#### Treatment Simulation, Planning and Delivery for **Stereotactic Body Radiation Therapy**



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# **Outline**

Immobilization and Simulation **Treatment Planning Target Localization & Plan Delivery** Summary

#### Immobilization

- Accurately re-position patient
   Reduce/Minimize patient voluntary and involuntary motion >Reduce/Minimize organ/target motion
- ---Abdominal compression
- Comfortable for long treatment
   Compatible with IGRT
- Not interfere with treatment beam
- Consider machine safety zones







#### **Target Motion Reduction**



Lung tumor motion under varying levels of abdominal compression (pressure plate) Heinzerling et al, UROBP 2008

#### Limitations

 Patient discomfort
 Variable daily distortion in abdominal anatomy



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#### Imaging

- Multimodality of high resolution(*1-2mm slice thickness*) images (CT/MRI, PET/CT)
- 4DCT/PET to evaluate internal motion



#### **Challenges for SBRT**

How to accurately define target? --- 4D imaging

How to accurately localize target?

How to obtain conformal dose and steep dose gradients? ---3DCRT, Inverse Planning, IMRT, VMAT...

How to minimize dose to surrounding critical organs? --- Gating, Tracking...













#### **Motion Analysis**

- Analyze target motion in different phase
- Consistence of motion of fiducial markers with target
- Analyze target size and shape change
- Determine residual error and target margin for gating treatment

PTV : ITV +3~5mm margin



Liver example



Pancreas example

Loo et al. LIR

#### Motion Management (Delivery)



#### **3DCRT or IMRT/VMAT?**

- Advantages:
  - Better dose conformality
  - Easy to control/constrain dose to OARs
  - Inverse planning
- Disadvantages:
  - Higher MU, longer treatment time
  - Interplay effect between target and MLC motion







#### **Coplanar or Non-Coplanar Beams?**

#### Advantages:

- Better dose gradients in axial planes
- Disadvantages:
  - Complicated treatment
  - Longer treatment time
  - Potential collision

8-12 non-overlapped beams (1-2 partial arcs) on the disease side can generate acceptable dose performances for most lung SBRT cases.





#### **Dose Calculation**

- Inhomogeneity correction algorithms
- PBC is not appropriate for lung SBRT
  - AcurosXB, convolution/superposition, MC should be used
- Dose calculation grid <= 2mm
- Couch top should be inserted





Irradiating through the Couch Top (from straight below) is equivalent to 12 mm of water. Data for Brainlab Exactrac 6D couch top





TomoTherapy CSA S. E. Davidson et al. M

**Inhomogeneity Correction** 



Dose difference for targets from PBC and AcurosXB could be more than 10%

- -----

PBC should not be used for lung SBRT



### **Target Localization & Plan Delivery**



|                 | Image-gui                                 | ded Ta                                  | arge              | t Localization  |  |
|-----------------|---|---|-------------------|---|--|
| After Treatment | er en | 8 1 1 1 1 1 1 1 1 1 1 1 1 1 1 1 1 1 1 1 | Se<br>Se          | Precion   |  |
|                 | A   | TABLE IV: Achieval                      | le accuracies rep | orted in the literature categorized by body site and immobil                                    | Ization/repositioning device.  |
|                 | Accuracy                                  | Autor, year                             | 346               | Wood frame/domestactic coordinates  | Reported accuracy  |
| Spine           | 1~3 mm                                    | Las, 1994                               | Abdomes           | on box to skin marks  | 3.7 mm Lat, 5.7 mm Long  |
| Lung            | -Emm                                      | Hatalion, 1992                          | open              | Francless/implaned fiducial markets with real-time  | 2 88   |
| Lung            | <0000                                     | Murphy, 1997 <sup>4</sup>               | Spine             | imaging and tracking  | 1.6 mm radial  |
| Abdomen         | <5mm                                      | Long, 1999"<br>Yenice, 2005"            | Spine             | Body cast with stereotacta: coordinates<br>Contours absorbactic frame, and in-more CT raidance. | 53.6 mm mean vector<br>1.5 mm restern accuracy, 2-3 mm positionian accuracy      |
| 7.600011011     | Somm                                      |   |                   | MITH BodyFix with storeotactic frameTisacCT on rails  |  |
|                 |   | Chang, 2004                             | Spine             | with 6D robotic coach   | 1 mm system accuracy   |
|                 |   | Tokunye, 1997<br>Nakasiwa, 2000         | Doneic            | Prone position jaw and arm straps<br>MVCT on line:  | 3 mm<br>Nor prosted  |
| Lung Ref        | CT: Ave-IP 50% CT                         | Wulf, 2000 <sup>8</sup>                 | Lang, liver       | Eleka <sup>na</sup> body frame  | 3.3mm lat,4.4 mm long  |
| Lang non        |   |   |                   |   | Bony anatomy translation 0.4, 0.1, 1.6 mm (mean                                  |
| EBH-CT          |   | Fass. 2004                              | Lane, liver       | MITH BodyFix  | X,Y,Z); tumor translation before image guidance 2.9,<br>2.5, 3.2 mm (mean X,Y,Z) |
|                 |   | Herfarth, 2001                          | Liver             | Leibinger body frame  | 1.8-4.4 nm   |
| Live/Panci      | eas/Prostate:                             | Nagata, 2002 <sup>4</sup>               | Long              | Elekta <sup>the</sup> body frame  | 2 mm   |
|                 |   | Fukumoto, 2002                          | Long              | Elekta <sup>rse</sup> body frame  | Not reported   |
| Fiducials       |   | Hara, 2002*                             | Long              | confirmatory scan   | 2 mm   |
|                 |   | Hof, 2003*                              | Long              | Leibinger body frame  | 1.8-4 mm   |
|                 |   | Timmerman, 2003 <sup>e</sup>            | Long              | Elekta <sup>tor</sup> body frame  | Approx. 5 mm   |
|                 | AAPM Task Group NO. 101                   | Ware Soul                               | Lana              | configure (0) transmission  | 03111 pp 48 -11132 pp 14 15137 pp 51   |



#### Target Positioning: Lung

| Table 4<br>Intrafractio | n, interfraction, c | orrection resid | luals, and t | arget marj  | gins by ir | nmobilization                  | device                      | ,   |     |                             |     |     | 100 In<br>90 - In      | trafraction Variation             |
|-------------------------|---------------------|-----------------|--------------|-------------|------------|--------------------------------|-----------------------------|-----|-----|-----------------------------|-----|-----|------------------------|-----------------------------------|
|                         | Interfraction       | Correction      |              |             |            | Final<br>position<br>variation | 2-parameter<br>margins (mm) |     |     | 4-parameter<br>margins (mm) |     |     | of Patients<br>0 20 30 | +                                 |
| Туре                    | vector (mm)         | (mm)            | (mm)         | 2 mm        | 5 mm       | (mm)                           | ML                          | AP  | cc  | ML                          | AP  | сс  | antage                 |                                   |
| a-cradio                | 8.3 ± 5.0           | 2.2 ± 1.3       | 3.0 ±<br>1.7 | 71.6%       | 10.0%      | 2.9 ± 1.6                      | 4.2                         | 5.7 | 5.0 | 3.7                         | 5.8 | 4.6 | 20 20                  |                                   |
| Body<br>frame           | $6.9\pm5.2$         | 2.3 ± 1.6       | 2.3 ±<br>1.4 | 49.0%       | 3.9%       | 2.2 ± 1.2                      | 2.9                         | 4.1 | 4.1 | 2.3                         | 4.0 | 3.7 | 0 0.5<br>Intr          | 1 1.5<br>afraction Variation (cm) |
| BodyFIX                 | 10.7 ± 8.7          | 2.4±2.4         | 3.0 ±<br>2.5 | 60.3%       | 15.1%      | 3.2±2.6                        | 5.4                         | 7.2 | 6.3 | 5.0                         | 7.3 | 6.1 |                        |                                   |
| None                    | 7.8 ± 4.1           | 2.6 ± 1.7       | 3.3 ±<br>2.2 | 66.7%       | 19.2%      | 3.3 ± 2.2                      | 4.4                         | 6.5 | 6.9 | 3.9                         | 6.7 | 6.5 | Intra-fractio          | on variation (m                   |
| Hybrid                  | 12.6 ± 10.2         | 1.8 ± 0.9       | 2.7 ±<br>1.6 | 64.5%       | 8.4%       | 2.7 ± 1.5                      | 3.6                         | 5.1 | 5.1 | 3.1                         | 4.6 | 4.2 | AP                     | 0.0±1.7                           |
| Wing<br>board           | 7.4 ± 4.1           | 2.5 ± 1.2       | 3.3 ±<br>1.7 | 72.7%       | 15.9%      | 3.2 ± 1.6                      | 4.5                         | 5.7 | 6.2 | 4.2                         | 5.1 | 5.8 | SI                     | 0.6±2.2<br>-1.0±2.0               |
| AP, antero              | posterior; CC, cr   | aniocaudal; IF  | ∨, intrafrac | tion variat | ion; ML,   | mediolateral.                  |                             |     |     |                             |     |     | 3D                     | 3.1±2.0                           |

A total of 409 patients with 427 tumors underwent 1593 fractions of lung SBRT

Shah C et al PRI

# Fluoroscopy Verification







# Beam-Level Imaging: Verification of Geometric Accuracy

Intra-fraction Verification of SABR

- 20 SABR patients (lung/liver/pancreas) RPM-based gating treatment
- Geometric error: 0.8 mm on average; 2.1 mm at 95th percentile



#### Beam-Level kV Volumetric Imaging



- Continuous fluoroscopy during dose delivery In-house program for CBCT reconstruction
  20 lung SABR patients
  Treatment verification
  Routine clinical use
- - - Li R, Xing L et al, IJROBP. 2013

# **Beam-Level MV Volumetric Imaging**



#### Summary

- 4D imaging is required for accurate motion management
- New techniques (Inverse planning, IMRT/VMAT, Gating/Tracking,...) can improve target conformity and critical structure sparing
- Patients should be positioned with IGRT
- Beam-level imaging is a necessary step to insure accurate SBRT delivery •

# **Question:** Which following algorithm should NOT be used for a lung SBRT dose calculation?

| 20% | 1. | Convolution/superposition |
|-----|----|---------------------------|
| 20% | 2. | Pencil Beam Convolution   |
| 20% | 3. | AcurosXB                  |
| 20% | 4. | Monte Carlo               |
| 20% | 5. | None of above             |
|     |    |                           |
|     |    |                           |

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### Discussion

# **Correction Answer:**

2. Pencil Beam Convolution

**Reference:** 

S. E. Davidson, R. A. Popple, G. S. Ibbott, and D. S. Followill, "Technical note: Heterogeneity dose calculation accuracy in IMRT: Study of five commercial treatment planning systems using an anthropomorphic thorax phantom", Med. Phys. 35, 5434–5439 2008.

Question: What localization accuracy can be achieved in CBCT-guided spine SBRT?

| 20% | 1. <1mm   |
|-----|-----------|
| 20% | 2. 1~3 mm |
| 20% | 3. 3~4 mm |
| 20% | 4. 4~5 mm |
| 20% | 5. >5mm   |

# Discussion

# **Correction Answer:**

2. 1~3mm

## **Reference:**

P. C. Gerszten et al, "Prospective evaluation of a dedicated spine radiosurgery program using the Elekta Synergy S system", J Neurosurg. 113:236–241, 2010

#### 1.1 ±0.7mm

E. L. Chang et al, "Phase I clinical evaluation of near-simultaneous computed tomographic image-guided stereotactic body radiotherapy for spinal metastases", Int. J. Radiat. Oncol., Biol., Phys. 59, 1288–1294 2004.

<1mm in AP, Lat, and SI direction

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