

Image Fusion, Contouring, and Margins in SRS

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Overview

Review SRS uncertainties due to:

- image registration
- contouring accuracy
- contouring variability

Assess levels of uncertainty and greatest contributors to overall uncertainty

Discuss appropriate PTV margins to account for uncertainties in SRS

Registration Accuracy

Registration Accuracy

- Accuracy depends on registration method:
- Local "box"-based rigid registrations can produce higher accuracy than global rigid registrations
 - ROIs should be in close proximity target

Registration Accuracy

- Site-dependent:
 - Registration of spinal sites is less straightforward and has lower accuracy
 - Deformable image registration is tempting for spine registrations but the associated uncertainties are too high for use in SRS

Rigid vs. Deformable Registration

- Accuracy depends on registration method:
- Rigid registration is more accurate than deformable registration
 - rigid: ~1-2 mm uncertainty*
 - deformable: ~5-7 mm uncertainty**

*Benchmark Test of Cranial CT/MR Registration • *IJROBP* • Kenneth *et al.* • 2010

**Need for application-based adaptation of DIR • *Med. Phys.* • Kirby *et al.* • 2013

**Performance of DIR in low contrast regions • *Med. Phys.* • Supple *et al.* • 2013

Registration Workflow Comparison

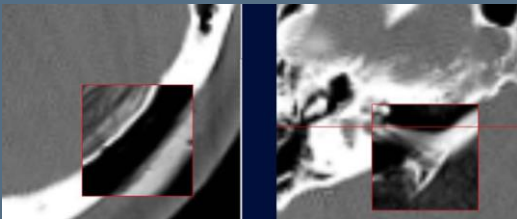
Simulation and planning images	Gamma Knife	Linac-based SRS
Planning	MRI*	CT
Contouring	MRI*	MRI or PET/CT
Fusion Type	single-modality rigid registration	multimodal rigid registration

* unless MRI is contraindicated

Modality

- Modality dependent:
 - Multi-modal registrations are typically less accurate than unimodal registrations, (especially for deformable registration)
 - Registering MRIs of differing sequences is not truly unimodal because of the difference in enhancement for certain regions
 - Different volumes may have different slice thicknesses

Co-Registration Accuracy



Visual evaluation of registration accuracy can be difficult.

Contouring Accuracy

Contouring Accuracy

Contouring accuracy is affected by:

- Modality
- Spatial resolution
- Signal to noise ratio (SNR)
- MR field strength
- Planning image timing
- Contrast injection timing
- Additional factors: slice thickness, image artifacts, motion blur, spatial distortion

Modality

Modality affects GTV & CTV contouring:

- Tumor volumes across sites are typically larger on CT+MRI

Modality	Mean Volume
CT only	29.6 cm ³
MRI only	51.4 cm ³
CT+MRI	56.5 cm ³

MR GTVs were 74% larger than CT only

CT+MRI GTVs were 10% larger than MR only

Influence of MRI on GTV delineation • *IJROBP* • Emami *et al.* • 2003

Modality

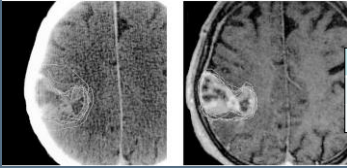
Modality affects GTV & CTV contouring:

- Tumor volumes across sites are typically larger on CT+MRI

CT only

CT + MRI

A difference of 10 cm³!



Modality	Mean Volume
CT only	59.5 cm ³
CT + MRI	69.6 cm ³

Interobserver variations GTV delineation • *Radio & Onc* • Weltens *et al.* • 2001

Spatial Resolution & SNR

- Spatial resolution and SNR also affect imaging accuracy
 - Slice thickness contributes substantially to contouring and image fusion accuracy
 - SNR is greater concern for MRI
- In most cases, visual inspection is employed to determine appropriate resolution and SNR levels

Slice Thickness

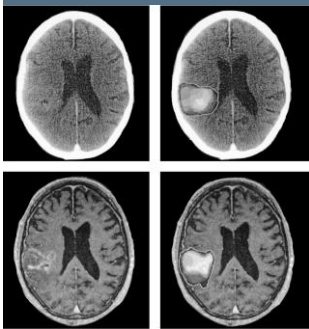
- Slice thickness affects image registration accuracy:
 - Thinner slices improve accuracy (improves interpolated image accuracy)
 - Typical planning CT and MRI slice thicknesses range from 1 mm to 3mm

Additional Factors

- Slice thickness
- Image artifacts (e.g. metal artifacts)
- Motion blur
- Spatial distortion (especially MRI)

Contour Variation

Contour Variation



5 patients, 9 observers

Modality	Volume Ratio (largest: smallest)
CT only	(2.8, 1.8, 1.8, 1.9, 1.7)
CT + MRI	(2.4, 1.7, 1.9, 2.7, 1.5)

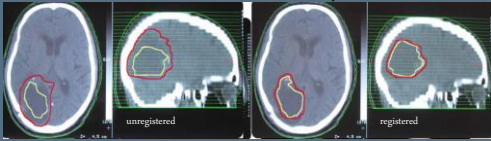
Volumes vary up to 30% of the mean volume

GTV range: as large as 174% and as small as 65.8% of mean volume

Interobserver variations GTV Delineation • *Radio & Onc.* • Weltens et al. • 2001

Contour Variation

7 patients, 5 observers



Modality	Concordance Index	Agreement Ratio (AR)
unregistered	14.1 +/- 12.7%	.24 +/- .18
registered	47.4 +/- 12.4%	.67 +/- .15

CT+ registered MR reduces interobserver GTV variability

$$\text{Agreement ratio (AR)} = \frac{\text{common overlapping volume}}{\text{encompassing volume}}$$

Target delineation: interobserver variability • *Radio & Onc.* • Cattaneo *et al.* • 2005

Contour Variation

31 patients, 6 observers

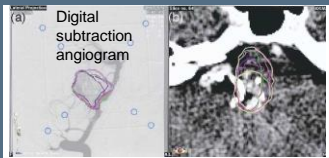


Fig. 1. Contouring variations in a patient with a brainstem arteriovenous malformation. (a) Target volume presented as different colors. All contours were automatically projected on computed tomography images used for further analysis (b).

Mean AR = 0.19 +/- 0.14

AR < 0.6 for all patients

$$\text{Agreement ratio (AR)} = \frac{\text{common overlapping volume}}{\text{encompassing volume}}$$

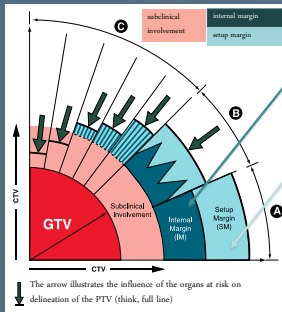
SRS for brain AVMs: Interobserver variability • *IJROBP* • Buis *et al.* • 2005

Margins

What margin for SRS?

- Margins should be sufficient to account for treatment uncertainties and guarantee target coverage
- They must be balanced to minimize potential negative side effects resulting from increased normal tissue dose (more important for SRS)
- Some clinics choose not to include margin expansions (CTV = PTV)

What is an appropriate margin?



- **Internal margin (IM):**
 - Residual motion, deformation
- **Setup margin (SM):**
 - Ensures adequate clinical coverage
 - Includes all uncertainties
 - Appropriate for hypofractionation

Journal of the ICRU: Volumes • Volume 4 Number 1 • 2004

Margins – not your simple PTV

Margin recipes based on standard fractionation (van Herk 1999) are not appropriate for few fractions:

$$M = 2.5 \Sigma_{tot} + 0.7\sigma_{tot}$$

Several groups have adapted the van Herk recipe for hypofraction:

- Stroom and Heijmen (2003)
- Gordon and Siebers (2007)

ICRU Report 62 • van Herk *et al.* • 1999

Geometrical uncertainties, planning margins • Rad & Onc • Stroom *et al.* • 2002

PTV margins finite fractions & small systematic errors • PMB • Gordon *et al.* • 2007

Herschtal Margin for SBRT

- Adjusted van Herk formula as lower limit
- Developed method for estimating upper limit
- Model interpolates between limits
- Verified using MC simulation
- Specific to each clinic

Calculating margins for hypofractionated RT • *PMB* • Herschtal *et al.* • 2013

Summary

Summary

- Contours can vary substantially from physician to physician
 - Minimize by appropriate imaging choices (modality, MR field strength, etc.)
 - Generally not accounted for in PTV
- Contouring accuracy: small contribution to overall uncertainty (~1-2mm)
 - Minimized by imaging choices (slice thickness, reduction of image artifacts, etc.)
- Image registration: small contribution (~1-2mm)
 - Rigid registration, manual vs. automatic

Which of the following SRS workflow choices is likely to contribute MOST to overall uncertainty?

- 10% 1. extend frame immobilization
- 19% 2. CTV contouring variability
- 33% 3. rigid image registration
- 24% 4. 3 mm MRI slice thickness
- 14% 5. 3 mm plan CT slice thickness

Which of the following SRS workflow choices is likely to contribute MOST to overall uncertainty?

1. Answer: CTV contouring variability

Refs: "Interobserver variations in gross tumor volume delineation of brain tumors on computed tomography and impact of magnetic resonance imaging", *Radiotherapy & Oncology* 60 (2001), p. 49-59.

"Target delineation in post-operative radiotherapy of brain gliomas: Interobserver variability and impact of image registration of MR (pre-op) images on treatment planning CTs", *Radiotherapy and Oncology* 75 (2005), p. 217-223.

Which of the following is currently LEAST appropriate for SRS?

- 11% 1. mask immobilization
- 4% 2. CBCT image guidance
- 18% 3. contouring using PET-CT
- 21% 4. deformable registration
- 14% 5. planning on MRI

Which of the following is currently LEAST appropriate for SRS?

1. Answer: deformable registration.
2. Rigid registration is sufficient for the majority of SRS cases. Moreover, the uncertainty associated with deformable registration (as high as 7 mm) is too high to warrant use in SRS.

Refs: "The need for application-based adaptation of deformable image registration", *Medical Physics* 40 (2012), p. 1-9.

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