


Advanced MR in Clinic

Diffusion MRI

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Learning Objectives

- To understand commonly-used diffusion MRI pulse sequences in clinic;
- To understand the common diffusion models in diffusion MRI analysis;
- To be able to implement diffusion imaging protocols and conduct quality assurance.

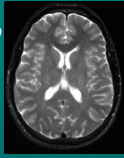
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Outline

- 1. Diffusion MRI signals
- 2. Diffusion models and protocols
- 3. Examples of clinical applications
- 4. Quality assurance

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Diffusion-Weighted Imaging



S_0

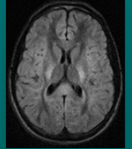
T2-weighted

diffusion gradient



$S = S_0 \exp(-bD)$

b: b-factor
D: diffusion coefficient



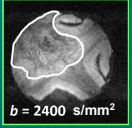
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Diffusion-weighted (DW) image

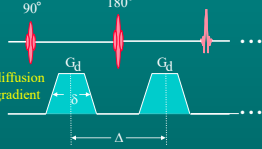
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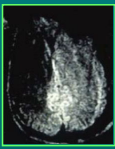
Diffusion Gradient in a Spin Echo Sequence

- Stejskal and Tanner gradient



$b = 2400 \text{ s/mm}^2$





• b-value

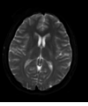
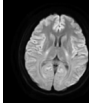
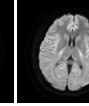
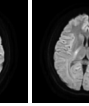
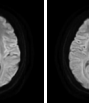
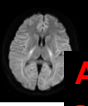
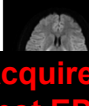
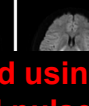
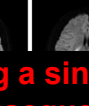
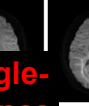
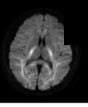
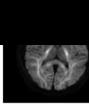
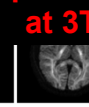
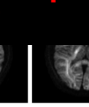
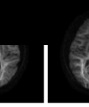
$$b \approx \gamma^2 G_d^2 \delta^2 (\Delta - \delta / 3)$$

$$S = S_0 e^{-bD}$$

The sequence is extremely sensitive to motion.

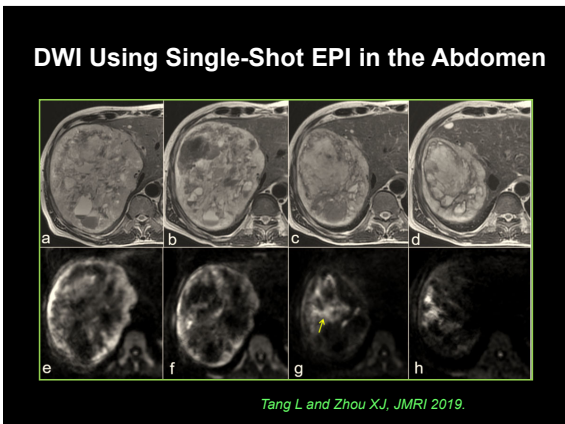
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DWI of the Human Brain Zhou X.J. et al., MRM 2010; 63:562-569.

Acquired using a single-shot EPI pulse sequence at 3T

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Single-Shot EPI for Diffusion Imaging

- Pros**
 - Motion insensitive
 - Low SAR
 - Time efficient
- Cons**
 - Image distortion (sensitivity to off-resonance)
 - Low spatial resolution
 - Sensitivity to eddy currents

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Multi-shot EPI diffusion

- Higher resolution (e.g., 256²)
- Less distortion
- Reduced sensitivity to eddy currents
- Less ghosting
- Slower
- Motion correction is needed (MUSE, RESOLVE, etc.)
- Residual motion artifacts

ADC maps

$b = 0, 800 \text{ s/mm}^2; \sim 5 \text{ min}$
van Pul et al., MRI 22: 1169-1180, 2004

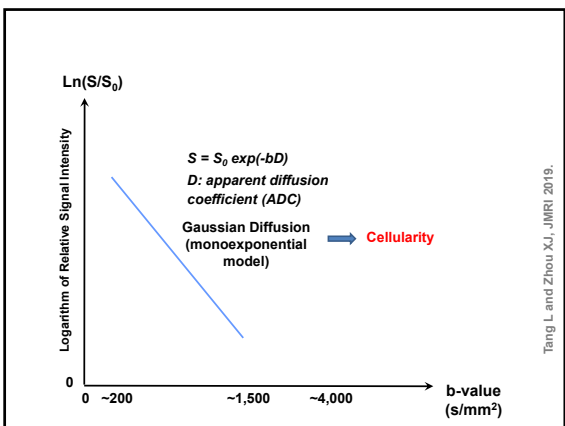
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PROPELLER/BLADE/Multi-VANE Diffusion

- Very robust against motion
- Distortion free
- Relatively slow

$b = 1000 \text{ s/mm}^2$
128x128
~1 min/image
Pipe et al., MRM 47: 42-52, 2002

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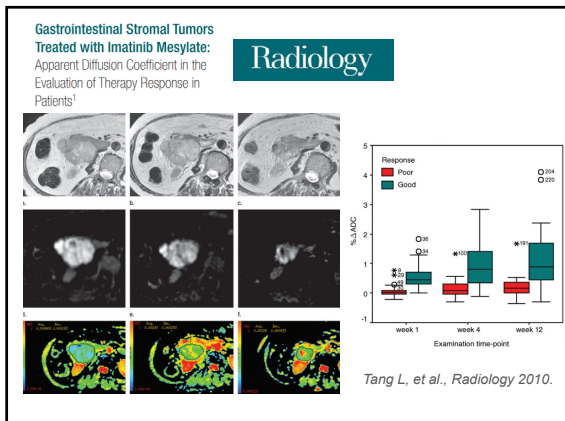
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ADC vs. Cellularity

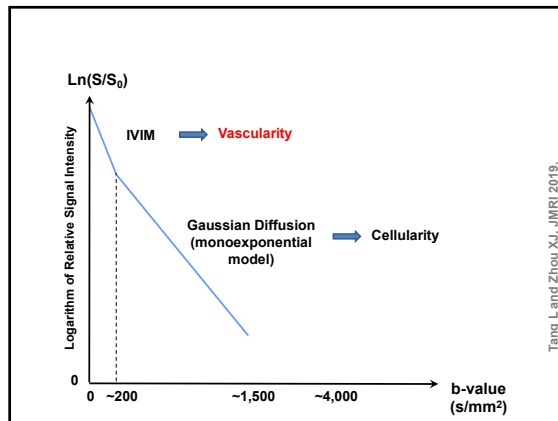
Clinical Demonstration on Patients

Average $r = -0.61$

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IVIM Diffusion Imaging

$$S / S_0 = f \exp(-bD^*) + (1 - f) \exp(-bD)$$

Perfusion fraction (f);
pseudo-diffusion coefficient (D*);
diffusion coefficient (D).

- "Note that $D \ll D^*$
- D^* mimics perfusion, but is not perfusion.
- 3-8 b-values are typically used.

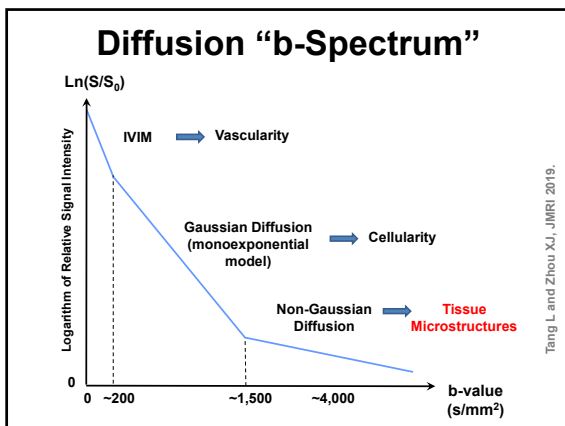
lima and Le Bihan, Radiology 2016.

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IVIM: Differentiation between Malignant and Benign Mediastinal Lymph Nodes (MLN)

Qi L, et al. Euro Radiol 2018; 28: 1301-1309

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Diffusion Models

Gaussian

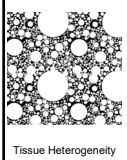
- Mono-exponential
- ADC
- DTI
- FA, MD, RD, AD, eigen-vectors, etc.

Non-Gaussian

- Compartmentalized models
- IVIM, NODDI, AxCaliber, Charmed, RSI, VERDICT, etc.
- Non-compartmentalized models
- DSI, q-Ball, QTI, DKI, stretch exponential, fractal, CTRW, FROC, FM, etc.

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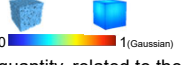
Fractional Order Calculus (FROC) Model



Tissue Heterogeneity

$$M_{xy} = M_0 \exp \left[-D \mu^{2(\beta-1)} (\gamma G_z \delta)^{2\beta} \left(\Delta - \frac{2\beta-1}{2\beta+1} \delta \right) \right]$$

D : Diffusion coefficient, similar to ADC
 β : Degree of intravoxel tissue heterogeneity



μ : Spatial quantity, related to the diffusion mean free length

Magin, et al., JMR, 2008; Zhou, et al., MRM, 2010; Sui, et al., Radiology, 2015.

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Example of Grading Pediatric Brain Tumors

	Low-grade			High-grade		
	Ependymoma	PA	PA	Medullo-blastoma	Medullo-blastoma	AT/RT
D						
β						
μ						
T2						

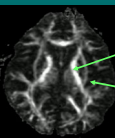
Y. Sui, et al., Radiology, 2015.

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Diffusion Tensor Imaging

- Applying the diffusion gradient in ≥ 6 directions
- Analyzing the signals using a diffusion tensor
- Fractional anisotropy (FA)
- Mean diffusivity (MD)
- Principal eigen-vector \rightarrow tractography


$$\begin{bmatrix} D_{xx} & D_{xy} & D_{xz} \\ D_{xy} & D_{yy} & D_{yz} \\ D_{xz} & D_{yz} & D_{zz} \end{bmatrix}$$



High FA

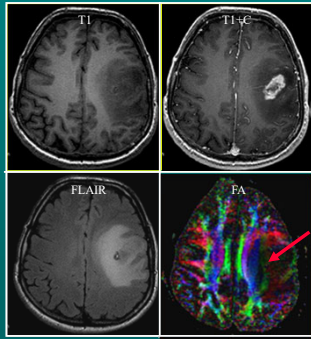


Low FA



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DTI for Pre-Surgical Planning



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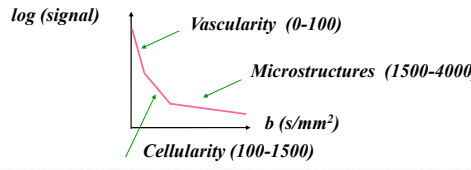
Quality Assurance for DWI

- Image distortion**
 - Use a spherical phantom
 - Check the distortion wrt the image with $b=0$
 - Eddy currents (time constants ~ 50 -100 ms)
- EPI-related image quality**
 - Ghosting level ($< 3\%$)
 - SNR
- ADC accuracy**
 - Use a standard water phantom at a fixed temperature
 - Check ADC value of the water phantom quarterly

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Conclusions

- DWI is typically acquired using a single-shot EPI pulse sequence, but other sequences are emerging.
- b-Value determines the degree of diffusion weighting, and probes the different tissue structural information.
- ADC is the most prevalent parameter used clinically.



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