

## Communication of Uncertainties in Radiation Therapy

Ben Mijnheer



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## Disclosure

The Netherlands Cancer Institute – Antoni van Leeuwenhoek Hospital has a research cooperation with Elekta concerning the development of cone-beam CT and EPID dosimetry software



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## Communication of Uncertainties in Radiation Therapy

Learning objective: To describe methods of uncertainty communication and display

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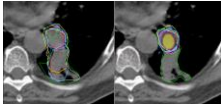
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### Communication of Uncertainties in Radiation Therapy

Learning objective: To describe methods of uncertainty communication and display

- in target volume delineation



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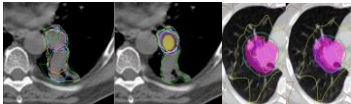
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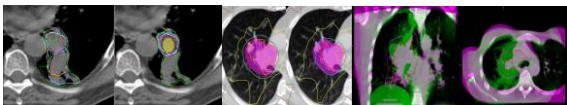
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Learning objective: To describe methods of uncertainty communication and display

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- in treatment delivery



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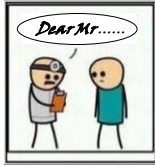
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### Communication of Uncertainties in Radiation Therapy



Radiation oncologist to physicist: What dose will this patient receive?

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### Communication of Uncertainties in Radiation Therapy



Radiation oncologist to physicist: What dose will this patient receive?

Physicist: 60 Gy with an uncertainty of  $\pm 3.5\%$

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### Communication of Uncertainties in Radiation Therapy



Radiation oncologist to physicist: What dose will this patient receive?  
Physicist: 60 Gy with an uncertainty of  $\pm 3.5\%$   
Radiation oncologist: I don't want any uncertainty, just 60 Gy to the target volume

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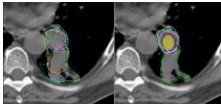
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### Communication of Uncertainties in Radiation Therapy

- in target volume delineation



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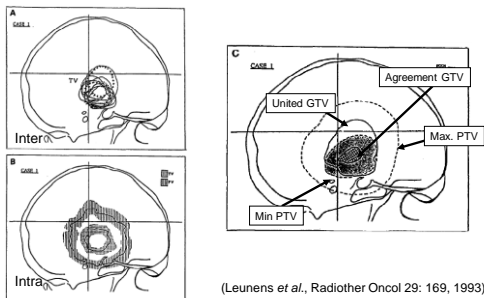
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### Intra- and inter-observer variability in contouring on CT



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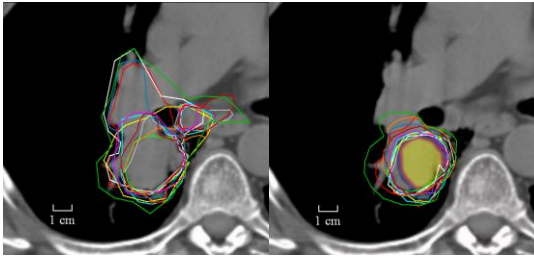
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Delineation variation: CT versus CT + PET



CT (T<sub>2</sub>N<sub>2</sub>)                      CT + PET (T<sub>2</sub>N<sub>1</sub>)  
SD 7.5 mm                      SD 3.5 mm  
(Steenbakkers *et al.*, IJROBP, 64, 435-448, 2006)

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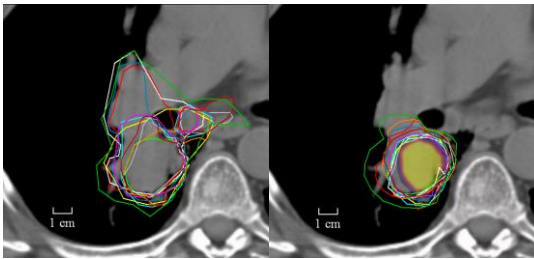
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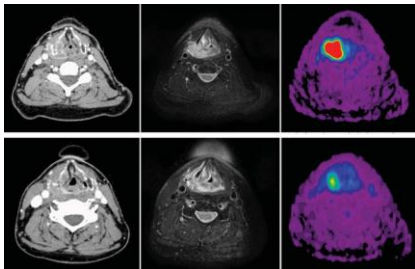
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Delineation variation: CT versus MRI and PET



Delineation of a GTV can vary according to the diagnostic modality (From ICRU Report 83)

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What can be done to reduce target delineation variation?



- A correct identification of the macroscopic extension of a tumour requires a long training of a radiation oncologist, and an awareness of the specific abilities of a given imaging method

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What can be done to reduce target delineation variation?



- A correct identification of the macroscopic extension of a tumour requires a long training of a radiation oncologist, and an awareness of the specific abilities of a given imaging method
- Image quality plays also an important role (slice thickness, patient motion during acquisition, equipment characteristics...)

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What can be done to reduce target delineation variation?



- A correct identification of the macroscopic extension of a tumour requires a long training of a radiation oncologist, and an awareness of the specific abilities of a given imaging method
- Image quality plays also an important role (slice thickness, patient motion during acquisition, equipment characteristics...)
- **Medical physicists and radiation oncologists should communicate about the possibilities and limitations of the various imaging tools available in their department**

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### Communication of Uncertainties in Radiation Therapy

- in target volume delineation
- in treatment planning



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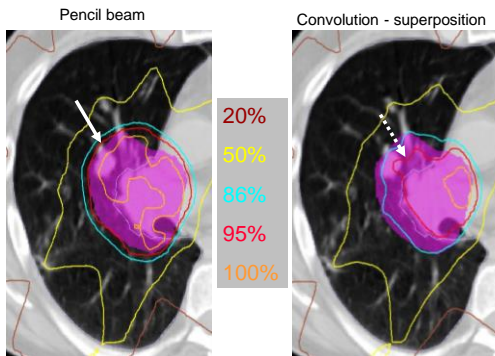
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### Comparison of isodose distributions



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### Clinical implementation of a more advanced dose calculation algorithm

- When introducing a more advanced (type b) dose calculation algorithm, e.g. convolution-superposition, instead of a (type a), e.g. pencil-beam algorithm, considerable lower dose in the PTV and a somewhat higher dose in most of the lung becomes visible for the same beam setup and number of MUs

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- Recalculate some old plans with the new algorithm for various approaches; e.g. coverage of the PTV by 95% (i.e. using larger field sizes) or by 90% at the lung side

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- Recalculate some old plans with the new algorithm for various approaches; e.g. coverage of the PTV by 95% (i.e. using larger field sizes) or by 90% at the lung side
- Optimize plans for the same constraints on PTV and/or OAR (lung) using the new approaches

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Discussion is needed between physicists and radiation oncologists to fully understand the differences and clinical consequences of the various approaches when introducing a more advanced dose calculation algorithm

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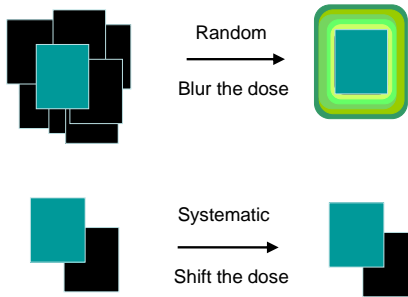
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Effect of type of geometric uncertainty on dose in the CTV




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CTV to PTV margin recipes

To cover 99% of the CTV with 90% of the specified dose:

$$\text{PTV margin} = 2.0 \Sigma + 0.7 \sigma \quad (\text{Stroom } et al., 1999)$$

To cover the CTV for 90% of the patients within the 95% isodose surface:

$$\text{PTV margin} = 2.5 \Sigma + 0.7 \sigma \quad (\text{van Herk } et al., 2000)$$

$\Sigma$  = SD of all **systematic uncertainties** combined quadratically

$\sigma$  = SD of all **random uncertainties** combined quadratically

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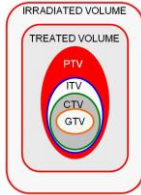
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### PTV margins

- CTV-PTV margin recipes are population based and do not cover the CTV in all patients



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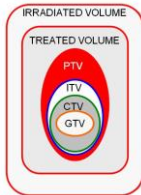
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### PTV margins

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- PTV margins are designed to cover geometrical uncertainties, but they should also cover microscopic disease



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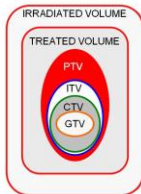
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### PTV margins

- CTV-PTV margin recipes are population based and do not cover the CTV in all patients
- PTV margins are designed to cover geometrical uncertainties, but they should also cover microscopic disease
- When using a GTV-CTV margin, there still is a finite chance that some patients of a population of "identical" patients have a microscopic extension outside this margin



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### PTV margins

- CTV-PTV margin recipes are population based and do not cover the CTV in all patients
- PTV margins are designed to cover geometrical uncertainties, but they do not cover microscopic extension
- When a time-dependent population is used, a microscopic extension outside this margin
- Reducing margins after introducing IGRT may therefore lead to poorer outcome and should be done with utmost care

Discuss margins with the whole team!




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### Probabilistic treatment planning

- The PTV is a surrogate for estimating the position of the CTV

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### Probabilistic treatment planning



- The PTV is a surrogate for estimating the position of the CTV
- Probabilistic treatment planning uses modeling of all geometric uncertainties in the position of the CTV and provides assessment of the most likely dose distribution, e.g. the 90% probability of a minimum dose in the CTV

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- A (Monte Carlo) mathematical model is often employed to simulate and evaluate many possible treatments

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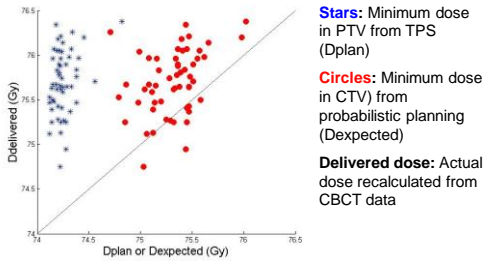
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### Results of probabilistic treatment planning of 56 prostate VMAT treatments



Probabilistic treatment planning leads to a better prediction of the delivered dose compared to conventional planning

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- A (Monte Carlo) mathematical model is often employed to simulate and evaluate many possible treatments
- Probabilistic treatment planning is still a research tool; commercial software is not (yet) available
- *Patient-specific* evaluation is performed, but based on *population-based*  $\Sigma$  and  $\sigma$  values




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### Another approach: worst case scenario

- Instead of using a population-based uncertainty calculation, every single case is evaluated separately

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- If the variation in the PTV/OAR position in the beginning of a specific patient treatment is known, design a worst case scenario to decide if the treatment can be continued

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- Example:
  - lung cancer treatment using 24x 2.75Gy on the lymph nodes and 3x18Gy on the tumor in the second week
  - measure the first week with CBCT the change in relative position of the tumor and the lymph nodes
  - generate a worst case plan

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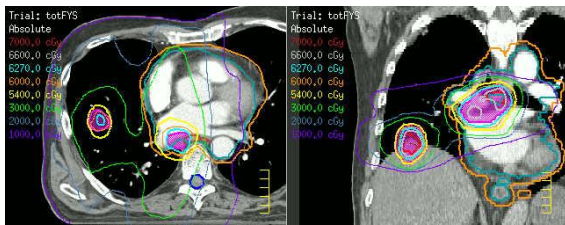
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### Hybrid plan of a lung cancer treatment 3x18Gy on tumor and 24x2.75Gy on lymph nodes



No shift

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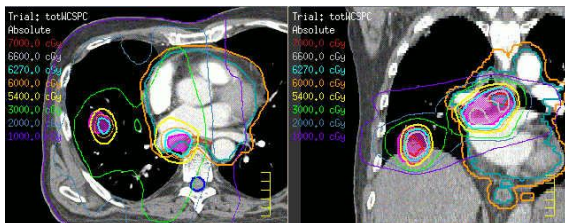
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### Hybrid plan of a lung cancer treatment 3x18Gy on tumor and 24x2.75Gy on lymph nodes



5 mm shift of tumor relative to lymph nodes

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- Example:
  - lung cancer treatment using 24x 2.75Gy on the lymph nodes and 3x18Gy on the tumor in the second week
  - measure the first week with CBCT the change in relative position of the tumor and the lymph nodes
  - generate a worst case plan
  - **the dosimetrist and/or physicist should discuss with the radiation oncologist if the dose in the OAR(s) is still acceptable**



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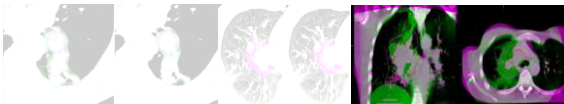
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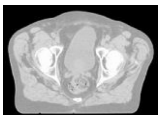
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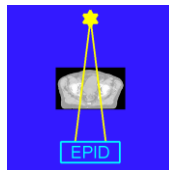
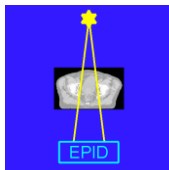
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### EPID-based *in vivo* 3D dose verification using a back-projection model

- 1) Calculate plan
- 2) Measure EPID dose
- 3) Reconstruct dose in multiple planes



Patient CT



- 4) Compare planned and reconstructed 3D dose distribution

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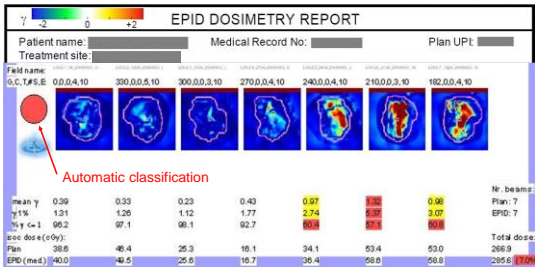
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### Lung step & shoot IMRT:



Fully automated dosimetry report generation showing results of 3D gamma evaluation and the dose at the isocenter

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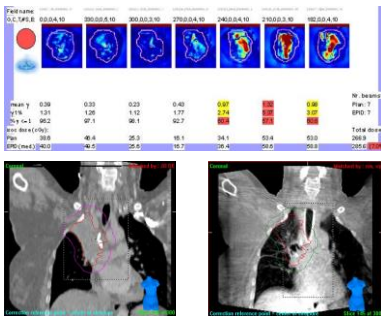
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### Lung step & shoot IMRT: recovery from atelectasis



Based on the in vivo dosimetry and CBCT result the physicist and radiation oncologist should discuss if replanning is necessary

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### Anatomical changes during a series of patient treatments: the traffic light protocol

- Uncertainties in dose delivery arise when anatomical changes, such as contour variation, tumor shrinkage or tumor growth, occur during the course of a treatment

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Anatomical changes during a series of patient treatments: the traffic light protocol

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- CBCT scans are often made to verify and correct patient setup

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- By using a "traffic light protocol" therapists contact radiation oncologists depending on the severity of change

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- The information available in a CBCT scan can also be used to observe and quantify changes in anatomy
- By using a "traffic light protocol" therapists contact radiation oncologists depending on the severity of change

	Action level 1	Action before next fraction	Communication by telephone
	Action level 2	No immediate action	Communication by email
	Action level 3	No action	Communication by email

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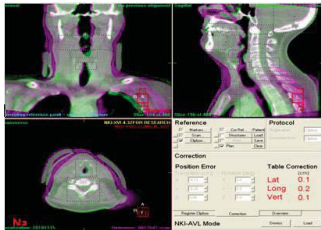
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### Anatomical changes during a series of patient treatments: the traffic light protocol

Purple: planning CT  
Green: CBCT



	Action level 1	Contour change > 1.5 cm
	Action level 2	Contour change 1.0 – 1.5 cm
	Action level 3	Contour change 0.5 – 1.0 cm

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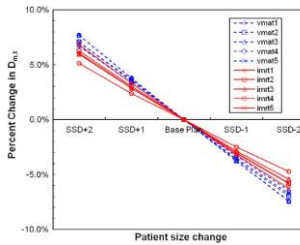
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### Dosimetric effects of weight loss or gain during IMRT and VMAT for prostate cancer



The target mean dose, decreased or increased by 2.9% per 1-cm SSD decrease or increase in IMRT and by 3.6% in VMAT.

(Pair *et al.*, Medical Dosimetry 38, 251–254, 2013)

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### Final remarks

- Reducing uncertainties in radiation therapy needs the expertise from radiation oncologists, physicists, dosimetrists and therapists



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### Final remarks

- Reducing uncertainties in radiation therapy needs the expertise from radiation oncologists, physicists, dosimetrists and therapists
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- Be pragmatic; the vast majority of our treatments are "correctly" delivered if a comprehensive QA program is performed



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### Final remarks

- Reducing uncertainties in radiation therapy needs the expertise from radiation oncologists, physicists, dosimetrists and therapists
- Talk to each other and discuss all (difficult) cases
- Be pragmatic: the vast majority of our treatments are "correctly" delivered if a comprehensive QA program is performed
- The challenge is to select those cases where knowledge of the uncertainty is of paramount importance for the optimal treatment of that particular patient



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Many thanks for your attention

and special thanks to

- Sanne Conijn
- Eugène Damen
- Tommy Knöös
- Angela Tjihuis
- Tomas Muller
- Marcel van Herk
- Marnix Witte



for borrowing some of their slides

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