



AAPM Meeting, Practical Medical Physics TU-G-201-0, July 14, 2015

Presentations

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4:30PM What Therapy Physicists Need to Know
About CT and PET/CT: Terminology and
Latest Developments
5:00PM An MRI Simulator from Proposal to
Operation
5:30PM PET/CT and MRI in Radiation Oncology:
Program Considerations
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What Therapy Physicists Need to Know About CT and PET/CT: Terminology and Latest Developments

Chia-ho Hua, PhD

Department of Radiation Oncology St. Jude Children's Research Hospital, Memphis TN

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CT Developments: Metal Artifact Reduction

- Estimating and subtracting the metal-only sinogram
- Improve anatomical visibility avoid subjective density overrides improve dose calculation accuracy improve proton range accuracy

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- Dual energy CT is another approach for reducing metal artifacts
- Siemens IMAR (Iterative Metal Artifact Reduction)
 Siemens MARIS (Metal Artifact reduction in Image Space)
 Philips O-MAR (Metal Artifact Reduction for Orthopedic Implants)
 GE MAR (Smart Metal Artifact Reduction)
 TOSHIBA SEMAR (Single Energy Metal Artifact Reduction)







CT Developments: Statistical Iterative Reconstruction

- New algorithms to reduce noises while preserving high contrast edges
- Improve 4DCT quality, GTV and OAR delineation, or reduce CT scan dose
- Previous non-model based

Siemens SAFIRE (Sinogram Affirmed Iterative Reconstruct Philips IDose4 GE ASIR (Adaptive Statistical Iterative Reconstruction) TOSHIBA AIDR (Adaptive Iterative Dose Reduction)

New model-based

Siemens ADMIRE (Advanced Modeled Iterative Reconstruction) Philips IMR (Iterative Model Reconstruction) GE MBIR (Model-based Iterative Reconstruction) TOSHIBA AIDR-3D (Adaptive Iterative Dose Reduction 3D)







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CT Developments: Ander Chieffith Dose Management Tools				
	Siemens	Philips	GE	Toshiba
Automatic Exposure Control Trade Name	CARE Dose 4D	DoseRight 3D- DOM	Smart mA	SURE Exposure 3D
Image Quality Reference Indicator	Quality reference mAs	Reference image	Noise index	Target image quality level
Available Features	Dose notification Dose alert DICOM dose report DoseLogs DoseMAP	Dose notification Dose alert DICOM dose report Locking protocols	Pre-scan dose estimates Dose check DICOM dose report	Dose notification Dose alert DICOM dose report
Dose notification: a message is triggered when a single planned scan is likely to exceed the pre-programmed CTDIver or DLP value Dose alert: a message is triggered when the cumulative dose at a location plus the dose for the next planned scan, is likely to exceed a pre-programmed value				

leads to a higher than usual dose index.



Important CT Terminology (A Partial List)

kV or kVp (tube potential, 120 KV typically the only one used for CT sim)

mA (tube current, modulation techniques to reduce patient scan dose)

mAs = mA × exposure rotation time per rotation effective mAs or mAs per slice = mAs/pitch (reflect the effect on absorbed dose when pitch is changed)

- pitch = table travel per gantry rotation/total nominal beam width
- collimation (affect thinnest available reconstructed slice, determined together with desired slice width, impact scan time and dose efficiency)

scout/topogram/surview/scanogram (projection radiograph for users to prescribe CT scan range) spatial resolution (typically specified as line pair/mm visible for high-contrast bar pattern)

Iow-contrast resolution (ability to discriminate between tissues with slightly different attenuation) AEC (automatic exposure control, scanner feature to adapt tube current to patient size to reduce dose) CTDIvol (CT dose index calculated by scanner, dose to 16 or 32 diameter PMMA phantom, independent of what patient is actually scanned)

DLP (dose length product, mGy-cm)= CTDIwi (mGy) x scan length (cm) (another dose metric, more direct bearing than CTDI on the overall radiation risk of CT scan)

beam hardening artifact (dark streaks near high attenuating objects or cupped appearance)

Good resources: AAPM website CT Lexicon McNitt-Gray presentation of key CT parameters at 3rd CT dose sur

CT Simulator: Technical Specification and Quotation

Technical specification and quotation are separate documents.

Key specifications of CT simulator include

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> gantry opening, rotation time, generator (power rating, kVp setting, mA range), Xray tube (focal spot sizes, heat capacity, cooling rate), CT detector (material, slices, z-axis coverage, material, slice thickness, scan FOV), image quality (spatial resolution, low contrast resolution, noise), reconstruction and display, table, and external localization laser

- Quotation lists items to purchase, part numbers, quantity, brief description for each item, rigging and installation, total price. Several revisions.
- Key quotation items of CT simulator include

CT scanner, selected slice configuration, power generator, image acquisition, 4D CT package, dose management tools, RTP table and tabletop, external lasers, cooling system, chiller, server, CT simulation and advanced applications (metal artifact reduction), iterative reconstruction package, old simulator trade-in, on-site and off-site training





PET-CT Developments: St. Jude Children's Research Hospital **Acquisition with Continuous Bed Motion**

Conventional PET acquisition is bedbased (stop and go, 1.5-3 min/bed position). Brain-only imaging acquired with a single bed position (5-10 mins).

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- 25-50% overlap between adjacent bed positions (scanner dependent) is needed to minimize the axial nonuniformity of the noise. This increases total acquisition time.
- Typical continuous acquisition 1-2 mm/sec (0.1-10 mm/sec)



 $\hfill \Box$ Allow physicians to scan the desired area without CT over-scanning in axial axis in step-and-go acquisition. Bed moving may give patients a sense of progress.



PET-CT Developments: St. Jude Children's Research Hospital **Ultra Low Dose CT for Attenuation** Correction

When CT is not used for diagnosis, anatomical localization, or treatment planning, CT tube current may be reduced but still sufficient for attenuation correction.

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- □ 5-10 mAs and < 1mSV effective dose with current scanners has been reported for children and selected adults
- Estimate attenuation maps of head based on PET data alone (Siemens Smart Neuro AC)
- MR-based PET attenuation correction (MRAC and UTE methods) in PET-MR





PET-CT Developments: St. Jude Children's Research Hospital **Time of Flight and Point Spread Function**

Time of Flight Imaging

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- Measure arrival time difference between two photons to determine the annihilation origin along the line of response with a smaller uncertainty.
- Improve structural detail (SNR) particularly in large patients
- Point Spread Function Modeling
- $\hfill\square$ PSF is the response of an imaging system to a point source.
- Modeling PSF in image reconstruction helps improve spatial resolution and correct partial volume effect.





Important PET Terminology (A Partial List)

transverse spatial resolution (FWHM of point spread function of a point source, typically specified at 1cm and 10cm from FOV center on the transverse plane) axial spatial resolution (same as above, resolution in the scanner axis direction) sensitivity (in cps/kBq/cc, measure of counting efficiency of a PET scanner, the number of coincidence events per unit time detected by the scanner for each unit of source activity) peak true count rate (in kcps, the maximum count rate, which occurs at a certain level of

activity, beyond which the system is paralyzed)

noise equivalent count rate (NECR in kcps, estimate of the number of true coincidences necessary in an ideal system to reach the SNR obtained in a real system with scatter and random coincidences, proportional to SNR² so good for scanner performance comparison) timing resolution (in picosecond, minimum time interval between two subsequent photon events in order for these to be detected as separate events)

energy resolution (the precision with which the PET system can measure the energy of incident photons)

scatter fraction (ratio of scatter counts to total counts)

OSEM (ordered subset expectation maximization, iterative algorithm for image reconstruction) time of flight (TOF, a technique to detect the difference in time between the detection of the two photons for better localizing the point of origin of the annihilation event)

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PET-CT: Technical Specification and Quotation

Key specifications of PET include

gantry opening, PET detector (crystal material and size, number of crystal, axial and transaxial FOV), Pet performance (transverse spatial resolution at 1 and 10 cm, axial low resolution at 1 and 10 cm, timing resolution, timeof-flight localization accuracy, system sensitivity, peak and clinical NECR, peak trues, scatter fraction, energy resolution)

Key quotation items of PET-CT include

PET-CT scanner, computer systems, RTP package for PET-CT simulator including flat table top and CT sim software, external lasers, cooling system, chiller, calibration sources and phantom, CT and PET respiratory gating package, respiratory trigger system, time-of-flight toolkit, CT dose management tools, CT iterative reconstruction, image fusion package, image transfer and storage, server, UPS, contrast injector, on-site and offsite training

Image: Summary Image:



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