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Resolving and characterizing breathing motion for radiotherapy with MRI

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Disclosures and Apologies

- No conflicts of interest
- Not an MRI scientist
- Only have 20 minutes

Many investigators' relevant/current methods will not be mentioned





Outline

- I. Introduction
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 - b) Pitfalls
 - c) 2D vs. 3D sequences
- II. (Breathing) motion characterization offline
 - a) Single-slice cine 2D MRI
 - b) Orthogonal-slice cine 2D MRI
 - i. Sequential
 - ii. Interleaved
 - c) Multi-slice cine 2D MRI to derive "4D-MRI"
 - i. Retrospective binning
 - ii. Un-binned for MIP generation
- III. Motion monitoring online
 - a) MRI-guided ⁶⁰Co unit
 - b) MRI-guided linac



Ia. Introduction: motivations for applying MRI to the motion problem

- MRI Offers the capability for 4D anatomical imaging, similar to 4D-CT
 - 4D-CT represents a snap-shot in time not ideal
- MRI is non-ionizing \rightarrow longer scans to characterize motion variability
- Sufficiently fast to minimize intra-scan motion
- Can scan in any orientation
- Flexibility in terms of achievable tissue contrast
 - Possibility to better visualize compared to CT for many disease sites (e.g., abdomen).
- Capability of 4D tumor tracking useful for both online and offline applications:
 - Online:

• Gated or motion-tracked therapies with reduction in treatment margins

- Offline:
 - Validation studies of different management techniques (gating, breathholding, tracking...)
 - Robust, patient specific margin determination

Ib. Introduction: pitfalls of applying MRI to the motion problem

- Not widely available; cost-prohibitive?
- Flexibility in MRI technology has led to lack of a defined 4D-MRI standard
 - Development/adoption largely limited to academic centers with resources
 - No current support for 4D-MRI in treatment planning systems
- Geometric image distortion
- Spatial resolution is more limited than CT (SNR tradeoffs)
- "4D-MRI planning simulations" take longer than 4D-CT planning simulations
- Other practical issues
 - Body/surface/flex coils complicate the procedure/setup
 - Claustrophobia is more likely than with CT
 - Not all patients are MRI-safe

Early adopters must continue to address these issues while demonstrating dosimetric/safety/clinical benefit to patients



Ic. 2D vs. 3D sequences – primer

- Excitation of tissue slab (thickness dictated by slice profile) via slice selection gradient
- Duration per slice = TR × NPy × Nex

NPy = number of phase encoding steps, hence number of rows Nex = number of (slab) excitations (or TR repetitions)

- Reconstruction via 2D Fourier transform
- (... Repeat over multiple slice locations to provide 3D image)
- Excitation slab = 3D volume at each (TR) repetition
- 3D spatial encoding via addition of phase encoding in another (3rd) dimension
- Duration per volume = TR × NPy × NPz × Nex NPz = Number of phase encoding steps in the z-axis
- Reconstruction via 3D Fourier transform
 - 3D sequences provide better signal (SNR) for given resolution.
 → Multi-planar viewing has higher fidelity with 3D
- <u>2D vs. 3D</u>:
 3D volume takes longer to encode -- therefore 3D is subject to more intrascan motion

 \rightarrow Methods exist to speed up 3D acquisition such as partial k-space filling

• 2D sequences more practical "out of the box" given acquisition speed



3D:

[Hoa D., Spatial encoding in MRI. https://www.imaios.com/en/e-Courses/e-MRI/Signal-spatial-encoding/3D-spatial-encoding]

IIa&b. Offline motion tracking with 2D cine MRI

Single-slice-plane acquisition

 Lung: Koch et al. [IJROBP 2004; 60 (5): 1459]
 Lung: Cai et al. [PMB 2007; 52: 365] [IJROBP 2007; 60(3): 895]
 Lung: Shi et al. [Med. Phys. 2014; 41 (3). 52304]

Orthogonal-slice-plane acquisition:

Sequential (sagittal-sagittal...; coronal-coronal...)

- 1. Liver: Shimizu et al. [IJROBP 2000; 48 (2); 471 (sagittal/coronal)
- 2. Liver: Kirilova et al. [IJROBP 2008; 71 (4): 1189] (sagittal/coronal/axial)
- 3. Liver: Akino et al. [Med. Phys. 2014; 41(11): 111704] (sagittal/coronal)
- 4. Pancreas: Feng et al. [IJROBP 2009; 74 (3): 884] (sagittal/coronal)

Interleaved (sagittal-coronal-sagittal-coronal...)

- 1. Lung/Abdomen: Tryggestad et al. [Med. Phys. 2013; 40 (9): 091712]
- 2. Kidney: Bjerre et al. [Phys. Med. Biol. 2013; 58 (14): 4943]



IIa&b. Offline motion: tracking with 2D cine MRI

• 2D cine MRI example (bSSFP on Siemens 1.5T Espree)



Interleaved orthogonal-slice cine acquisition:

- ~4 frames/second
- 2x2 mm² pixels in plane
- 5 mm slice profile



IIa&b. Offline motion: Template matching with orthogonal slice planes

 Cross-correlation-based template matching

Tryggestad et al. [Med. Phys. 2013; 40 (9): 091712]

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Imaging time

13 min.

12 min.

9 min.

IIb&c. What is a "cross-correlation" in image processing?



<pixel-wise (*i*,*j*) comparison>





Normalized cross-correlation:

 $\operatorname{ncc}_{k,N} = \sum_{i,j} (\mathbf{I}_k \cdot \mathbf{I}_N) / \sqrt{\{\sum_{i,j} (\mathbf{I}_k \cdot \mathbf{I}_k) \times \sum_{i,j} (\mathbf{I}_N \cdot \mathbf{I}_N)\}}$



IIa&b. Offline motion: Template matching with orthogonal slice planes

• Results for volunteer "S3"







Tryggestad et al. [Med. Phys. 2013; 40 (9): 091712]

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IIa&b. Offline motion: Template matching with orthogonal slice planes

- Results from a numerical simulation:
 - 3 cm spherical lesion

MAYO CLINIC • ITV₁ was determined during first 60 seconds of tracking



Tryggestad et al. [Med. Phys. 2013; 40 (9): 091712]



Respiratory bellows system [Picture: GE]

Example: PMU (Physiological Monitoring Unit, Siemens)



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Time (seconds)



Diaphragmatic monitoring with edge detection filter



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<u>USE CAUTION</u> when employing bellows-type systems



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@start of acquisition

@end of acquisition



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External markers (belts/tubes around patient)



Koch et al. [IJROBP 2004; 60 (5): 1459]





R. Farah and J. Lee [JHU / WIP]

External markers providing 3D information from single-plane tracking







Thresholded/segmented "Body Area"



Cai *et al.* [Med. Phys. 2011; 38 (12): 6384]

R. Farah and J. Lee [WIP / JHU] "4D-MRI reconstruction using groupwise registration." AAPM 2015. Snap oral: SU-F-303-1







IIa&b. Offline motion tracking with 2D cine MRI

Opportunities for simultaneous monitoring of motion surrogates

• Pencil Beam Navigators:

[Ehman and Felmlee, Radiology 1989; 173: 255] [Pauly, Nishimura and Makovski, JMRI 1989; 81: 43-56]

- Excitation of a column of tissue and generation of a corresponding 1D image, i.e., spatial intensity profile
- Can be inserted into sequence progression, e.g., in between 2D frames (or in between phase encoding steps)
- Oriented arbitrarily relative to the 2D/3D imaging orientation
- Commonly used in commercial sequences to trigger acquisition during a portion of breathing (amplitude-based)

• Can produce banding artifacts if overlapping with 2D/3D image region







[Nehrke and Manke, IJBEM 2000; 2(2)]

IIc. Offline motion: Retrospective binning of multi-slice cine 2D MRI to derive "4D-MRI"

• 2D cine MRI example (bSSFP on Siemens 1.5T Espree)



"Sequential" multi-slice:

- ~5 frames/second
- 2x2 mm² pixels in plane
- 5 mm slice profile



IIc. Offline motion: Binning of multi-slice 2D MRI to derive "4D-MRI"

Two general constructs:

Virtual cine 3D (over duration of exam):

1. von Siebenthal et al. [PMB 2007; 52 (6): 1547]

Representative single-cycle cine 3D (analog to 4D-CT):

- 1. Cai et al. [Med. Phys. 2011; 38 (12): 6384]
- 2. Tryggestad E. et al. [Med. Phys. 2013; 40 (5): 051909]

3. Farah and Lee et. al. [WIP JHU]

"4D-MRI reconstruction using group-wise registration." AAPM 2015. Snap oral: SU-F-303-1

- 4. Liu Y. et al. [Med. Phys. 2015; 42 (2): 534] *k-space binning*
- 5. Phantom and Liver: Tokuda et al. [Mag. Res. Med. 2008; 59 (5): 1051] navigator echoes to determine respiratory state and trigger acquisition
- 6. Hu et al. [IJROBP 2013; 86 (1): 198]

bellows to determine respiratory state and trigger acquisition

IIc. Offline motion: Retrospective binning of multi-slice 2D MRI to derive virtual 3D cine MRI
•Multi-slice abdominal 2D cine study in volunteers
•Demonstrated principle of "navigator slice"-based retrospective sorting

[von Siebenthal et al. PMB 2007; 52 (6): 1547]



•1.5 T (Philips Achieva)
•Custom bSSFP sequence
•Pixel size: 1.8² mm²
•Slice profile (~thickness): 3-4 mm

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•Acq. speed: 5.3-5.6 frames/sec.

➔ Effective acq. speed: 2.6-2.8 frames/sec.

Sequential sagittal slice acquisitionContinuous acquisition over tens of minutes

IIc. Offline motion: Retrospective binning of multi-slice 2D MRI to derive virtual 3D cine MRI

• Each <u>pair</u> of consecutive or "embracing" navigator frames defines a liver "state" for sorting from which an <u>entire</u> 3D volume can be reconstructed.



$$c(i, j) = \sum_{r=1}^{P} \left\| \begin{pmatrix} x_{j-1}^{r} - x_{i-1}^{r} \\ y_{j-1}^{r} - y_{i-1}^{r} \end{pmatrix} + \begin{pmatrix} x_{j+1}^{r} - x_{i+1}^{r} \\ y_{j+1}^{r} - y_{i+1}^{r} \end{pmatrix} \right\|$$
$$= \sum_{r=1}^{P} \left\| \Delta \vec{X}_{-1}^{r} + \Delta \vec{X}_{+1}^{r} \right\|.$$

Cost function:

combines template-matching-derived shifts from multiple ROIs within the 2D navigator



- IIc. Offline motion: Retrospective binning of multi-slice cine 2D MRI to representative "4D-MRI"
- First pass reconstruction based on bellows all frames/bin were averaged
- Normalized cross-correlation based scoring to determine best matching frames for 2nd pass reconstruction:



•Clear indication of best matching phase (despite poor SNR in raw image in this case)



Tryggestad E. et al. [Med. Phys. 2013; 40 (5): 051909]

IIc. Offline motion: Retrospective binning of multi-slice cine 2D MRI to representative "4D-MRI"



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Tryggestad E. et al. [Med. Phys. 2013; 40 (5): 051909]

IIc. Offline motion:

Retrospective binning of multi-slice cine 2D MRI to representative "4D-MRI"

• k-space binning with T2-weighted sequence



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Liu Y. et al. [Med. Phys. 2015; 42 (2): 534]

IIc. Offline motion: Retrospective binning of multi-slice cine 2D MRI to representative "4D-MRI"

 For retrospective binning with un-triggered cine 2D multi-slice acquisition, how do we know how many repetitions over set of slices to fill all 4D bins per slice location?



%-completeness of k-space filling (over all slices/bins)



Number of repetitions required for 95% completeness



Liu Y. et al. [Med. Phys. 2015; 42 (2): 534]

IIc. Offline motion:3D MIP generation using multi-slice cine 2D MRI

- Potentially very practical, low-tech solution for ITV delineation
- Previously demonstrated by Adamson et al. [Med. Phys. 2010; 37 (11): 5914]



In-house example using GE 750w 3T





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3D LAVA Flex breath-hold at end expiration

MIP from Sagittal FIESTA Multiphase 8 slices; 30 dynamics/repetitions

III. Motion online: Example ViewRay "MRIdian" system

Mutic and Dempsey [Semin. Radiat. Oncol. 2014; 24(3): 196]





[http://www.viewray.com/system]

- Three-head ⁶⁰Cobalt teletherapy unit delivering IMRT
- On-board 0.35T MRI
- Cine 2D MRI and DIR-based real-time tracking for beam gating:
 - Single sagittal plane at 4 frames/second
 - Three sagittal planes at 2 frames/second



III. Motion online: Example from hybrid linac-MRI

Cross Cancer Institute, Edmonton, Canada

[http://medicalphysicsweb.org/cws/article/research/50521]



[http://www.mp.med.ualberta.ca/linac-mr/index.html]



Yun et al. [Med. Phys. 2013; 40 (5): 051718]



Demonstration of MLC-tracked delivery to 1D motion phantom:

- 0.2 Tesla B0 Field
- Varian 52-leaf MK-II MLC
- Cine 2D (single-slice) bSSFP sequence
- Predictive tracking algorithm

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Conclusion:

We are at the dawn of a new era in clinical implementation of MRI-based motion characterization and management!