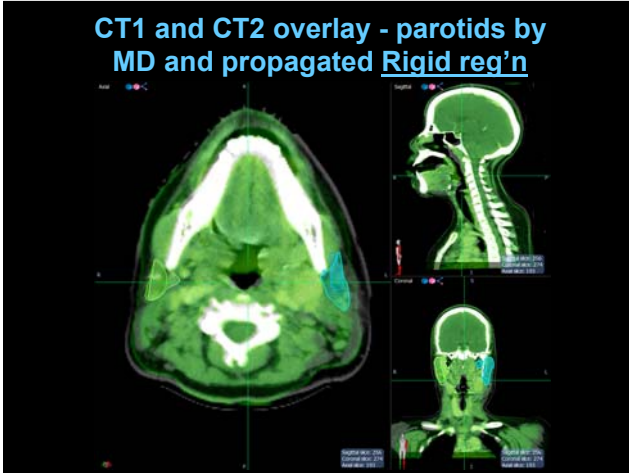
## Overview of the plan

Shiva Das

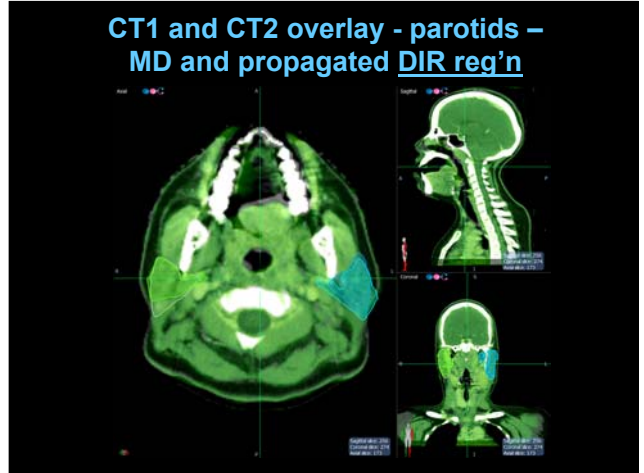




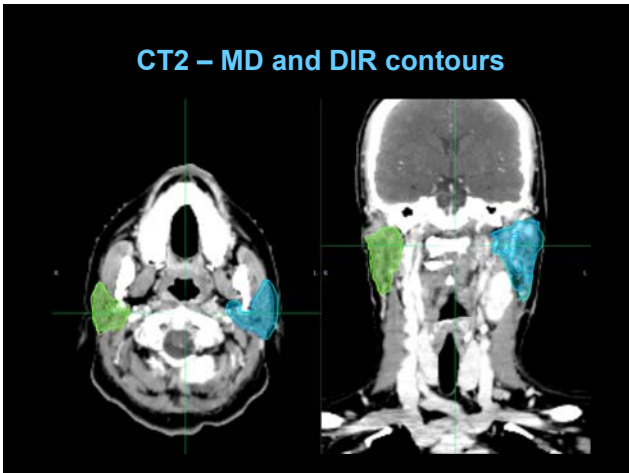
CT1 and CT2 overlay - parotids by MD and propagated Rigid reg'n



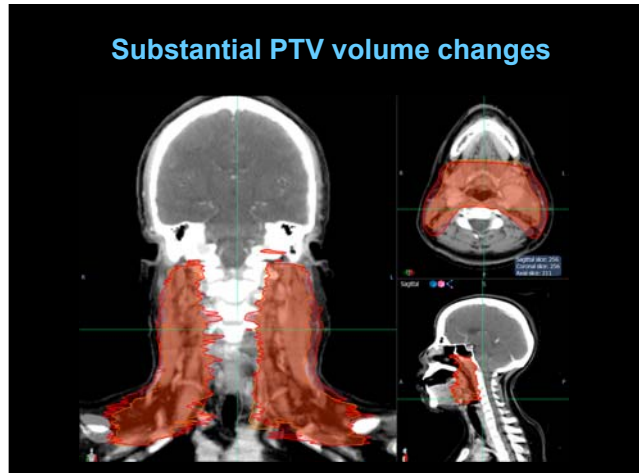
CT1 and CT2 overlay - parotids - MD and propagated DIR reg'n



CT2 - MD and DIR contours

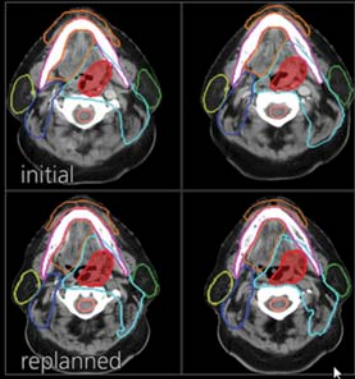


Substantial PTV volume changes

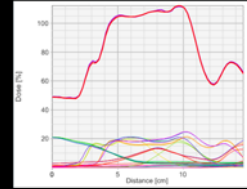


## Adaptive re-contouring MIM

- Deformably contour replanning CTs
- Generates entire structure sets automatically
- Timesavings of 75% demonstrated
- Makes true adaptive therapy possible

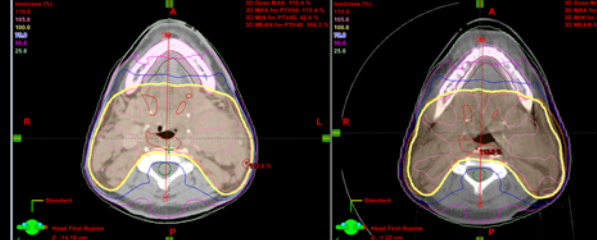


## Dose of the day ?

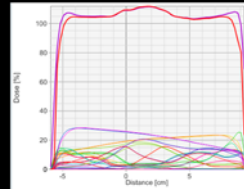


CT1

CBCT (re-calc)

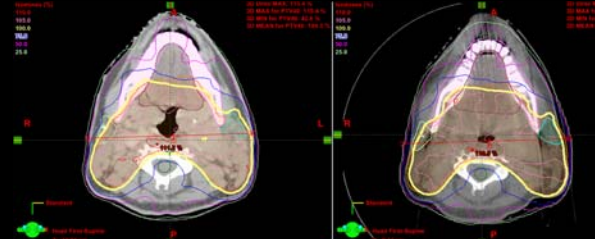


## Dose of the day ?



CT1

CBCT (re-calc)



## What is the final accumulated dose ?

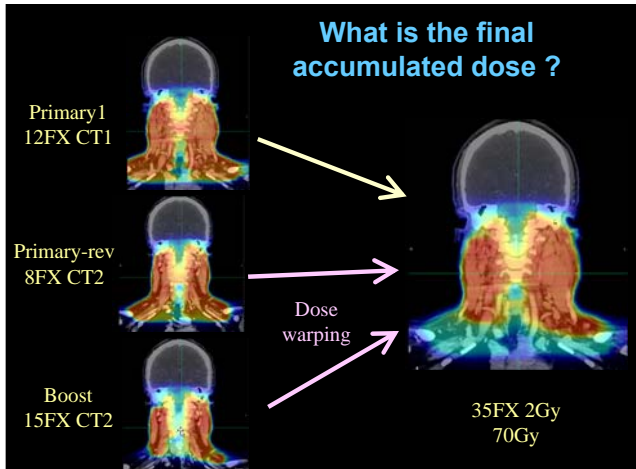
Primary1  
12FX CT1

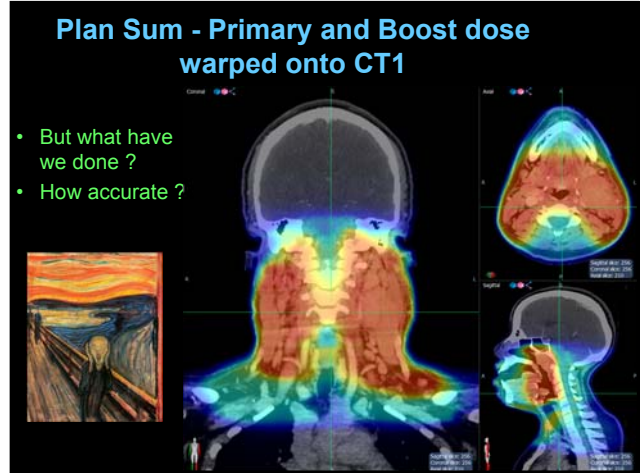
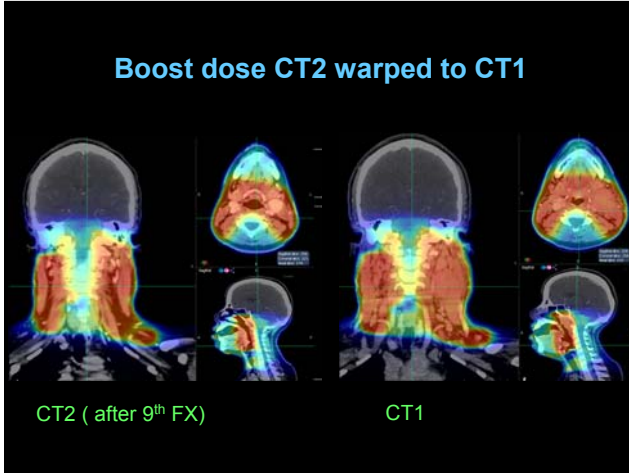
Primary-rev  
8FX CT2

Boost  
15FX CT2

Dose  
warping

35FX 2Gy  
70Gy





### Challenges of dose warping ?

- DIR assumes
  - Every point in one image has a corresponding point in the other
- Not valid when ....
  - Tissue shrink/swells
  - Dose in deformed voxel ?

Physical Dose is defined as  
**Energy per unit mass (J/Kg)**

When dose is assigned to a voxel of a different volume, either energy or density is affected.  
-> Implementation is critical

2013 AAPM Annual Meeting  
Session: Deformable Image Registration, Contour Propagation and Dose Mapping: 101 and 201

Marc Kissler, PhD  
The University of Michigan

Jean Pouliot, PhD  
University of California

Velocity (Theo Lazarkis)

### Can 3D Dosimetry help ?

- Radiochromic Plastic: Presage
- Contrast: light absorption
- Good dosimetry properties
- Flexible

CN(C)C1=CC=C(C=C1)C2=CC=C(C=C2)C3=CC=C(C=C3)N(C)C

Leuco malachite Green (LMG)

→

CN(C)C1=CC=C(C=C1)C2=CC=C(C=C2)C3=CC=C(C=C3)N(C)C

Malachite Green

$\lambda_{max} = 633 \text{ nm}$

5 Beam Tx

Heuris Inc, [www.presage3d.com](http://www.presage3d.com)

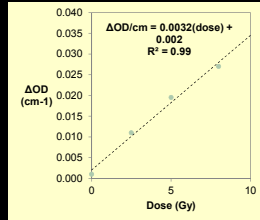
### Presage-Def Deformable 3D Dosimeter



- Elastic polyurethane
- Radiochromic leuco dye
  - ▶ Linear  $\Delta OD$  with dose

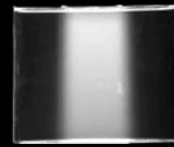
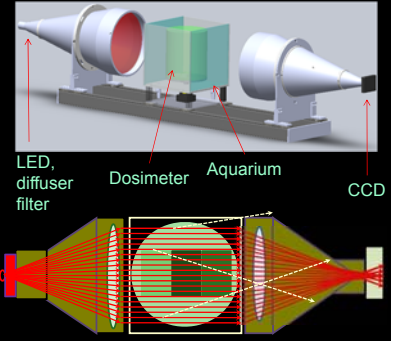


Increasing Dose  $\longrightarrow$



### DLOS : Duke Large Field-of-View Optical-CT Scanner

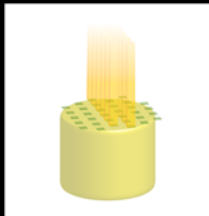
Design Specifications		
FOV	240	mm
resolution	2 - 0.2	mm
Time	10 - 30	mins



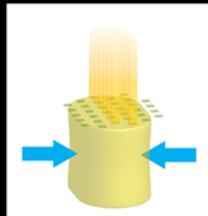
Thomas A , et al. Med Phys, 2011

“On the need for validation of deformable dose accumulation (DIR) with a novel 3D dosimeter.”

Juang et al. IJROBP, 2013



Control  
(No Deformation)

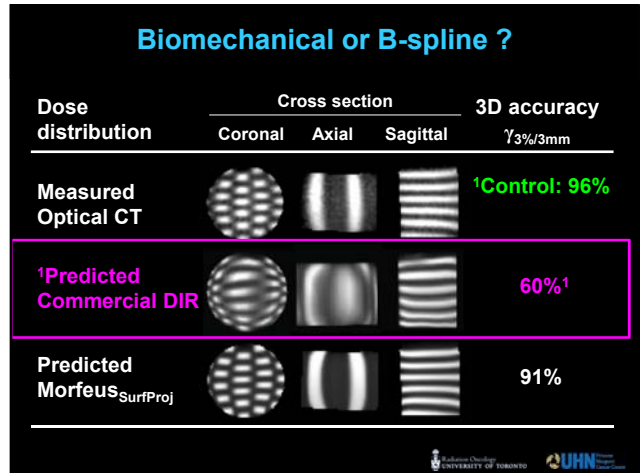
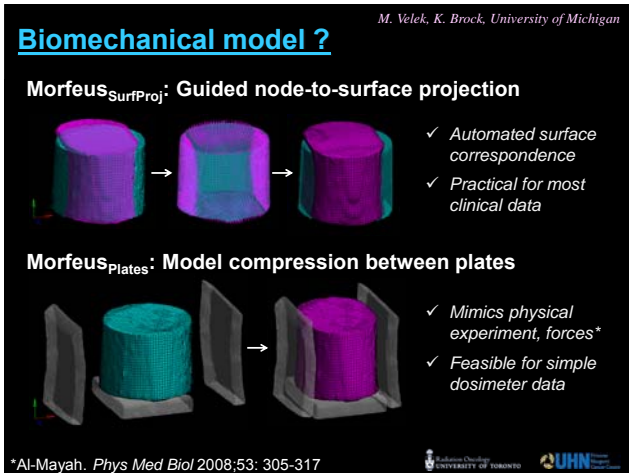
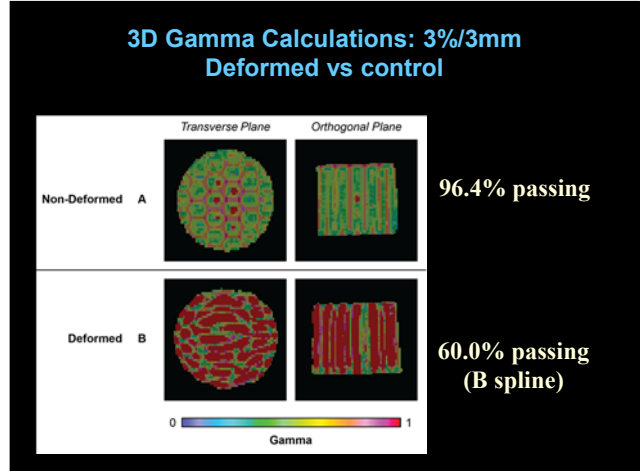
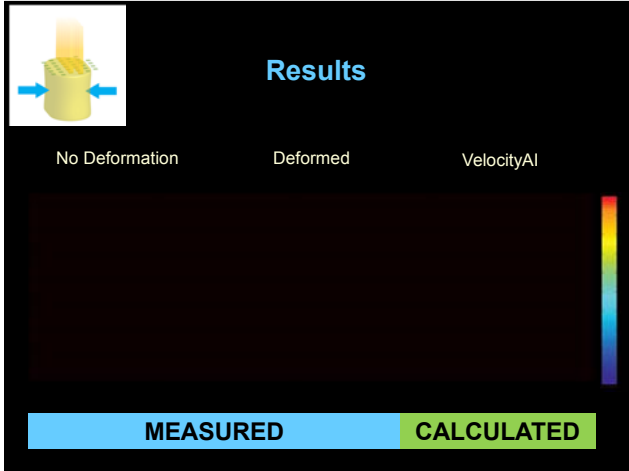


Deformed  
(27% Lateral Compression)

	Measured	Velocity	Difference
Non-deformed			
Deformed			

<sup>1</sup>Juang, IJROBP 2013;87(2): 414-421





### 3D deformable phantoms containing bony and cavity inserts.

Presage-Def (15.7 cm)  
High Z Rigid Insert (2.8 cm)  
Air Cavity (4.0 cm)  
Complex, Non-Uniform Deformation

Titania Juang

### Compatible with optical-CT 3D dosimetry – 1mm<sup>3</sup> voxels

8.6 cm  
7.4 cm

OD/mm<sup>2</sup>

### Compatible with 3D Printing

Steve Bache

- 3D print anatomically accurate dosimeters
- ProtoGen (plastic)  
– 0.23mm x 0.23mm x 0.1 mm
- Optical-CT projection
- Un-irradiated dosimeter

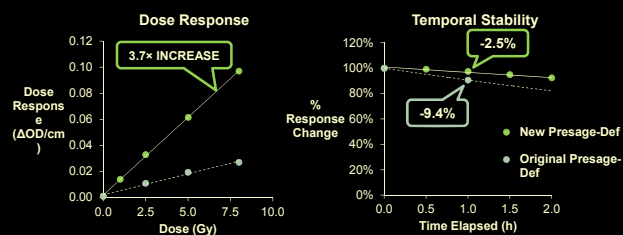
### 3D Printed Presage dosimeter

2.5 mm cone, 0.5mm<sup>3</sup>

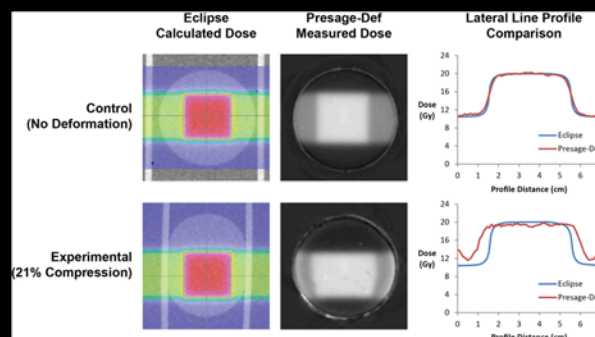
Optical-CT un-irradiated  
X-ray-CBCT showing spinal

## Recent developments

- **New Presage-Def formulation**
  - Improved dose sensitivity and response stability
  - Higher durometer (30-50A versus 10-20A)

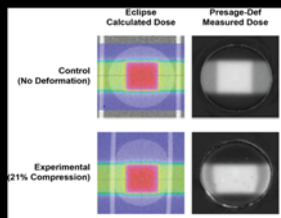


## Presage-Def 4-field box dosimetry



## Can we measure dose in a deformed dosimeter ?

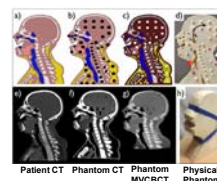
- Integral dose within 75% isodose line consistent with planned dose in both DIR and control



	Control Integral Dose (Gy·cm <sup>3</sup> )	Deformation Integral Dose (Gy·cm <sup>3</sup> )
Eclipse	558.5	549.4
Presage-Def	537.0	527.5
% Difference	<b>3.9%</b>	<b>4.0%</b>

## UCSF University of California San Francisco 3D H&N Deformable Phantom For DIR Performance Evaluation

The phantom splits along the sagittal plane to reveal optical markers that are used to measure the ground truth deformation between the undeformed and deformed phantom.



This enables the ground-truth deformed dose to be known, which is the basis for checking the accuracy of any DIR algorithm.

Singhroo K., Kirby N. and Pouliot J., A three-dimensional head-and-neck phantom for validation of multi-modality deformable image registration for adaptive radiotherapy, Med. Phys. 2014. (submitted).

Jean Pouliot, University of California San Francisco

UCSF  
University of California  
San Francisco

## The Ground Truth

Undeformed Phantom CT Images      Deformed Phantom CT Images

Measured deformation

$\Delta x$        $\Delta y$        $\Delta z$

MSR

Use your **favorite DIR** on the two phantom images and compare predicted deformation with measured deformation (ground truth)

*Jean Pouliot, University of California San Francisco*

## Conclusions

- **Promise**
  - Efficiency – contouring
    - ATLAS's
    - Contour propagation
  - Efficacy - accuracy
    - Improve adaptive therapy
    - Dose accumulation
- **Pitfalls ?**
  - Contour accuracy
    - Physician approval essential
  - Dose accumulation
    - Extreme caution
    - Validate/commission your algorithm TG132
  - Know your algorithm ?!